

(12) **United States Patent**
Donner et al.

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(45) **Date of Patent:** **Mar. 24, 2020**

(54) **SPINOPELVIC FIXATION TECHNOLOGY**

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(73) Assignee: **JCBD, LLC**, Fort Collins, CO (US)

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(65) **Prior Publication Data**

US 2019/0343640 A1 Nov. 14, 2019

Related U.S. Application Data

(60) Continuation-in-part of application No. 16/041,372, filed on Jul. 20, 2018, which is a continuation of (Continued)

(51) **Int. Cl.**
A61F 2/44 (2006.01)
A61F 2/30 (2006.01)
(Continued)

(52) **U.S. Cl.**
CPC **A61F 2/30988** (2013.01); **A61B 17/1626** (2013.01); **A61B 17/1739** (2013.01); **A61B 17/1757** (2013.01); **A61B 17/7055** (2013.01); **A61B 17/7074** (2013.01); **A61F 2/4455** (2013.01); **A61F 2/4611** (2013.01); **A61B 17/025** (2013.01); **A61B 17/7043** (2013.01); **A61B 17/8645** (2013.01); **A61B 2017/0046** (2013.01); **A61F 2002/304** (2013.01); **A61F**

2002/3055 (2013.01); **A61F 2002/30163** (2013.01); **A61F 2002/30382** (2013.01); **A61F 2002/30401** (2013.01); **A61F 2002/30428** (2013.01); **A61F 2002/30484** (2013.01); **A61F 2002/30504** (2013.01); **A61F 2002/30509** (2013.01); **A61F 2002/30579** (2013.01); **A61F 2002/30601** (2013.01); **A61F 2002/30622** (2013.01); **A61F 2002/30774** (2013.01);
(Continued)

(58) **Field of Classification Search**
CPC **A61F 2002/30995**; **A61F 2002/4455**
See application file for complete search history.

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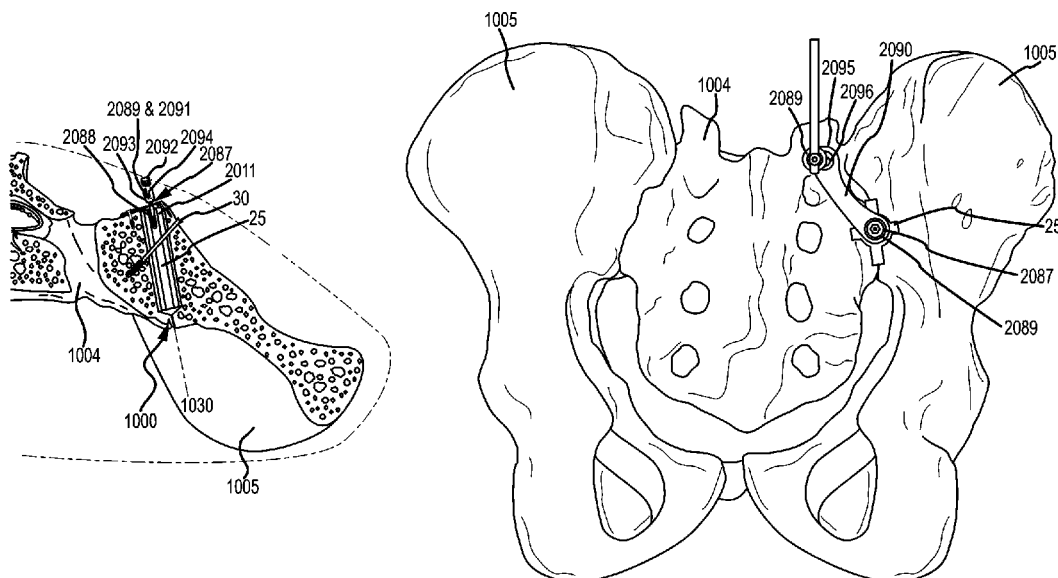
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Primary Examiner — Christian A Sevilla
(74) *Attorney, Agent, or Firm* — Polsinelli PC; Joshua J. Prancun; Samuel Wade Johnson

(57) **ABSTRACT**

Systems and methods for treating musculo skeletal disorders of the spinopelvic anatomy including treating spinal deformities by spinopelvic fixation including fusion of the sacroiliac joint at the base of long spinal fusion construct cases. The system may include implants designed to be used as an adjunct to long spinal fusions to further the immobilization and stabilization of the sacroiliac joint. The implants may be designed to augment an S2AI screw and an S1 screw in order to improve durability of the foundation of the spinal construct. The implants may have a triangular cross section.

27 Claims, 217 Drawing Sheets



Related U.S. Application Data

application No. 15/992,987, filed on May 30, 2018, now Pat. No. 10,130,477, which is a continuation of application No. 15/910,753, filed on Mar. 2, 2018, now Pat. No. 10,058,430, which is a continuation of application No. 15/828,677, filed on Dec. 1, 2017, now Pat. No. 9,931,212, which is a continuation of application No. 15/061,524, filed on Mar. 4, 2016, now Pat. No. 9,833,320, which is a division of application No. 13/946,760, filed on Jul. 19, 2013, now Pat. No. 9,333,090, and a continuation-in-part of application No. 13/475,695, filed on May 18, 2012, now Pat. No. 9,381,045, which is a continuation-in-part of application No. 13/236,411, filed on Sep. 19, 2011, now Pat. No. 9,017,407, which is a continuation-in-part of application No. 12/998,712, filed as application No. PCT/US2011/000070 on Jan. 13, 2011, now Pat. No. 8,979,928, said application No. 16/041,372 is a continuation-in-part of application No. 14/344,876, filed as application No. PCT/US2012/055892 on Sep. 18, 2012, now Pat. No. 10,034,676, which is a continuation-in-part of application No. 13/475,695, filed on May 18, 2012, now Pat. No. 9,381,045, which is a continuation-in-part of application No. 13/236,411, filed on Sep. 19, 2011, now Pat. No. 9,017,407, which is a continuation-in-part of application No. 12/998,712, filed as application No. PCT/US2011/000070 on Jan. 13, 2011, now Pat. No. 8,979,928, application No. 16/455,308, filed on Jun. 27, 2019, which is a continuation-in-part of application No. 15/729,273, filed on Oct. 10, 2017, now abandoned, which is a continuation of application No. 14/127,119, filed as application No. PCT/US2012/042823 on Jun. 15, 2012, now Pat. No. 9,788,961, and a continuation-in-part of application No. 13/475,695, filed on May 18, 2012, now Pat. No. 9,381,045, which is a continuation-in-part of application No. 13/236,411, filed on Sep. 19, 2011, now Pat. No. 9,017,407, which is a continuation-in-part of application No. 12/998,712, filed as application No. PCT/US2011/000070 on Jan. 13, 2011, now Pat. No. 8,979,928, application No. 16/455,308, filed on Jun. 27, 2019, which is a continuation-in-part of application No. 15/664,862, filed on Jul. 31, 2017, now Pat. No. 10,441,318, which is a division of application No. 14/216,975, filed on Mar. 17, 2014, now Pat. No. 9,757,154, which is a continuation-in-part of application No. 13/475,695, filed on May 18, 2012, now Pat. No. 9,381,045, which is a continuation-in-part of application No. 13/236,411, filed on Sep. 19, 2011, now Pat. No. 9,017,407, which is a continuation-in-part of application No. 12/998,712, filed as applica-

- tion No. PCT/US2011/000070 on Jan. 13, 2011, now Pat. No. 8,979,928, application No. 16/455,308, filed on Jun. 27, 2019, which is a continuation-in-part of application No. 15/385,446, filed on Dec. 20, 2016, now Pat. No. 10,335,197, which is a continuation of application No. 14/413,318, filed as application No. PCT/US2013/051381 on Jul. 19, 2013, now Pat. No. 9,554,909.
- (60) Provisional application No. 61/800,120, filed on Mar. 15, 2013, provisional application No. 61/674,277, filed on Jul. 20, 2012, provisional application No. 61/674,130, filed on Jul. 20, 2012, provisional application No. 61/335,947, filed on Jan. 13, 2010, provisional application No. 61/520,956, filed on Jun. 17, 2011, provisional application No. 61/798,225, filed on Mar. 15, 2013, provisional application No. 61/798,922, filed on Mar. 15, 2013, provisional application No. 61/674,233, filed on Jul. 20, 2012.
- (51) **Int. Cl.**
A61B 17/17 (2006.01)
A61F 2/46 (2006.01)
A61B 17/70 (2006.01)
A61B 17/16 (2006.01)
B33Y 80/00 (2015.01)
A61B 17/00 (2006.01)
A61B 17/86 (2006.01)
A61B 17/02 (2006.01)
- (52) **U.S. Cl.**
 CPC *A61F 2002/30828* (2013.01); *A61F 2002/30995* (2013.01); *A61F 2002/4623* (2013.01); *A61F 2002/4687* (2013.01); *A61F 2310/00017* (2013.01); *A61F 2310/00023* (2013.01); *A61F 2310/00179* (2013.01); *A61F 2310/00359* (2013.01); *B33Y 80/00* (2014.12)

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					606/264

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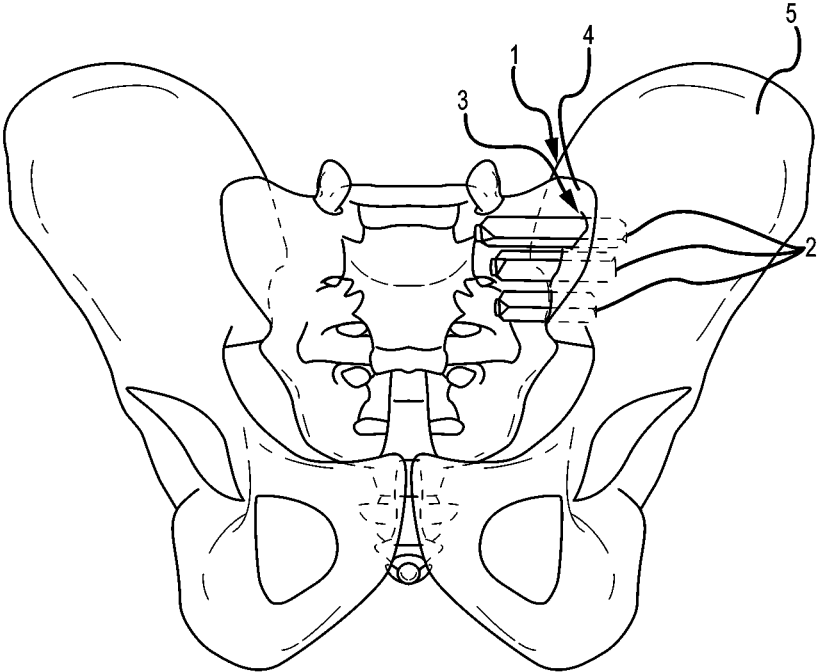
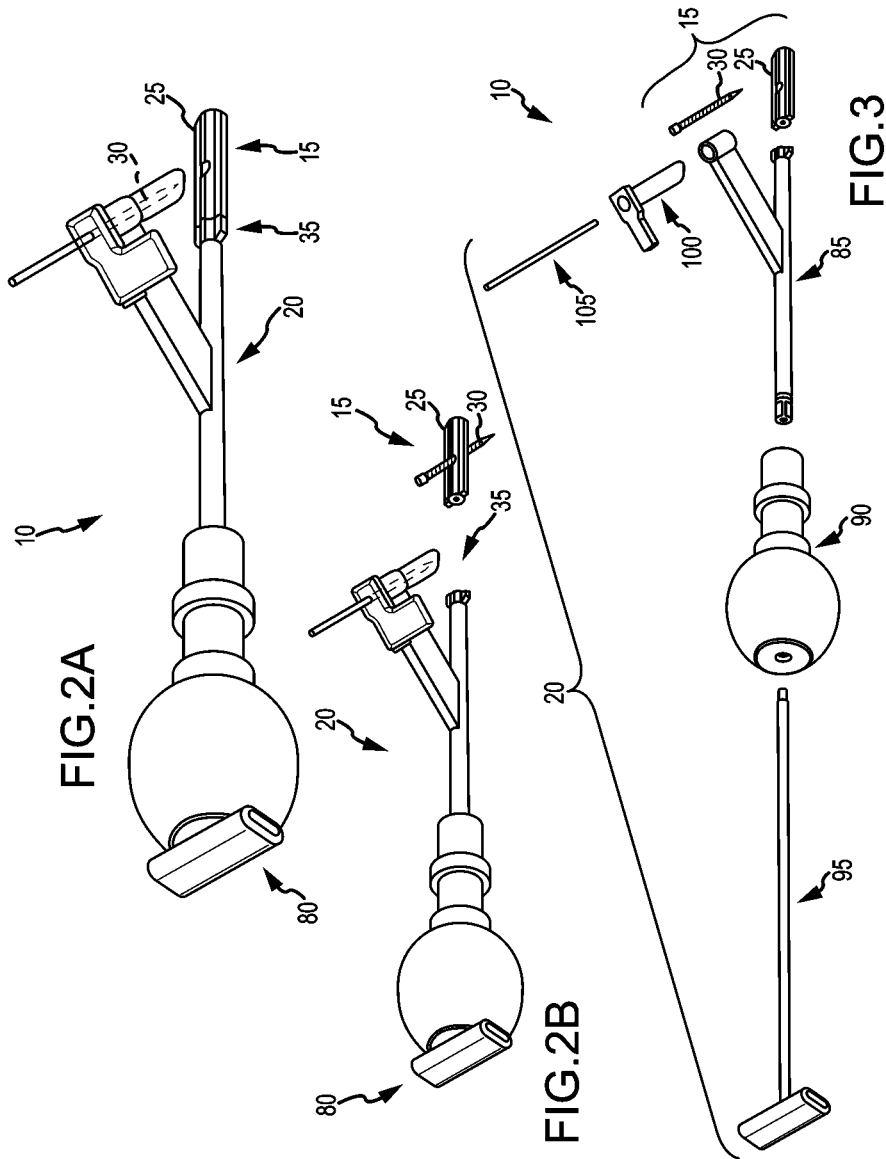


FIG. 1
CONVENTIONAL ART



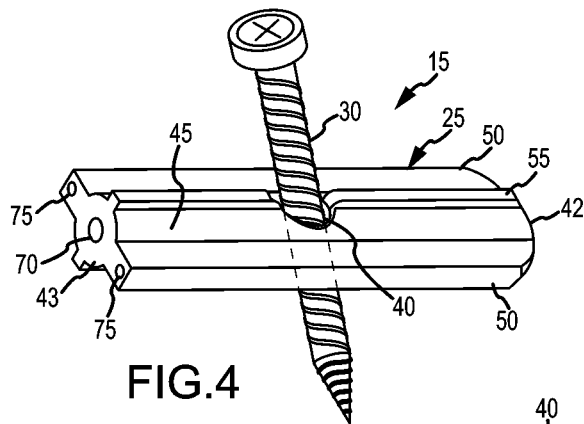


FIG. 4

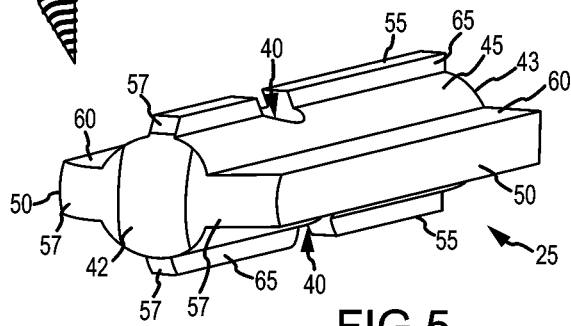


FIG. 5

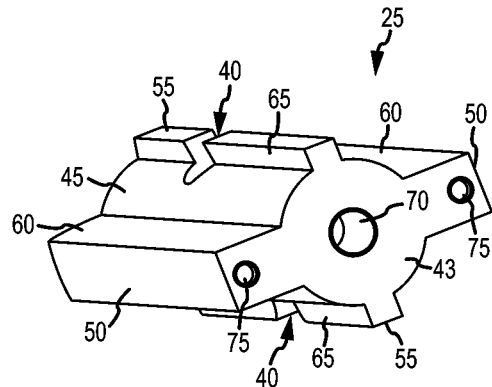


FIG. 6

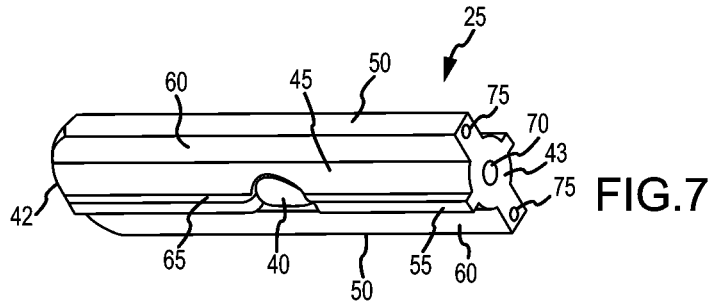


FIG. 7

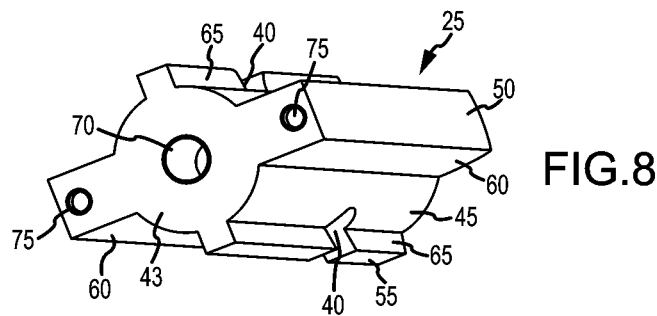


FIG. 8

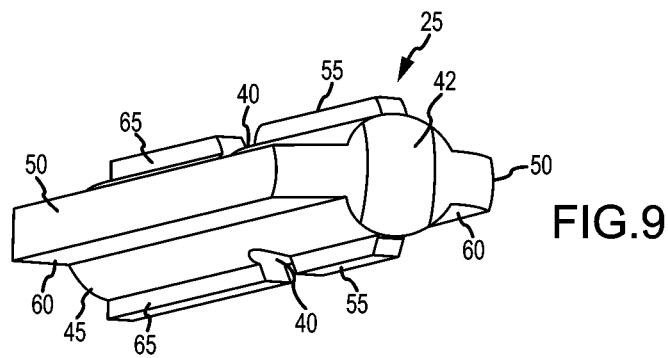
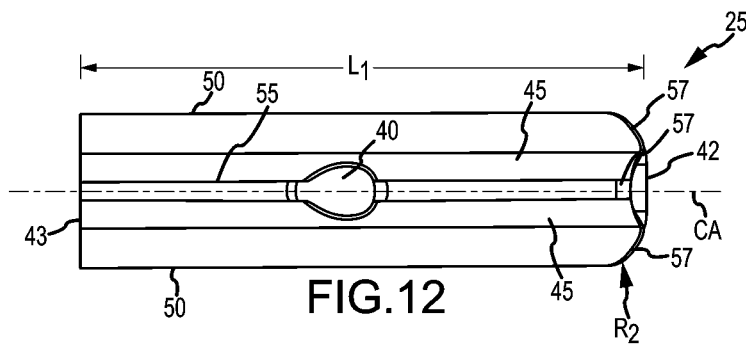
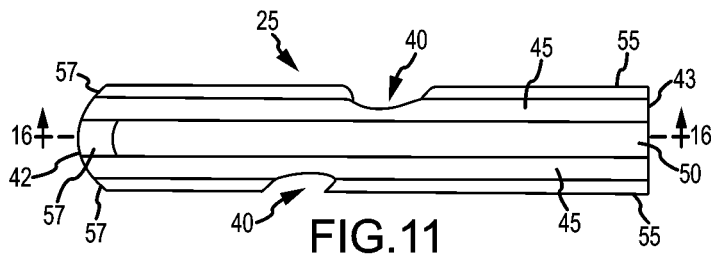
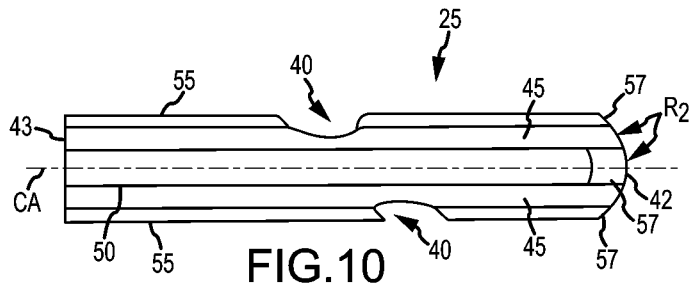
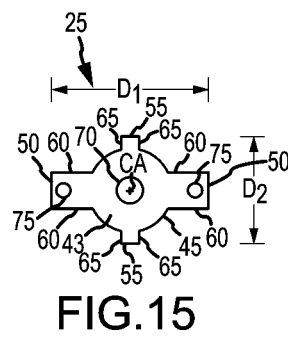
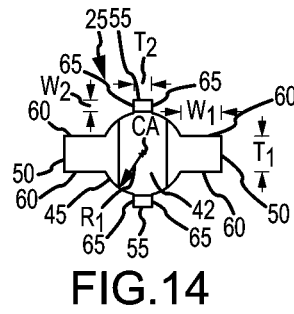
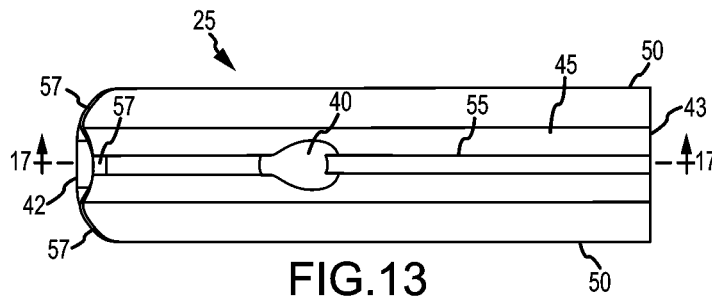


FIG. 9





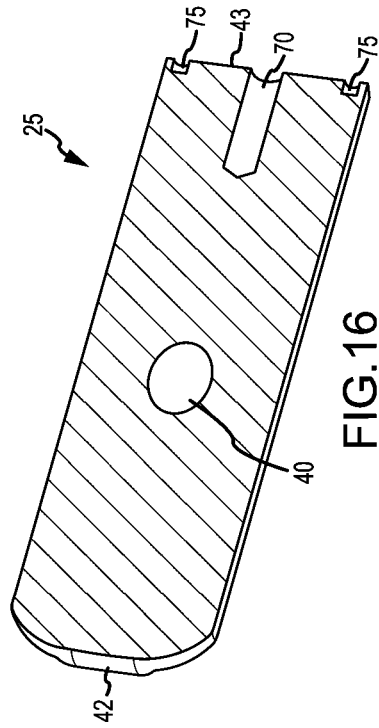


FIG. 16

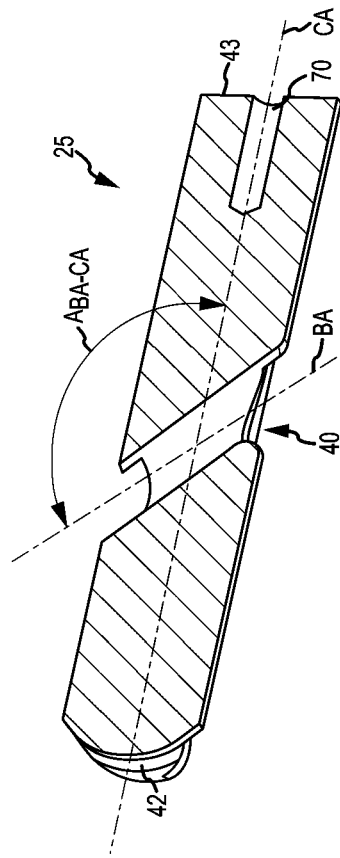
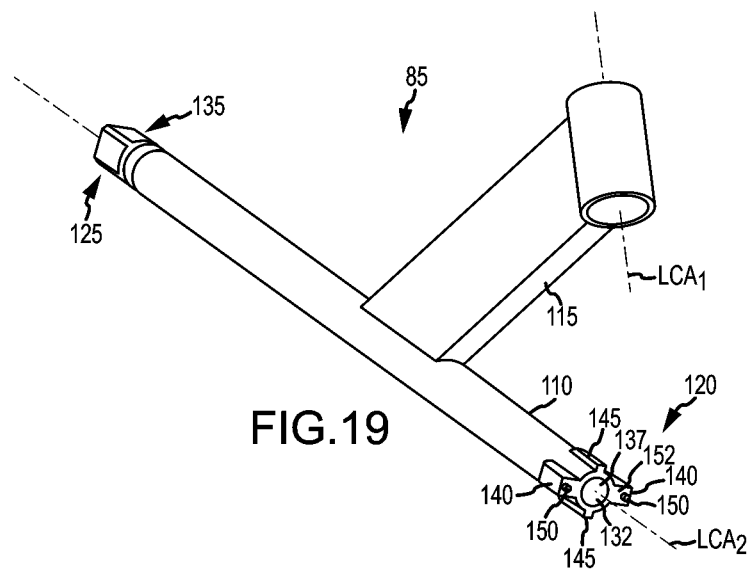
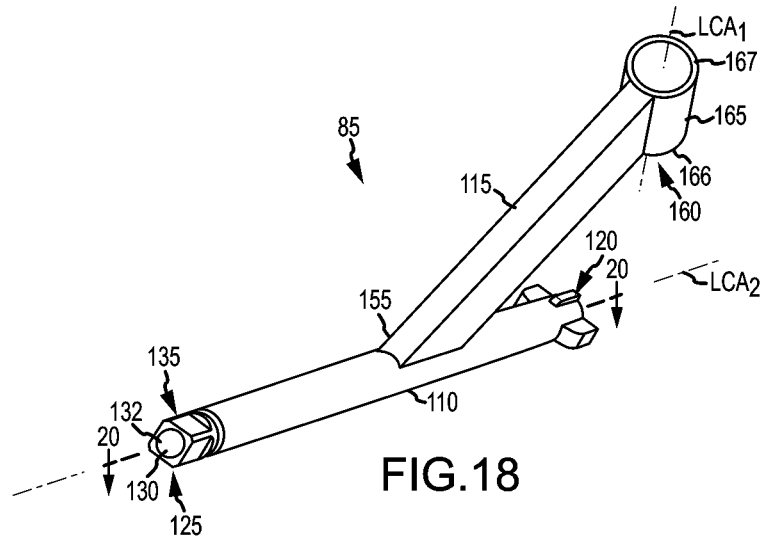
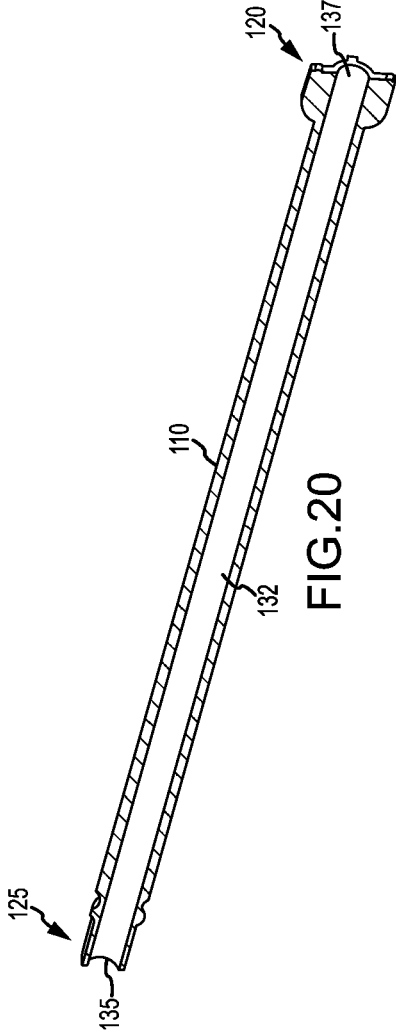


FIG. 17





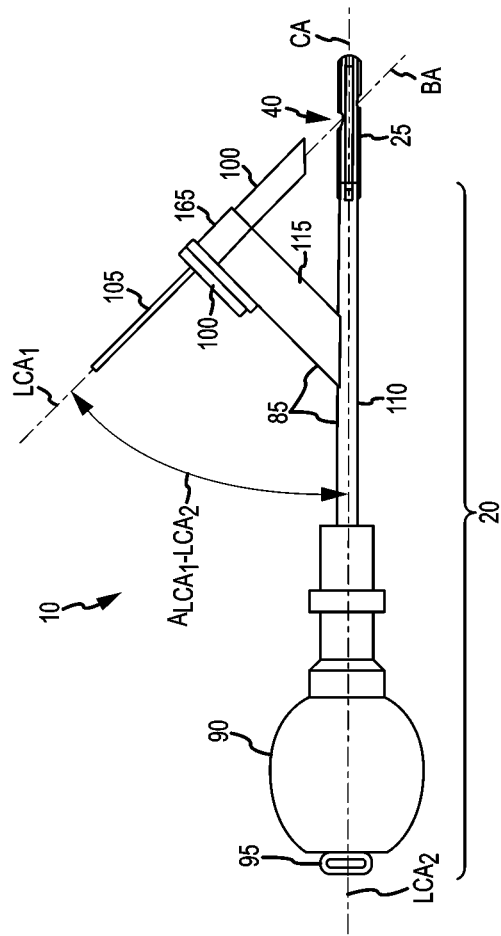


FIG.21A

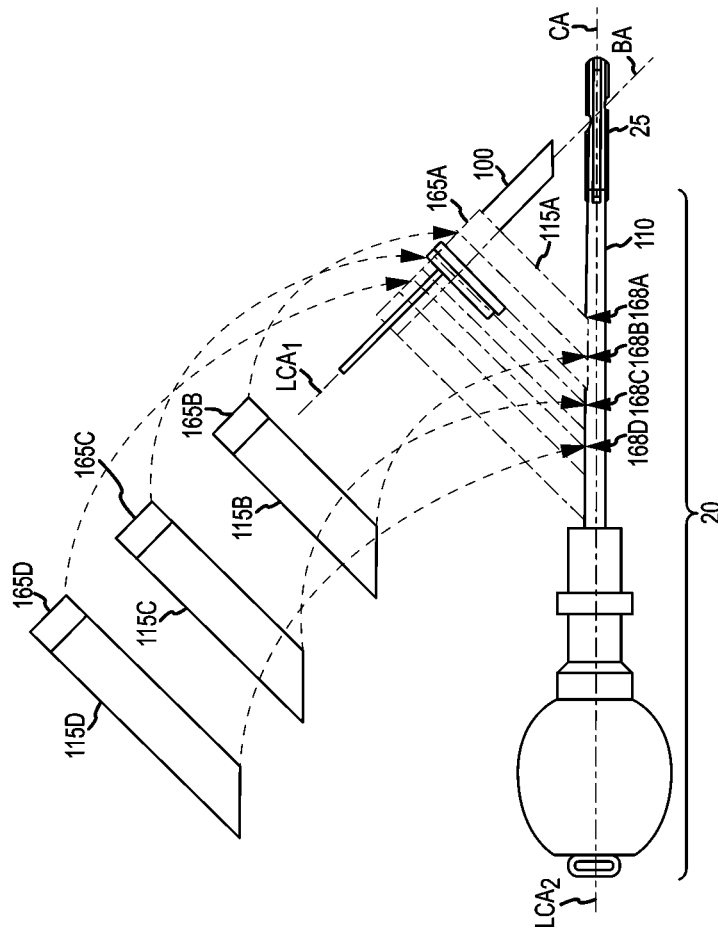


FIG. 21B

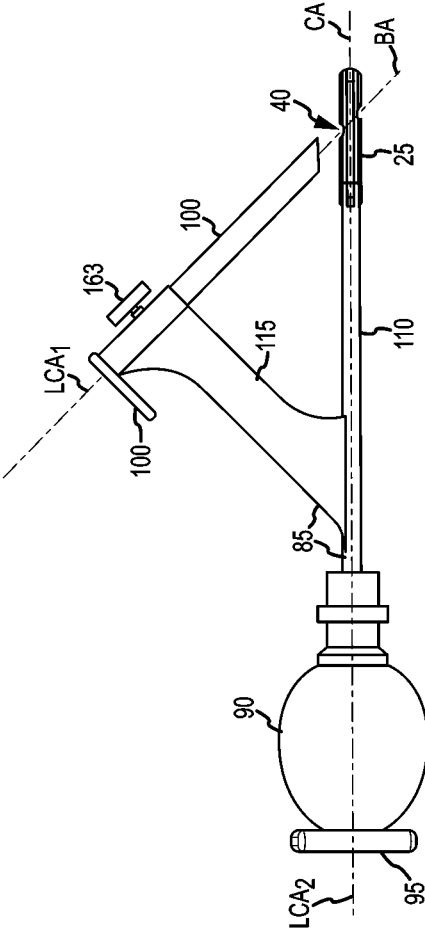
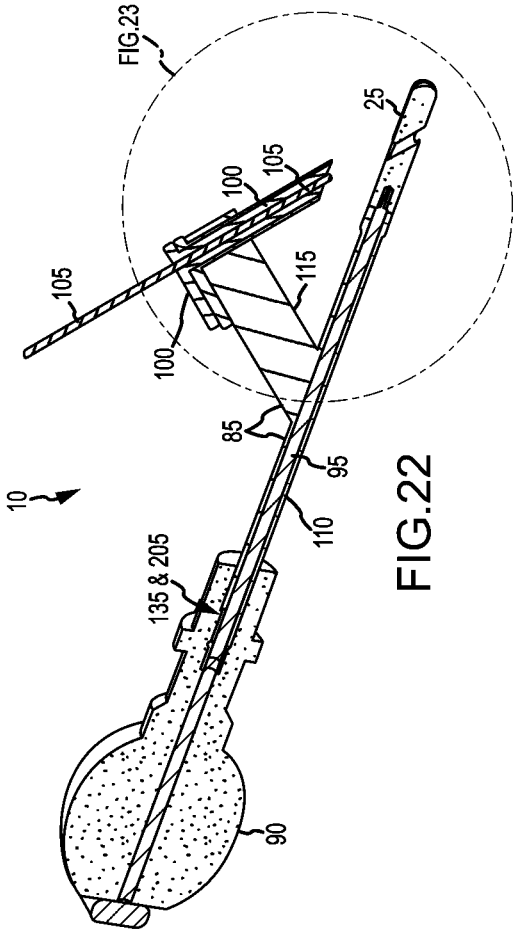


FIG.21C



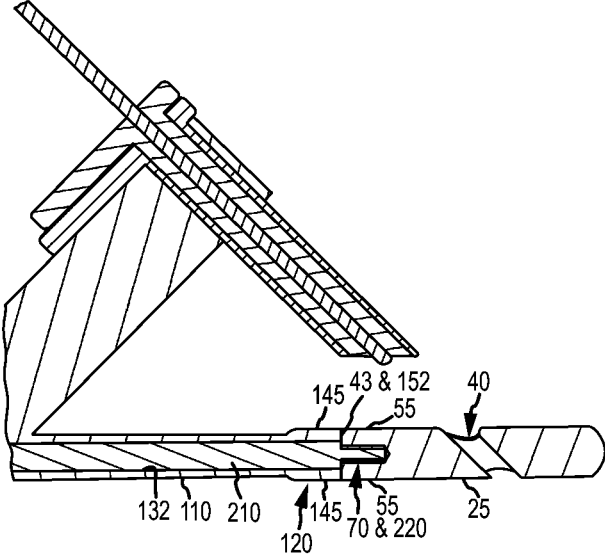


FIG.23

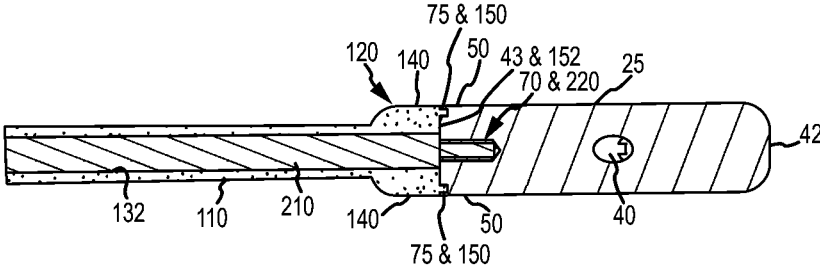


FIG.24

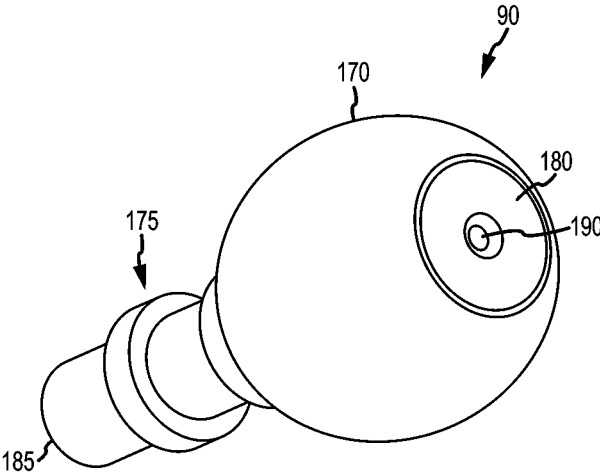


FIG. 25

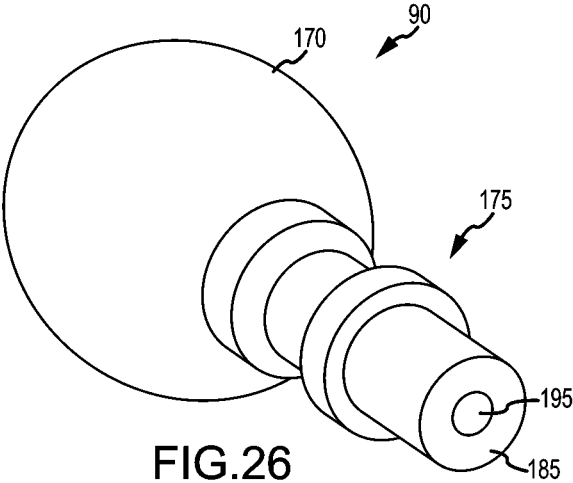


FIG. 26

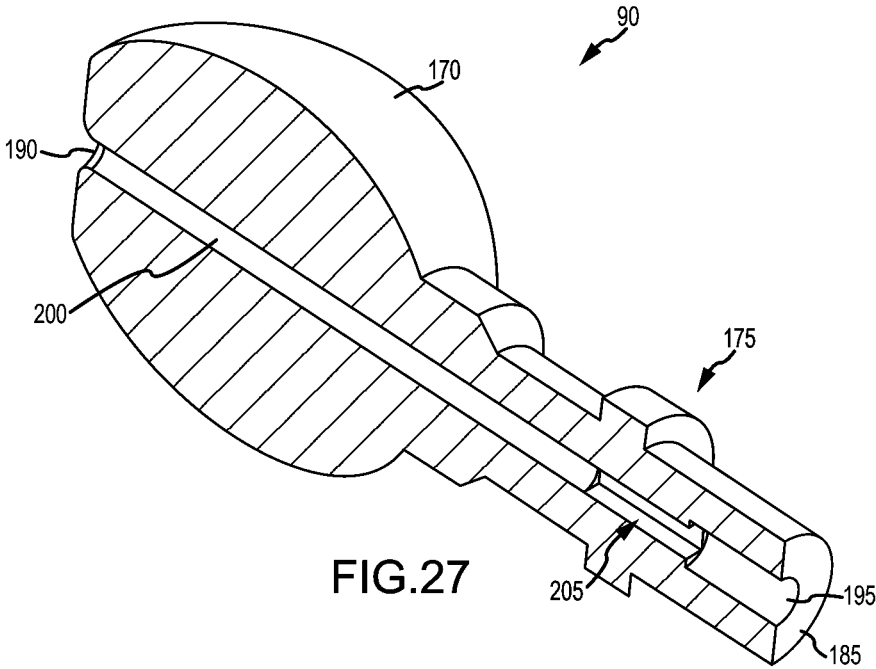
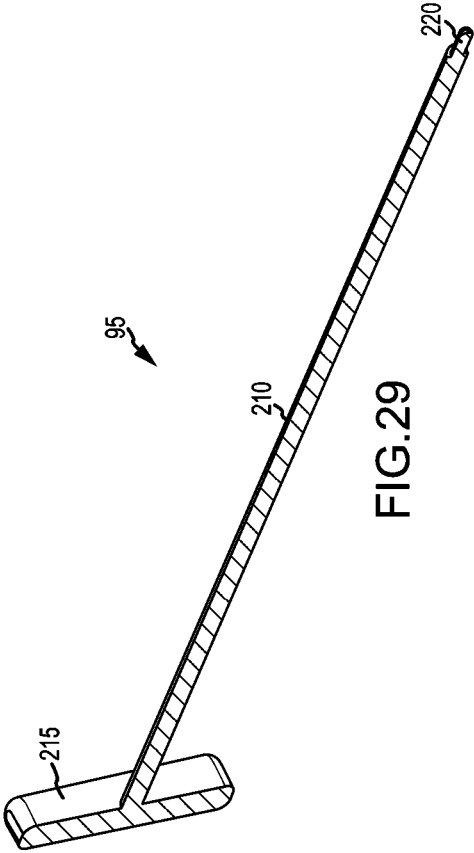
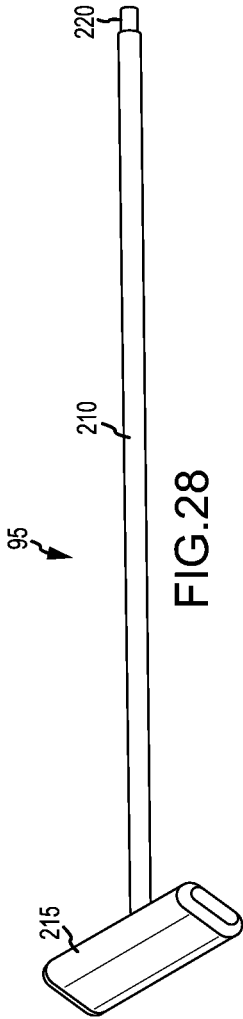


FIG.27



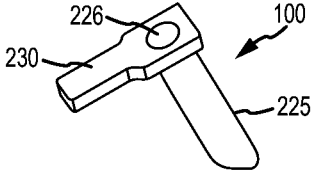


FIG.30A

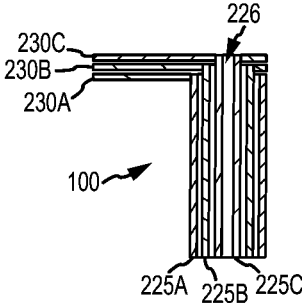


FIG.30B

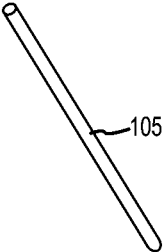
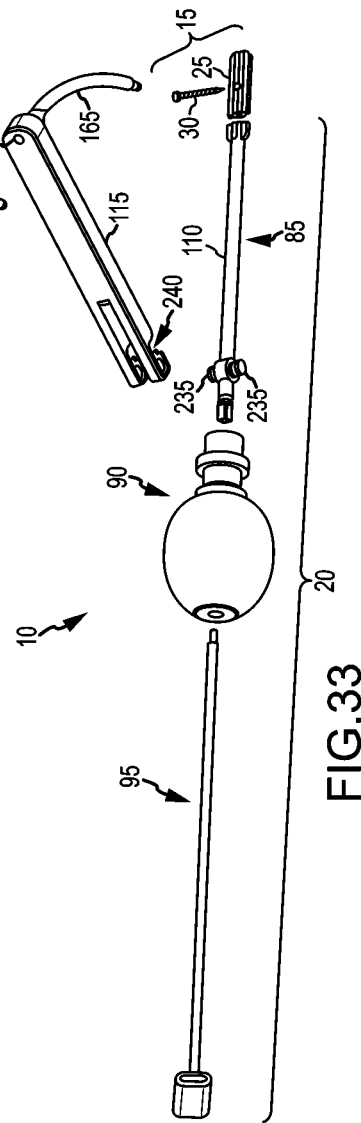
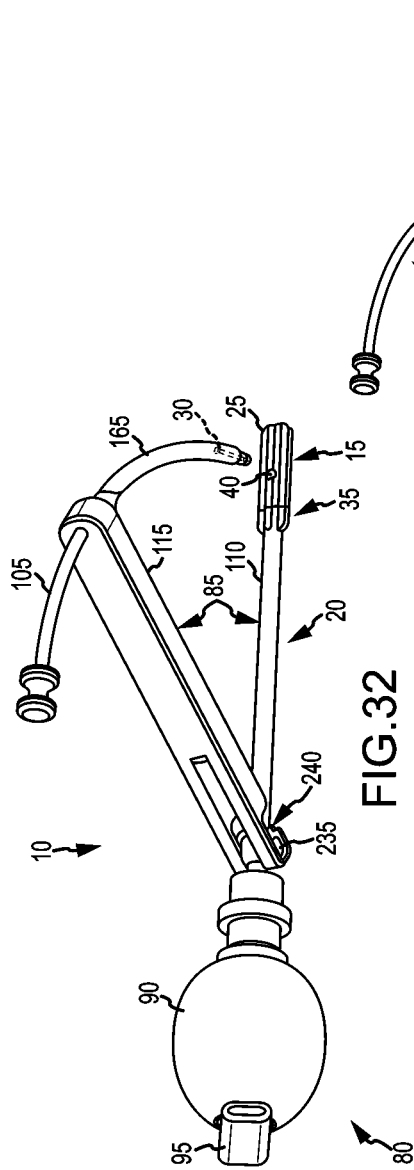


FIG.31



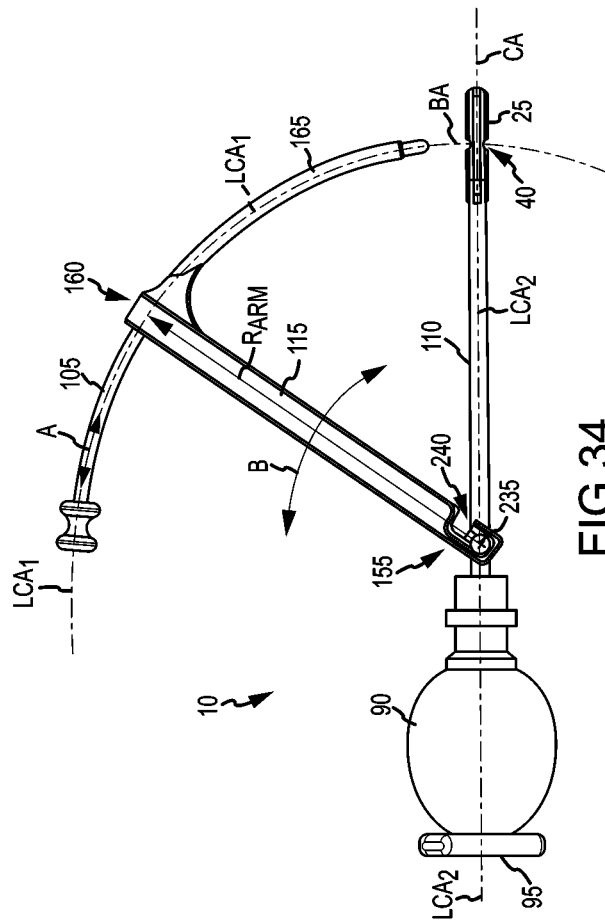


FIG. 34

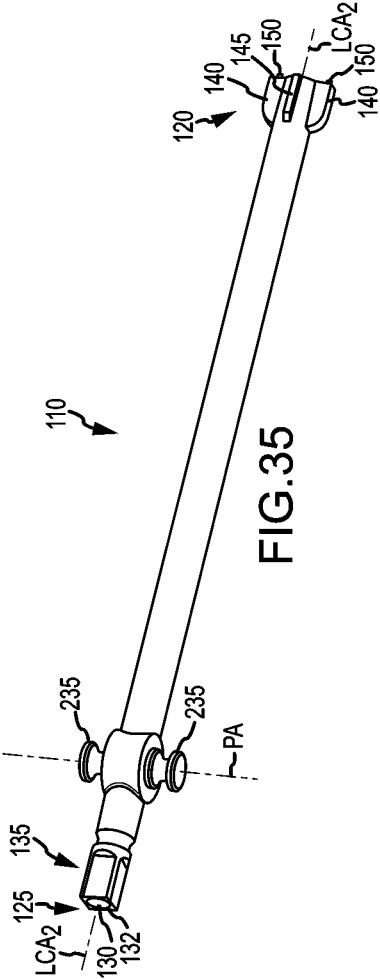


FIG.35

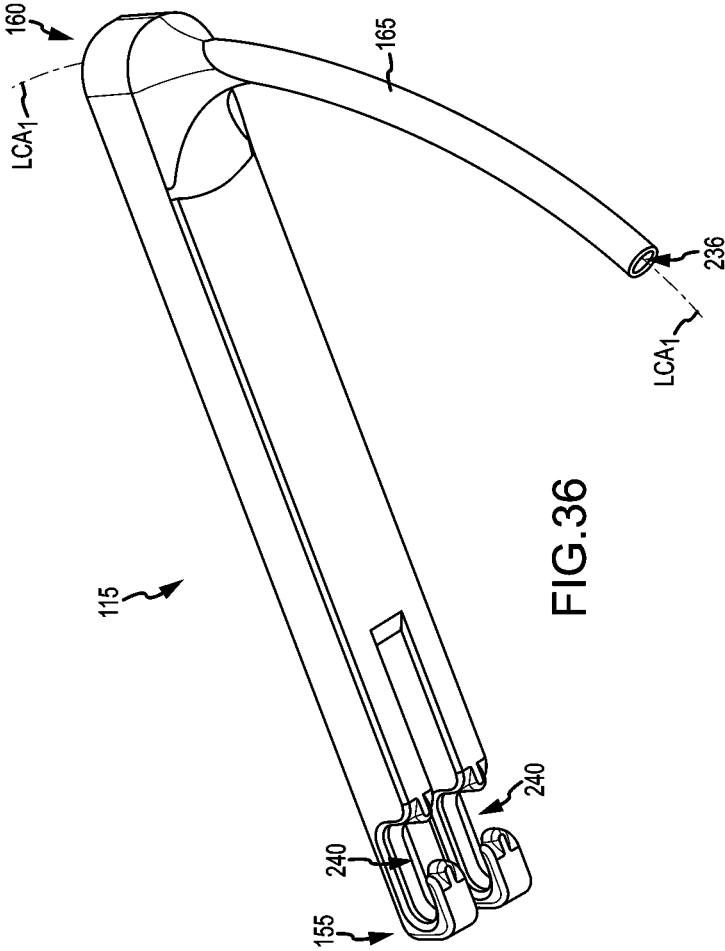
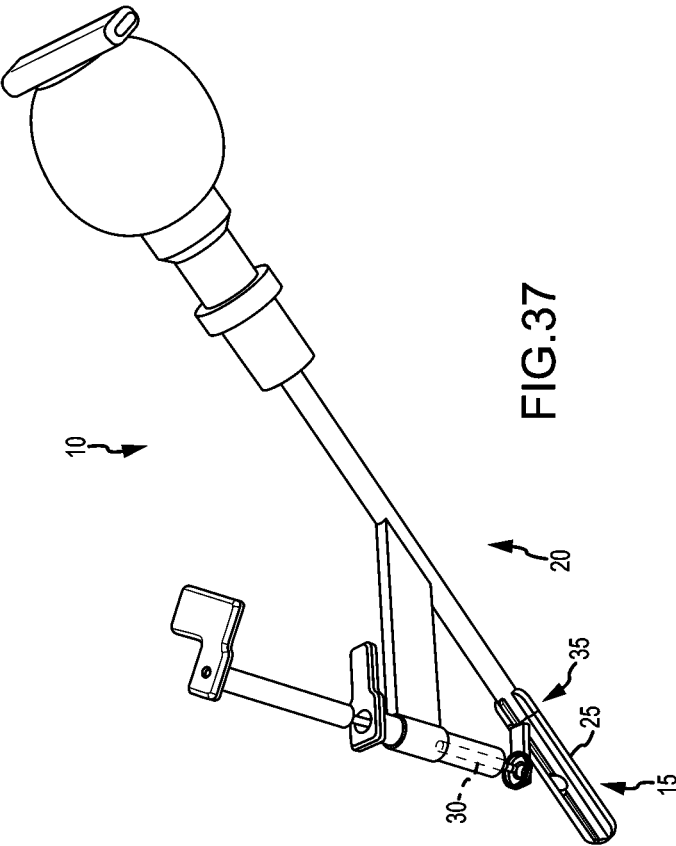
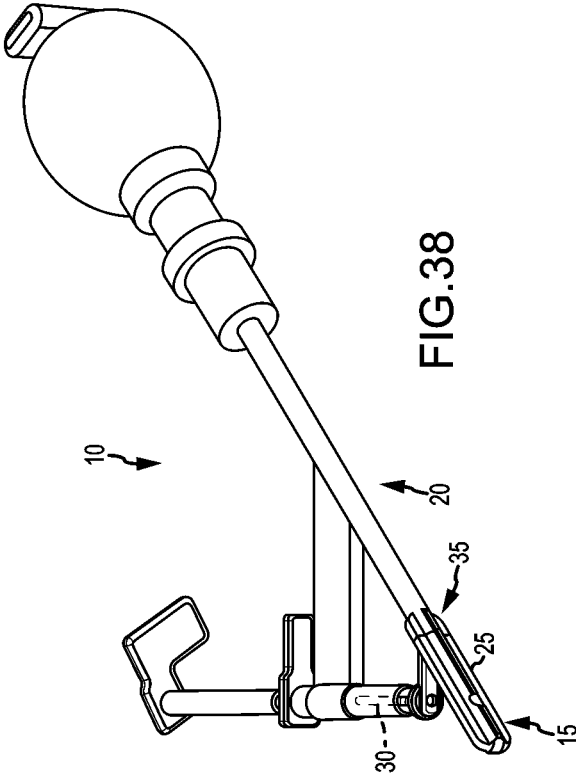
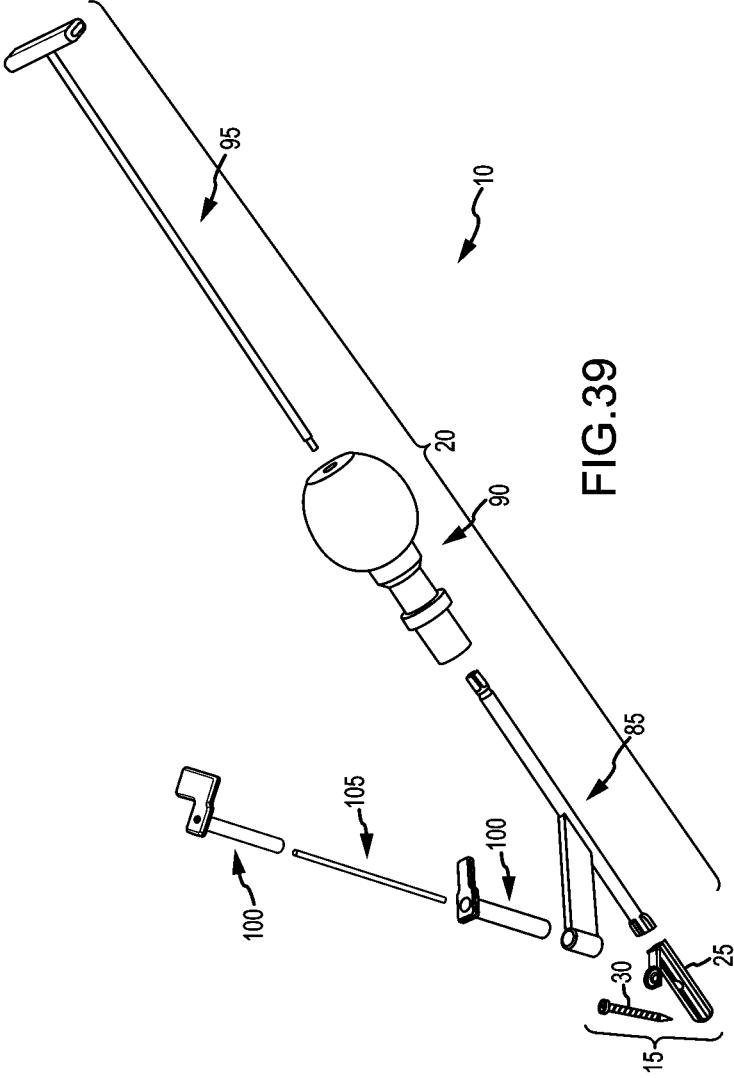


FIG. 36







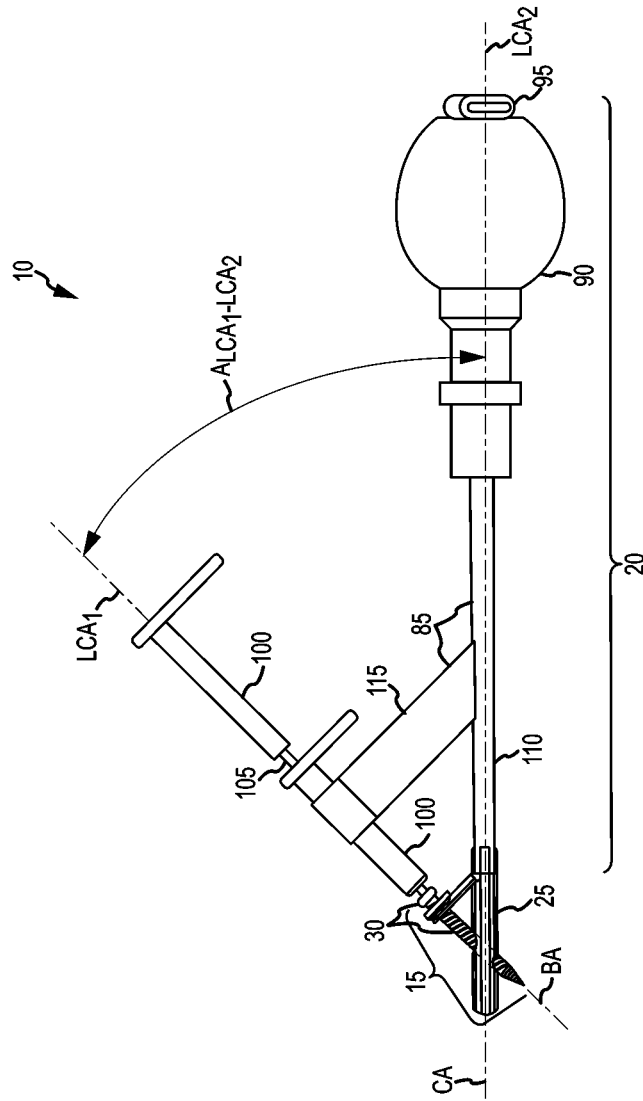


FIG. 40

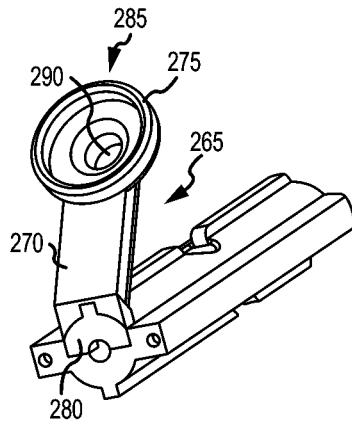


FIG. 41

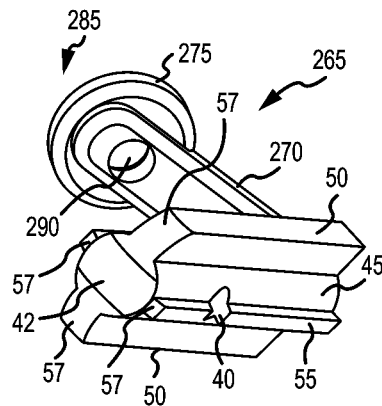


FIG. 42

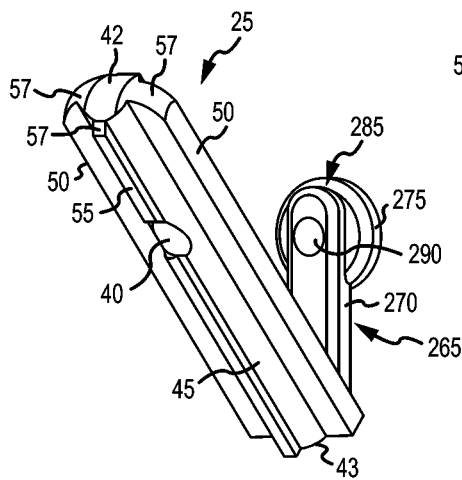


FIG. 43

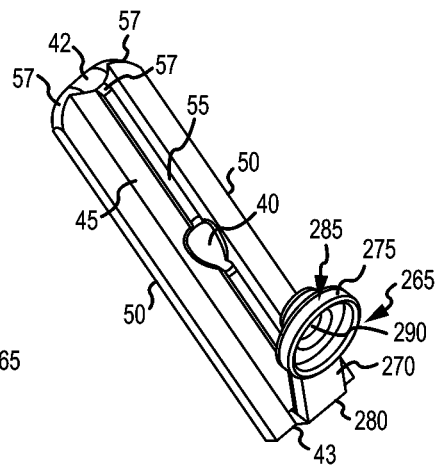


FIG. 44

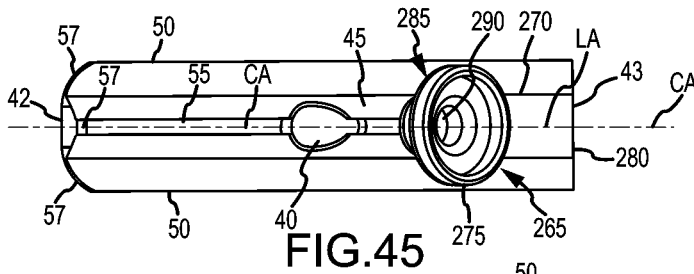


FIG. 45

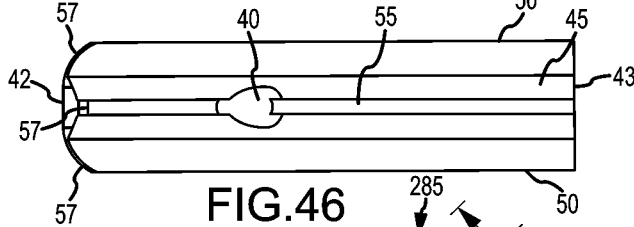


FIG. 46

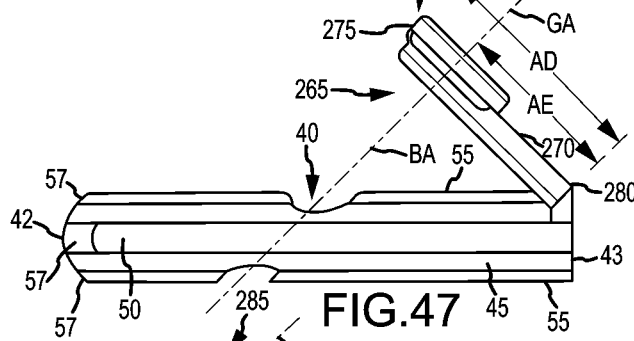


FIG. 47

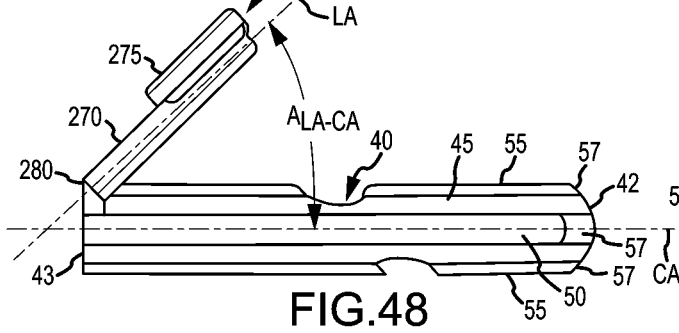


FIG. 48

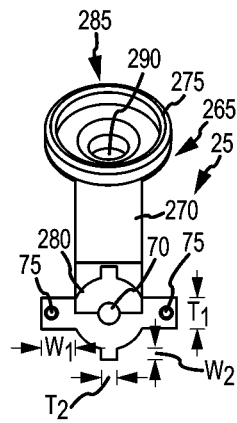


FIG. 49

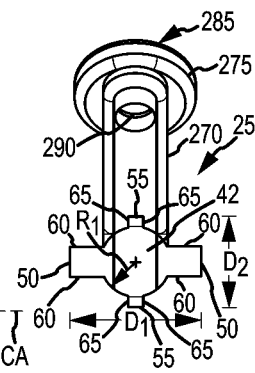
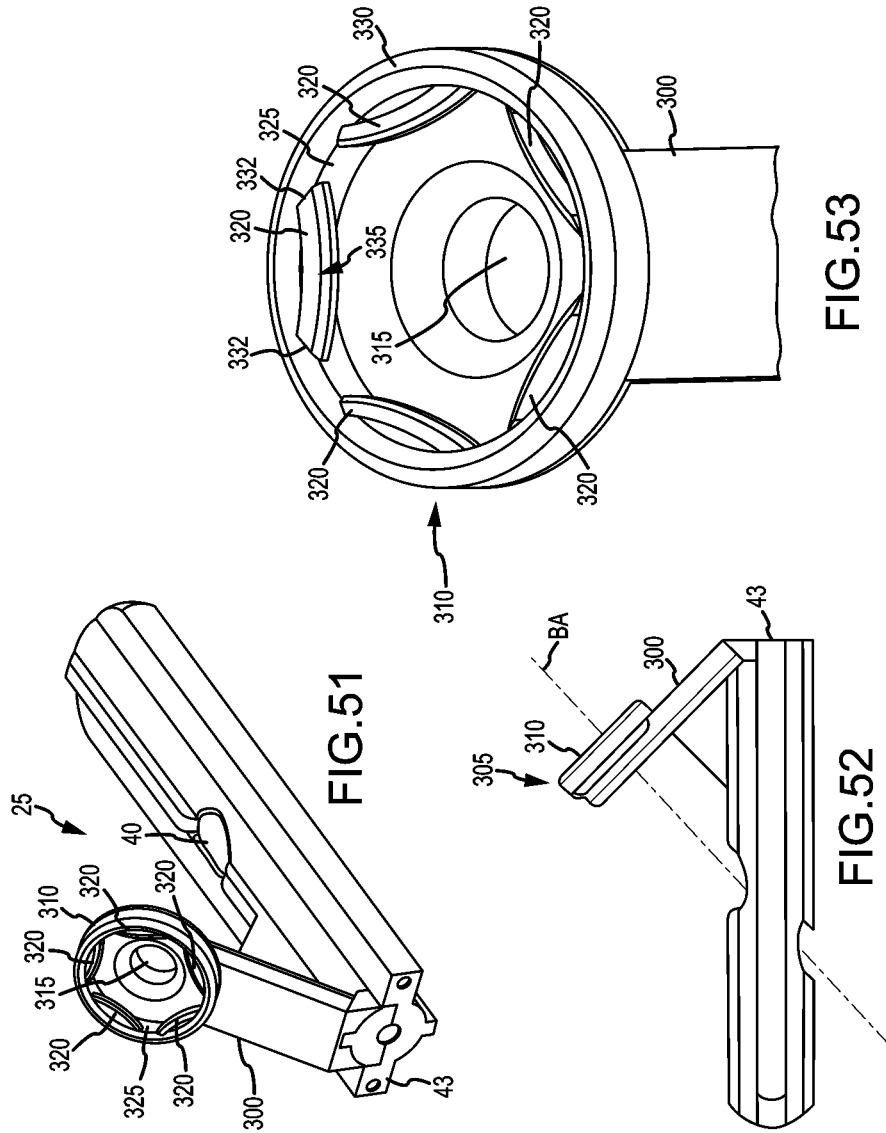


FIG. 50



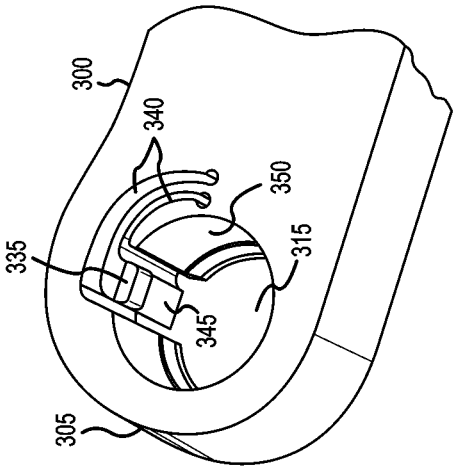


FIG. 55

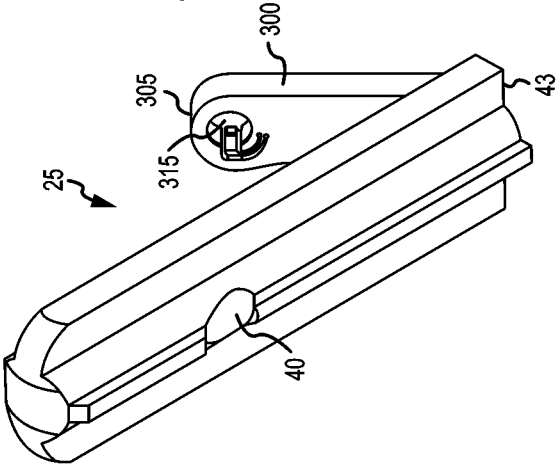
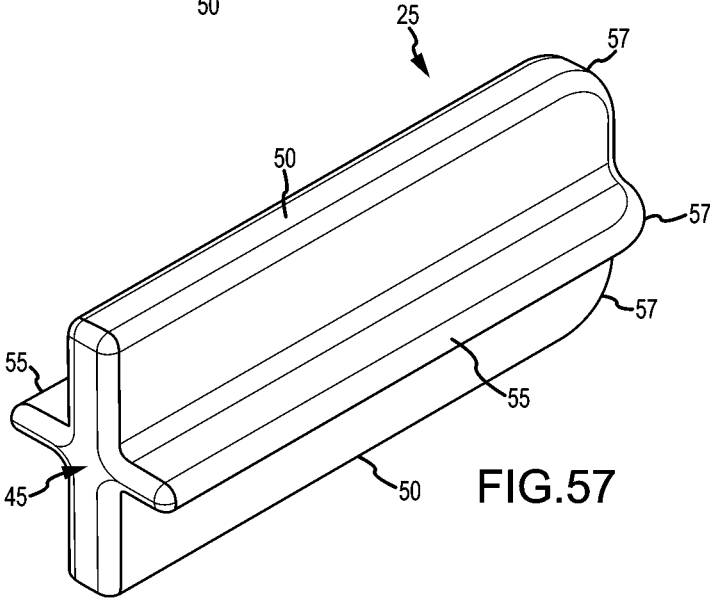
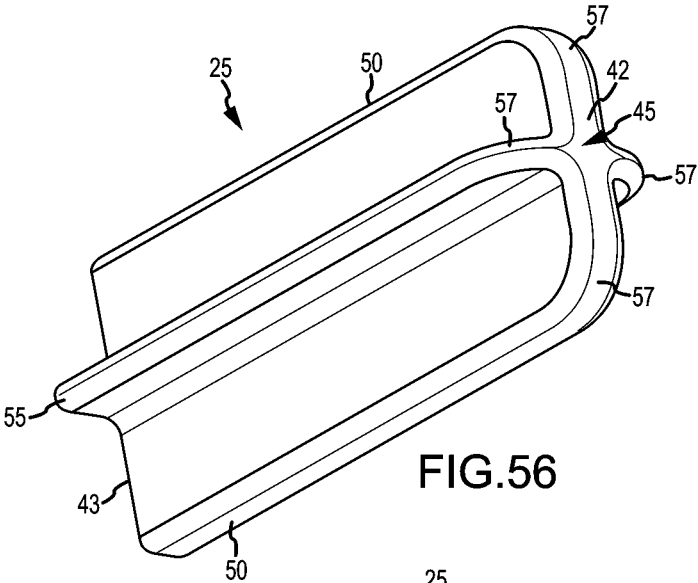


FIG. 54



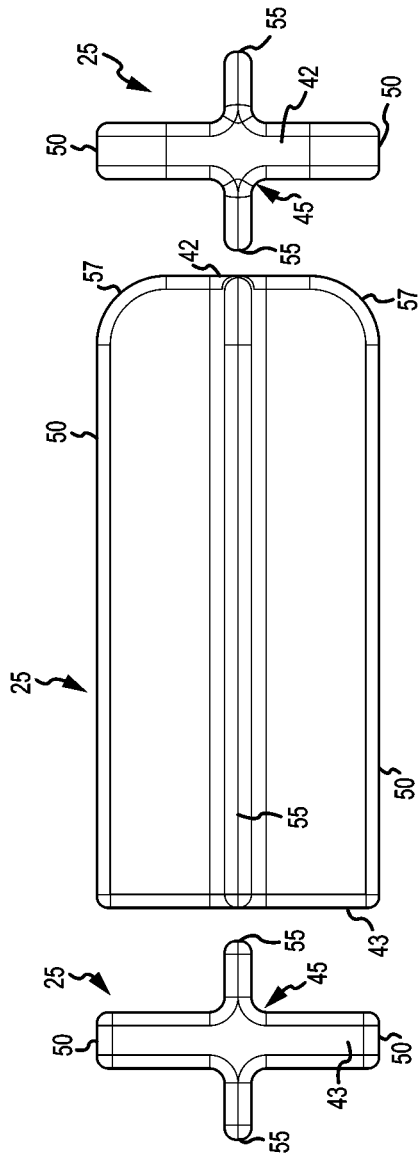


FIG. 61

FIG. 58

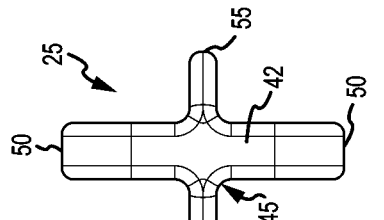


FIG. 60

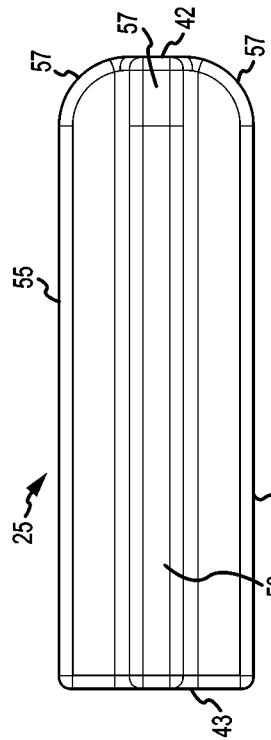
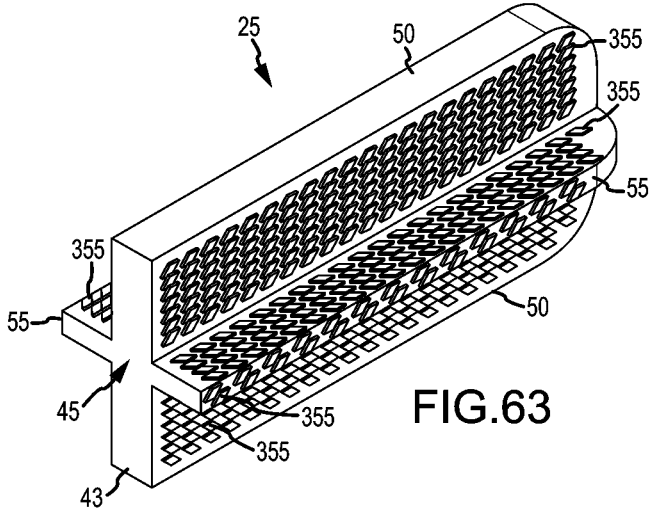
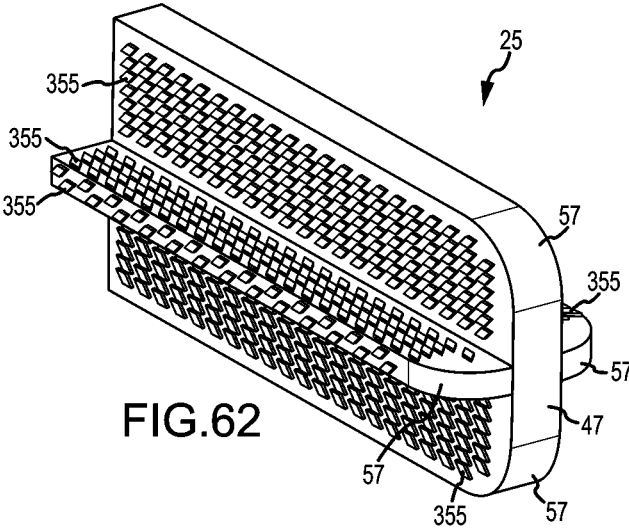


FIG. 59



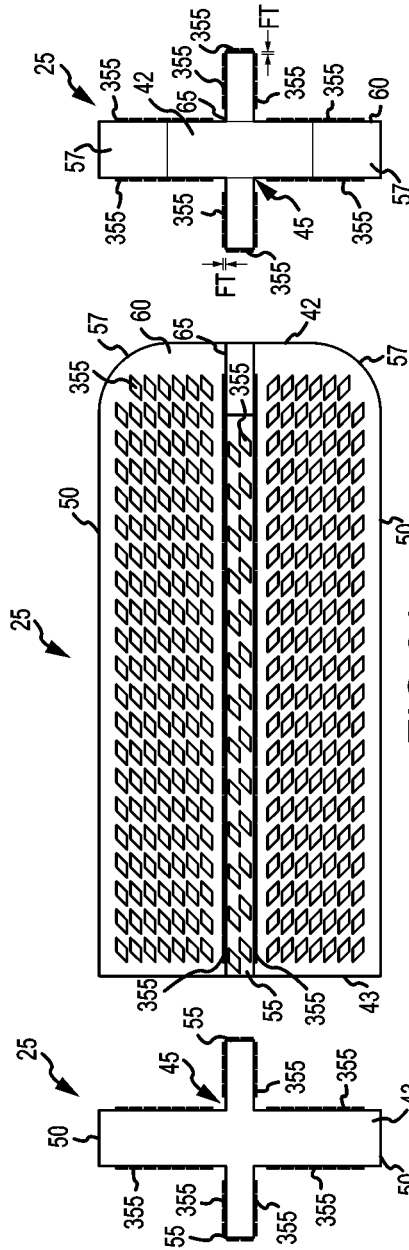
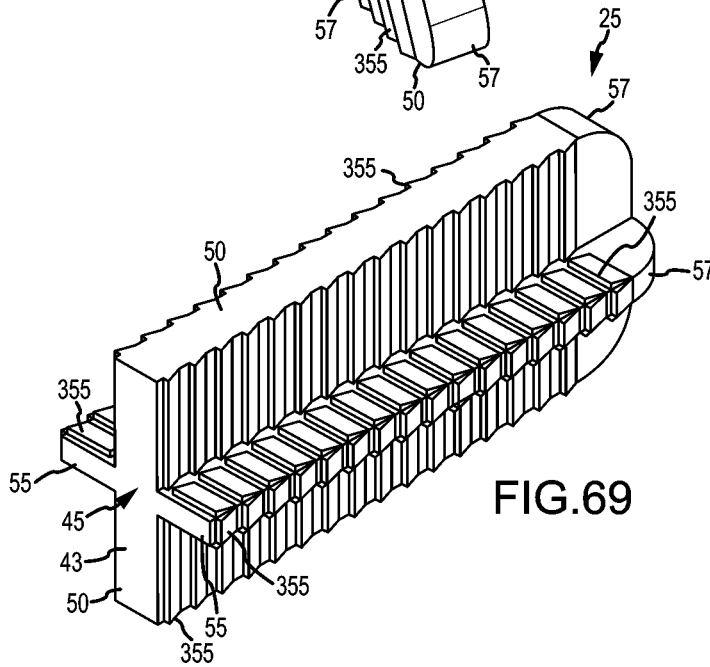
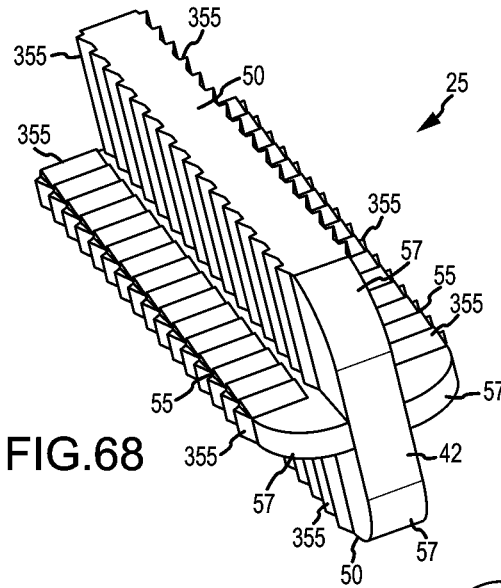


FIG. 66

FIG. 64

FIG. 65

FIG. 67



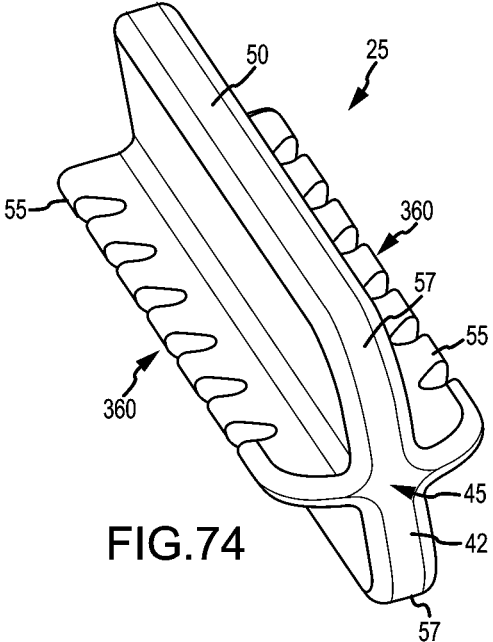


FIG. 74

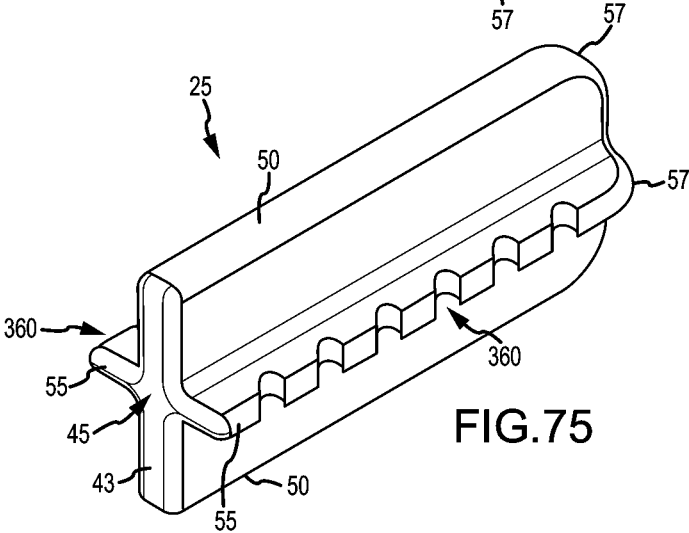
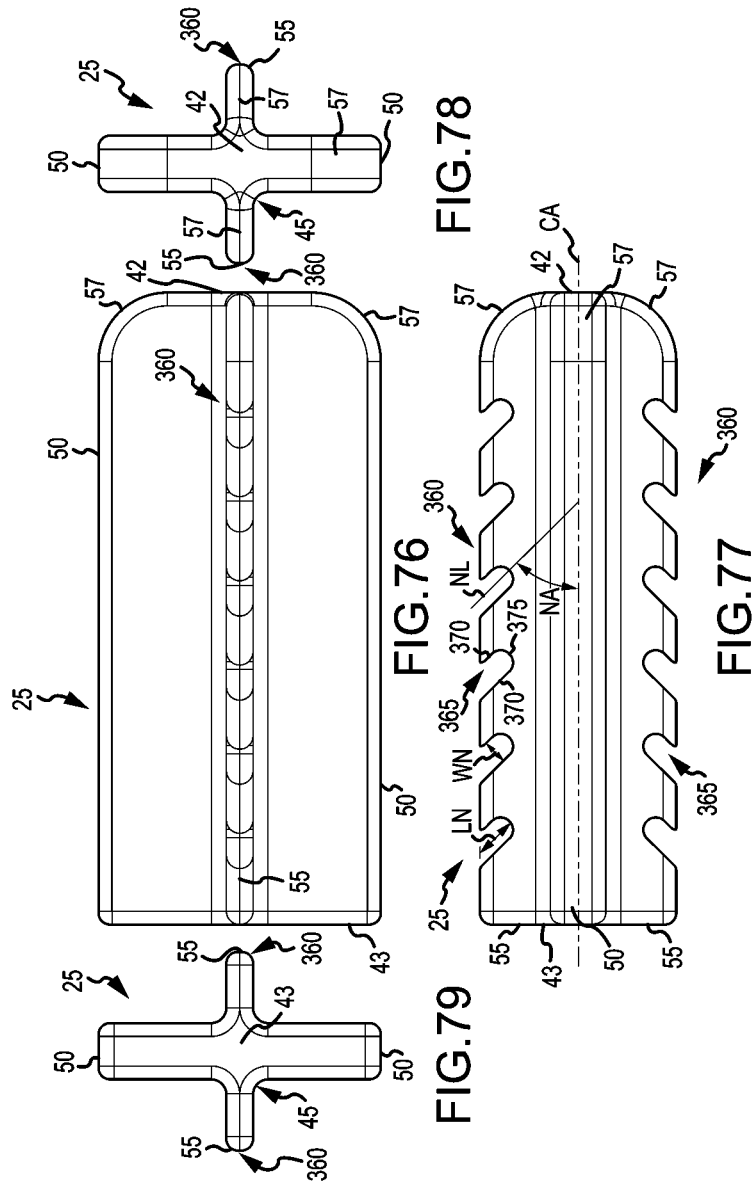


FIG. 75



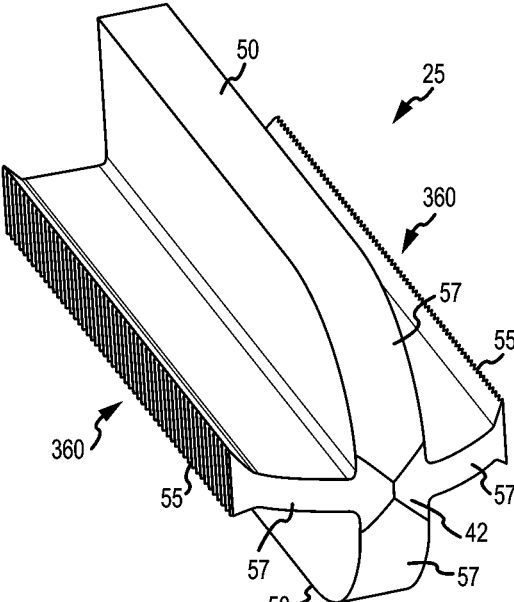


FIG. 80

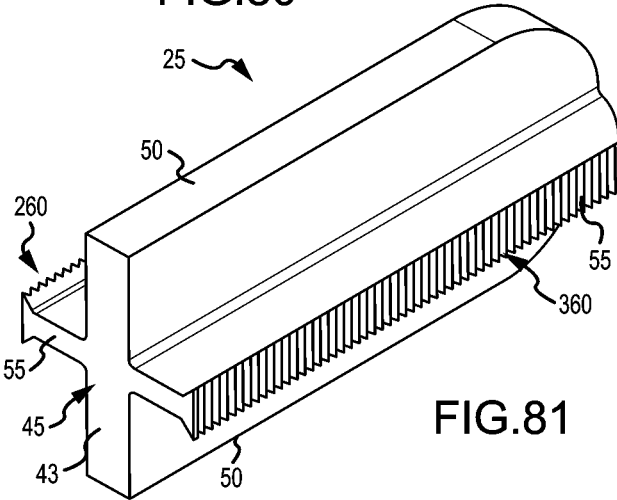


FIG. 81

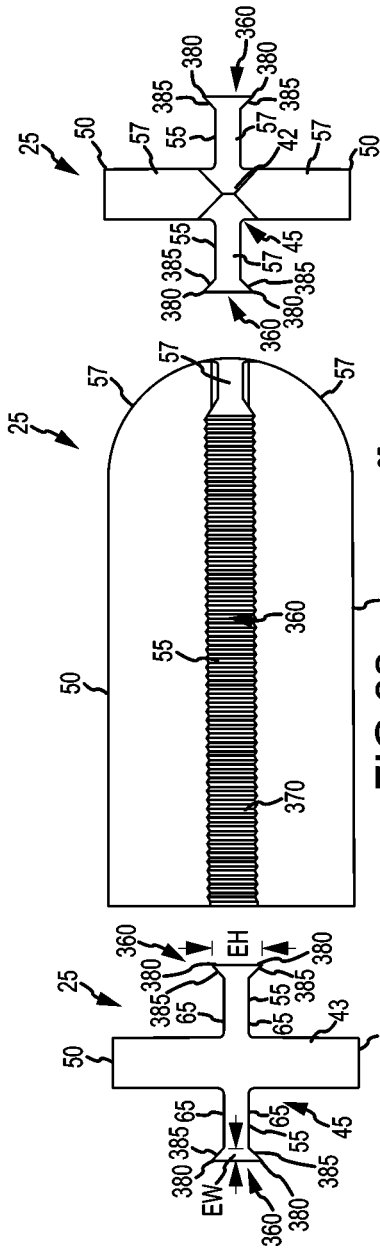


FIG. 82

FIG. 84

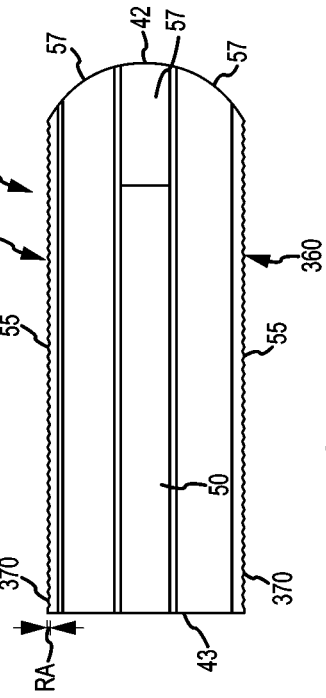


FIG. 83

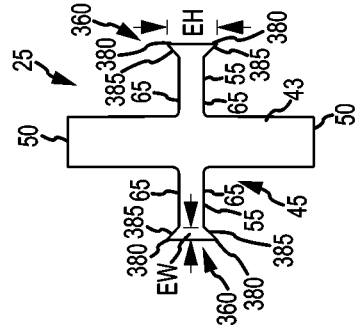


FIG. 85

RA

EH

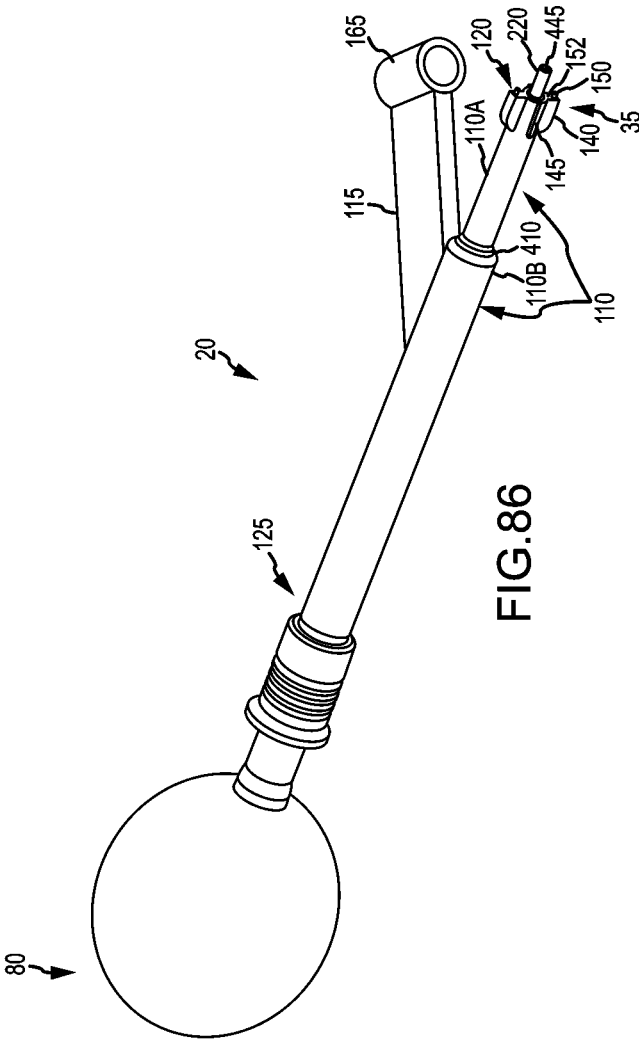


FIG. 86

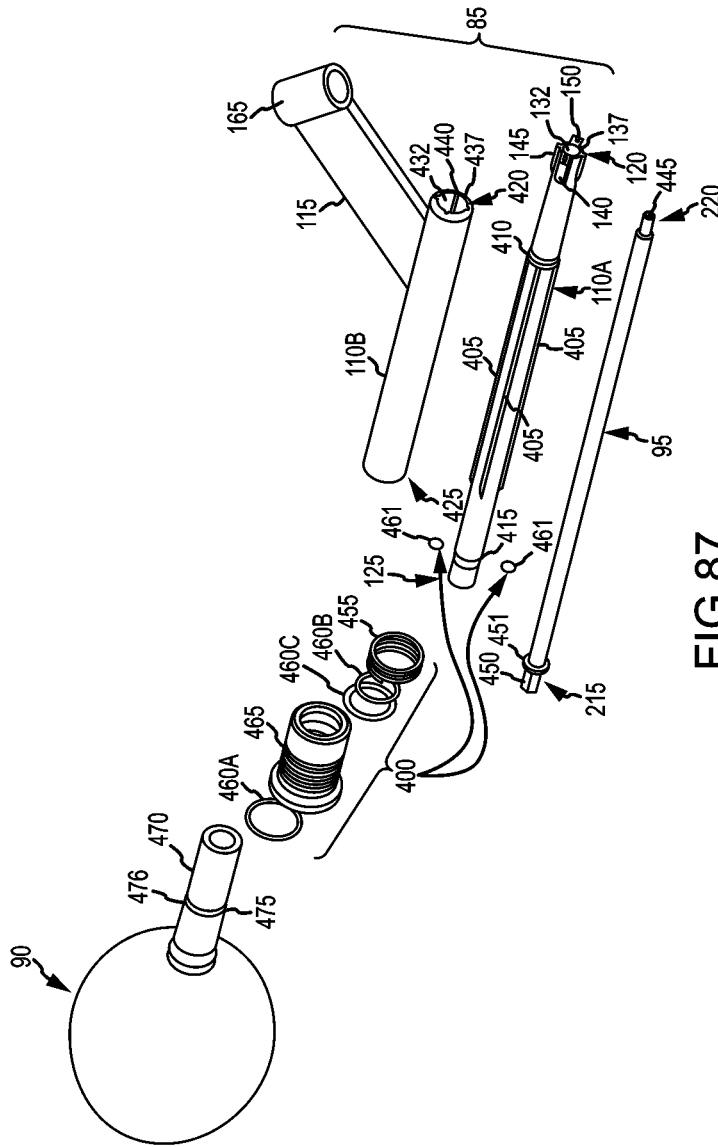


FIG. 87

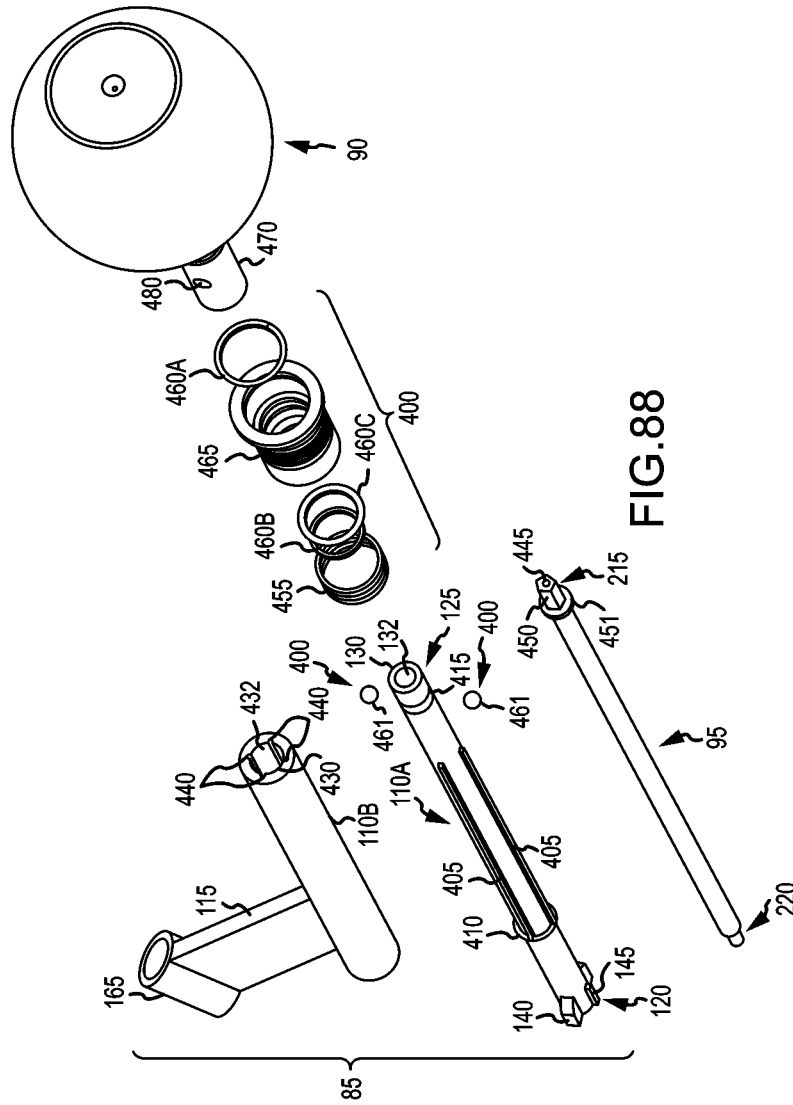
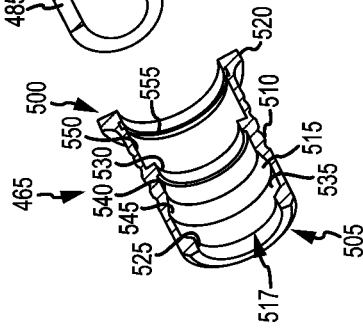
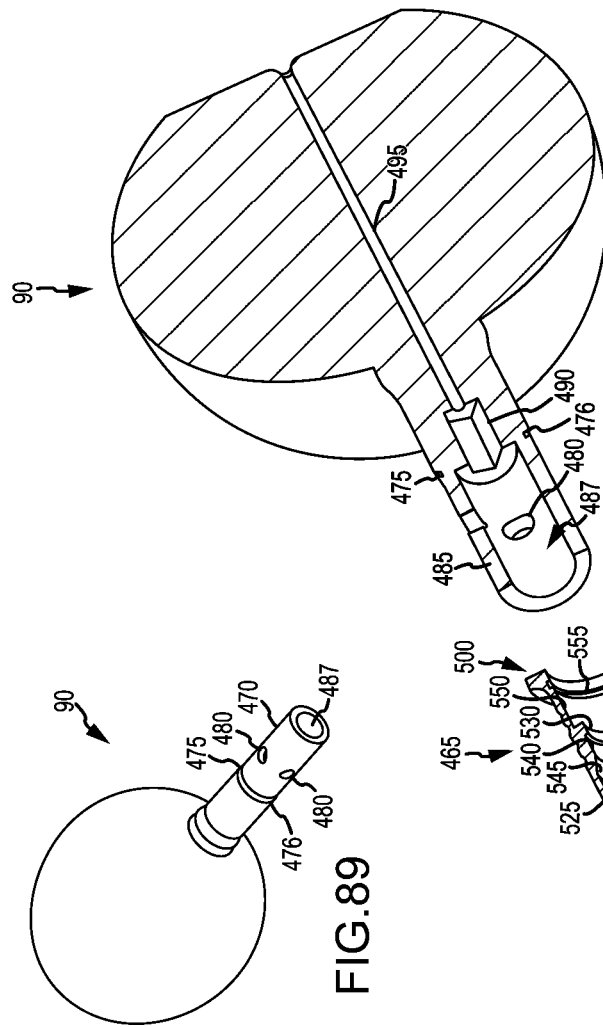


FIG.88



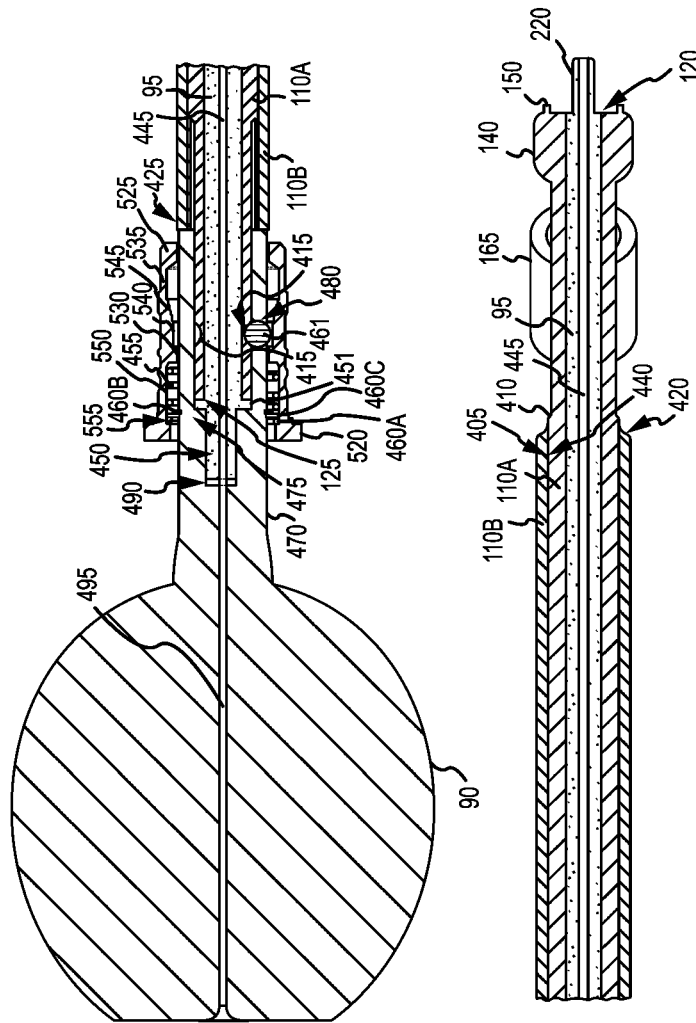


FIG. 91

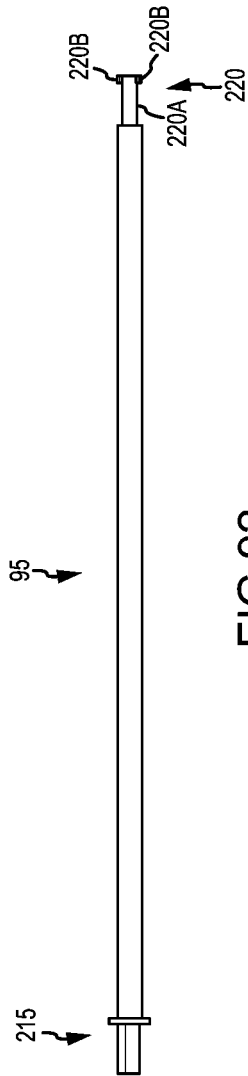


FIG. 92

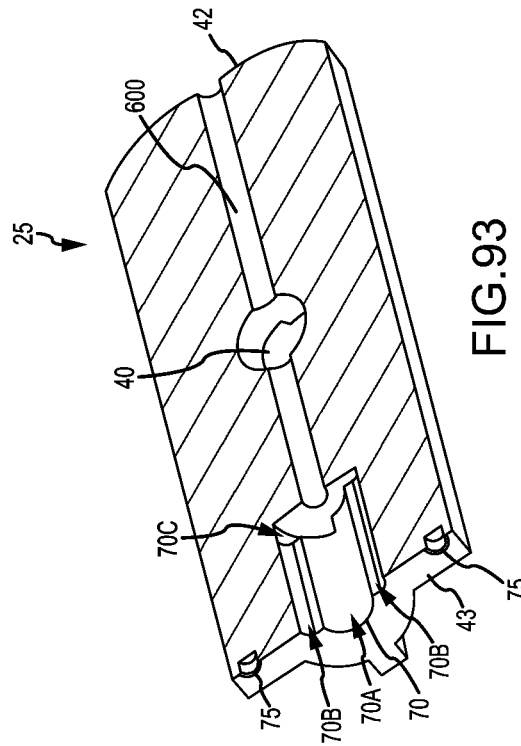


FIG. 93

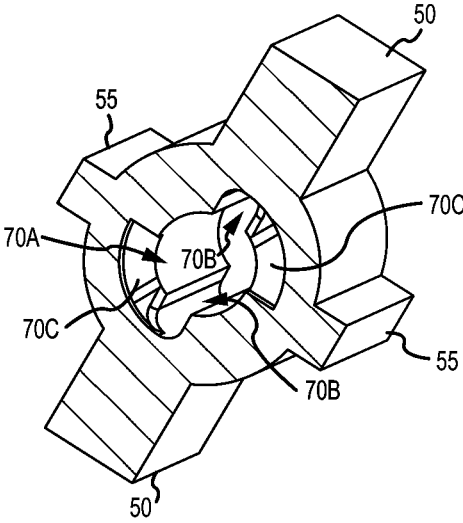


FIG.94

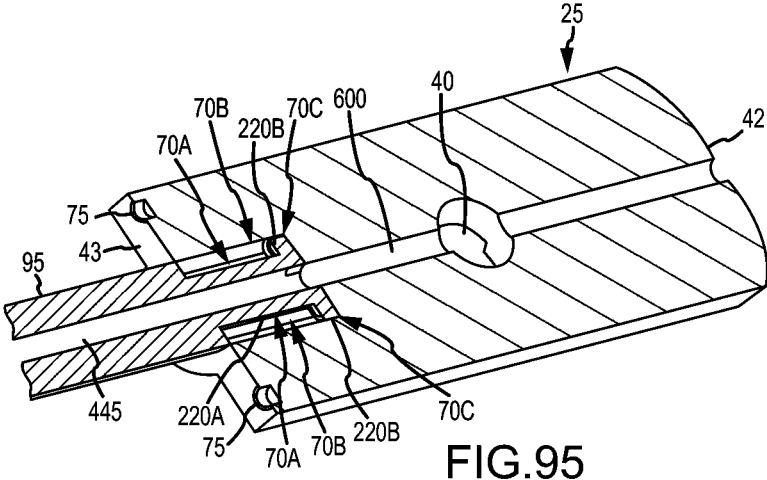


FIG.95

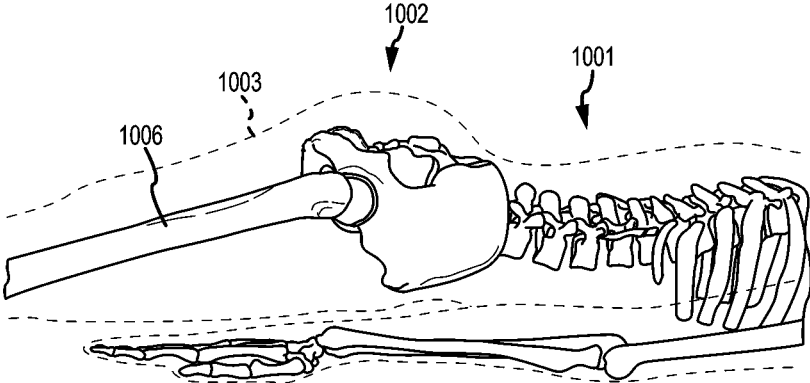


FIG.96A

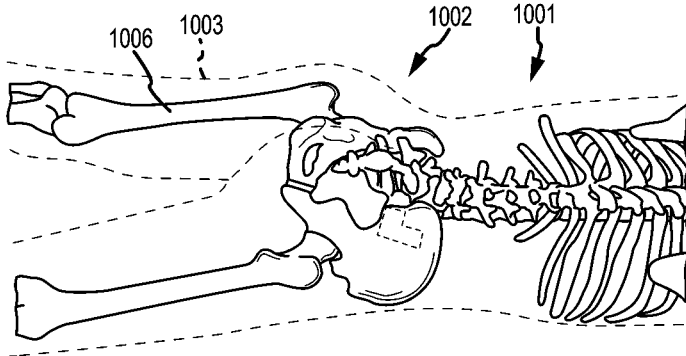


FIG.97A

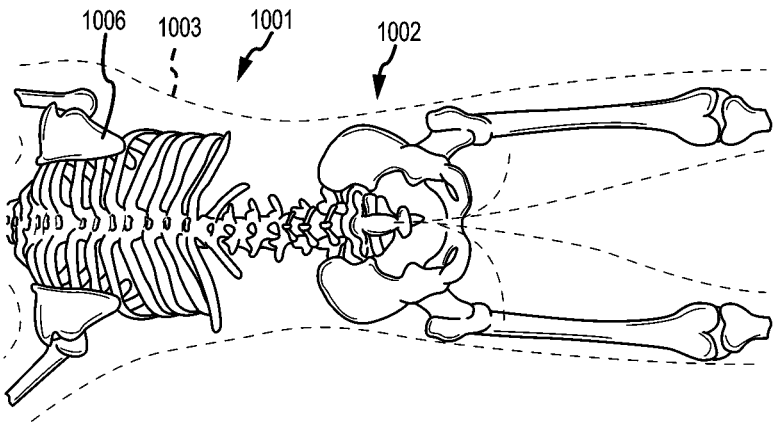


FIG.98A

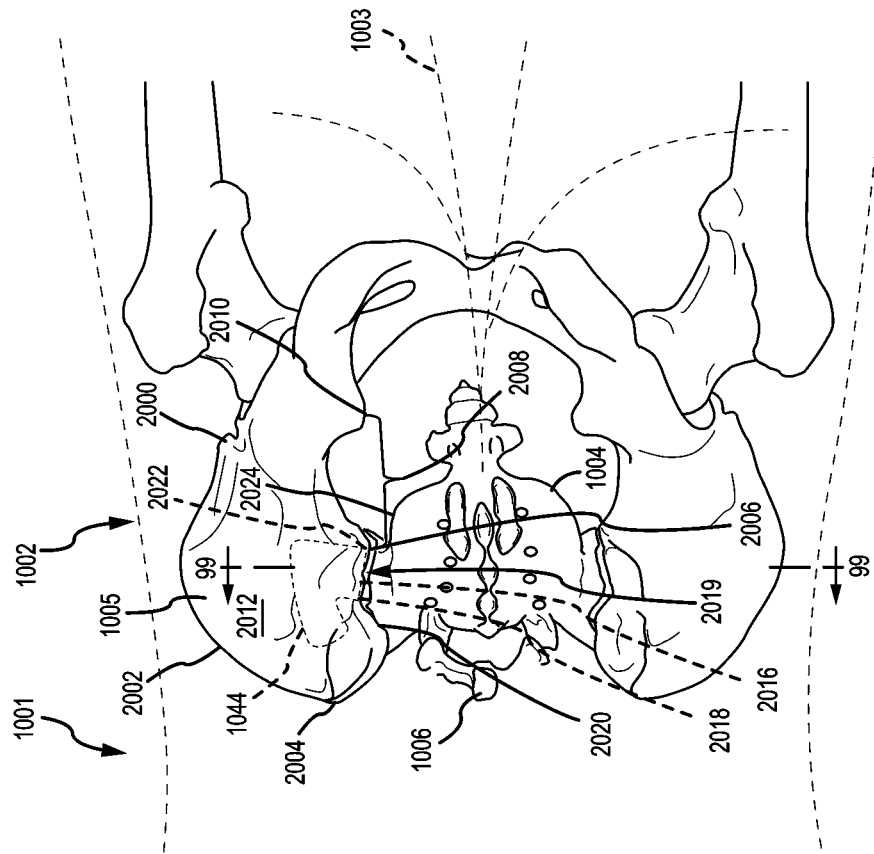


FIG. 98B

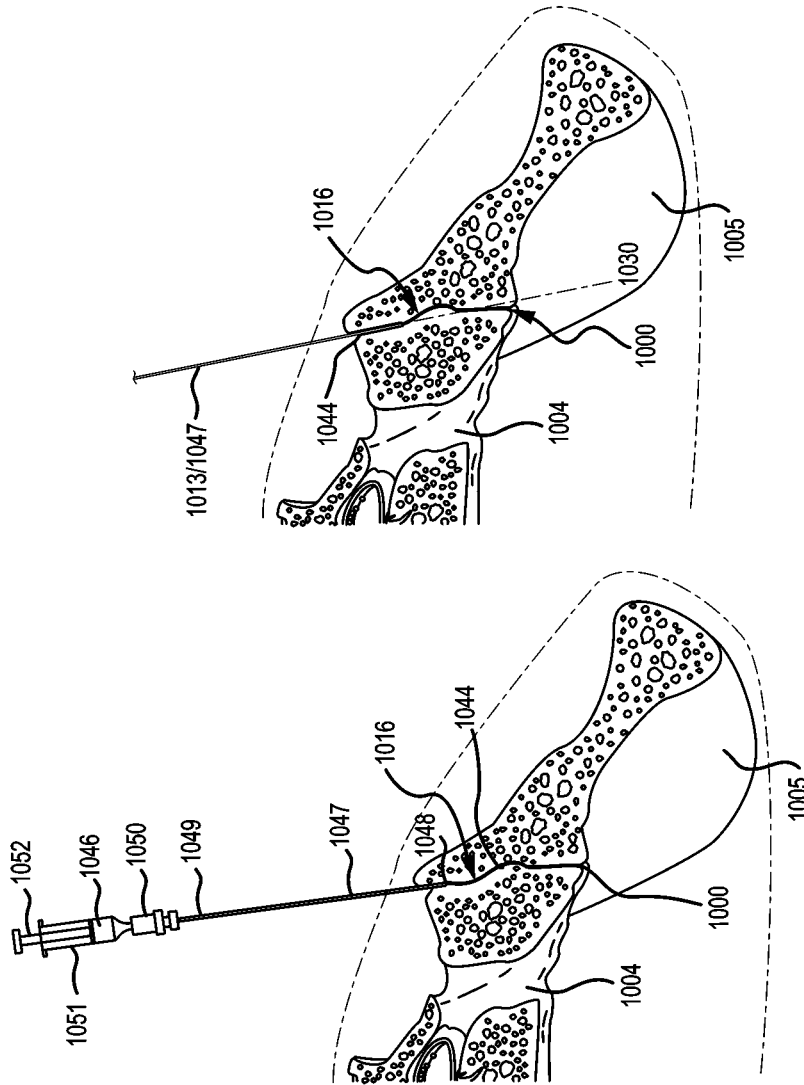


FIG. 99B

FIG. 99A

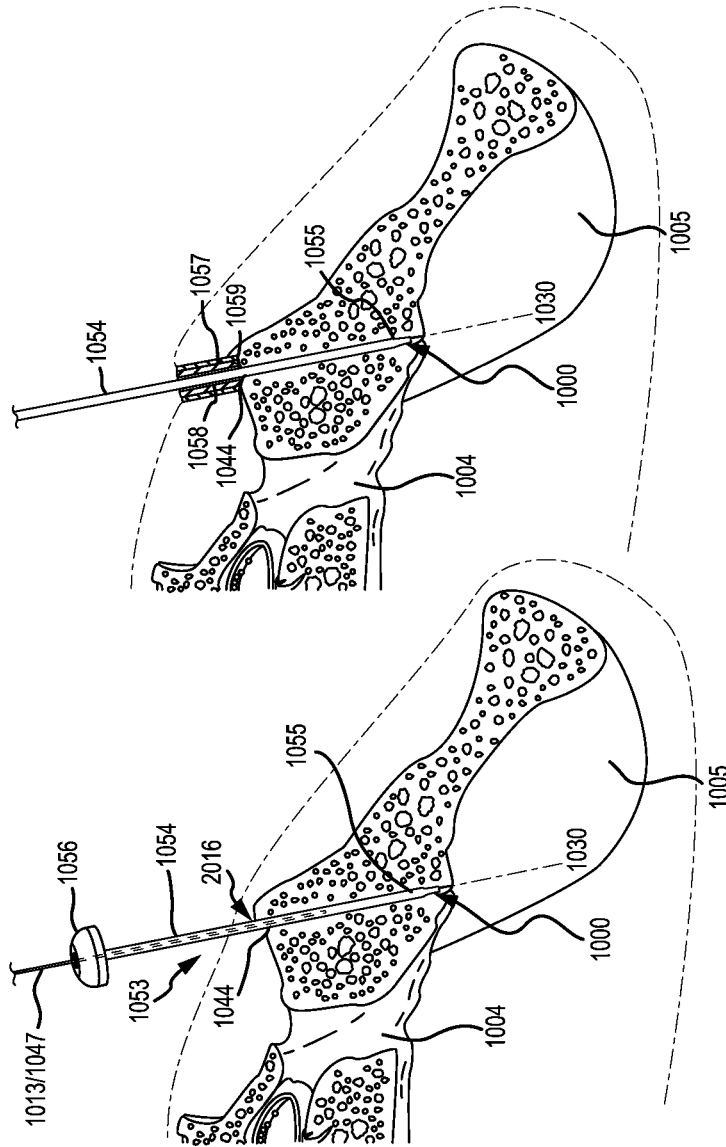


FIG. 99D

FIG. 99C

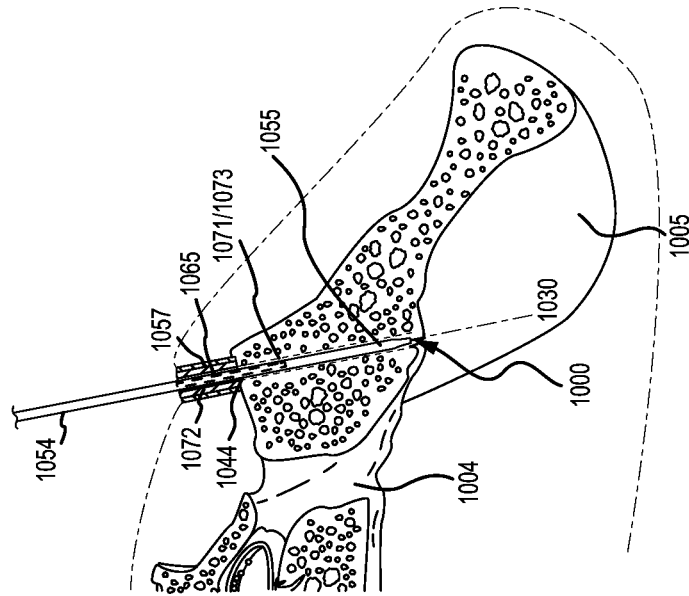


FIG. 99E

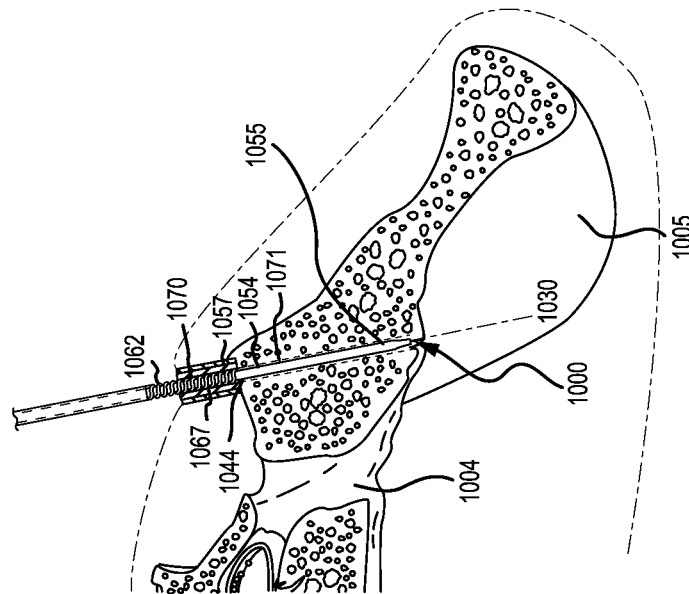


FIG. 99F

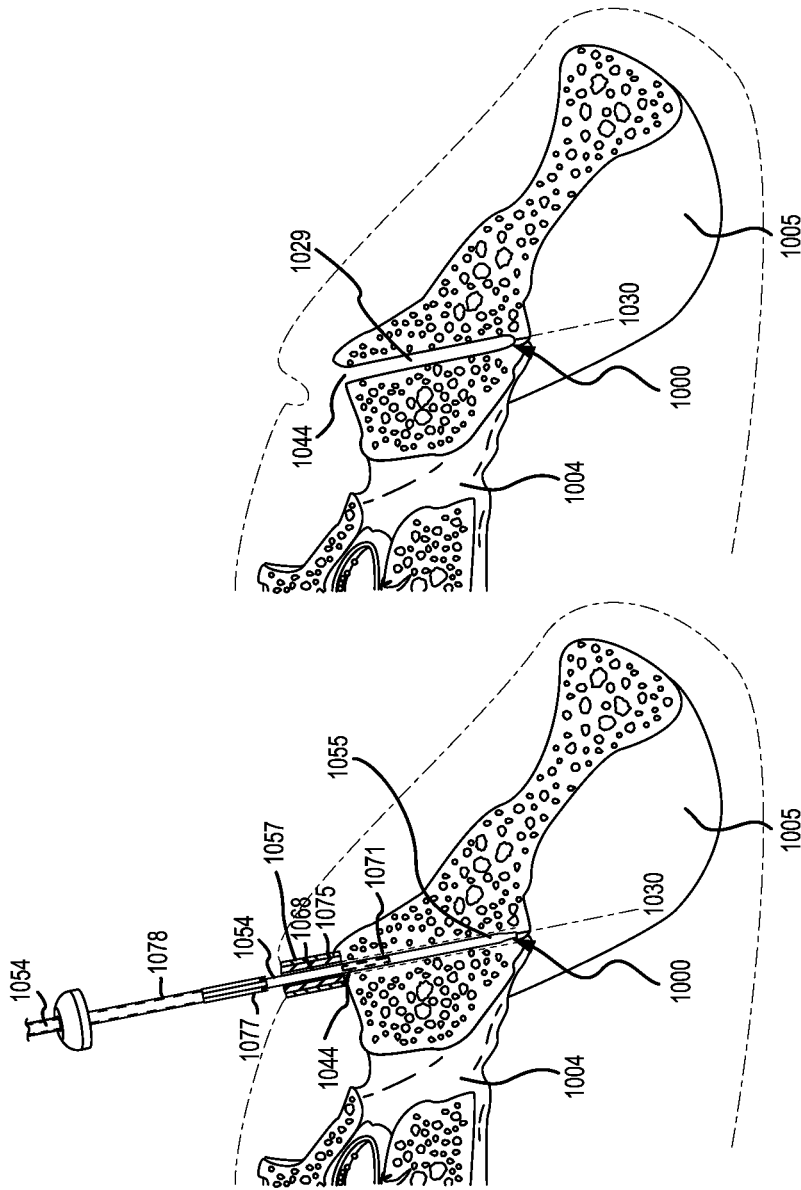


FIG. 99H

FIG. 99G

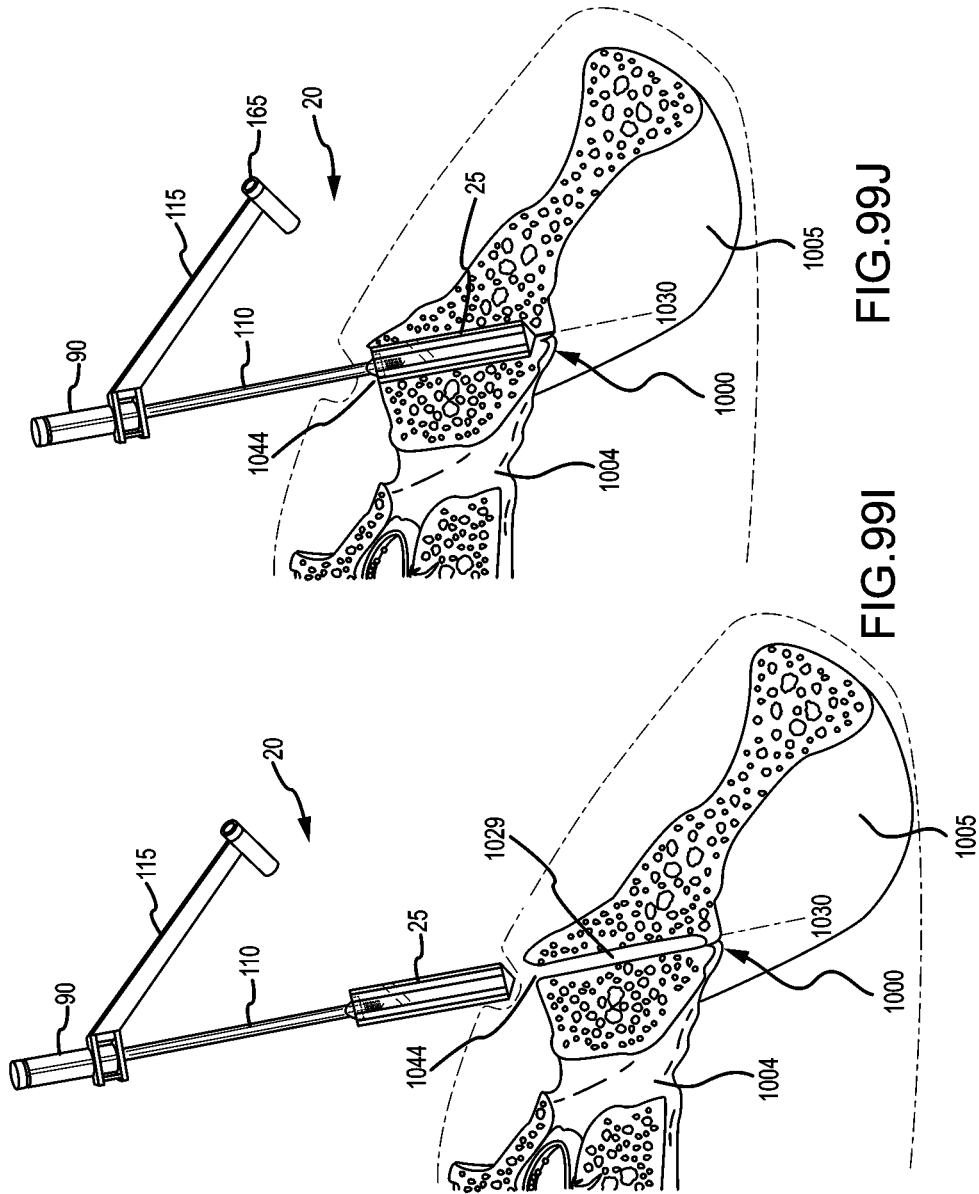


FIG. 99J

FIG. 99I

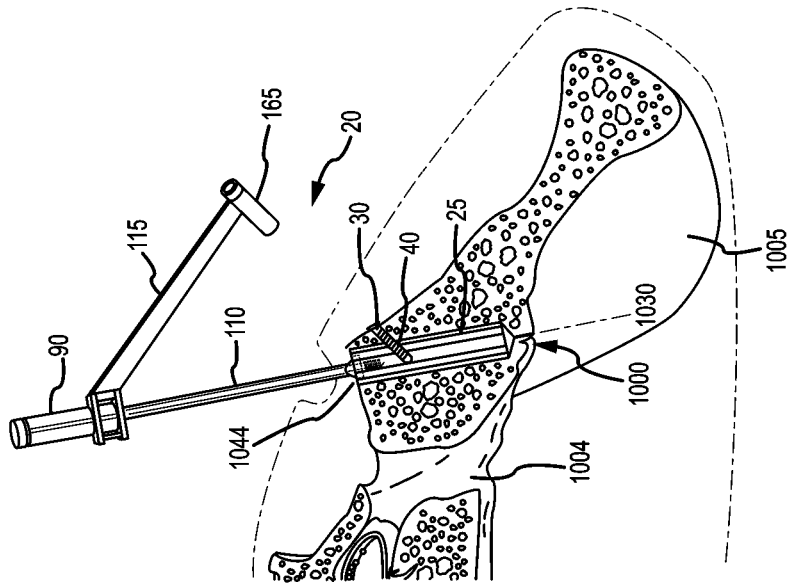


FIG. 99N

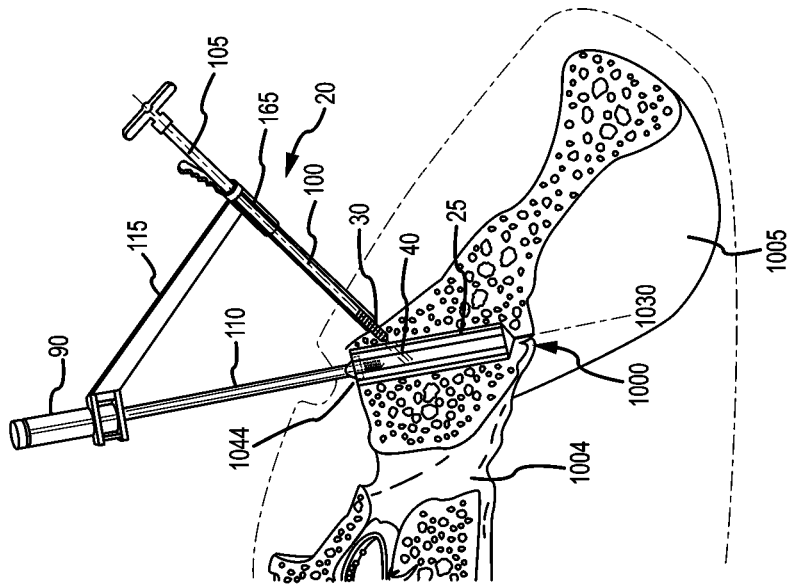


FIG. 99M

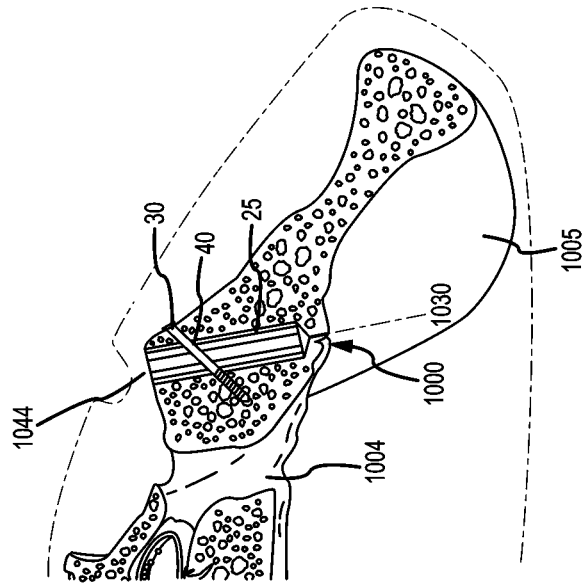


FIG. 99P

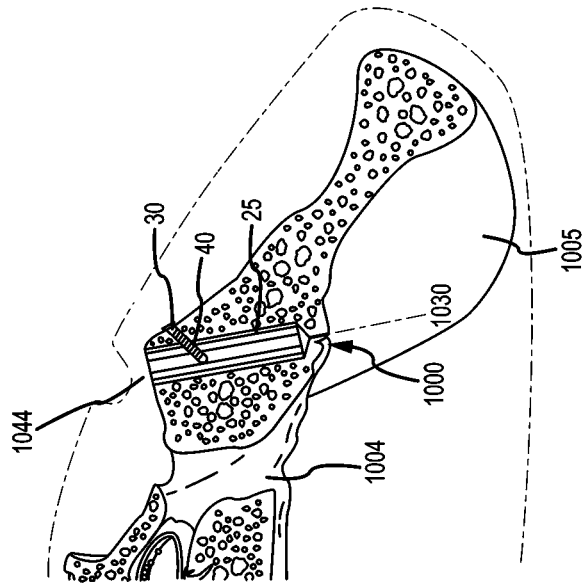


FIG. 99O

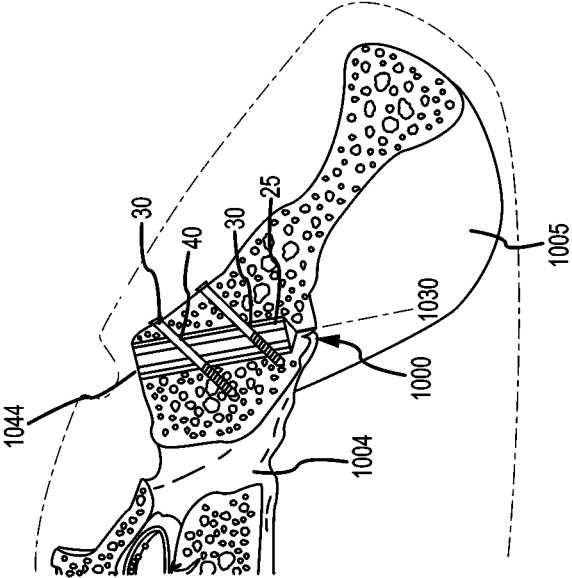


FIG. 99Q

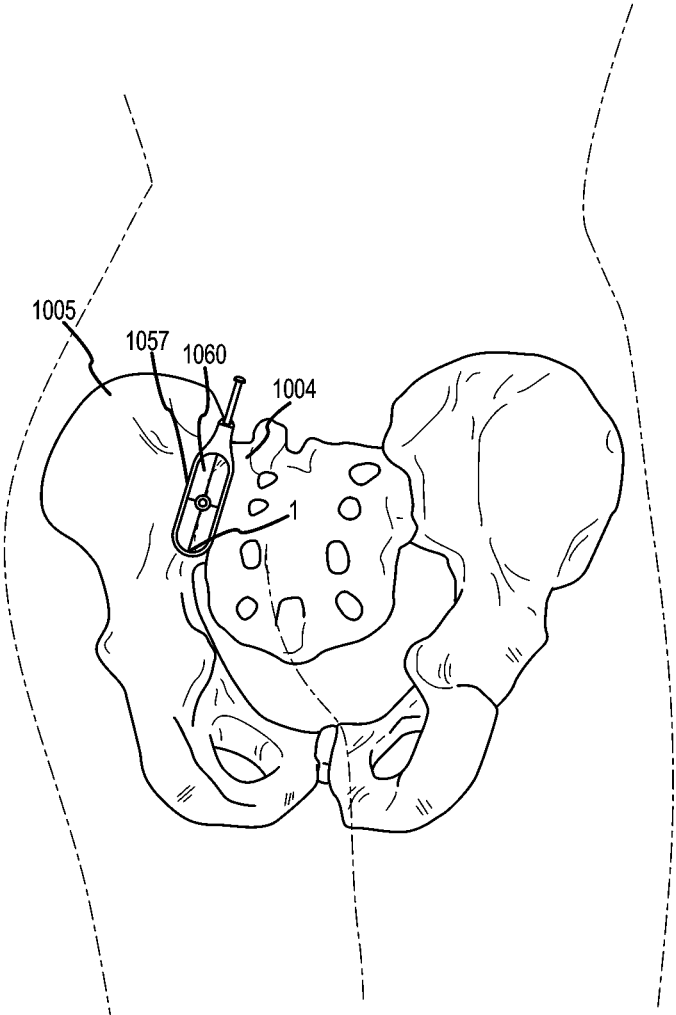


FIG.100A

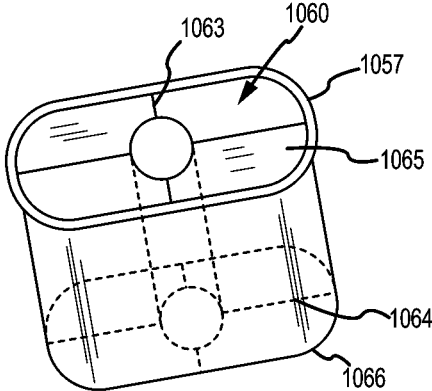


FIG.100B

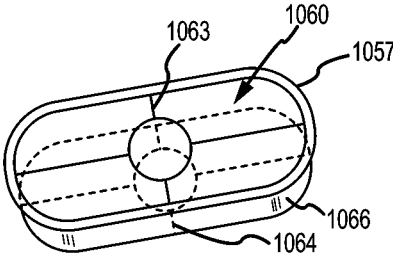


FIG.100C

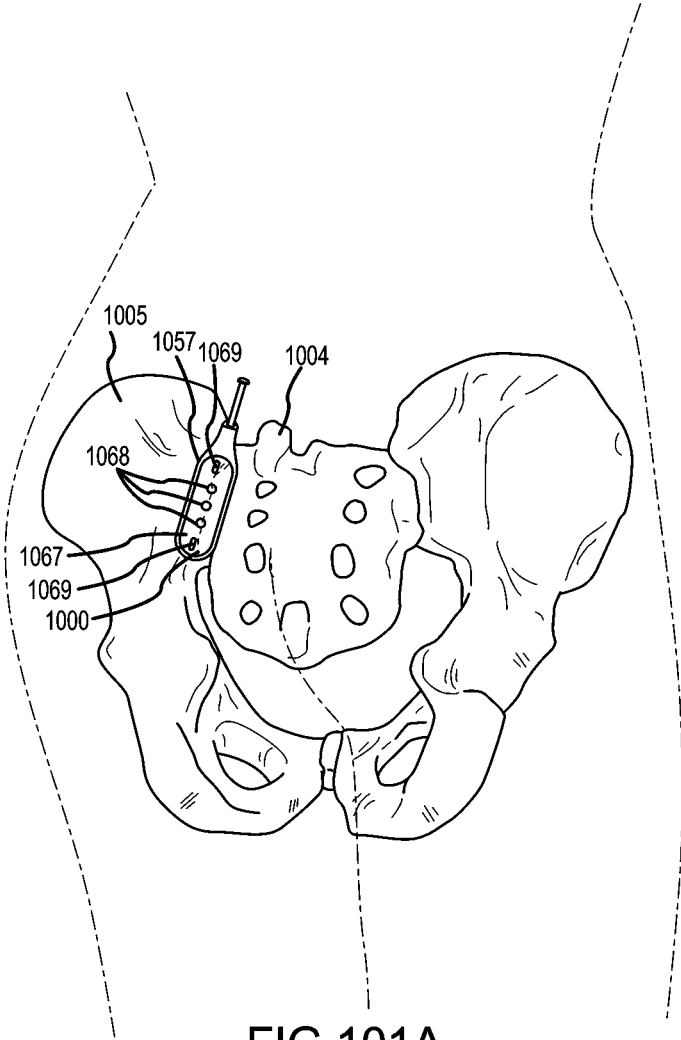


FIG. 101A

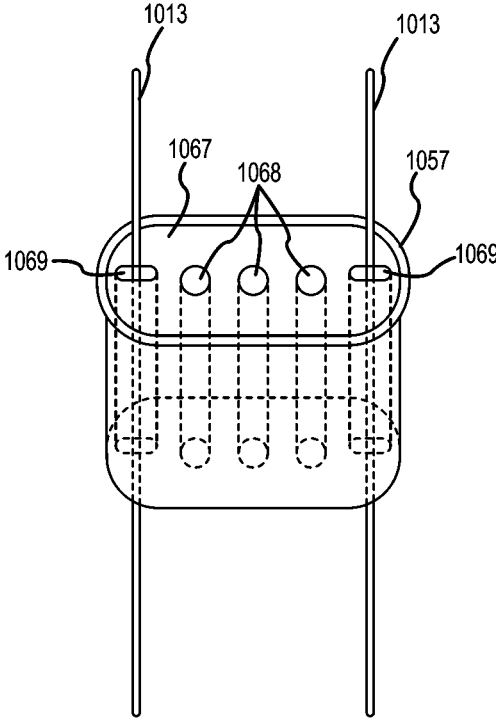


FIG.101B

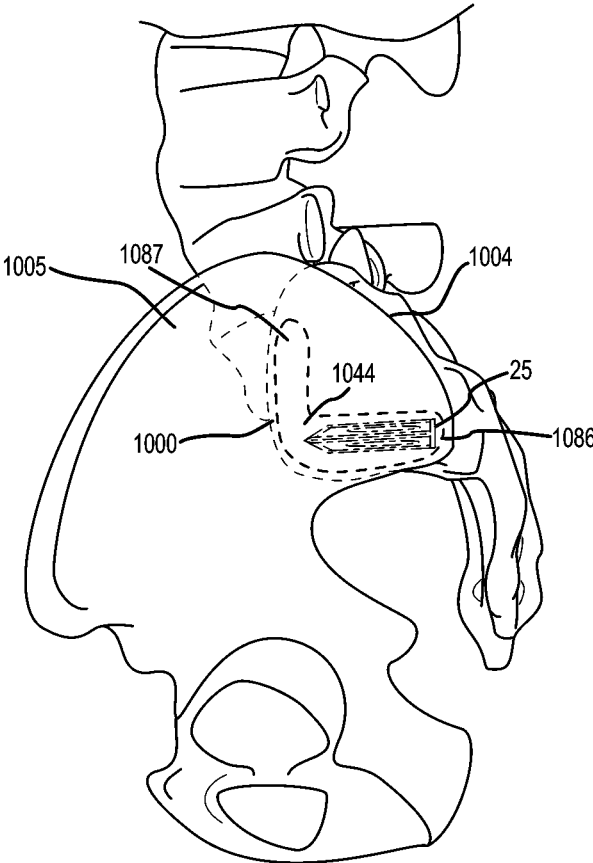


FIG.102A

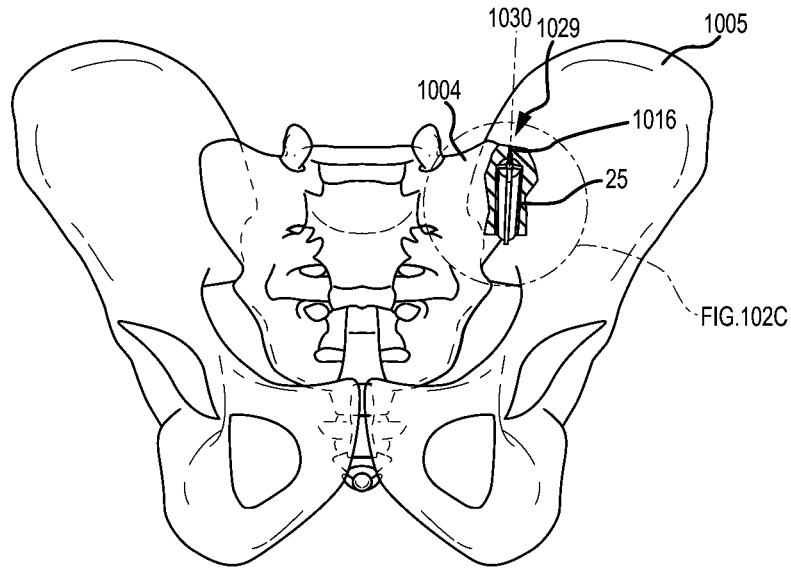


FIG. 102B

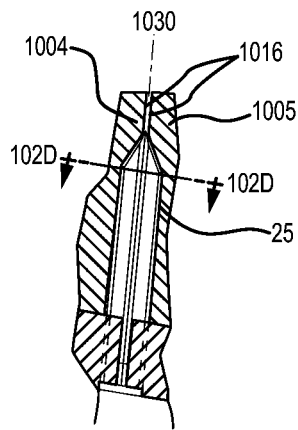


FIG. 102C

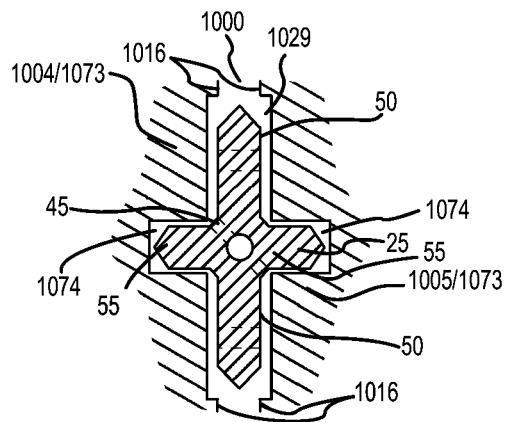


FIG. 102D

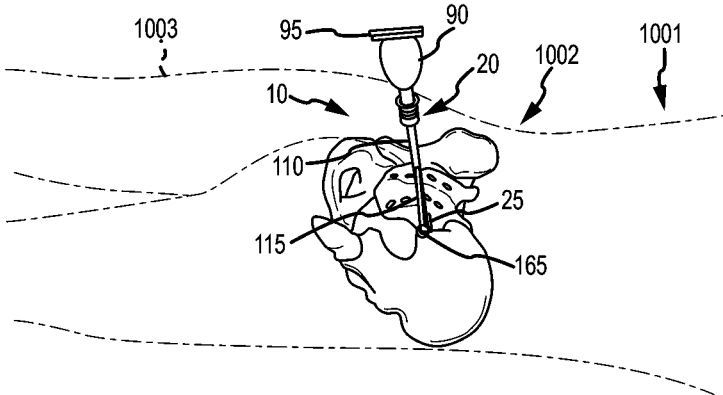


FIG.103A

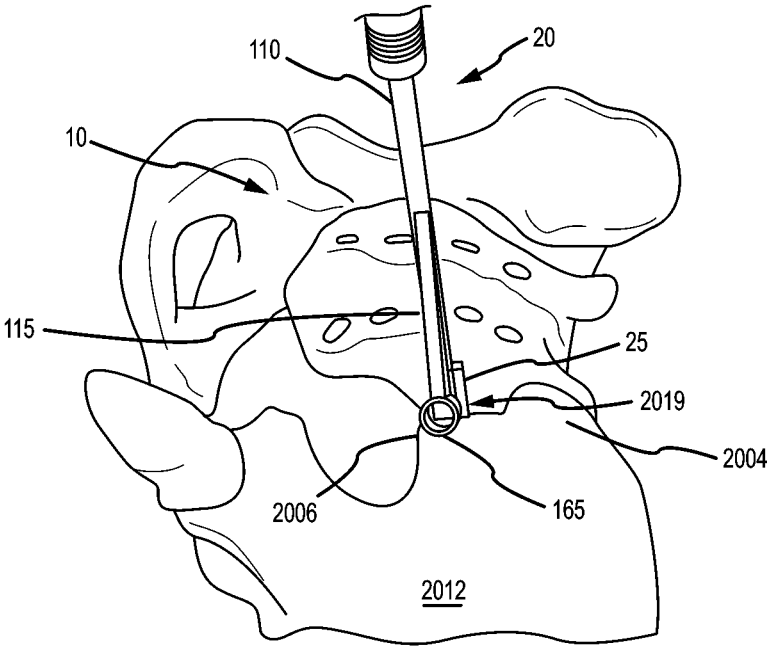
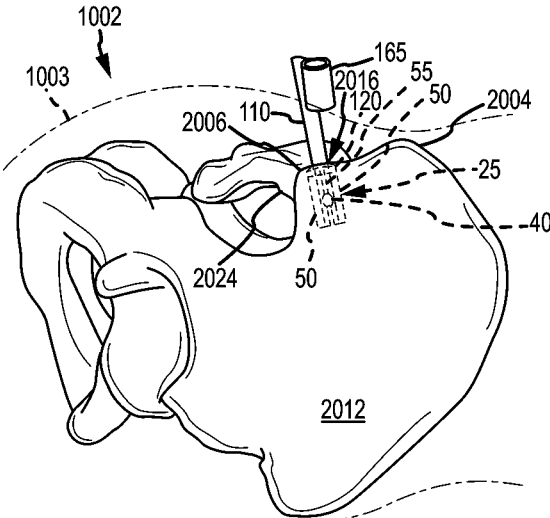
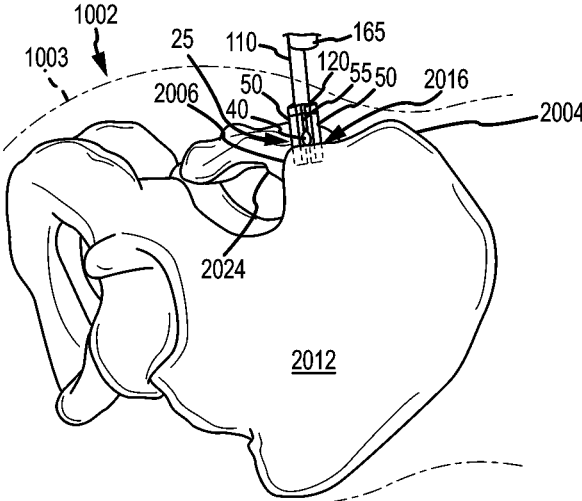


FIG.103B



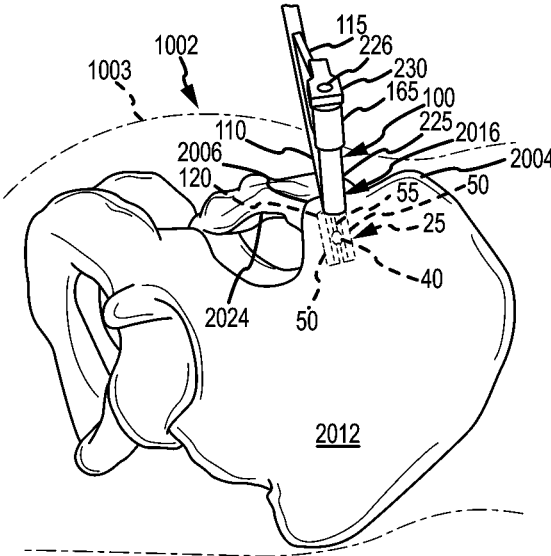


FIG.106A

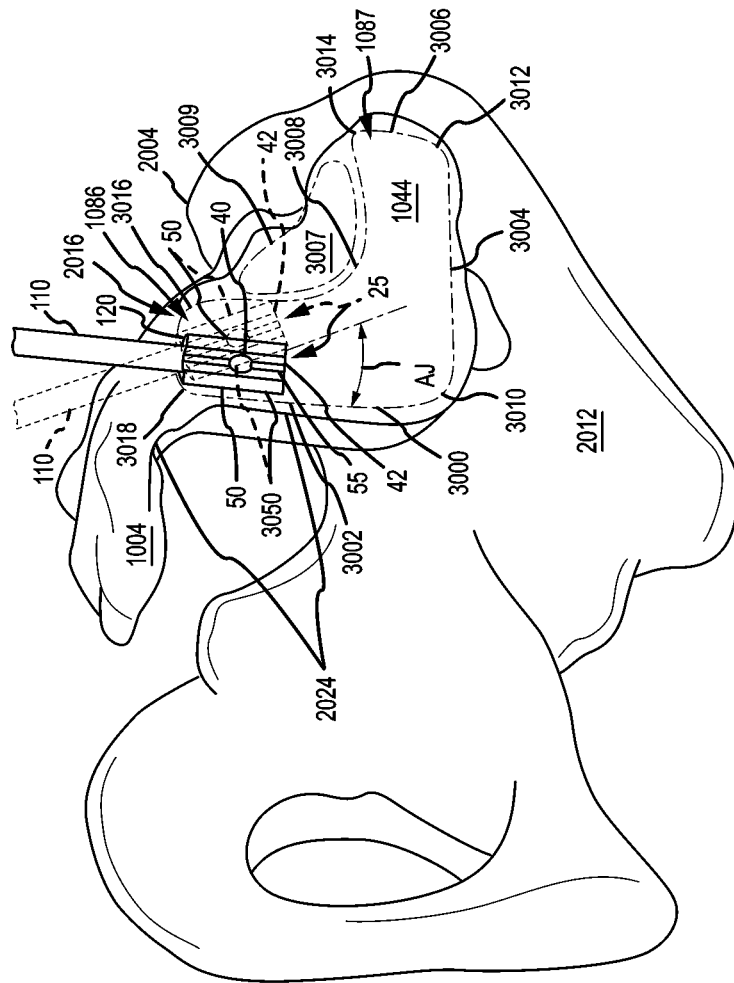


FIG. 106B

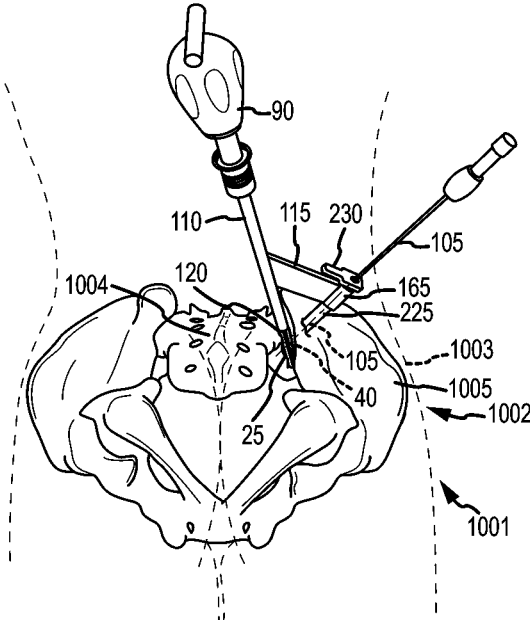


FIG. 107A

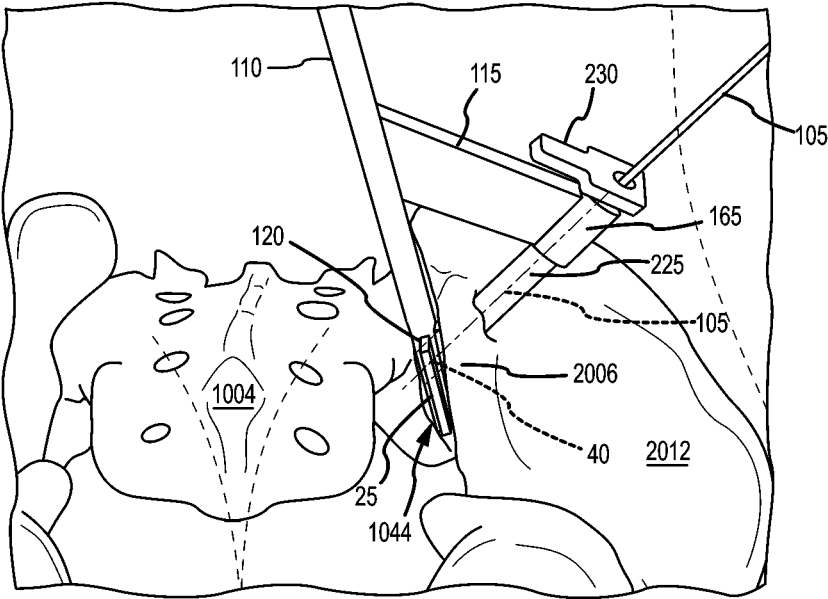


FIG.107B

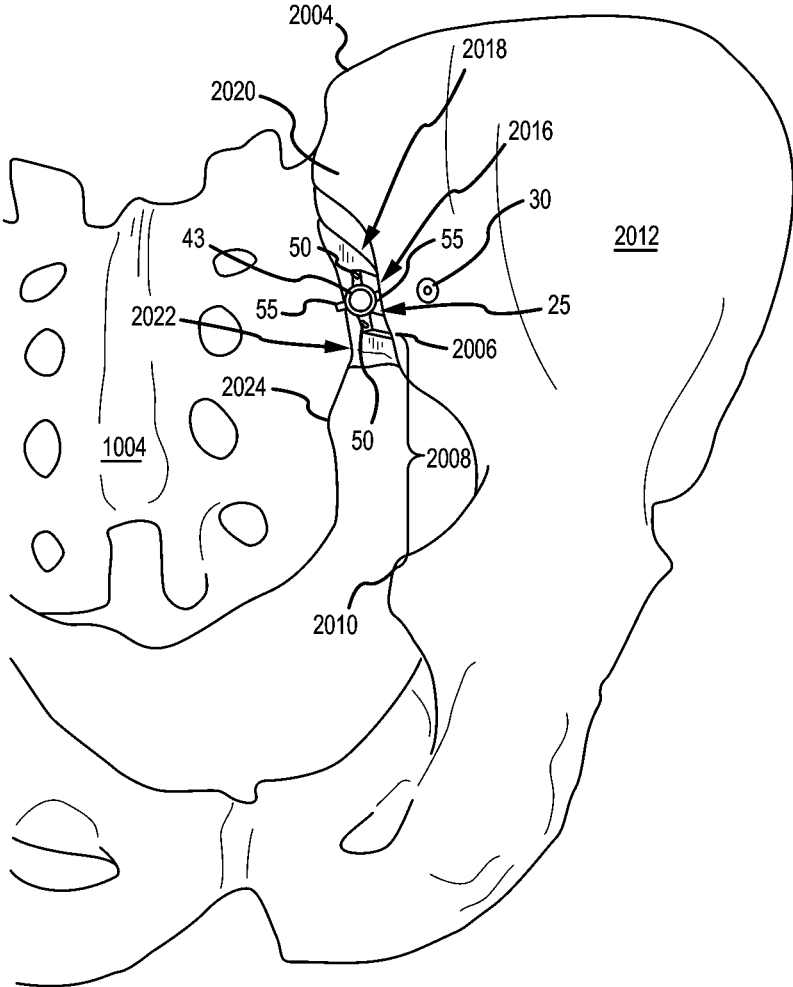


FIG.108A

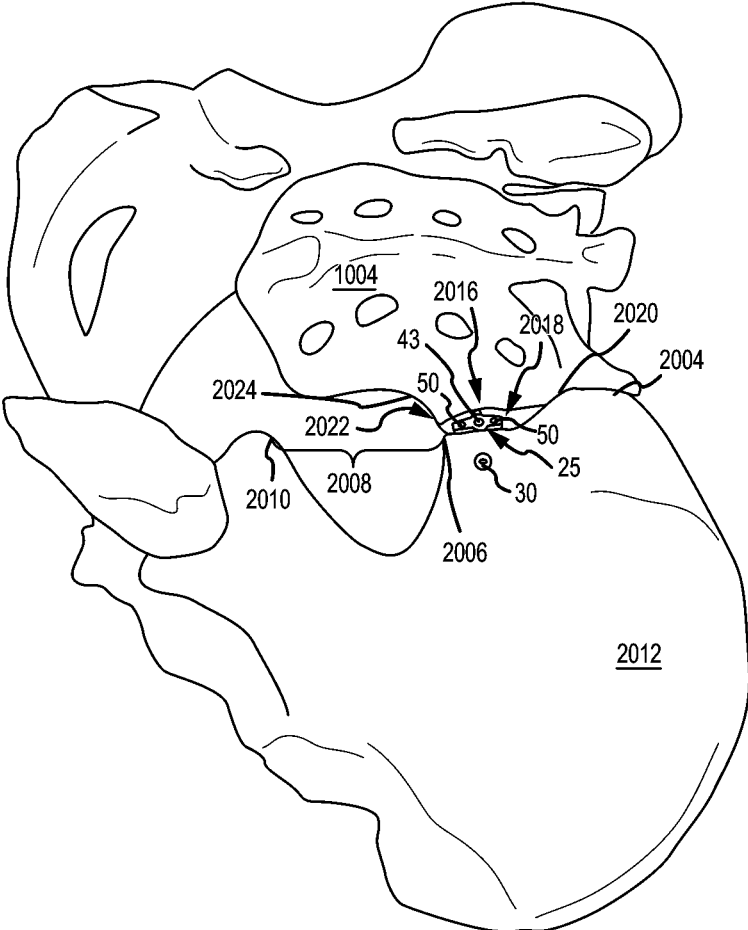


FIG.108B

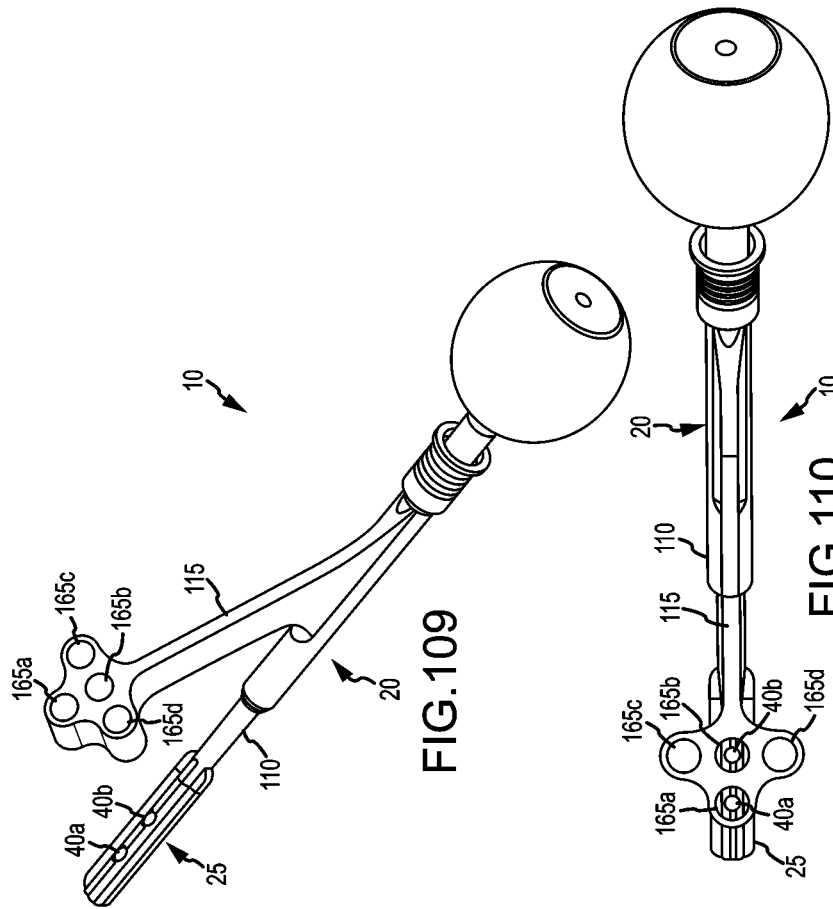


FIG. 109

FIG. 110

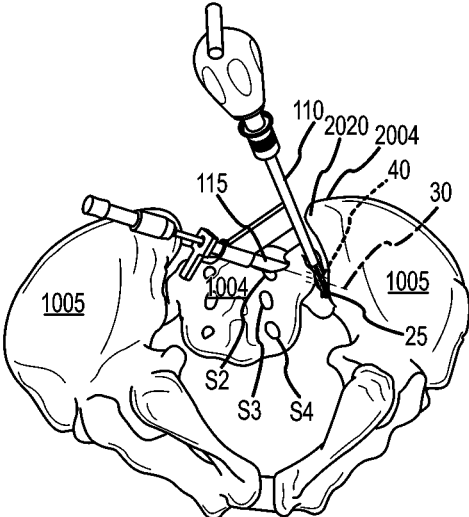


FIG.111A

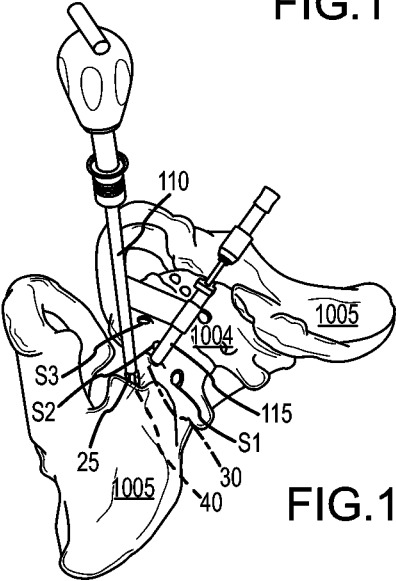


FIG.111B

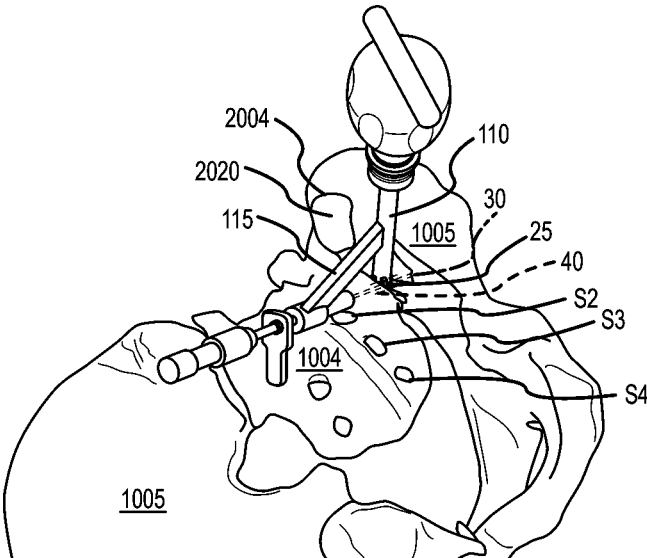


FIG.111C

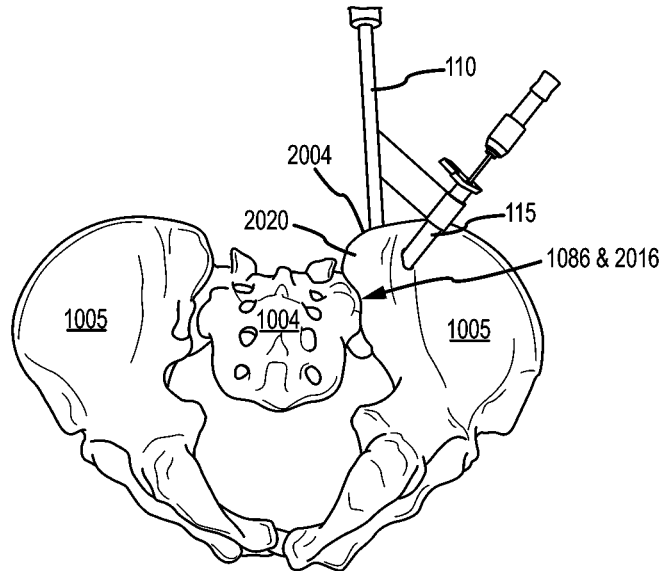


FIG. 112A

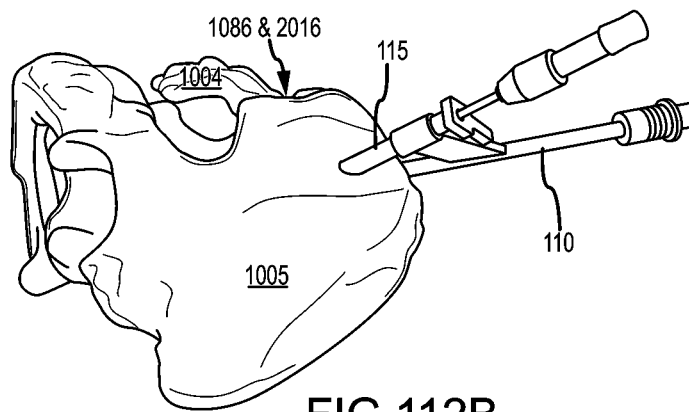


FIG. 112B

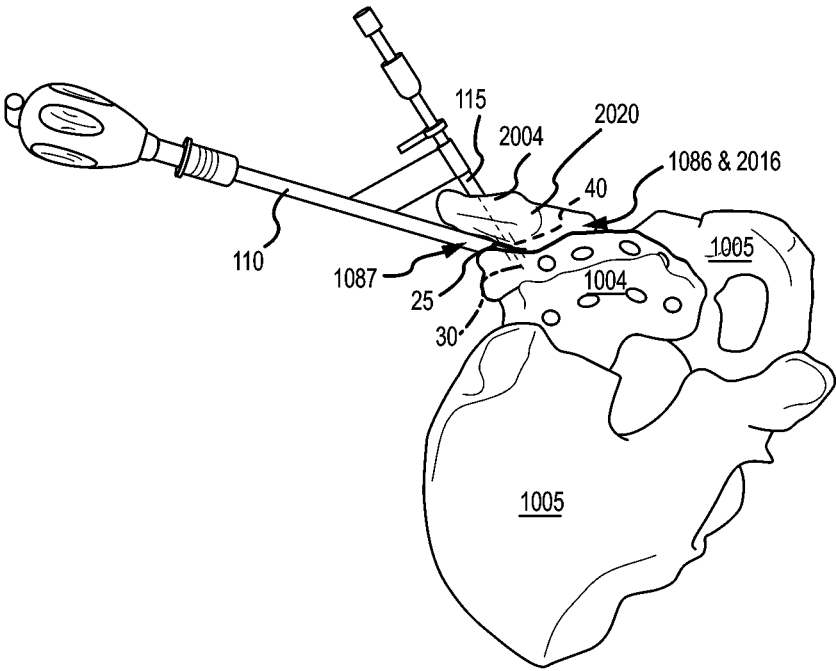


FIG.112C

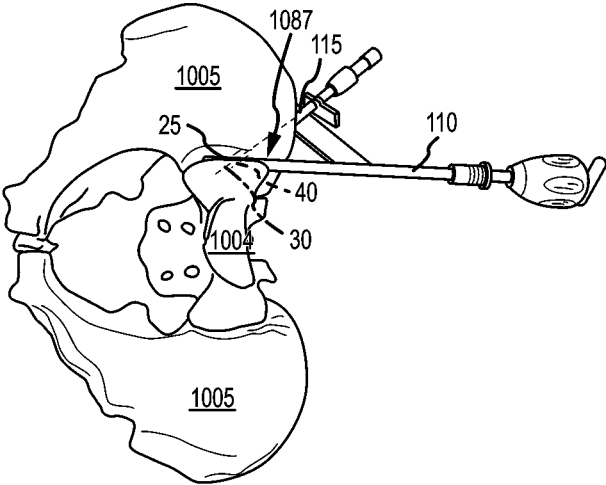
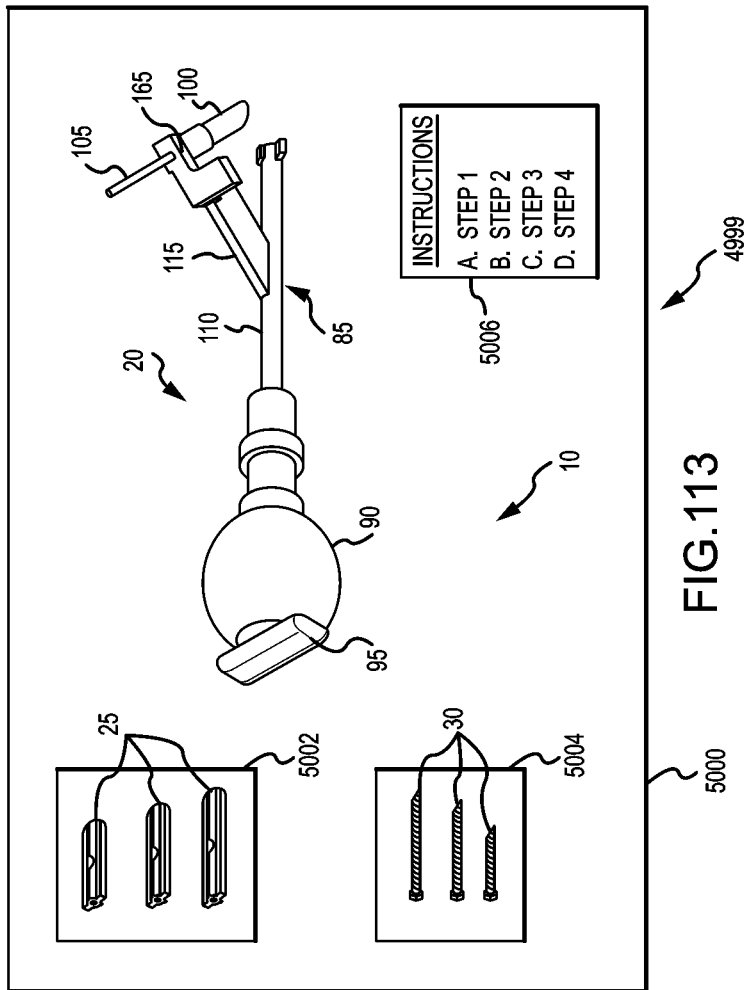


FIG.112D



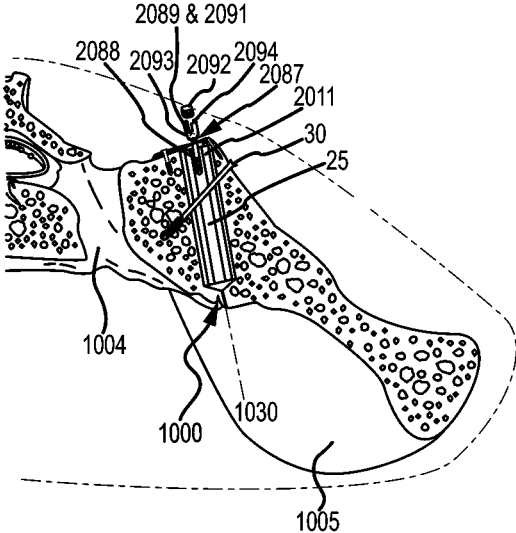


FIG.114

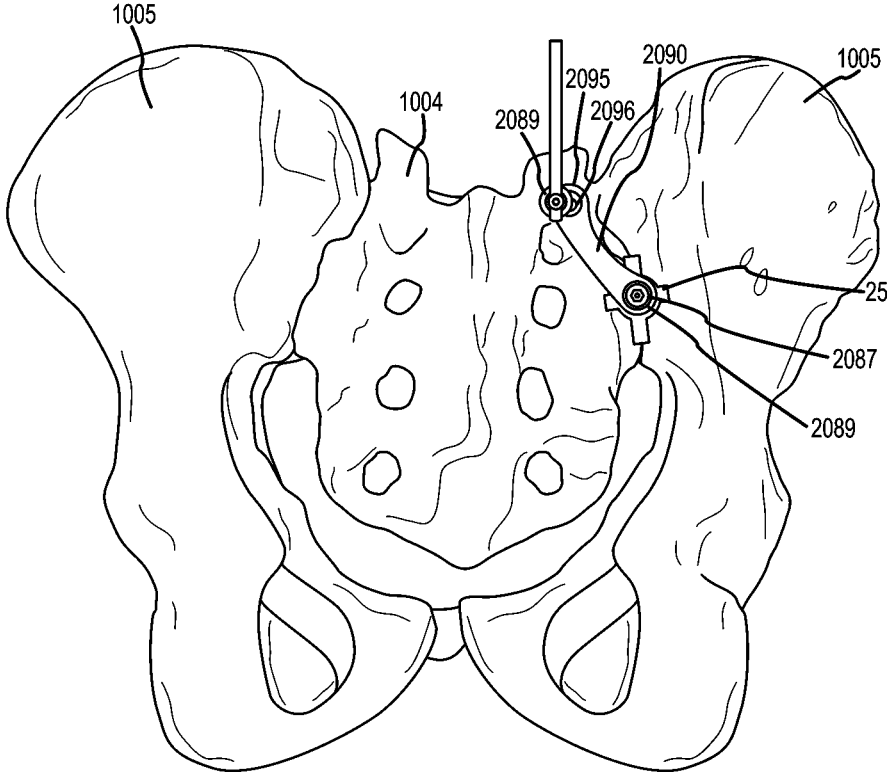


FIG.116

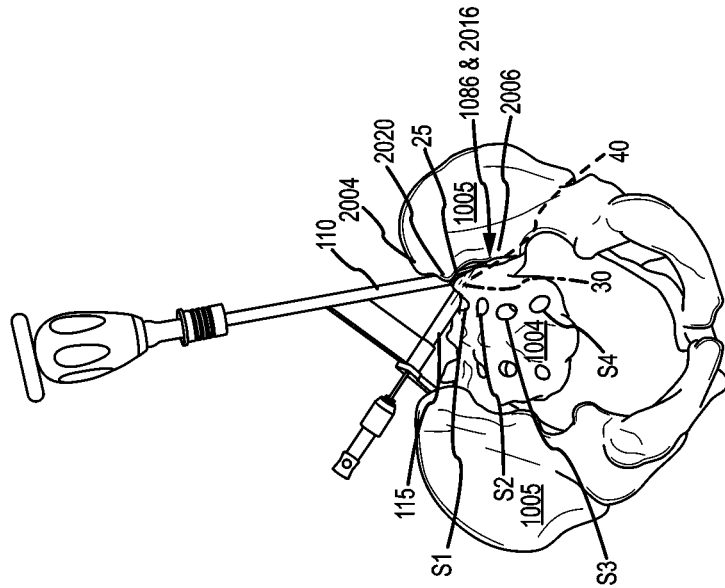


FIG. 117A

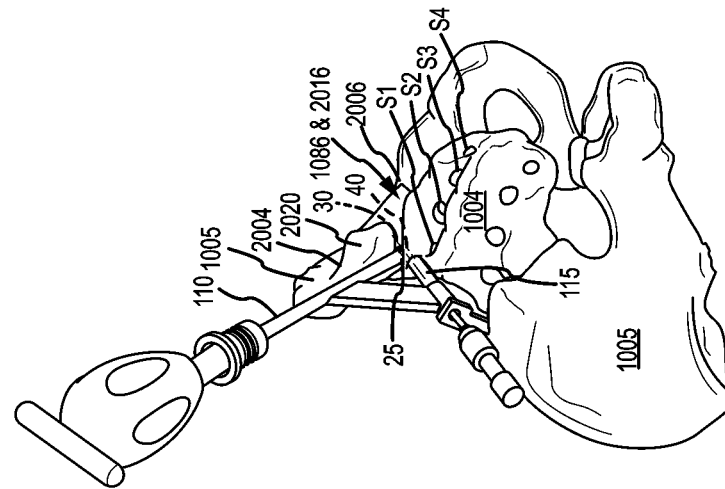


FIG. 117B

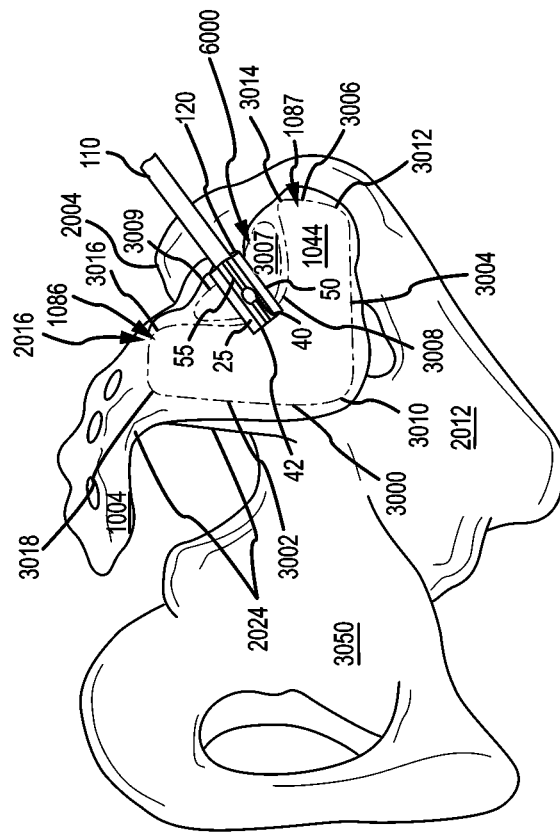


FIG.117C

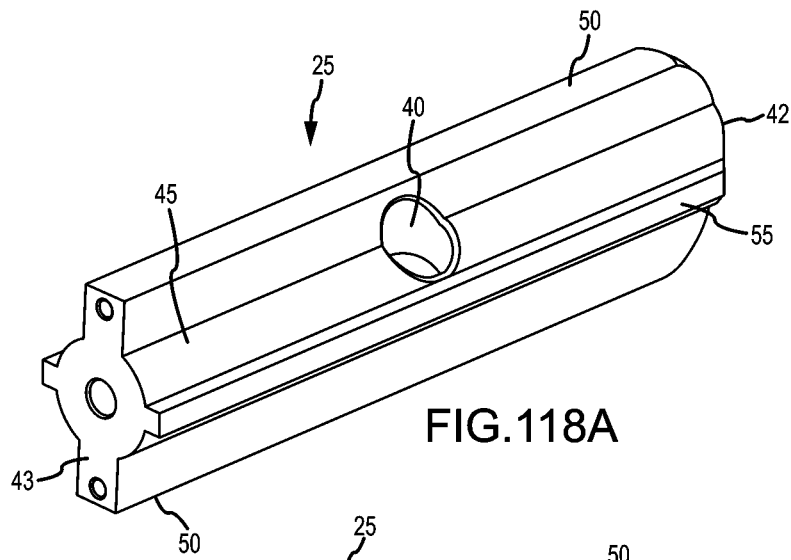


FIG. 118A

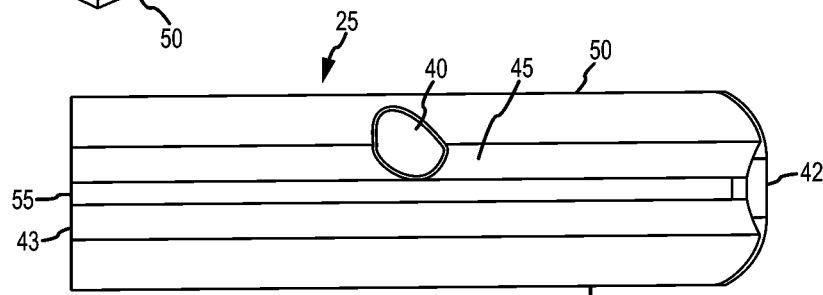


FIG. 118B

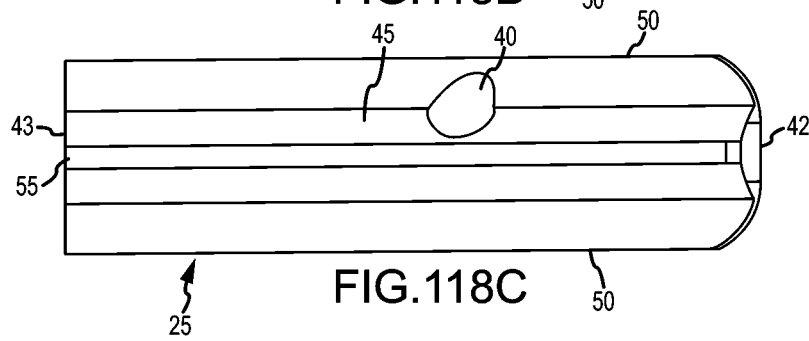


FIG. 118C

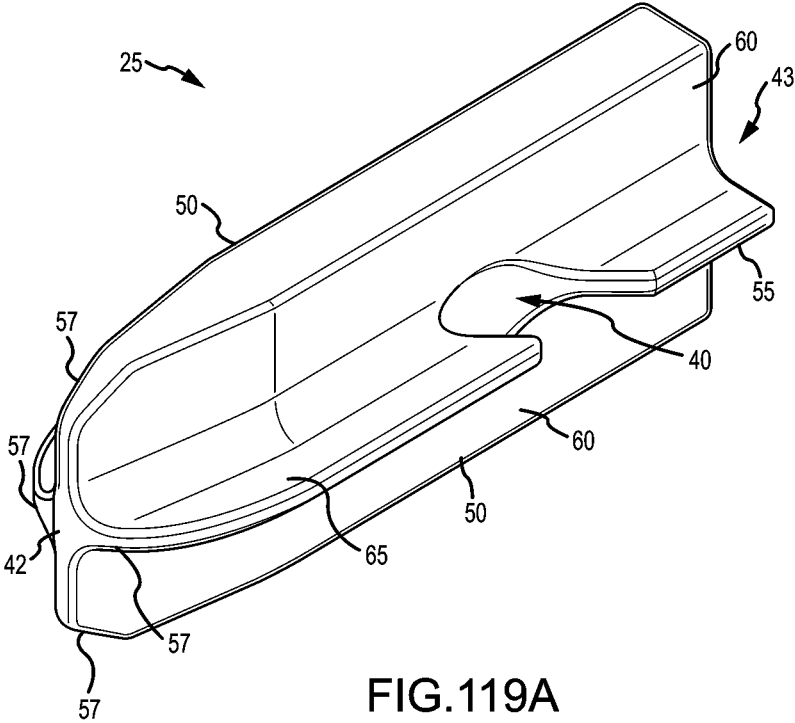


FIG. 119A

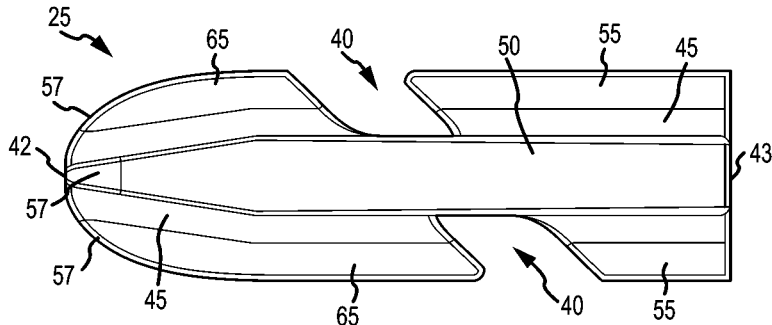


FIG. 119B

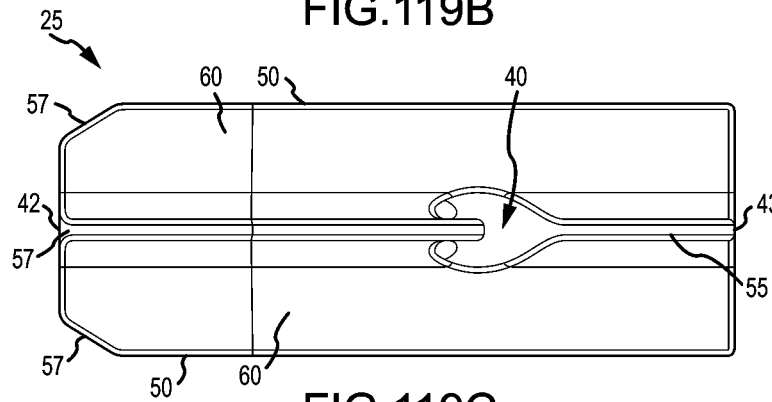


FIG. 119C

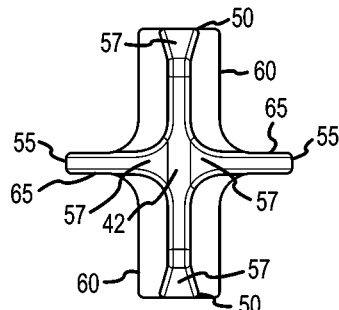


FIG. 119D

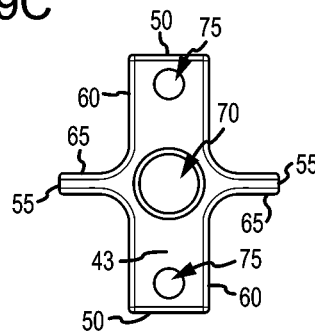
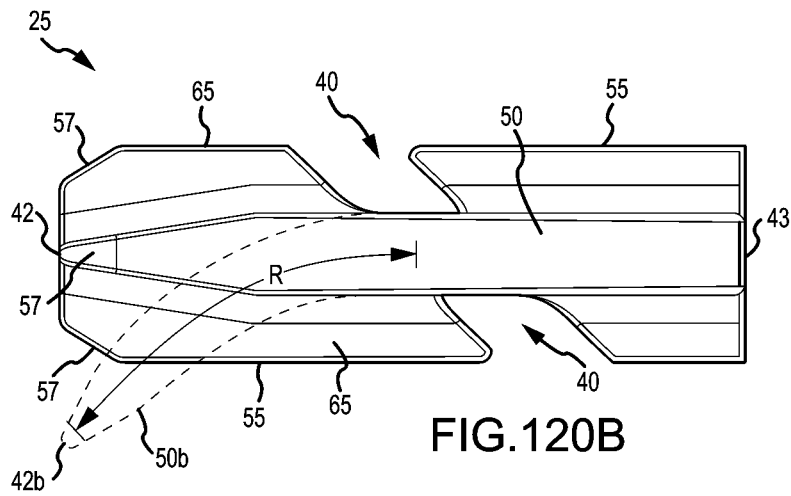
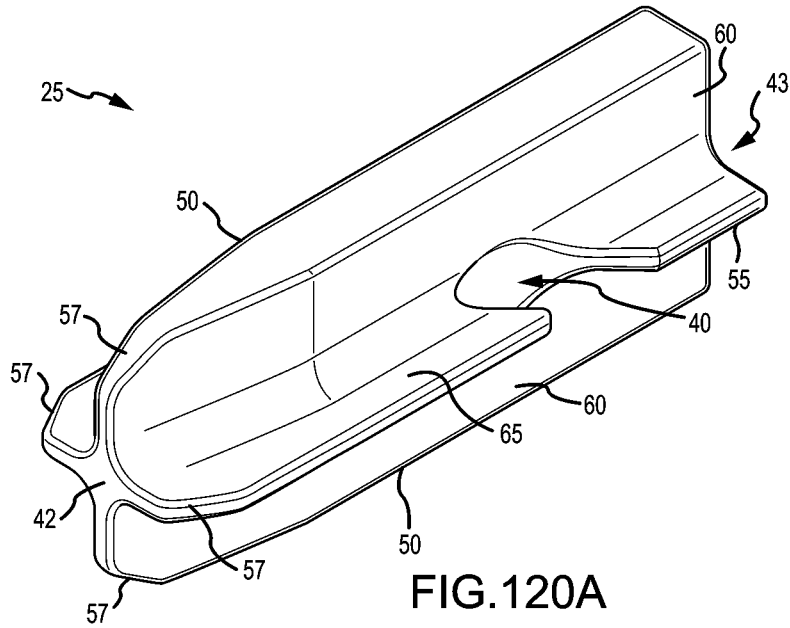


FIG. 119E



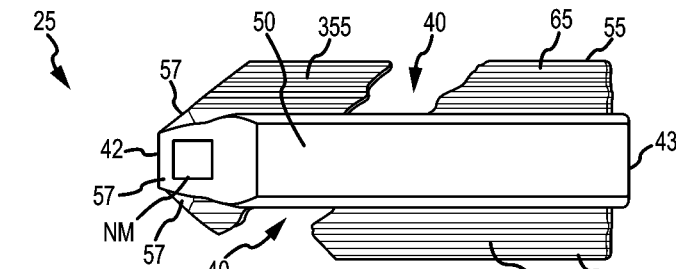


FIG. 121B

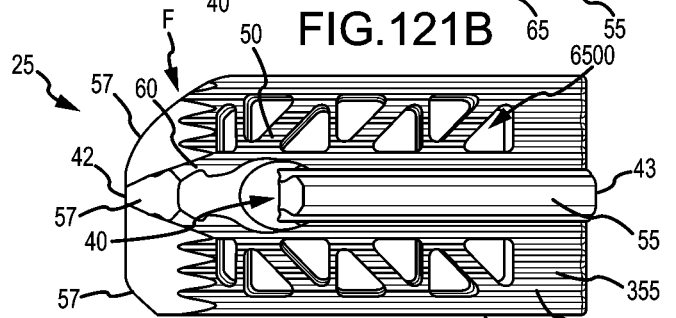


FIG. 121C

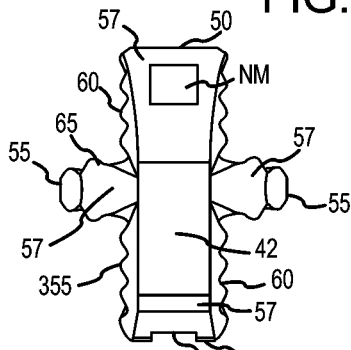


FIG. 121D

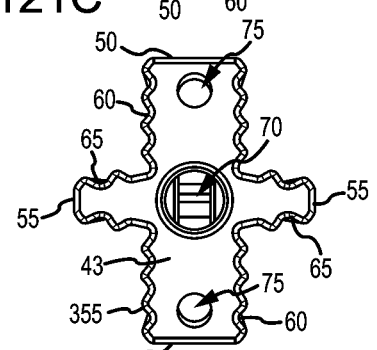


FIG. 121E

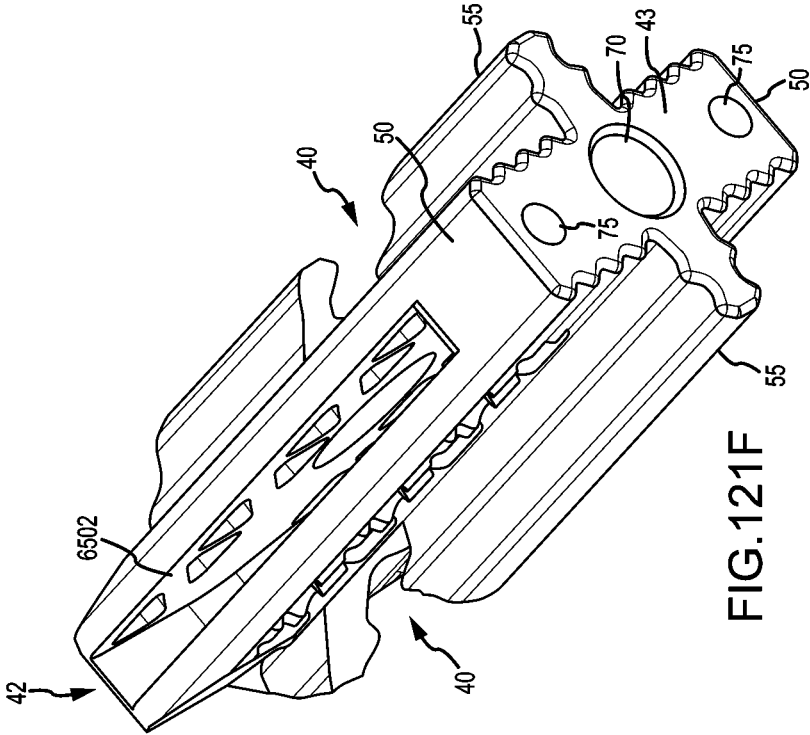


FIG. 121F

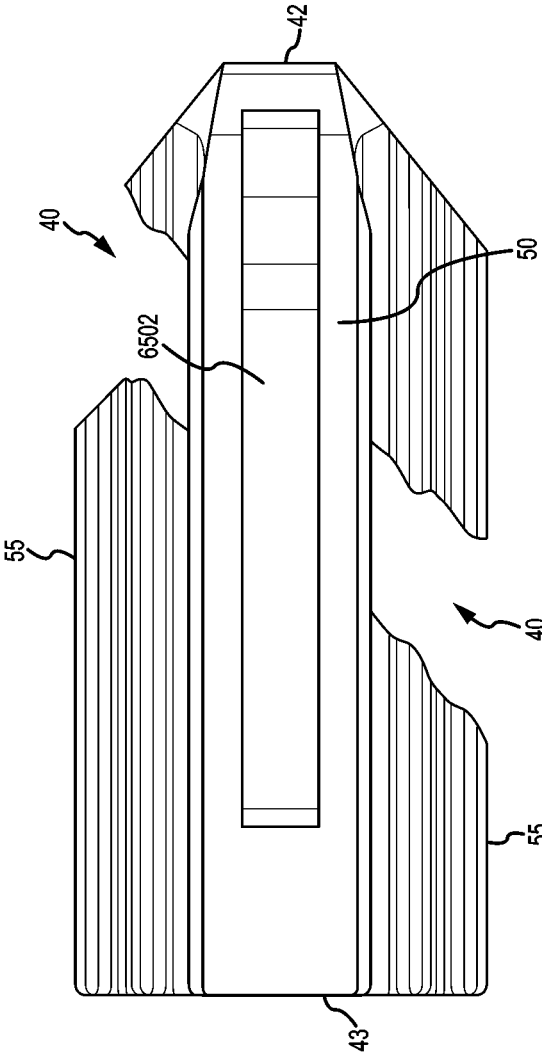


FIG.121G

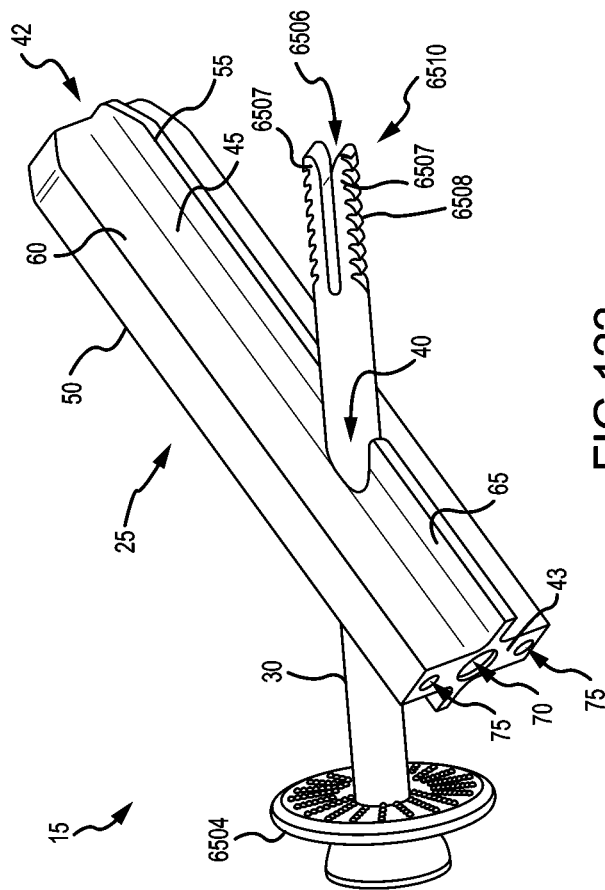


FIG. 122

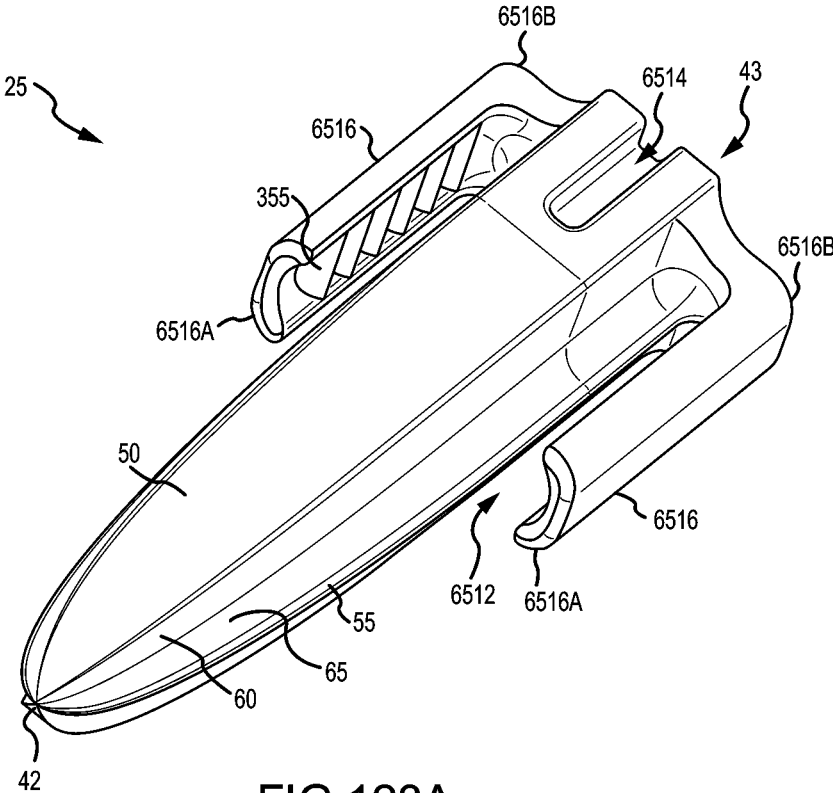


FIG. 123A

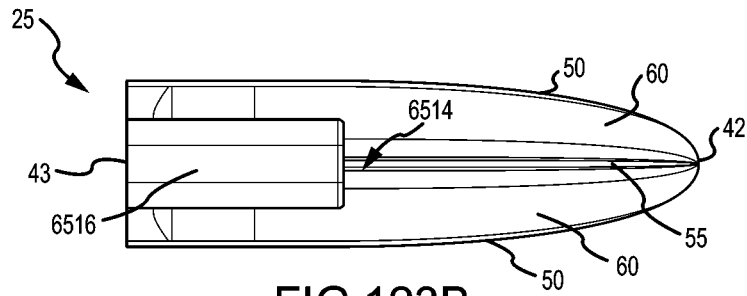


FIG. 123B

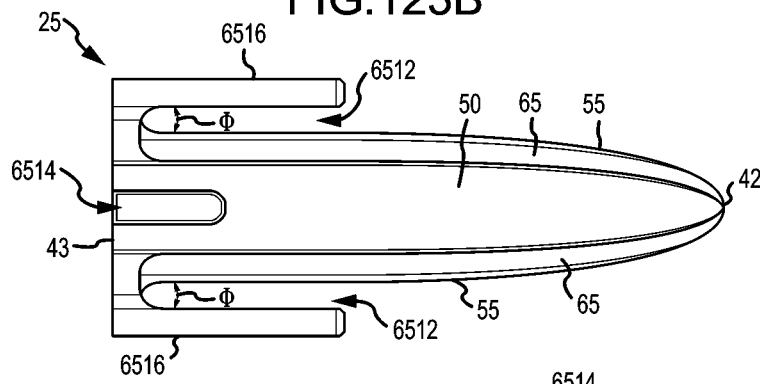


FIG. 123C

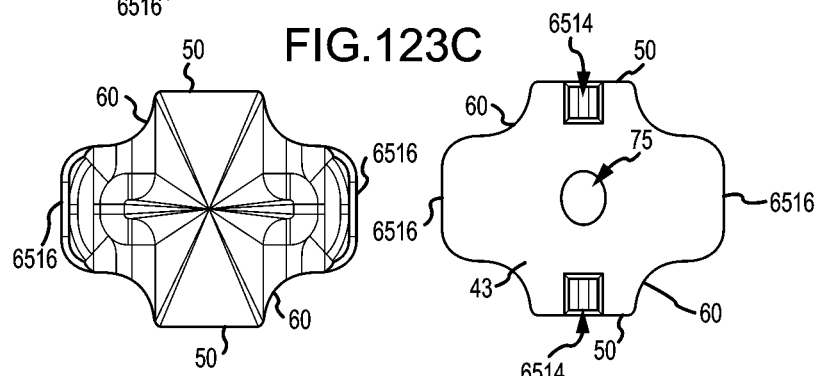


FIG. 123D

FIG. 123E

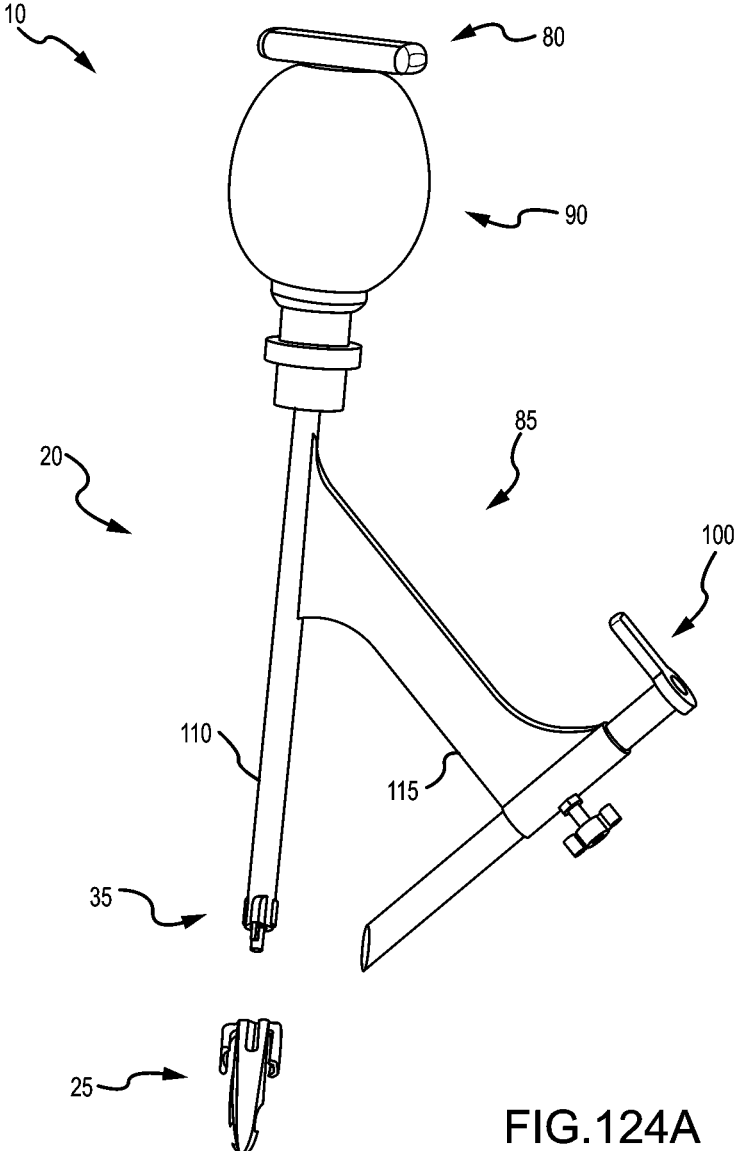


FIG.124A

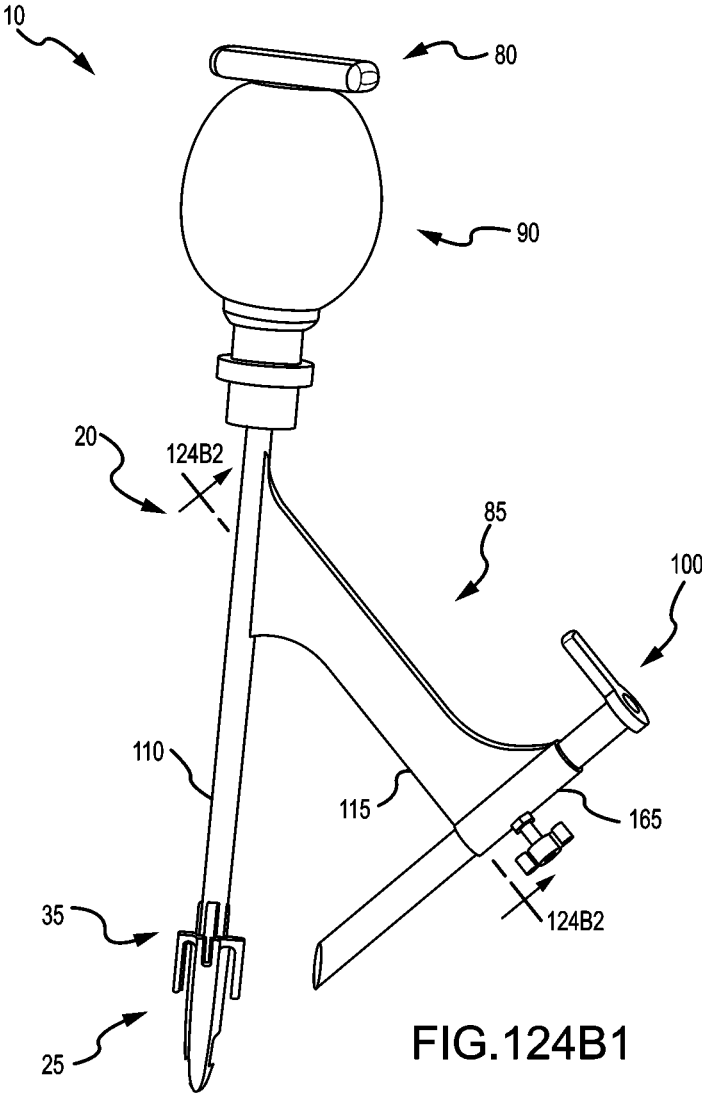


FIG.124B1

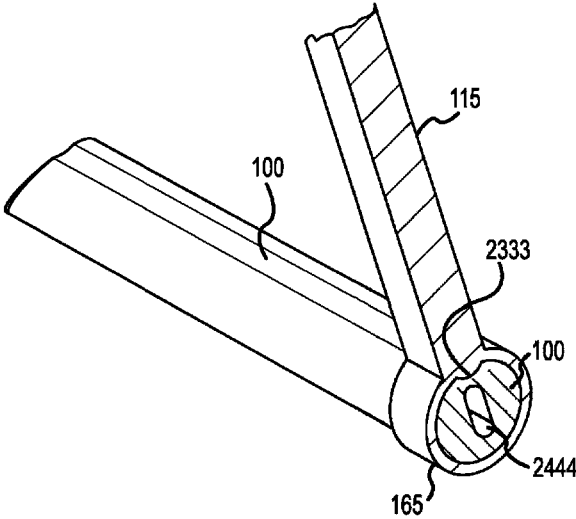


FIG.124B2

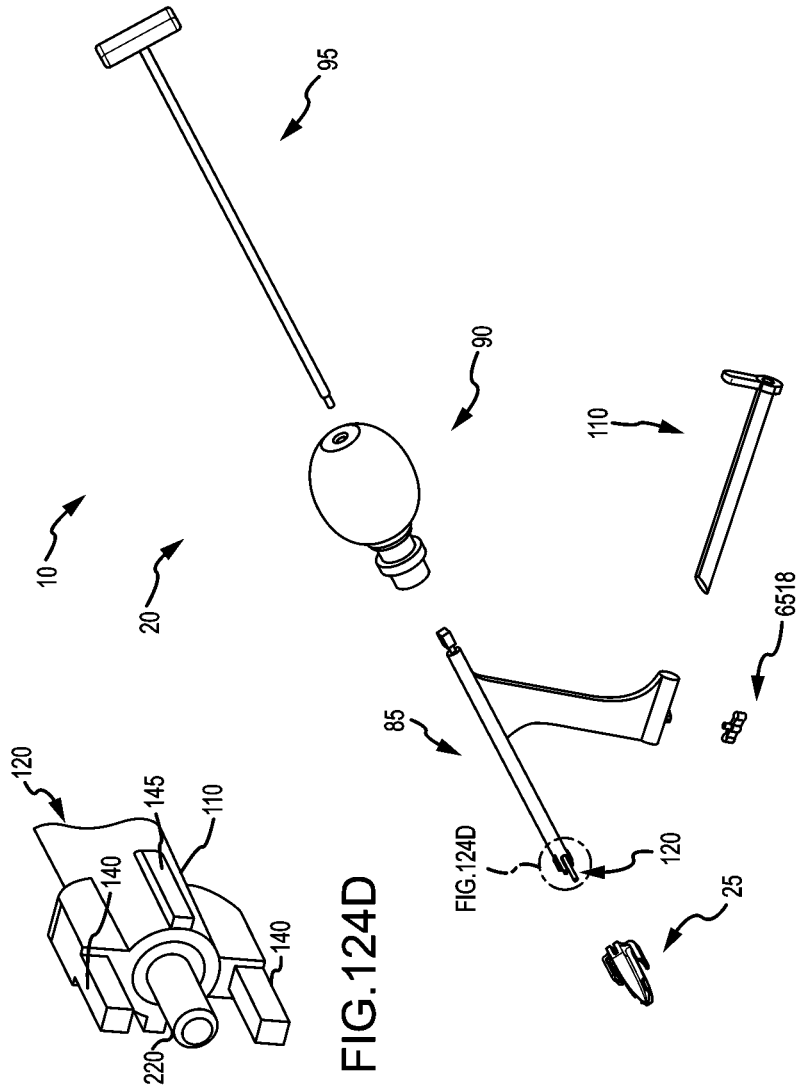


FIG. 124D

FIG. 124C

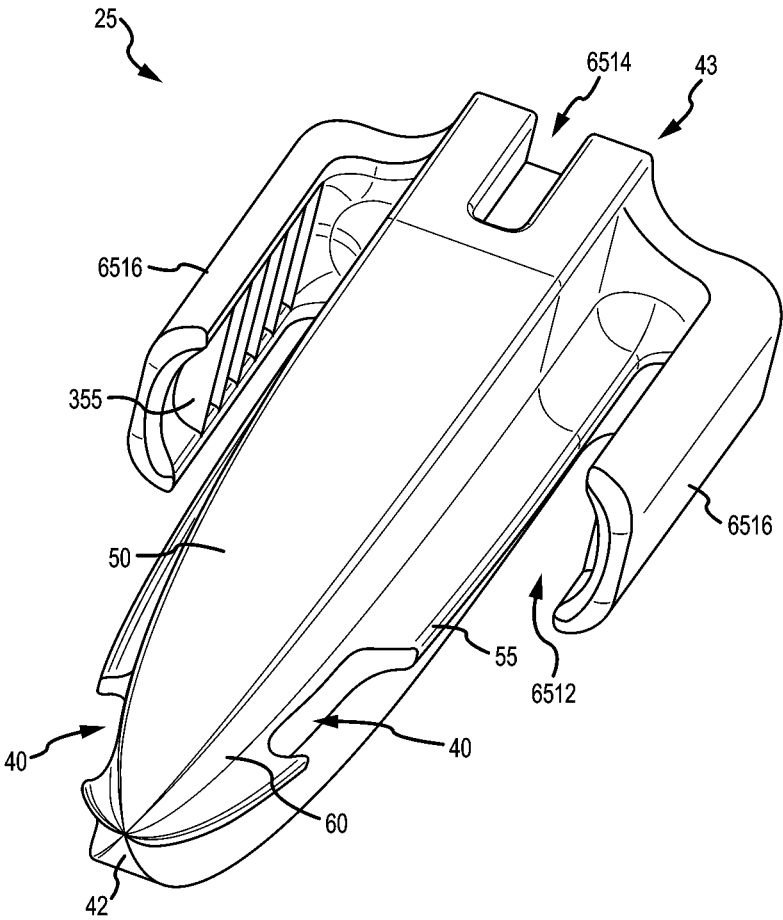


FIG.124E

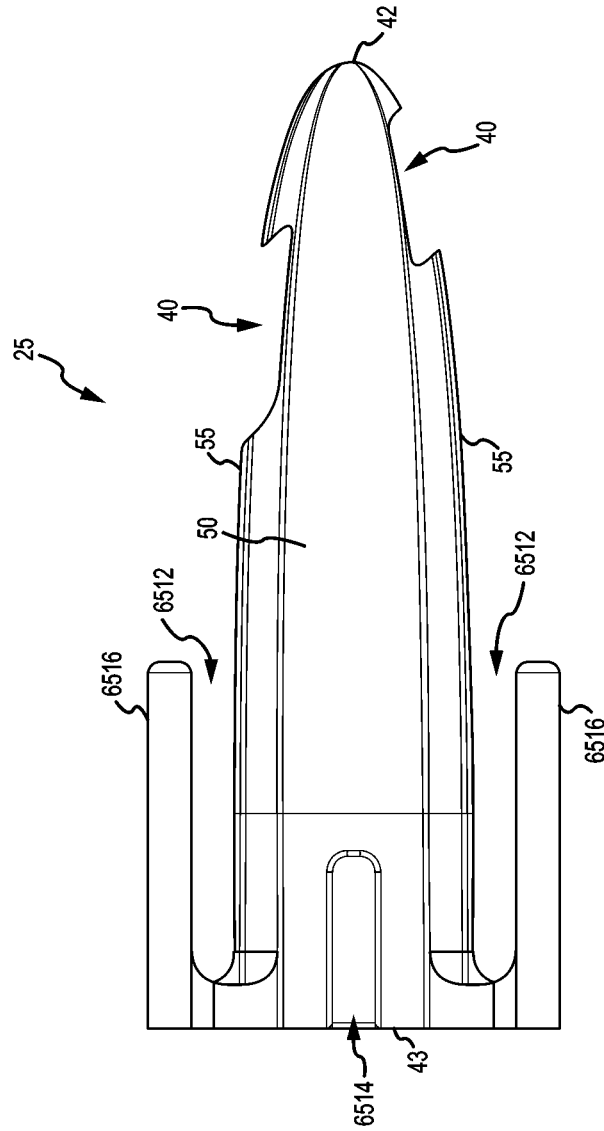


FIG. 124F

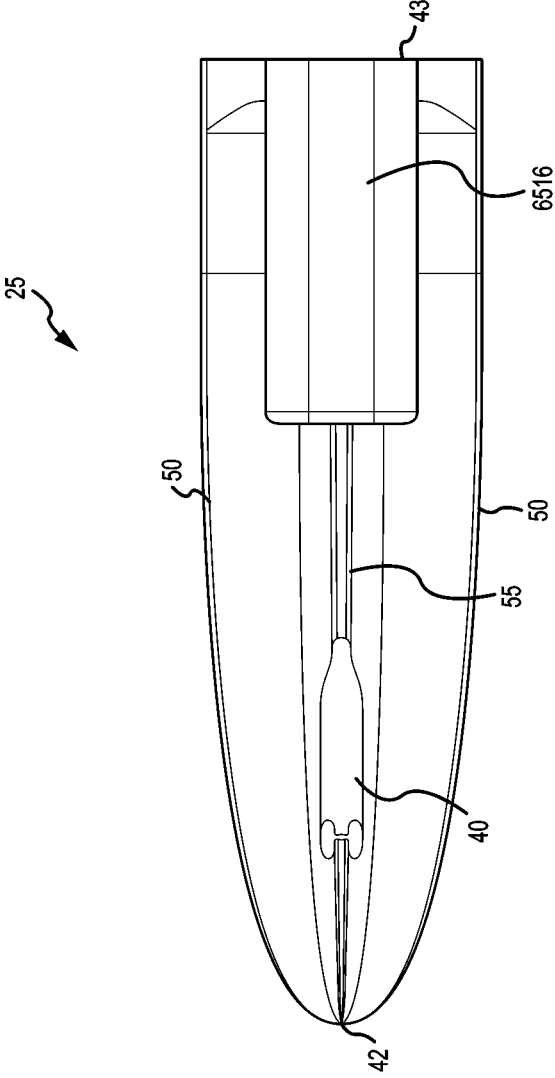


FIG. 124G

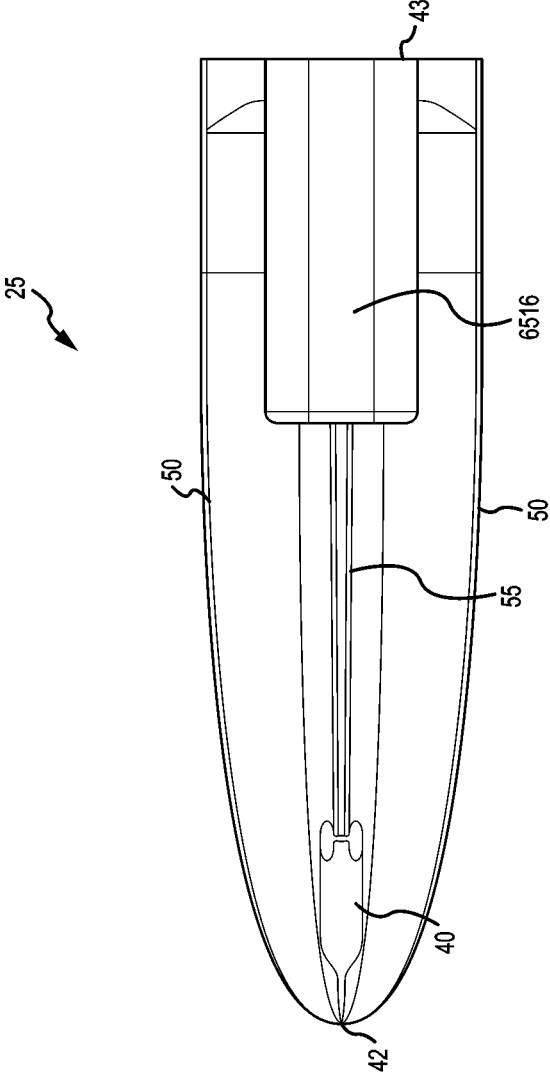


FIG. 124H

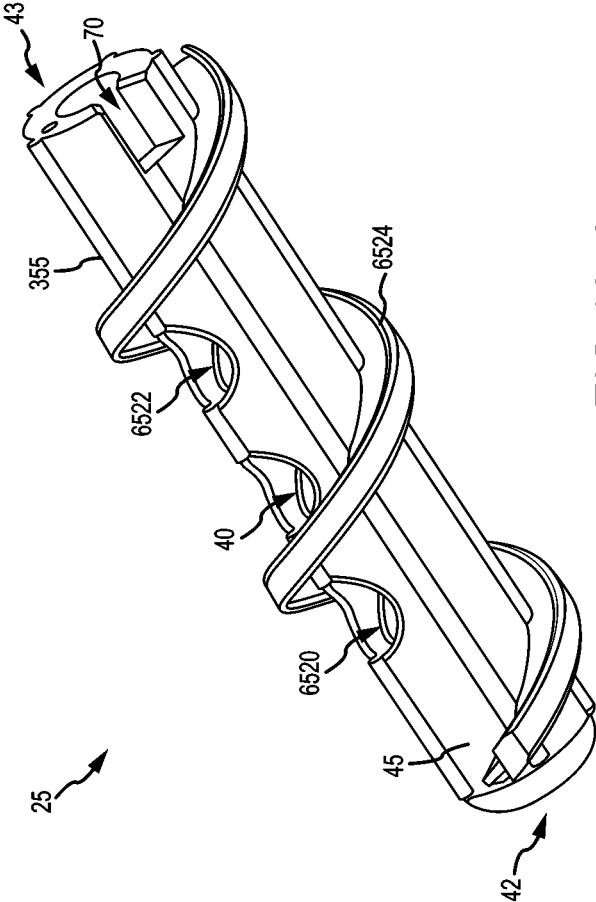


FIG.125A

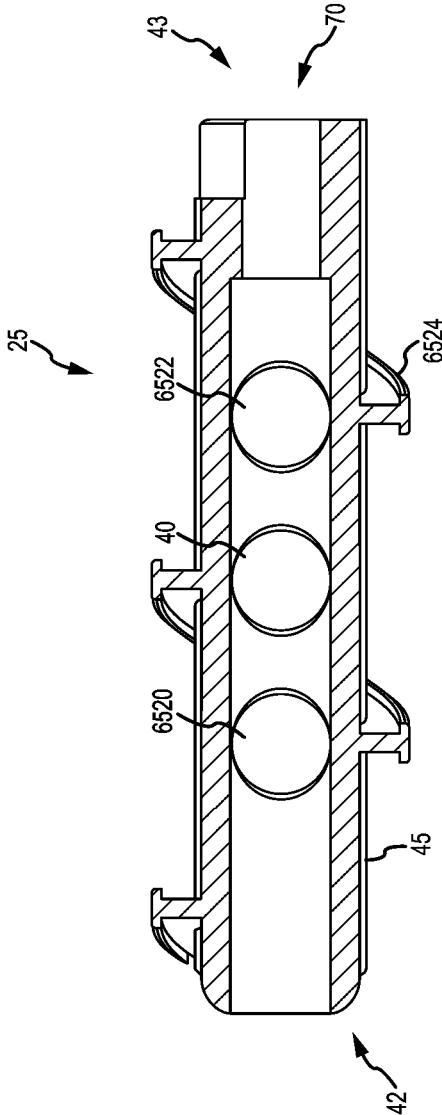


FIG.125B

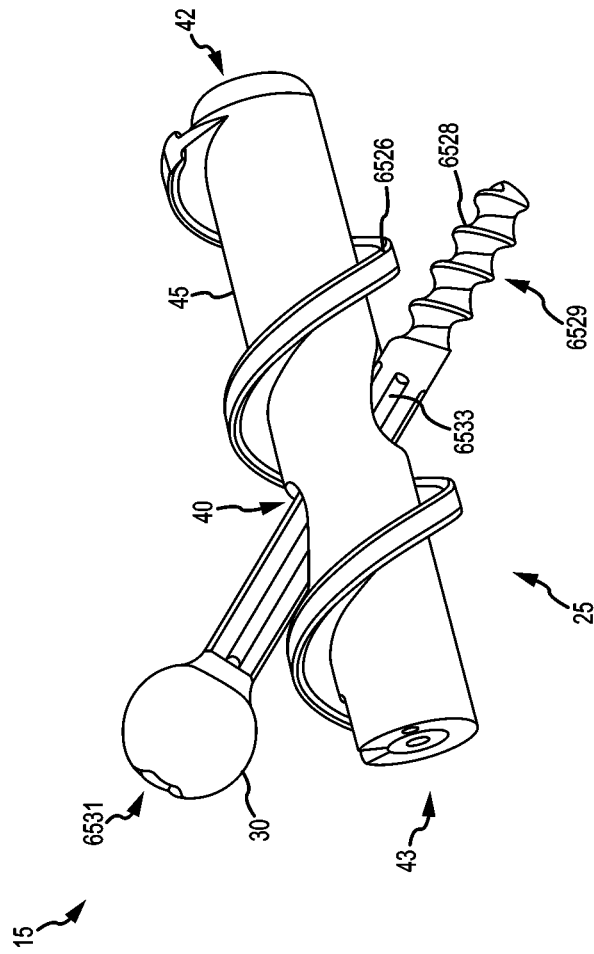


FIG. 126A

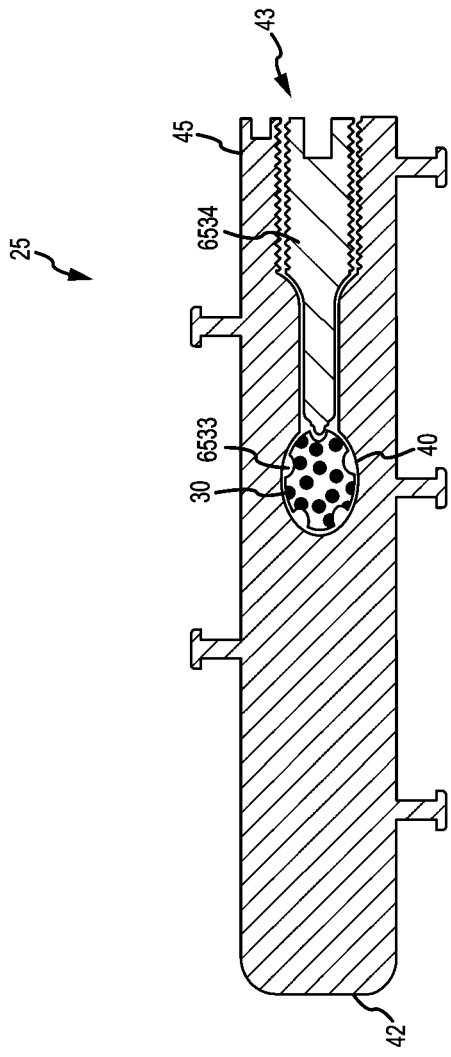


FIG. 126B

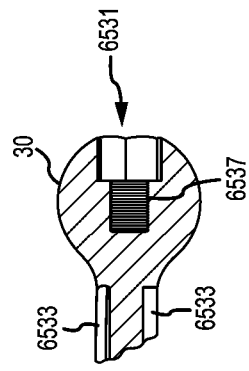
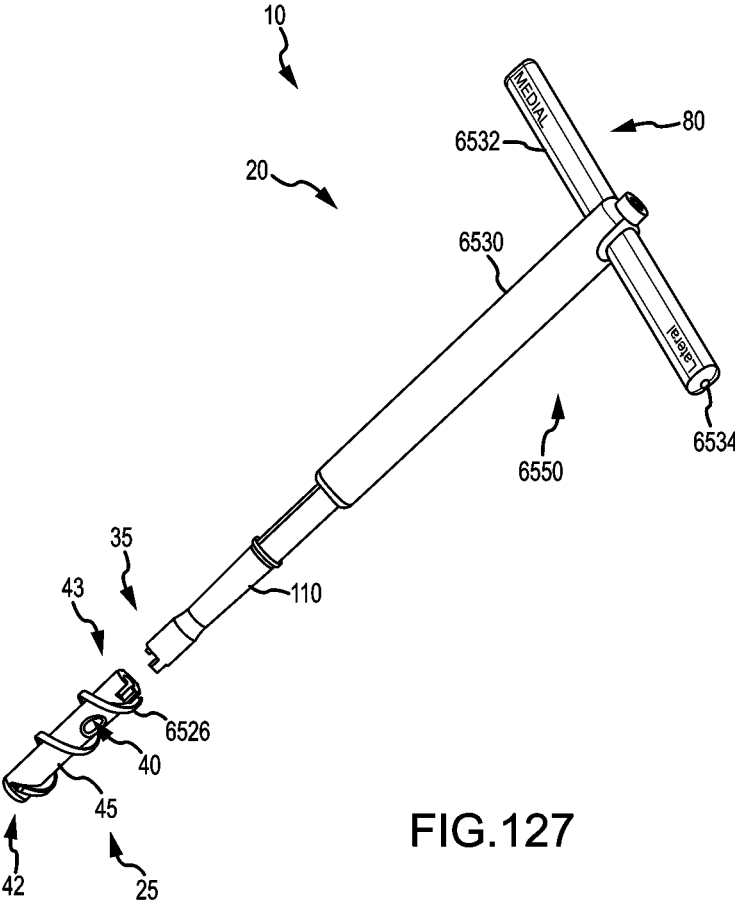


FIG. 126C



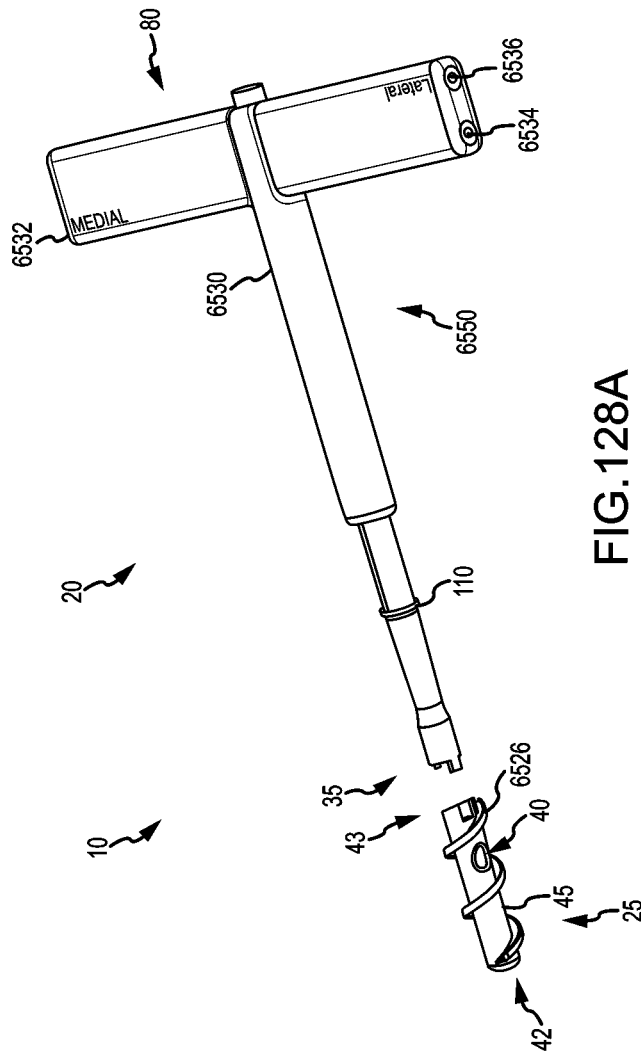


FIG. 128A

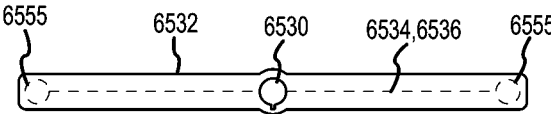


FIG. 128B

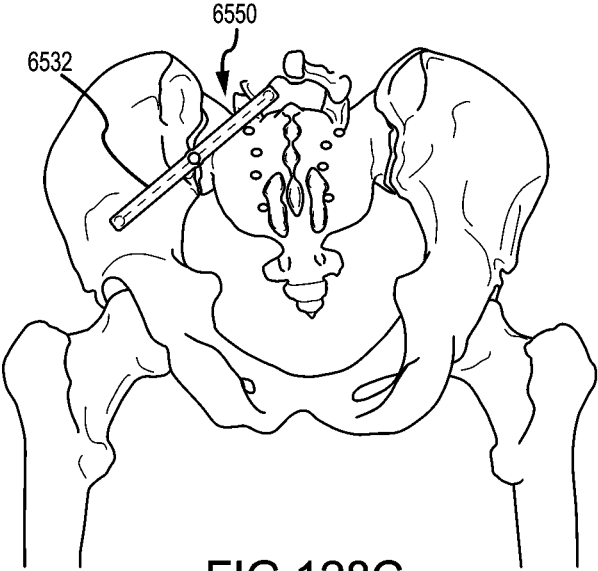


FIG. 128C

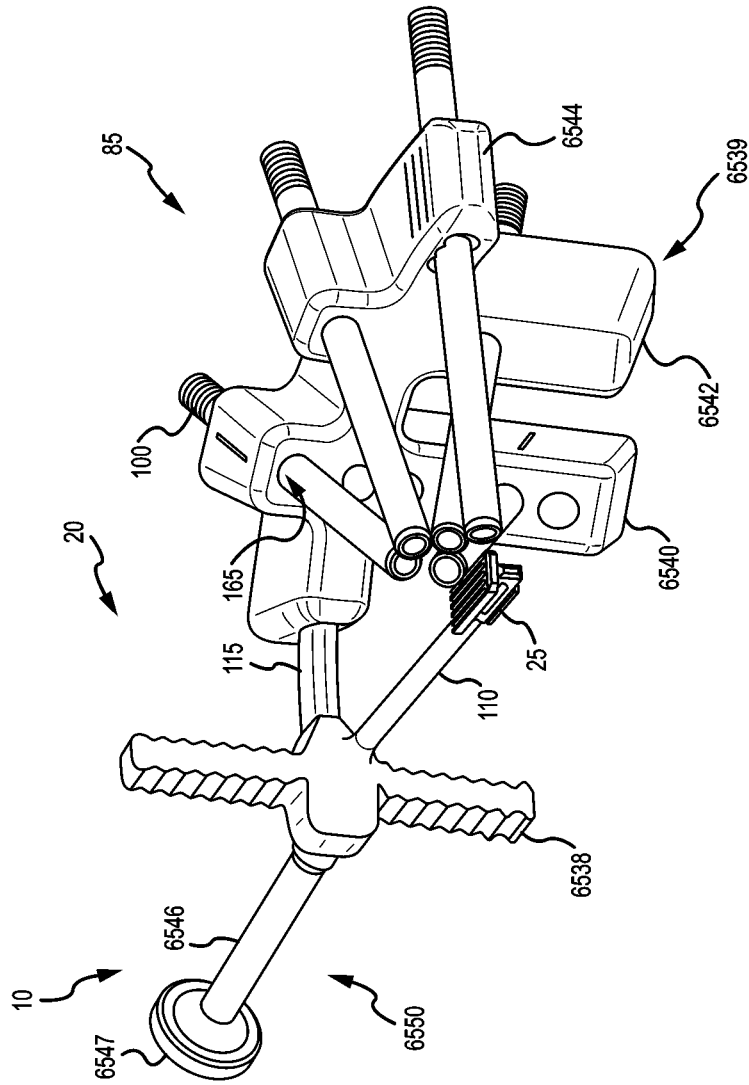


FIG.129A

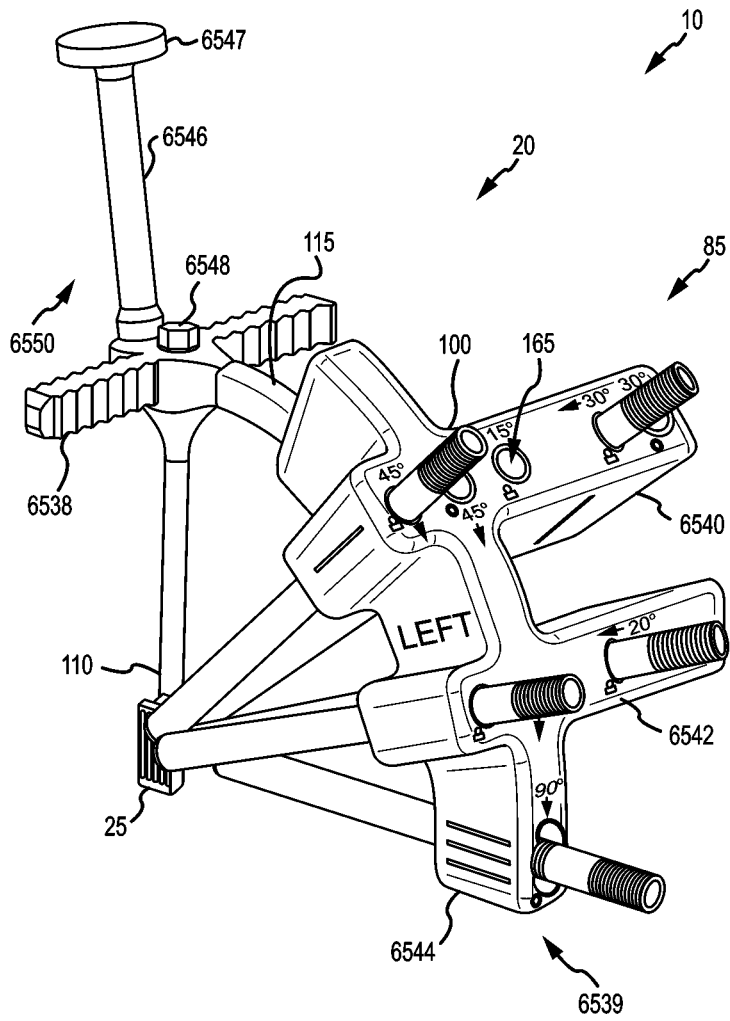


FIG. 129B

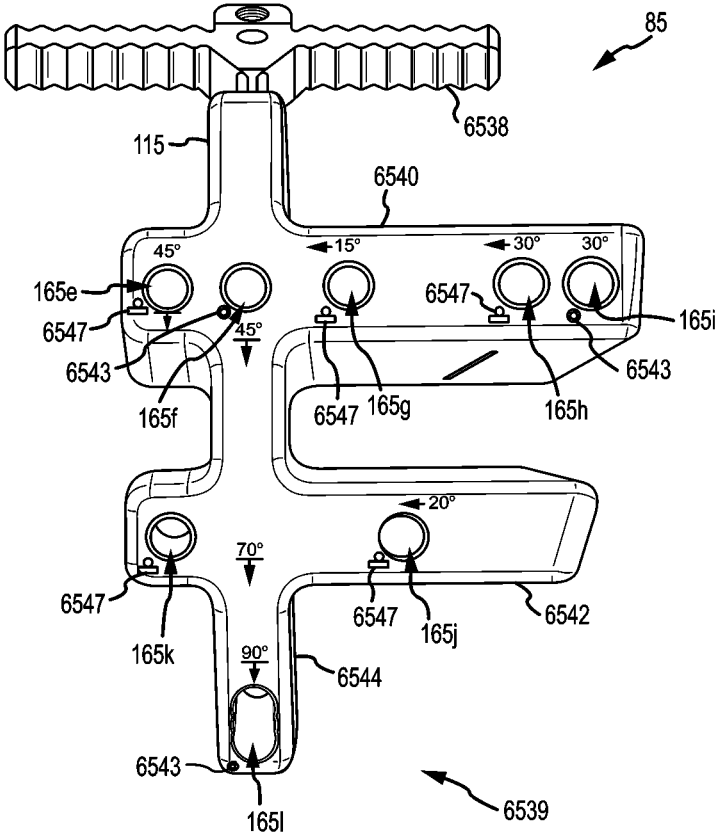


FIG.129C

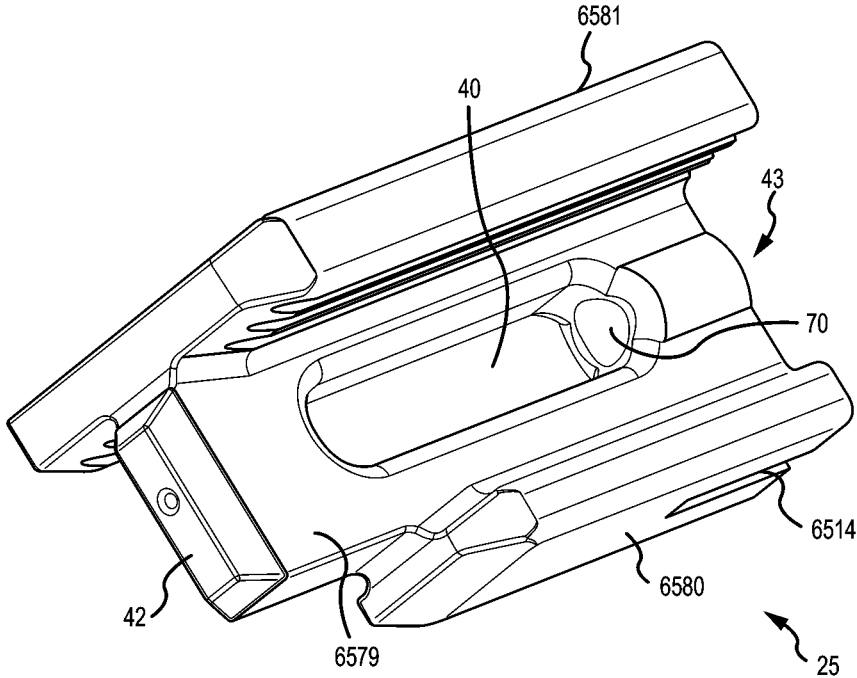


FIG. 129D

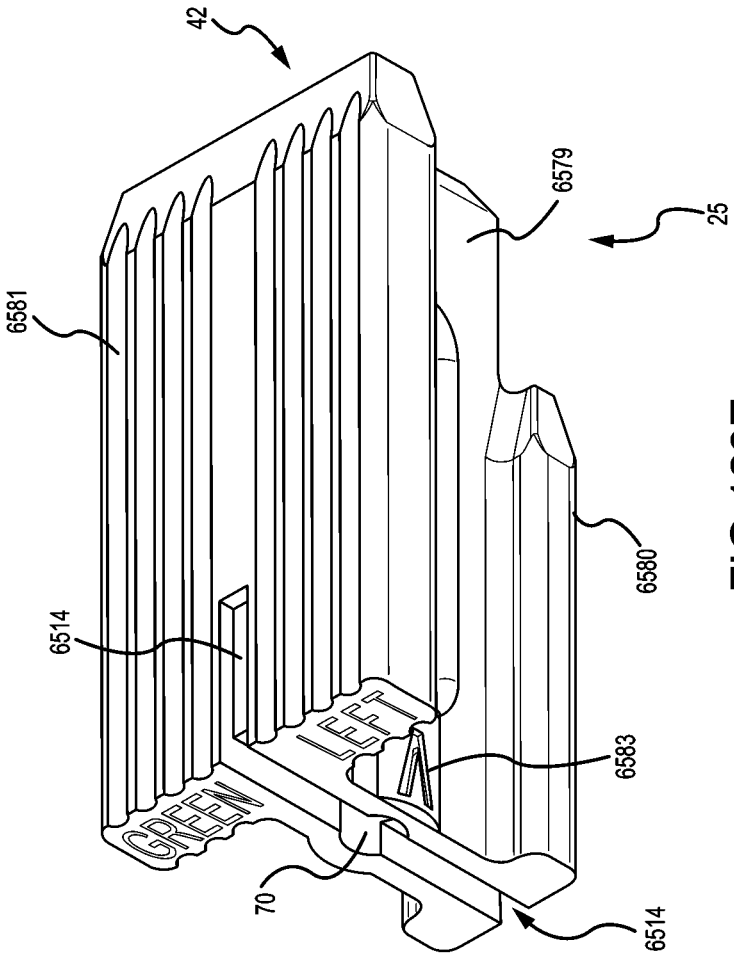


FIG. 129E

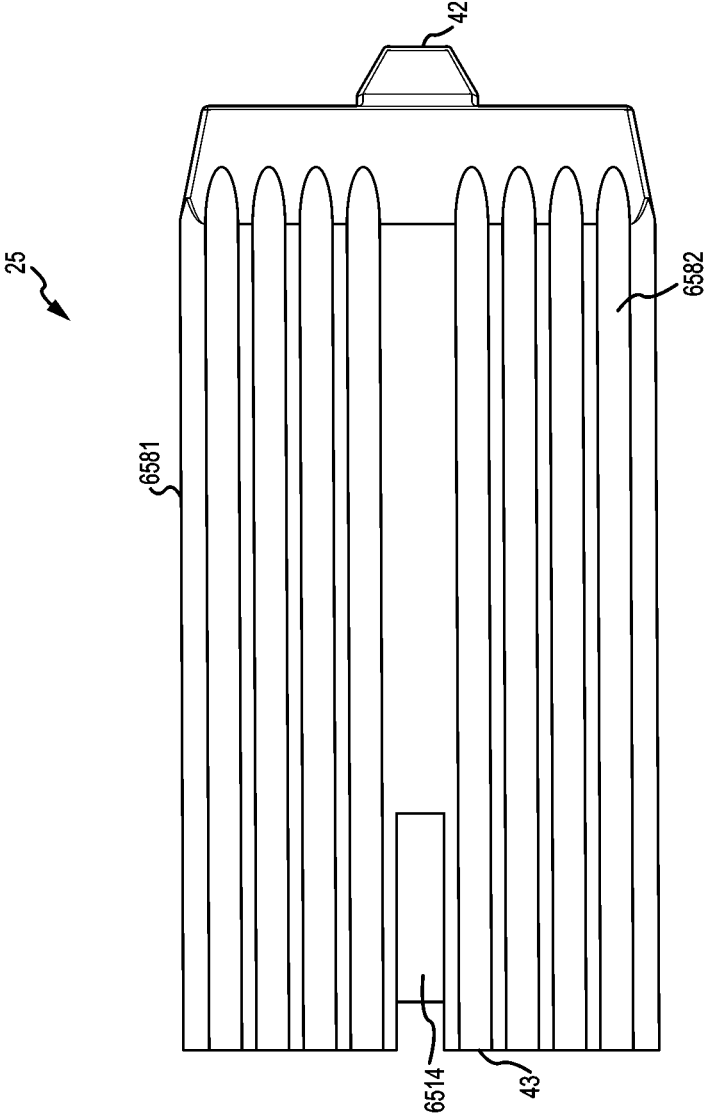


FIG.129F

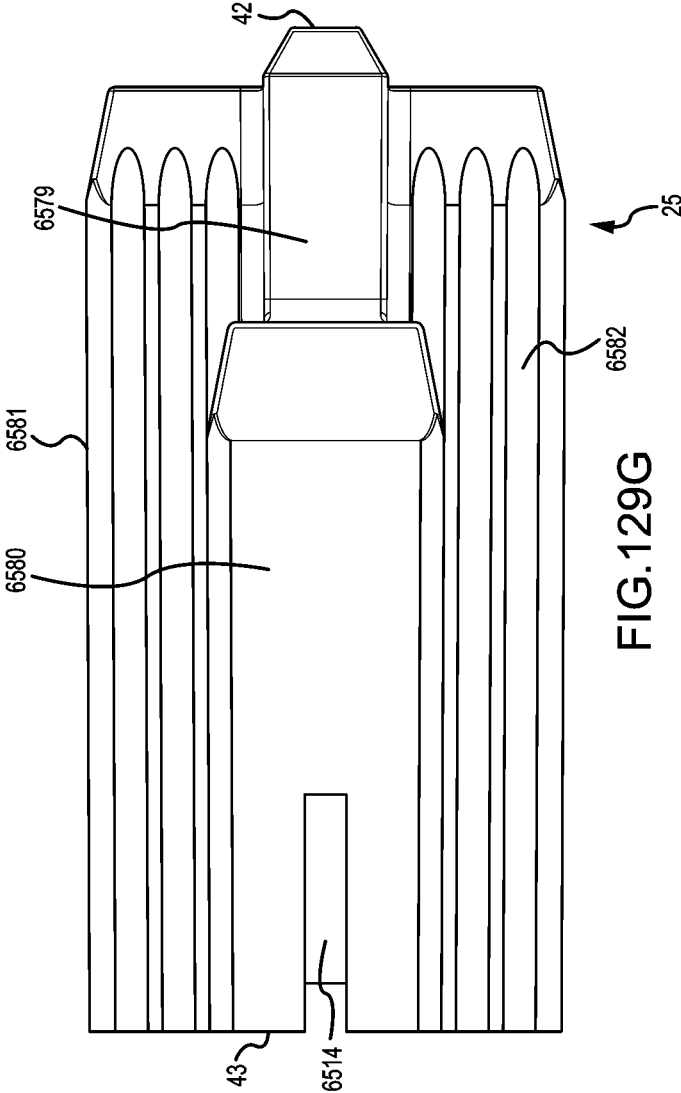


FIG. 129G

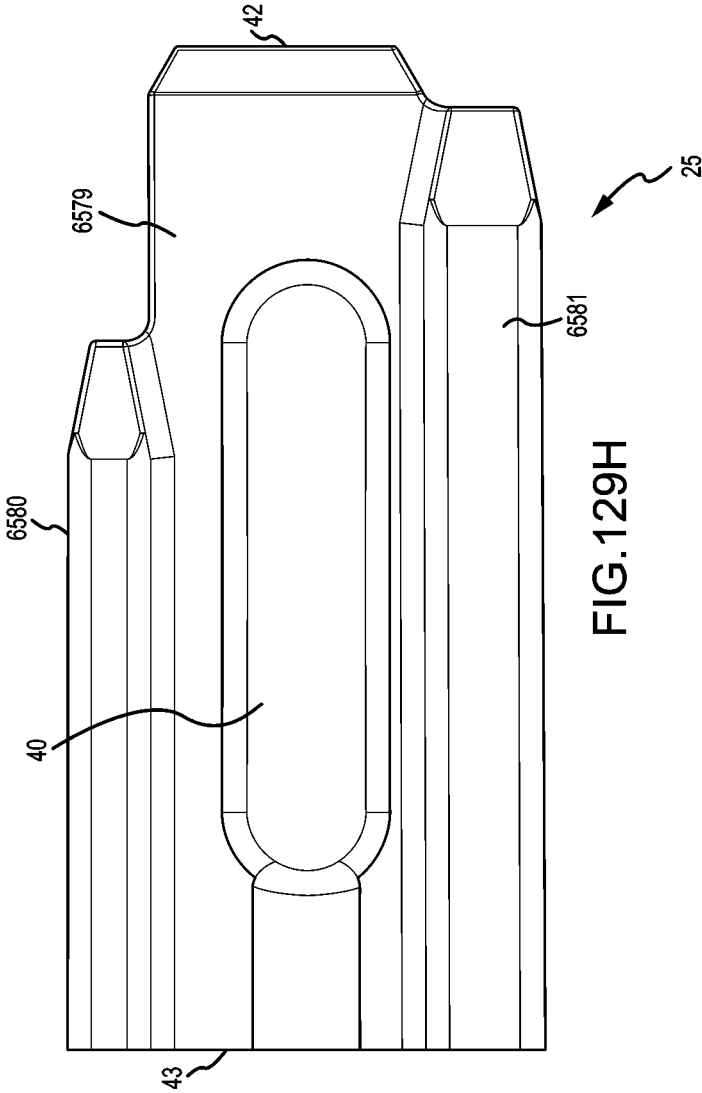


FIG. 129H

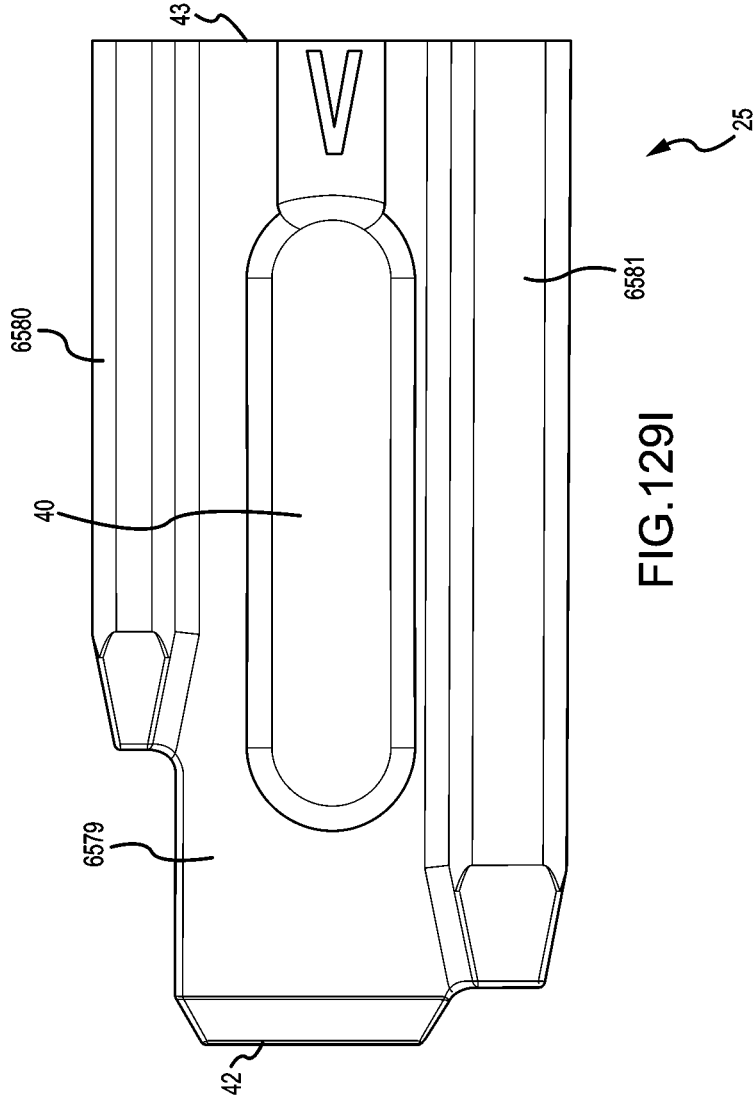


FIG. 129I

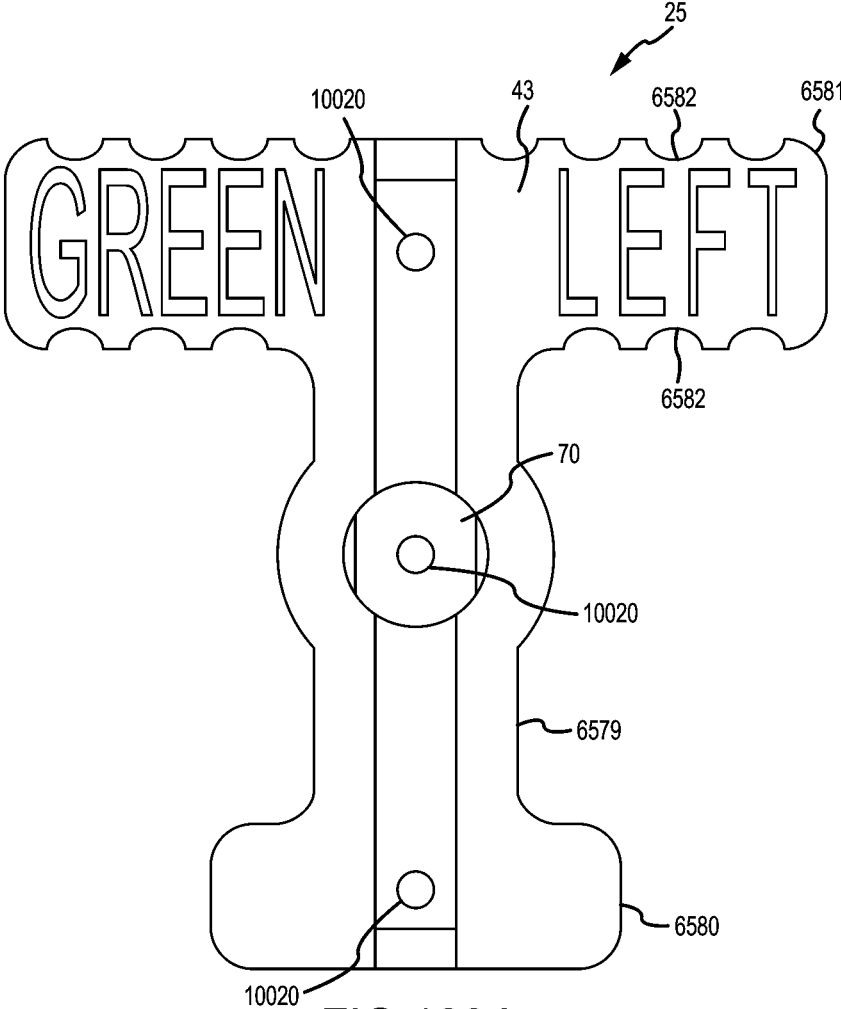


FIG.129J

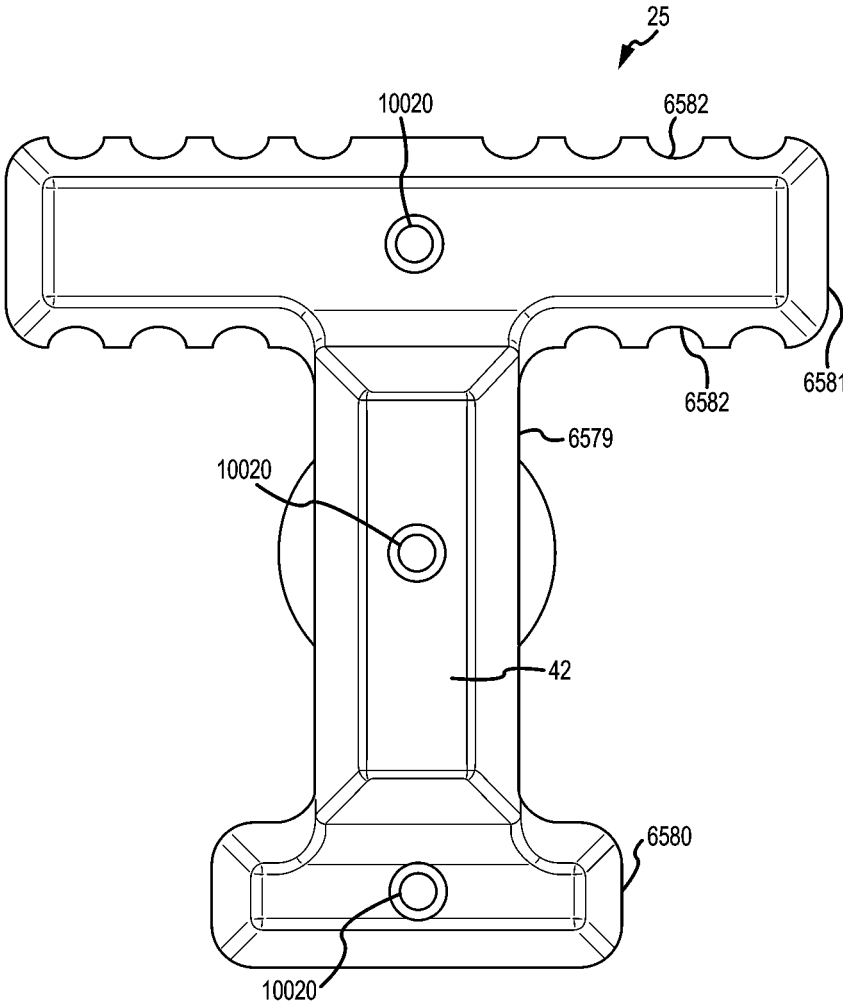


FIG.129K

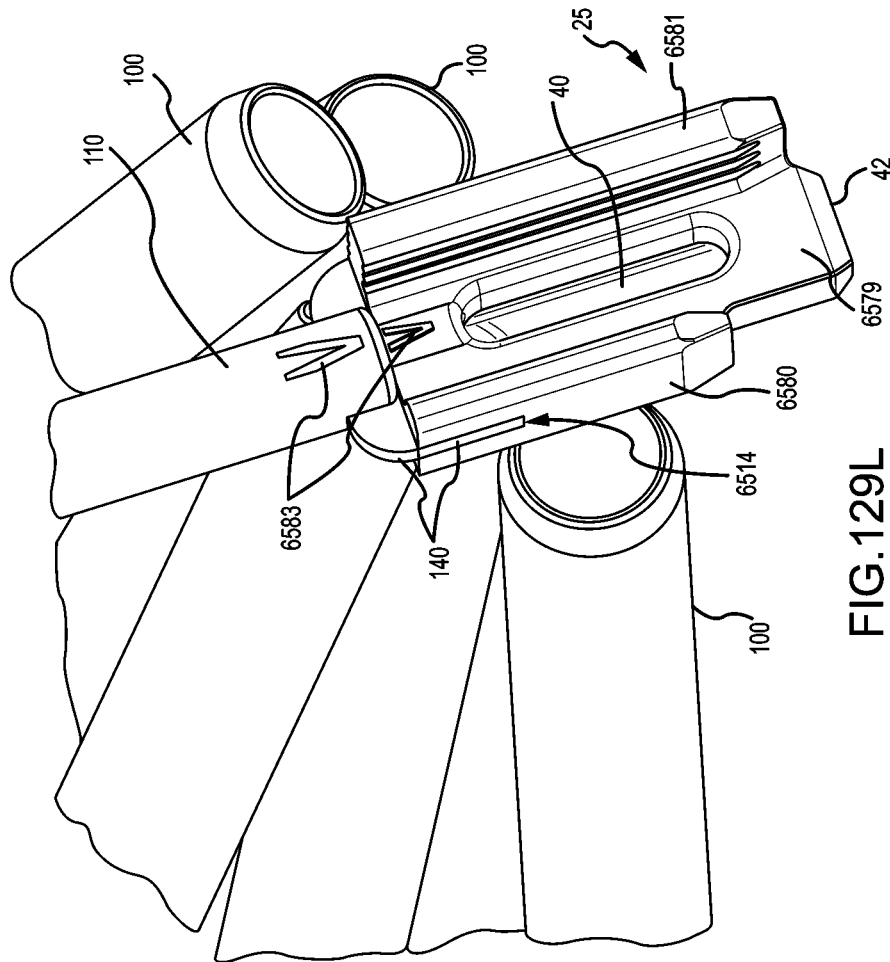


FIG. 129L

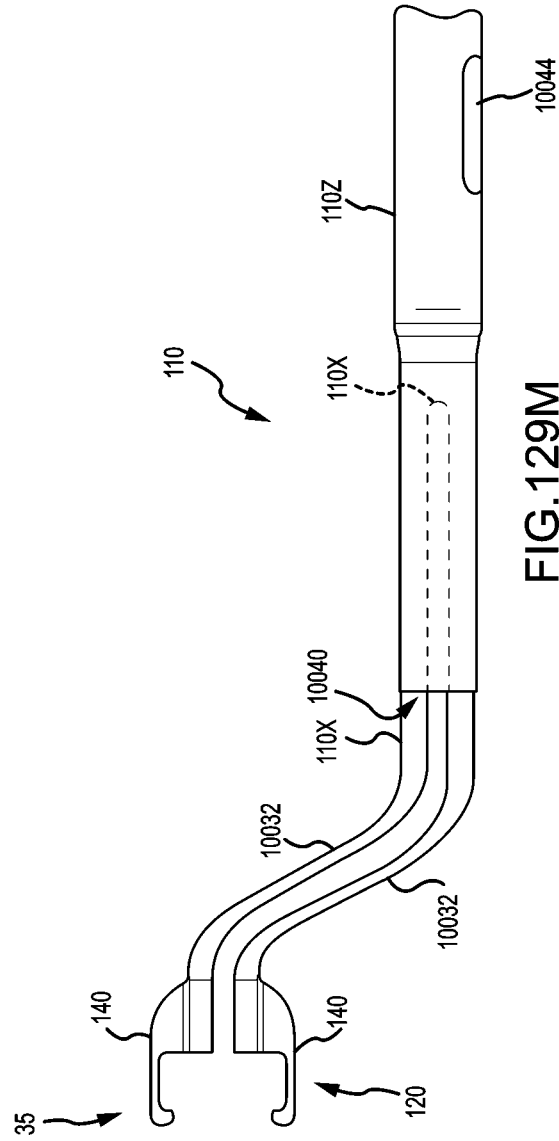


FIG. 129M

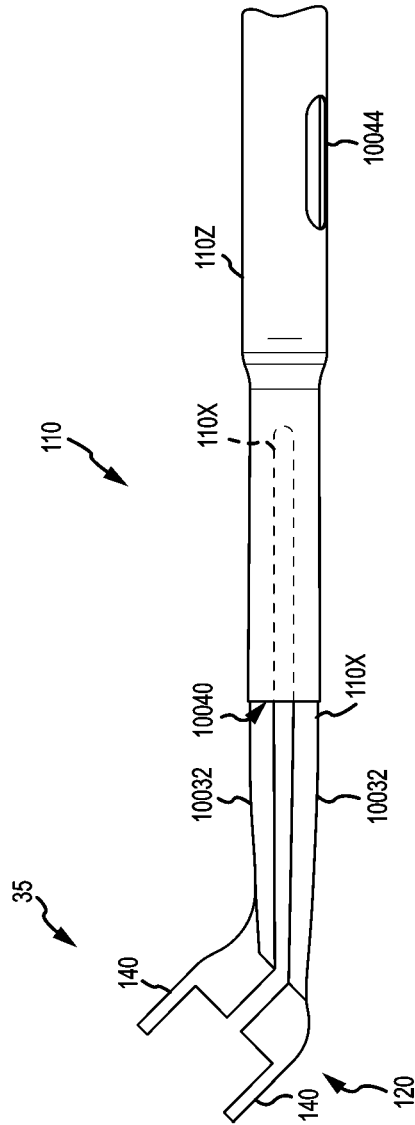


FIG. 129N

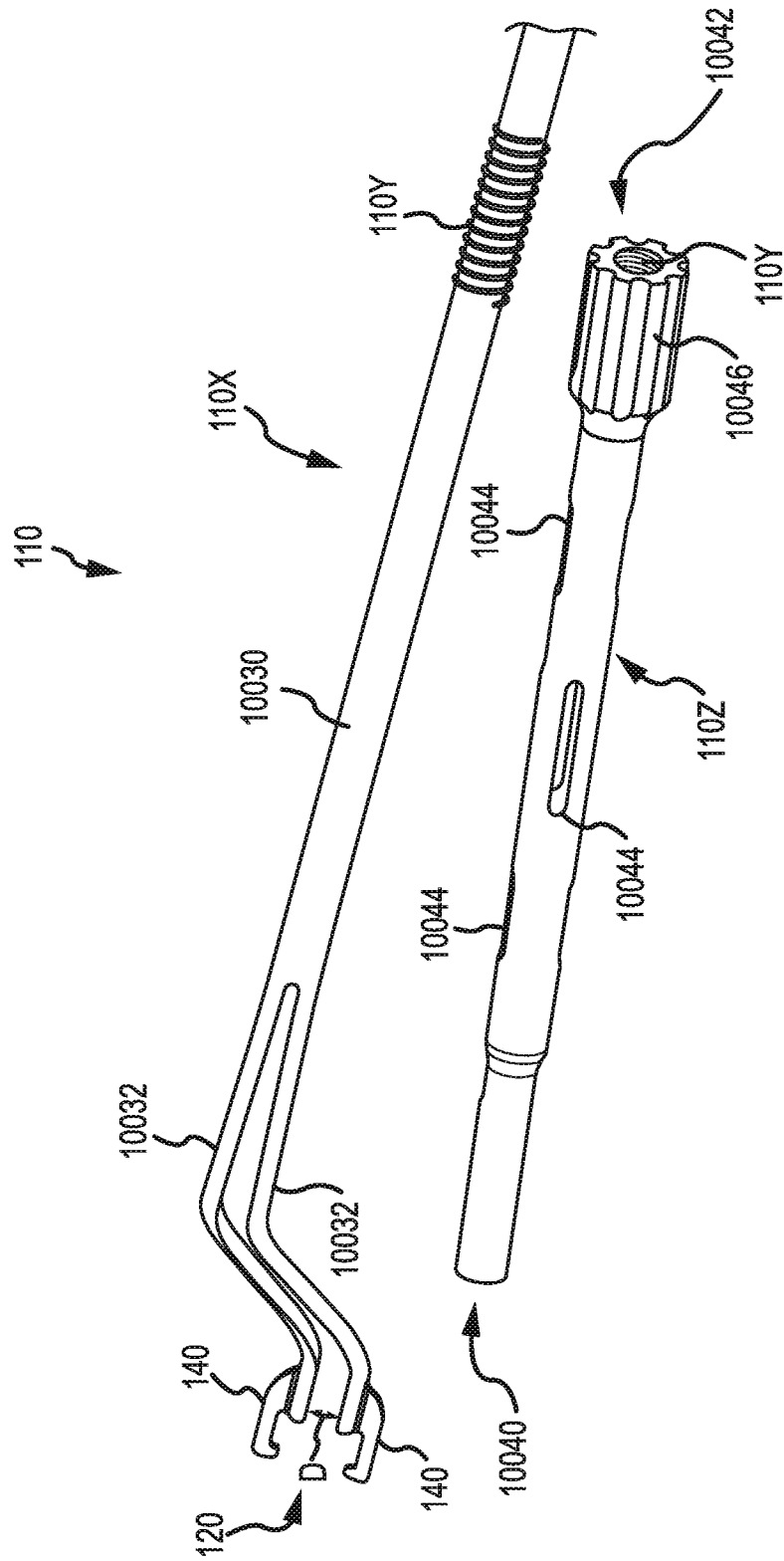


FIG. 1290

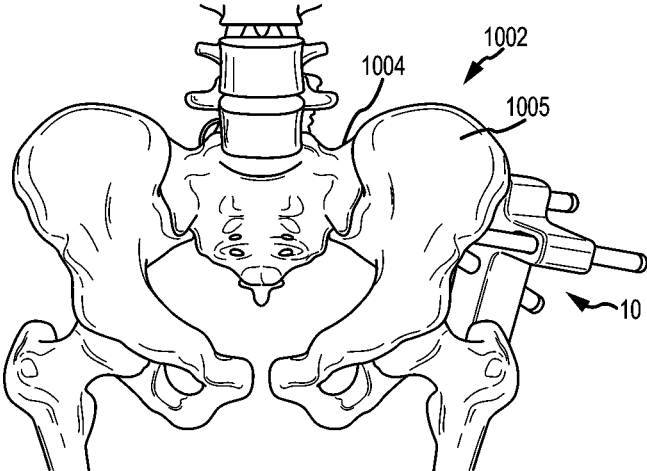


FIG. 130A

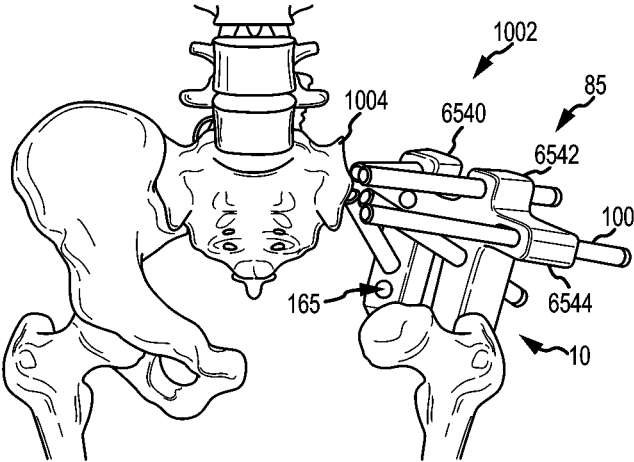
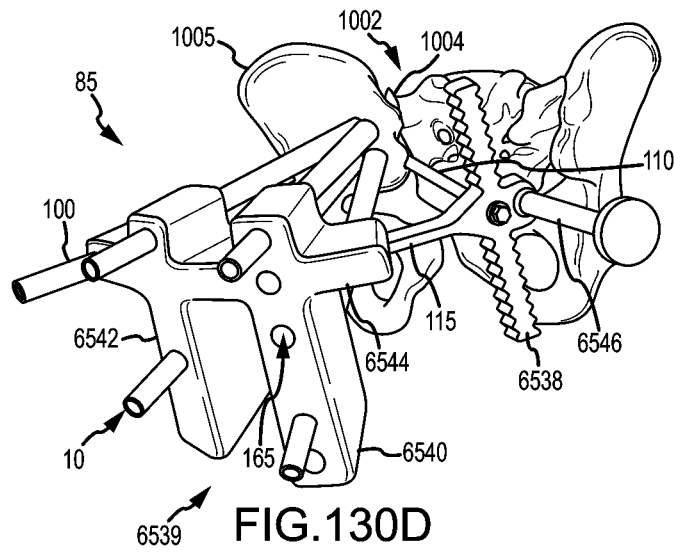
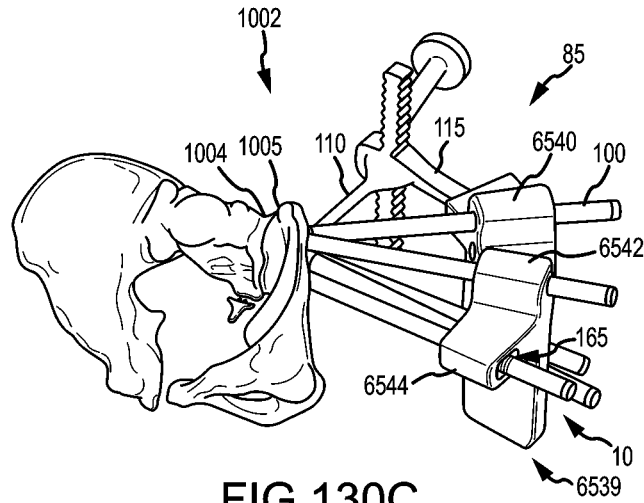


FIG. 130B



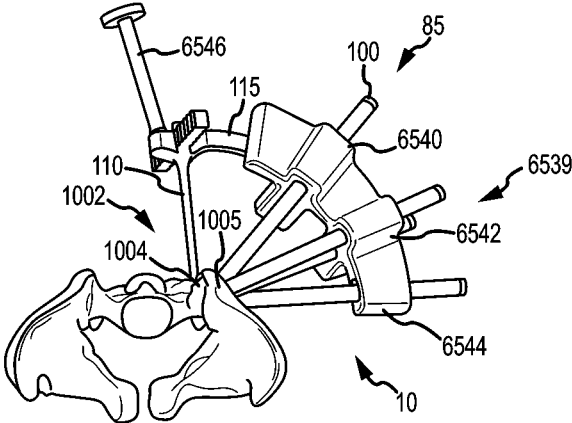


FIG. 130E

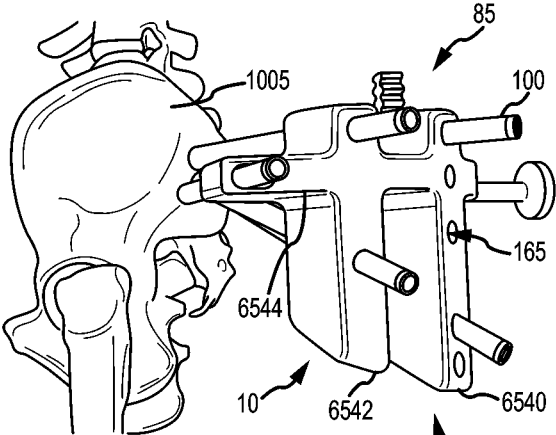


FIG. 130F

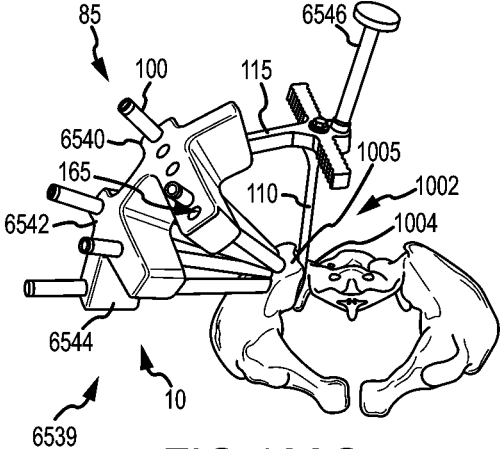


FIG. 130G

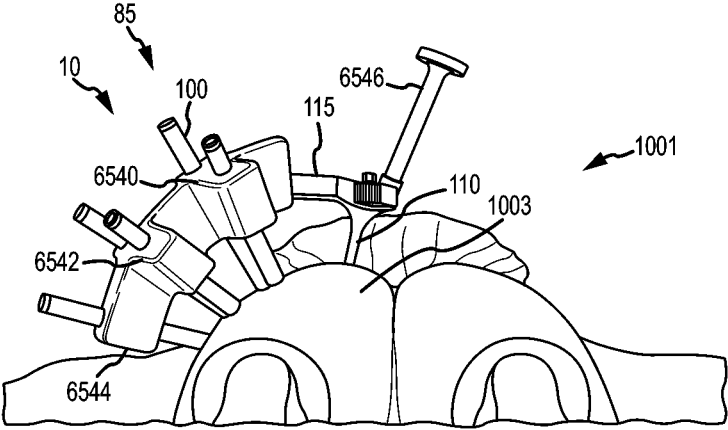


FIG. 130H

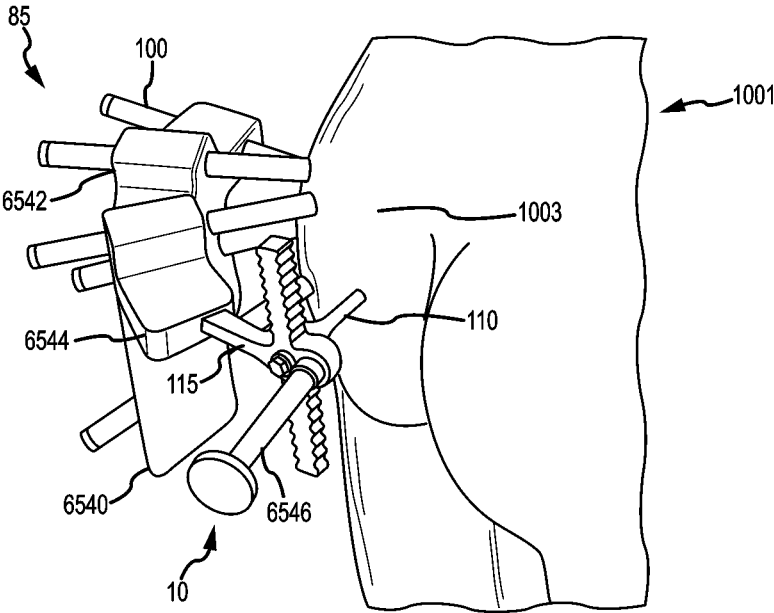


FIG.130I

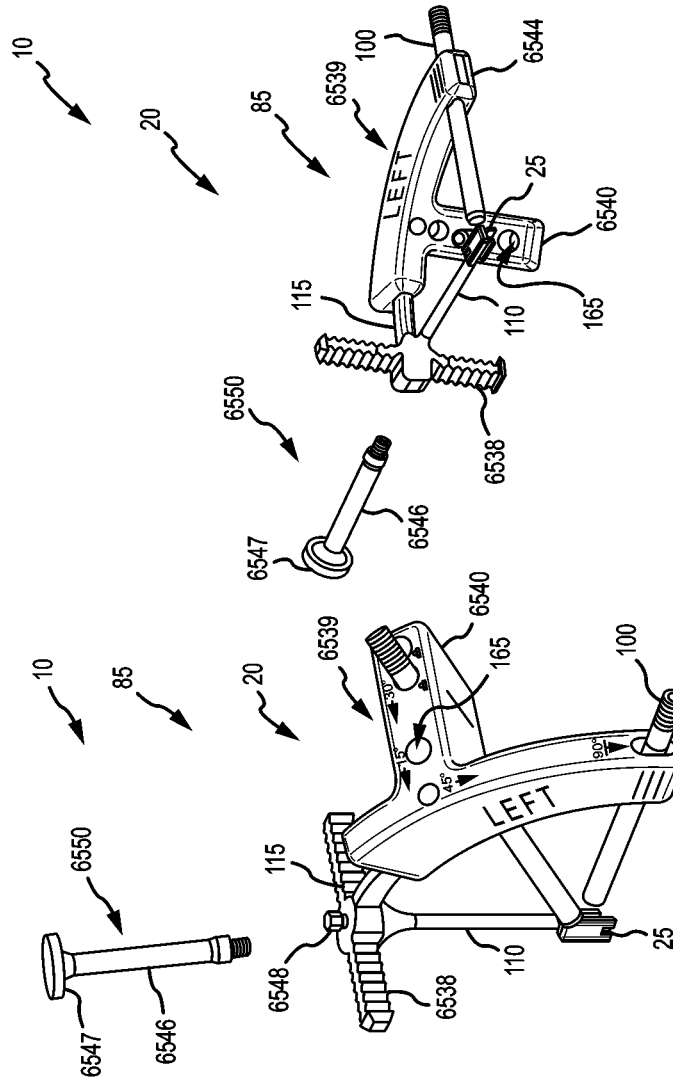


FIG.131B

FIG.131A

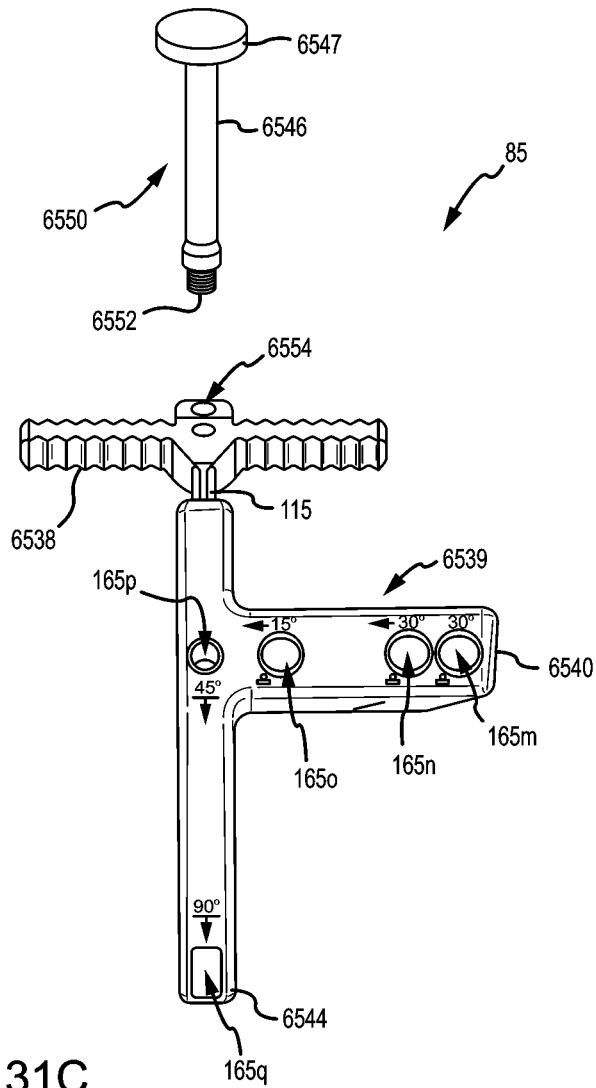


FIG.131C

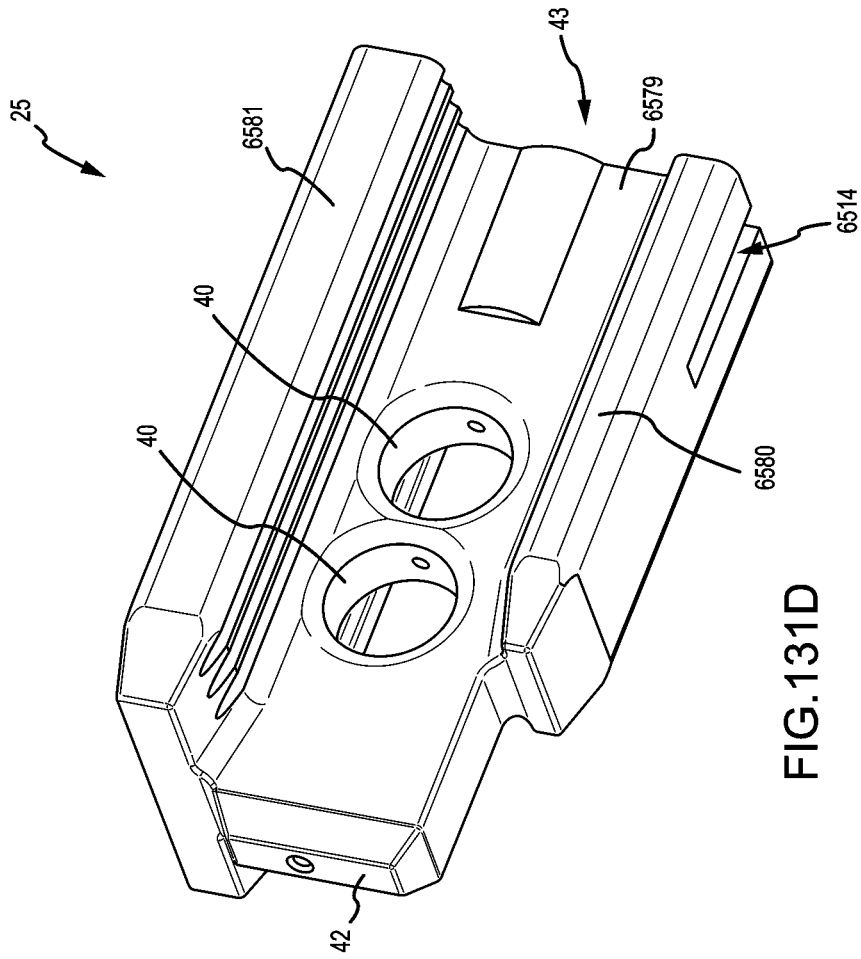


FIG. 131D

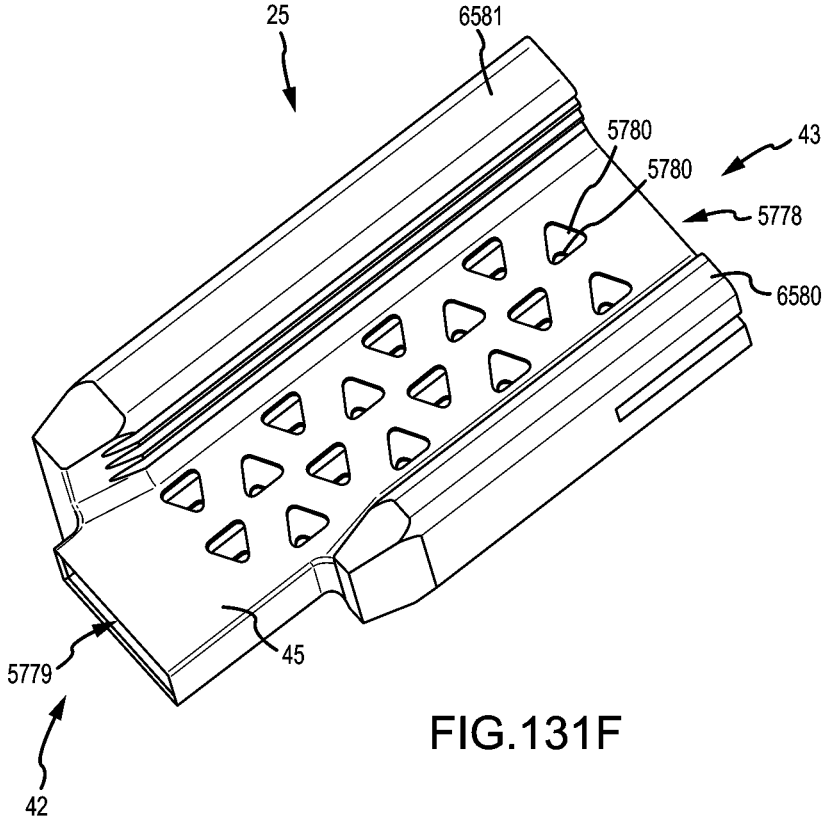


FIG. 131F

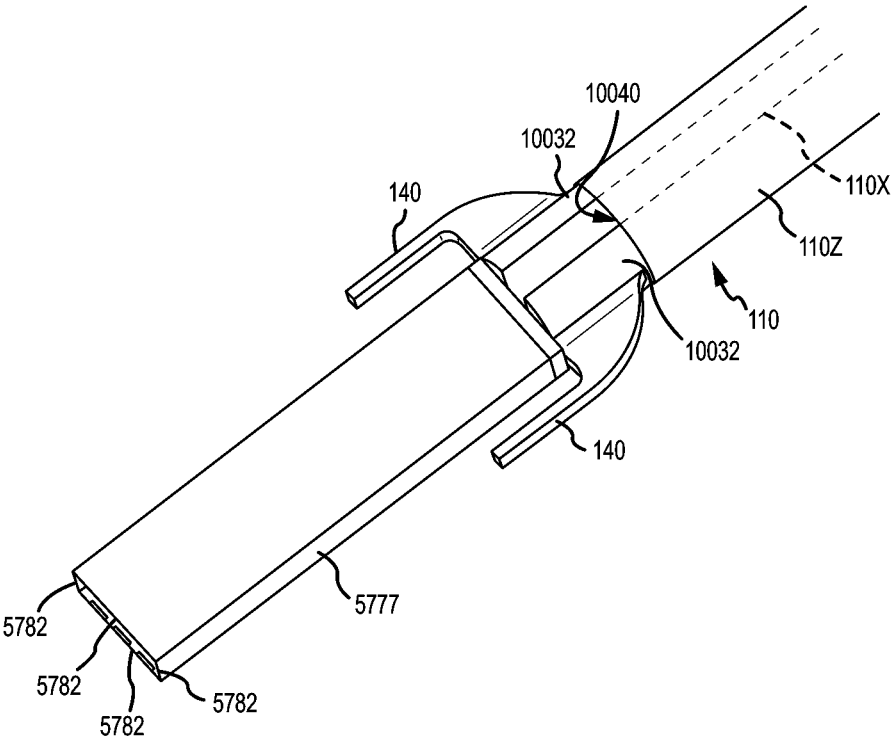


FIG.131G

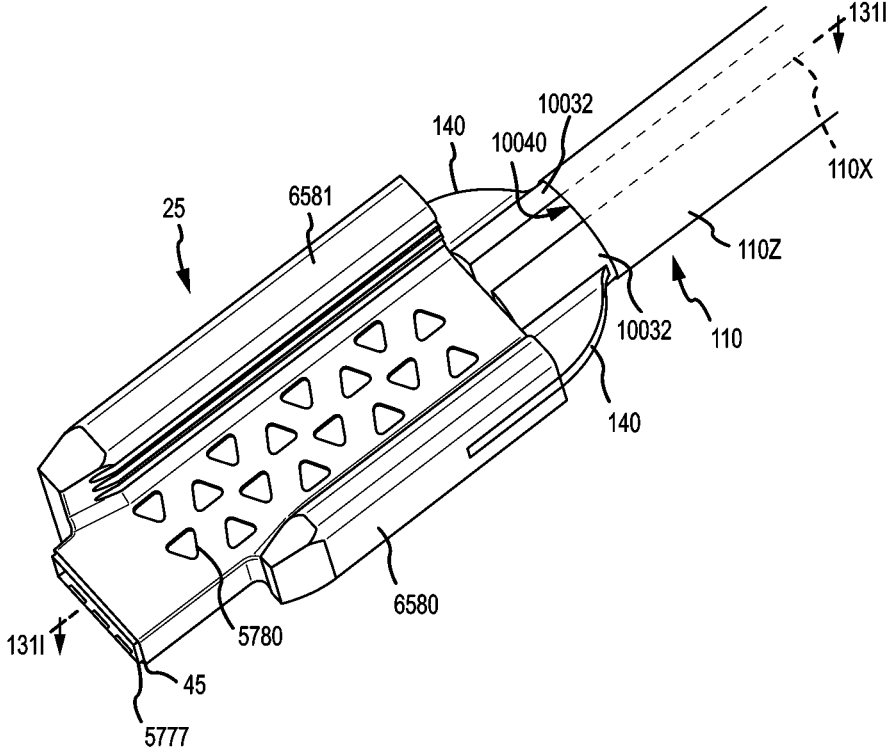


FIG.131H

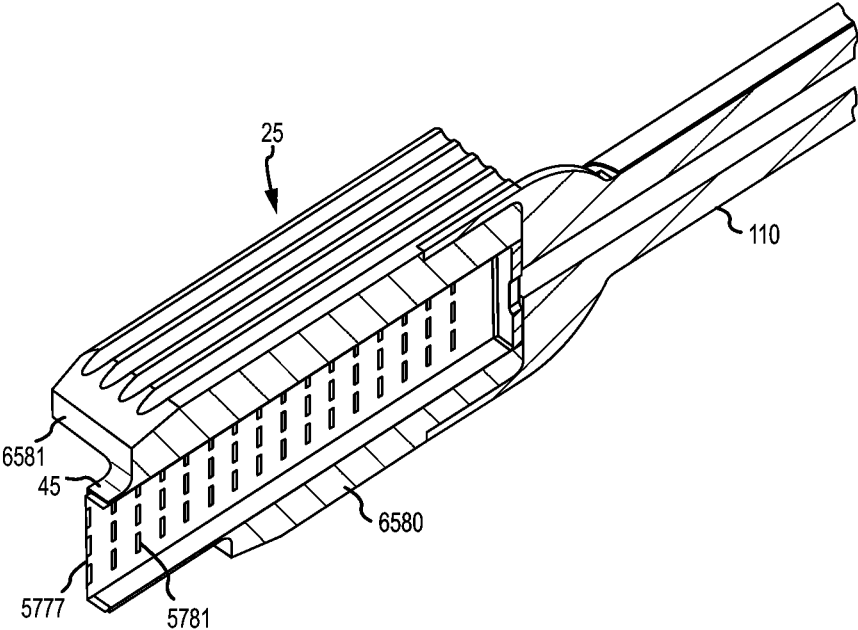


FIG.131I

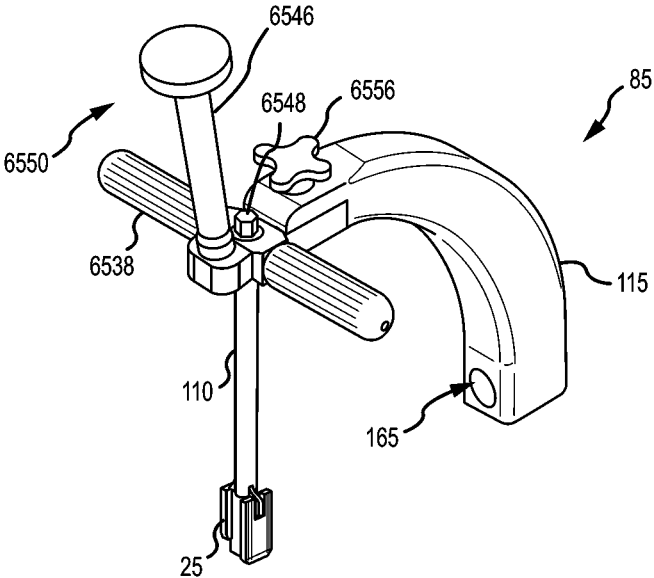


FIG.132A

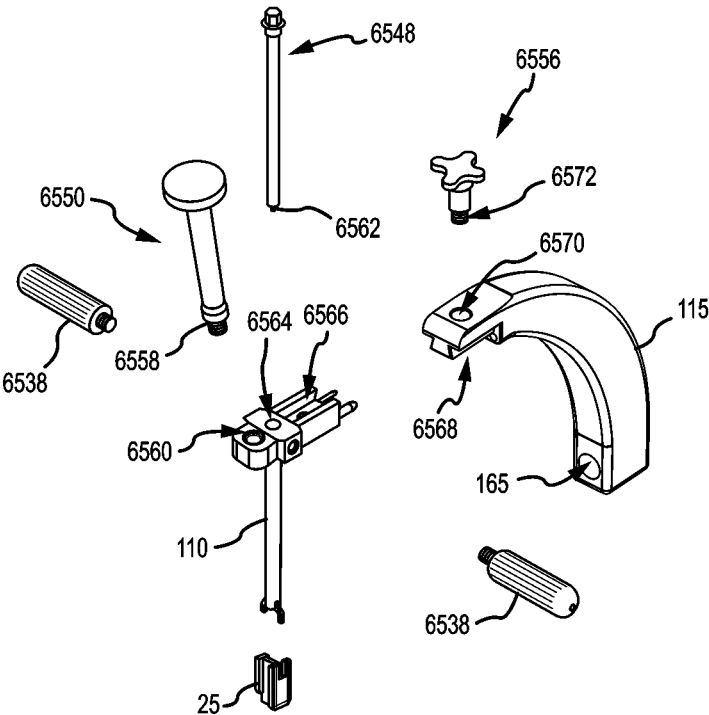


FIG.132B

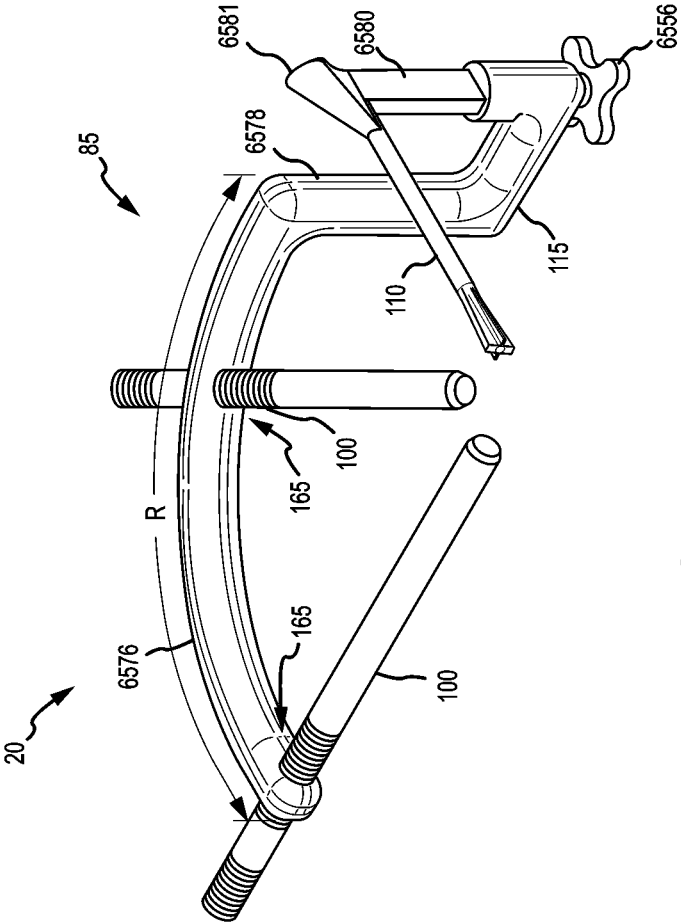


FIG.133A

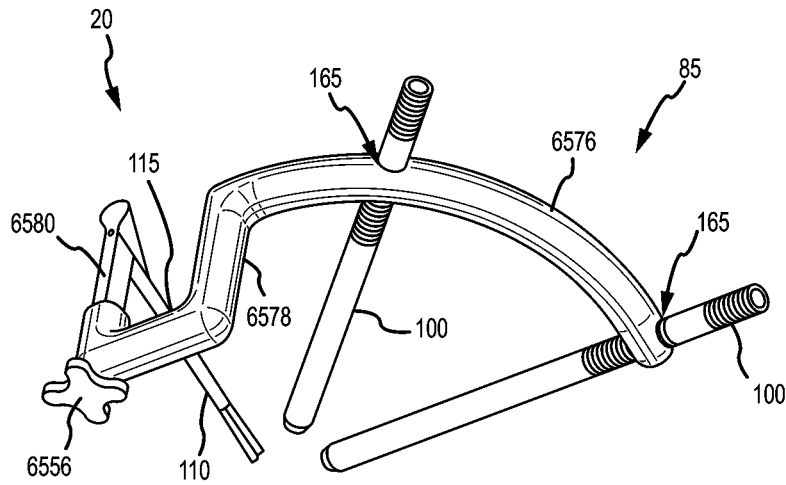


FIG. 133B

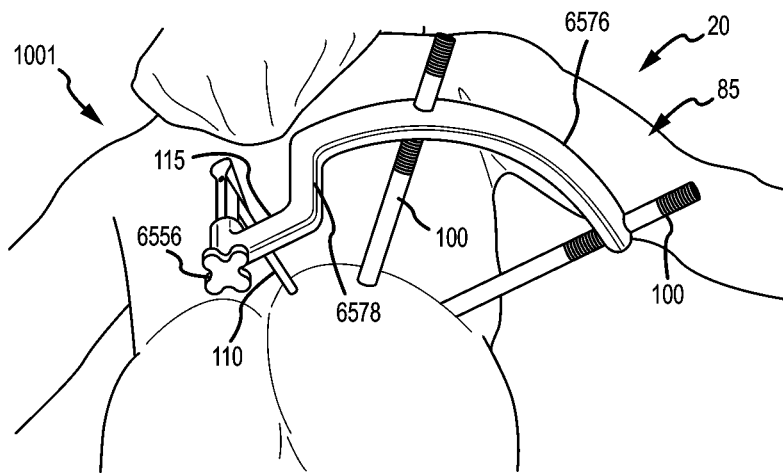


FIG. 133C

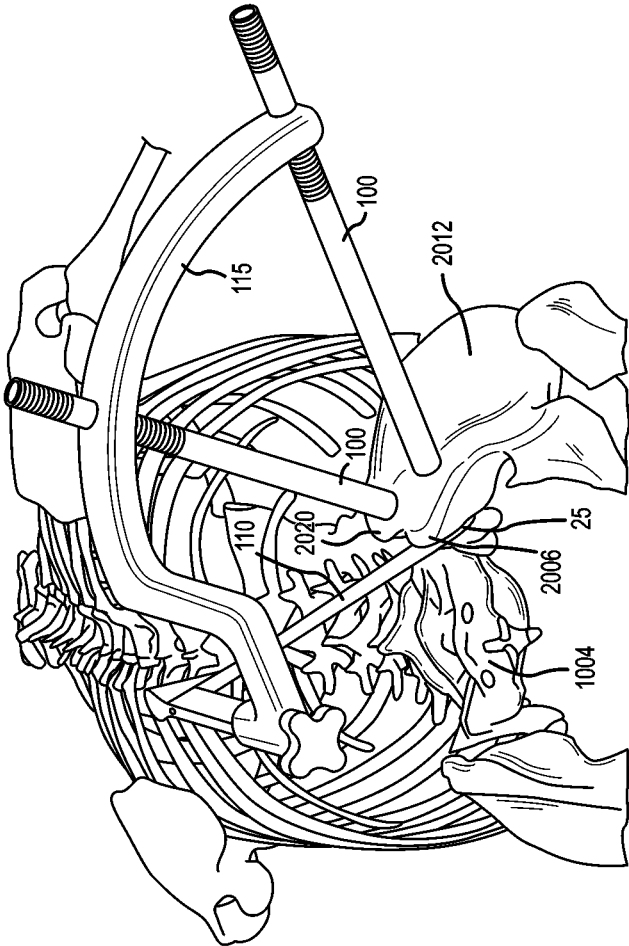


FIG. 133D

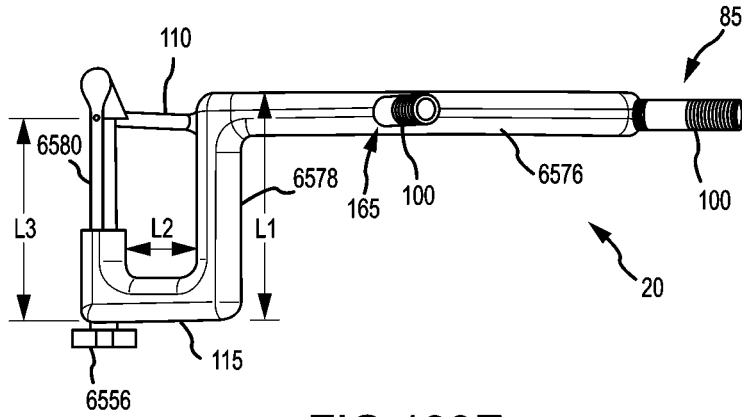


FIG. 133E

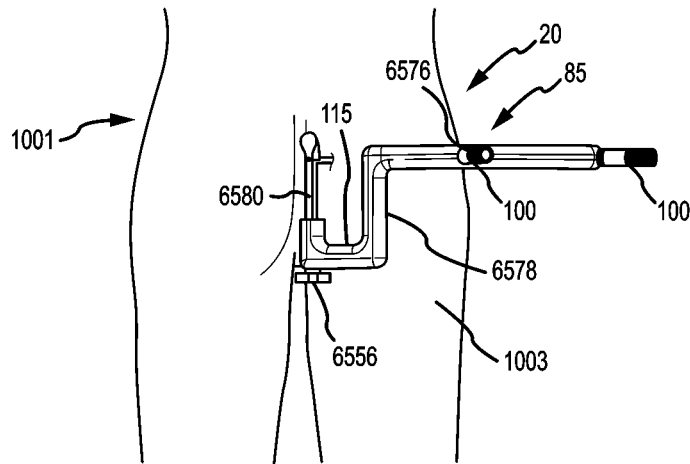


FIG. 133F

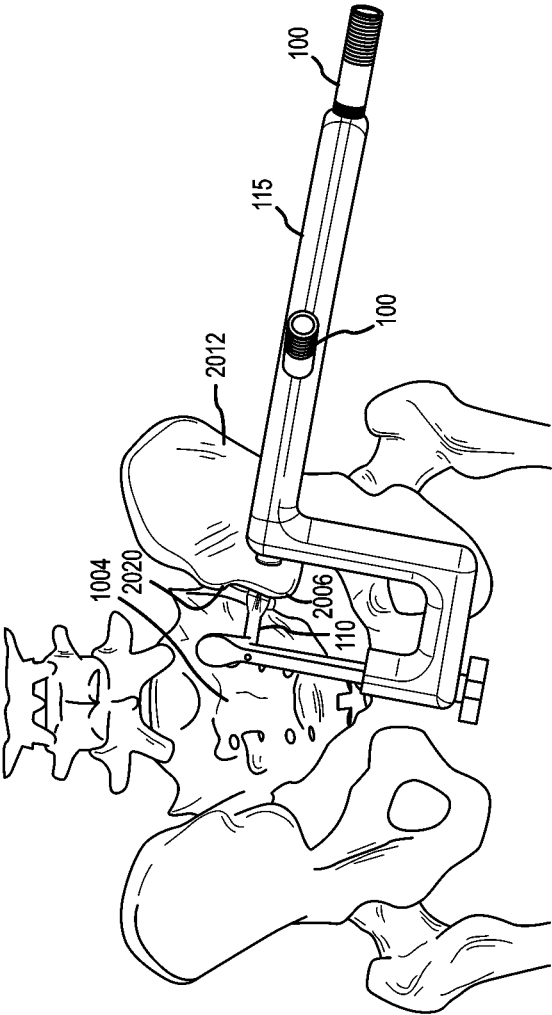
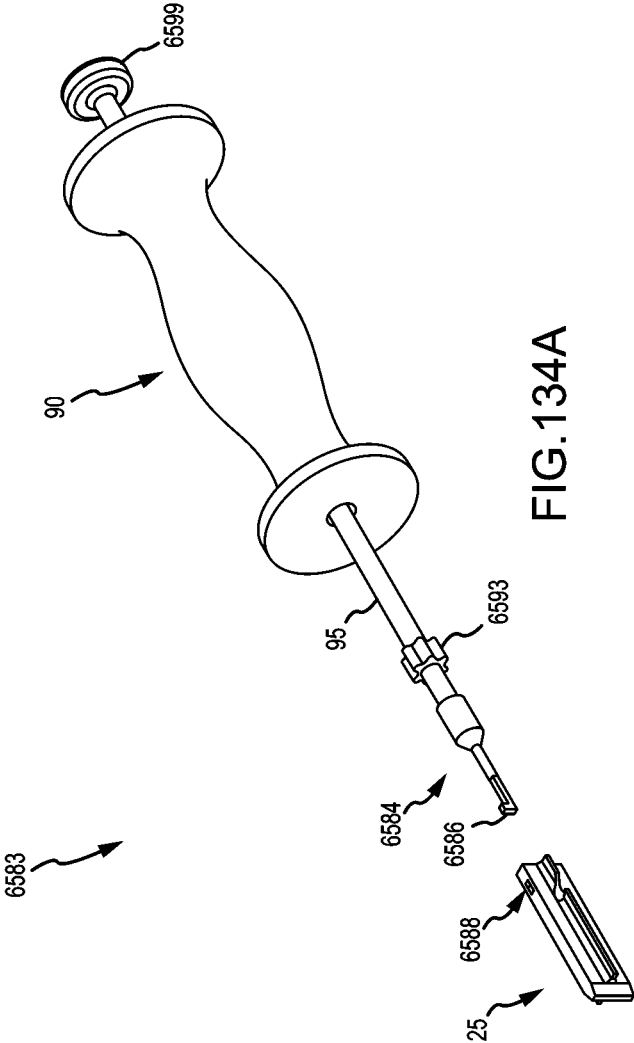


FIG. 133G



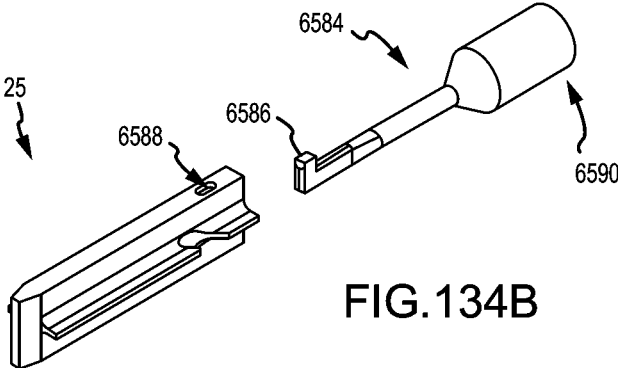


FIG. 134B

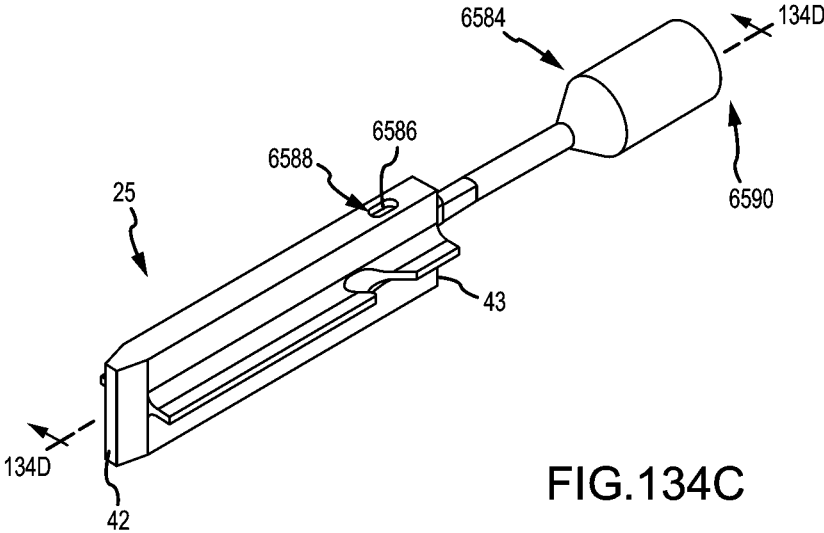


FIG. 134C

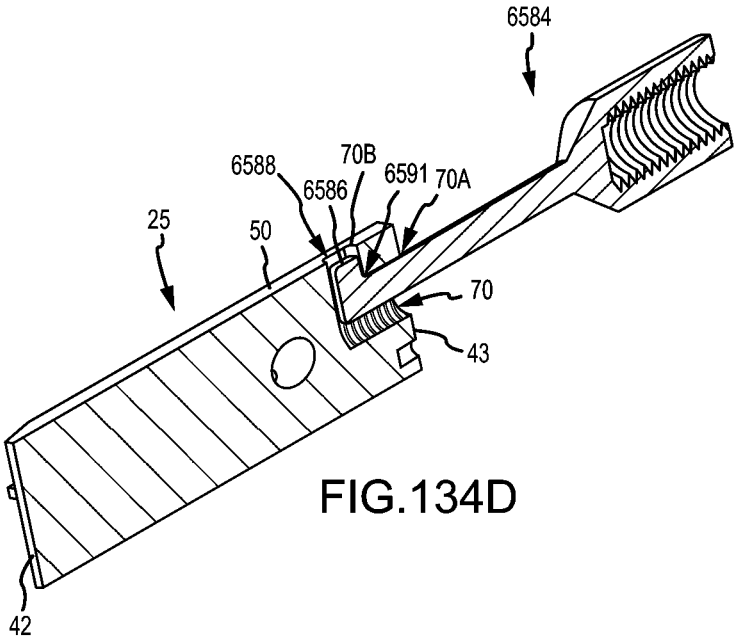


FIG. 134D

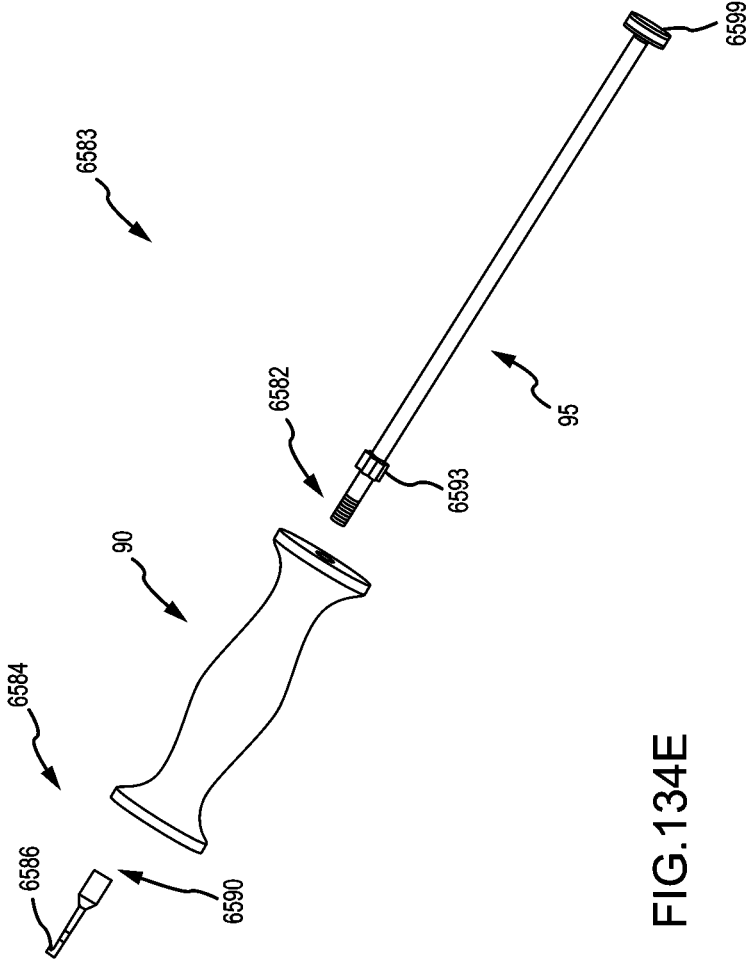


FIG. 134E

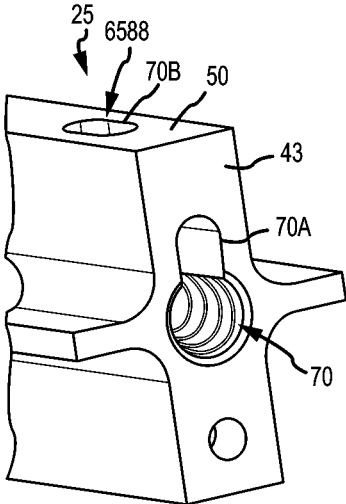


FIG.134F

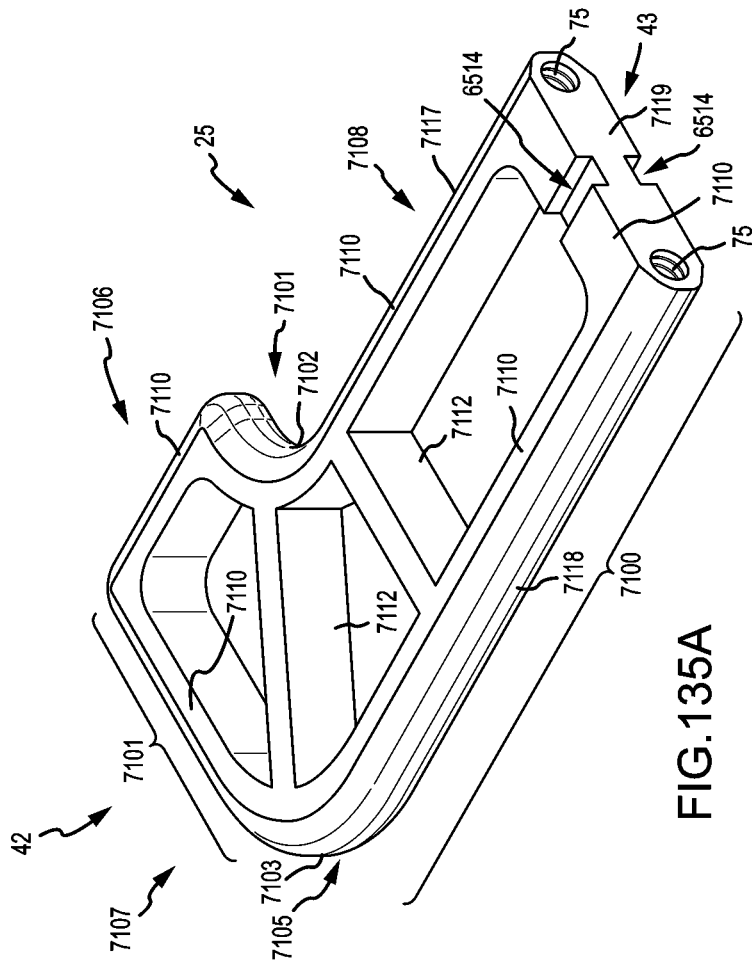


FIG. 135A

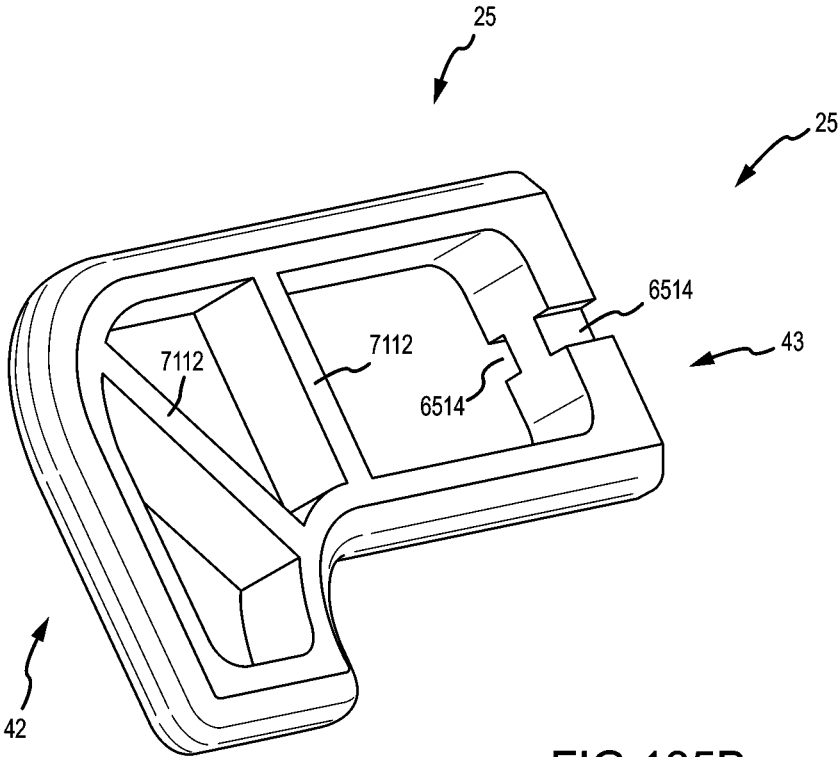


FIG. 135B

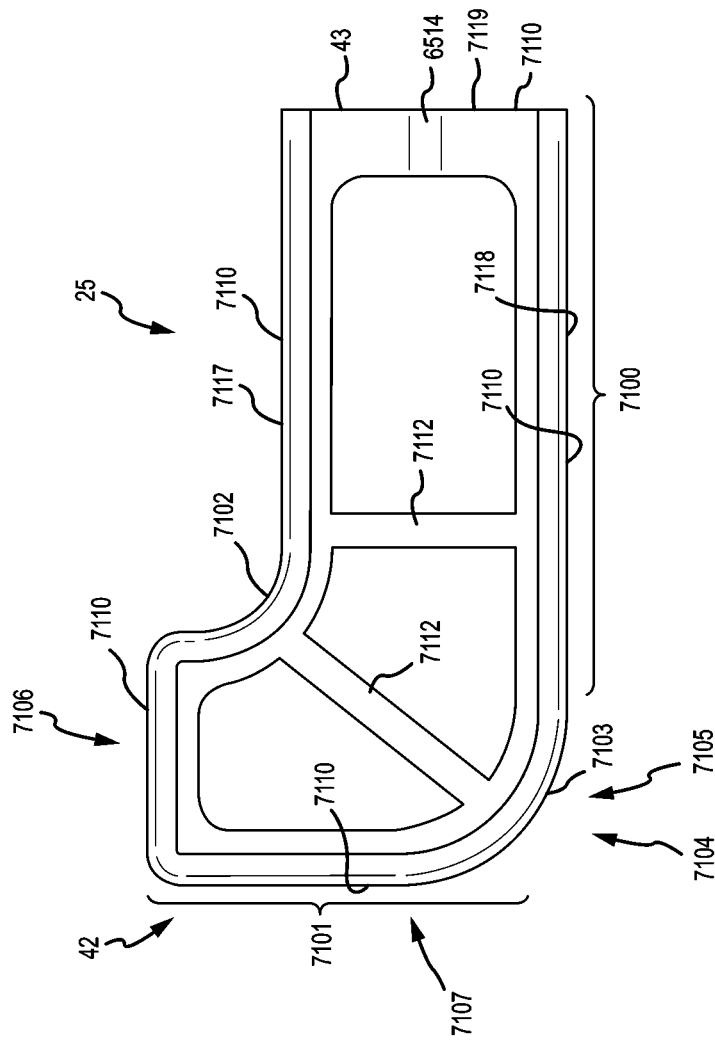


FIG.135C

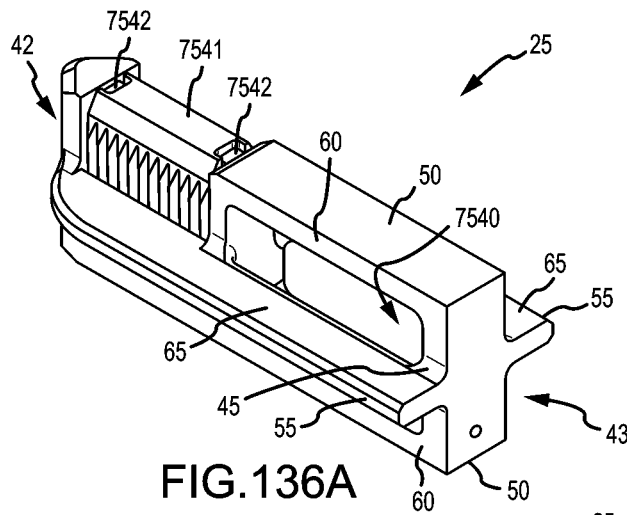


FIG. 136A

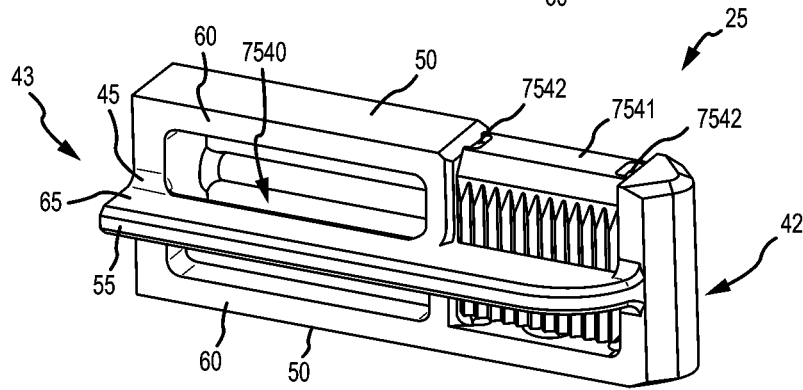


FIG. 136B

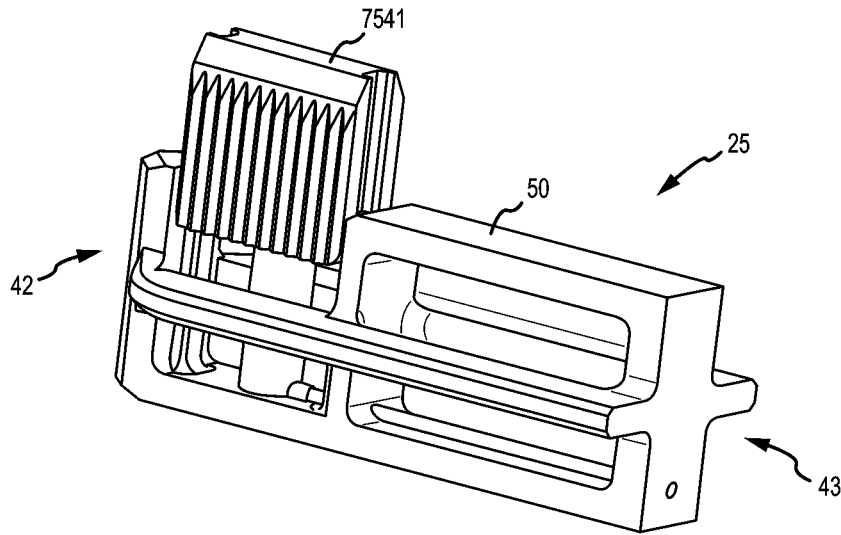


FIG. 136C

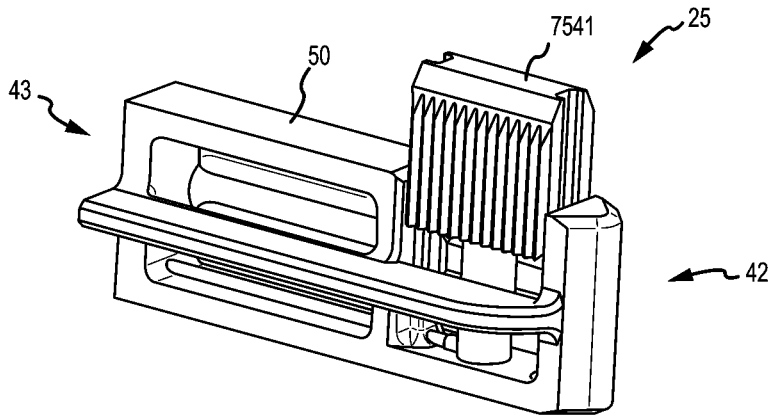


FIG. 136D

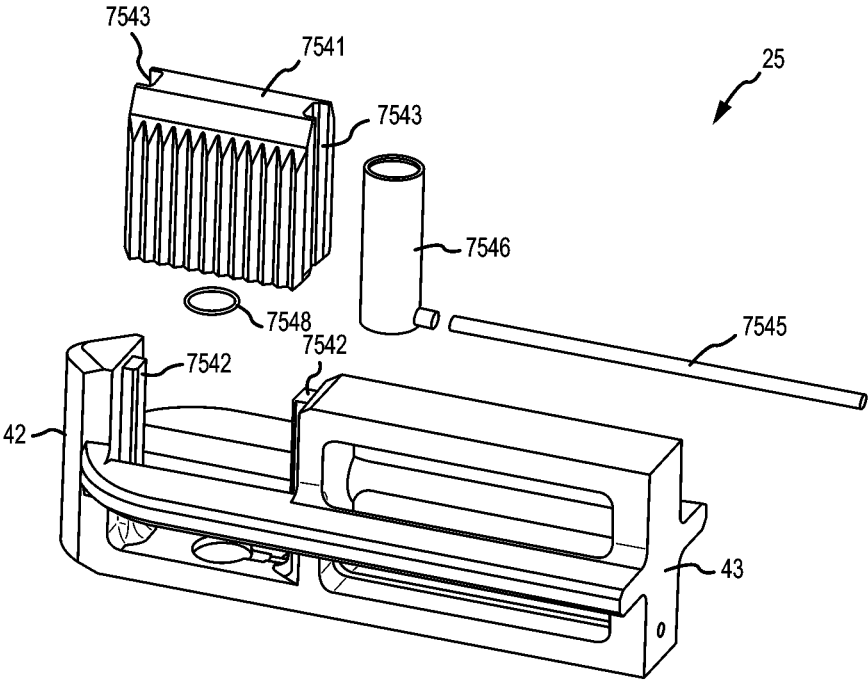


FIG.136E

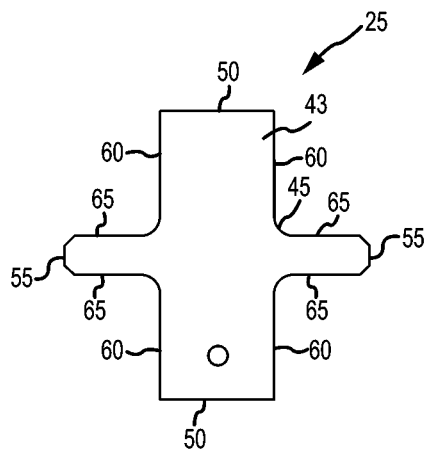


FIG. 136F

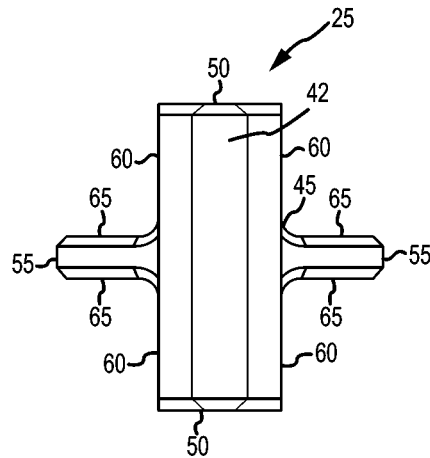


FIG. 136G

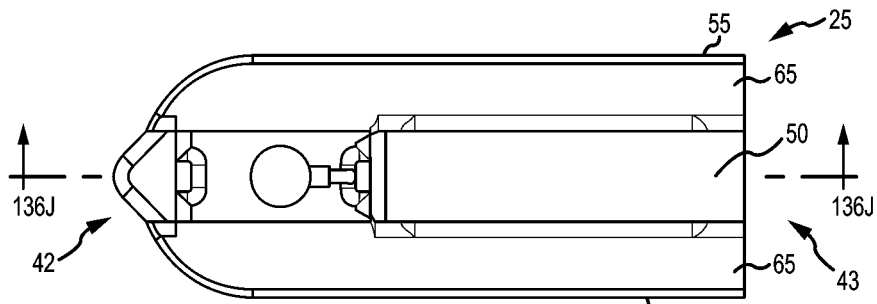


FIG. 136H

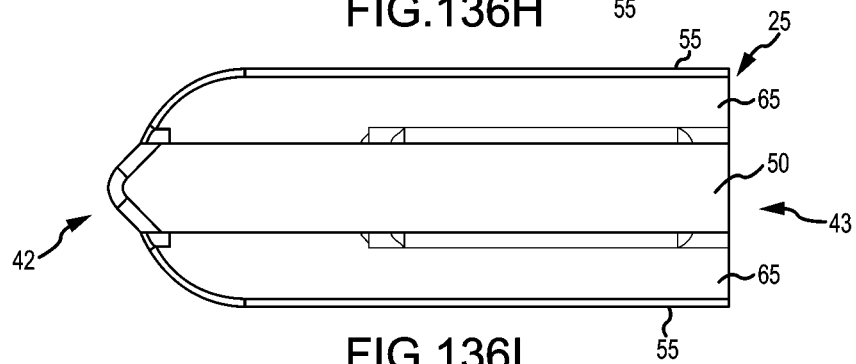


FIG. 136I

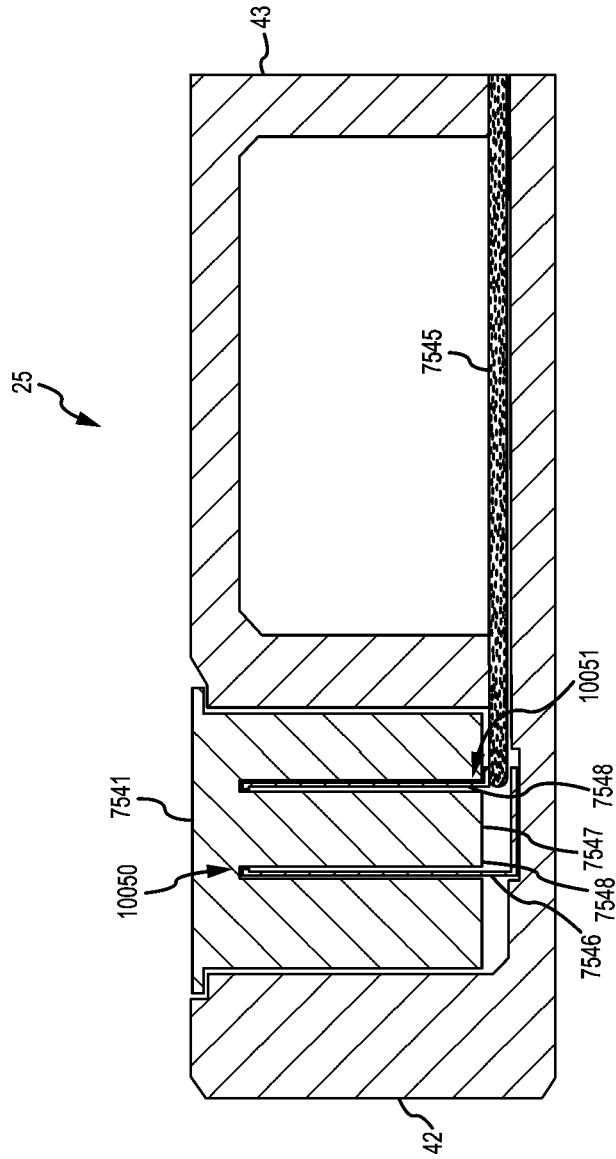


FIG. 136J

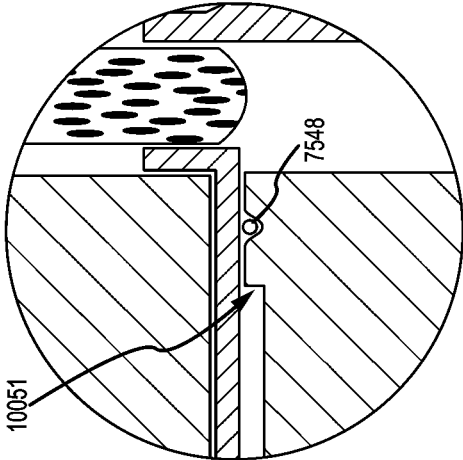


FIG. 136L

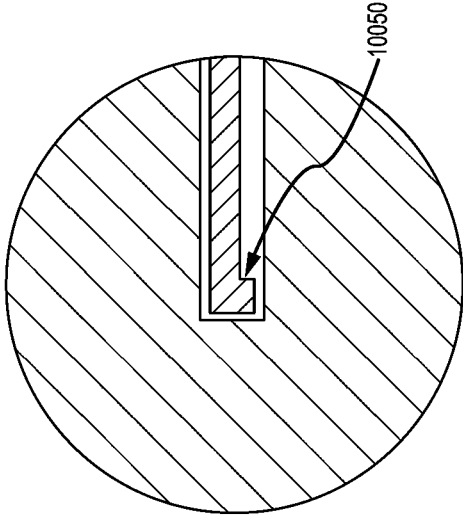


FIG. 136K

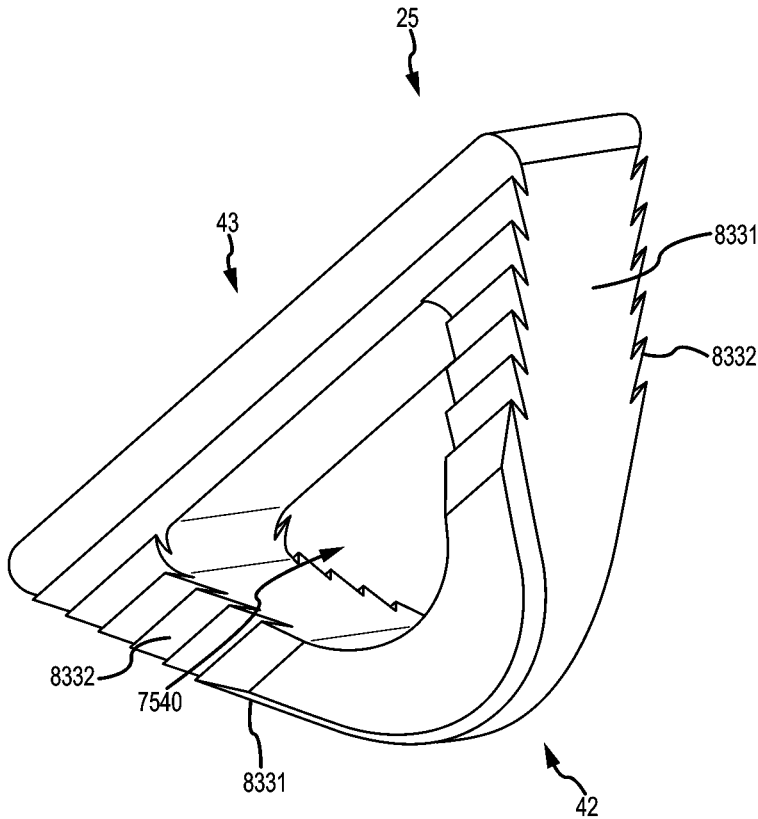


FIG.137A

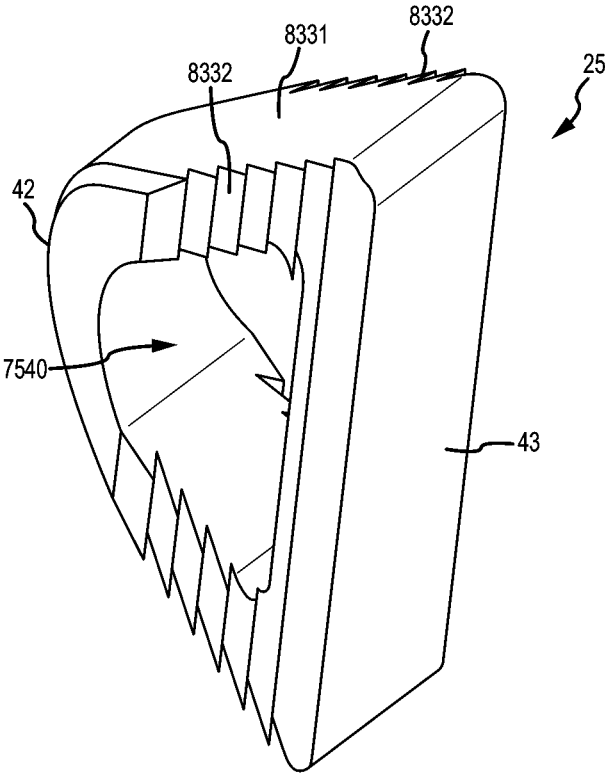


FIG.137B

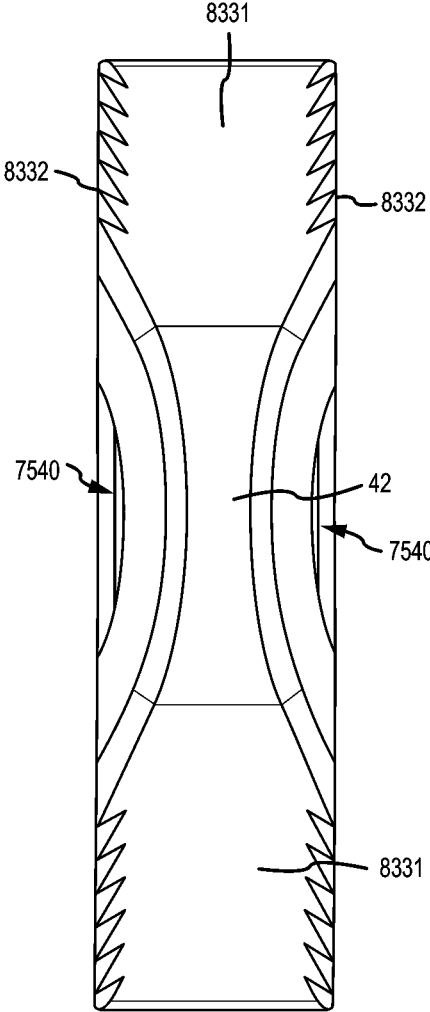


FIG.137D

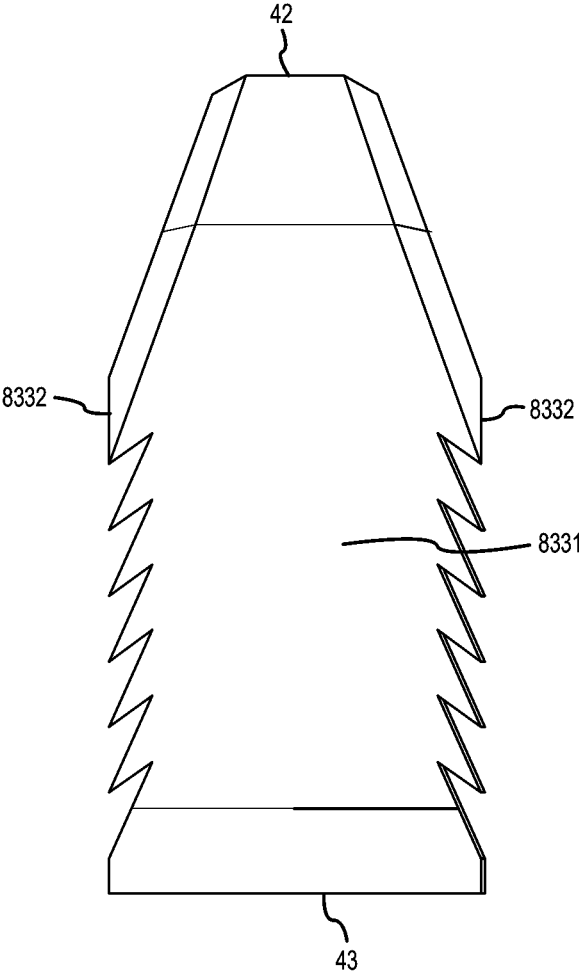


FIG.137E

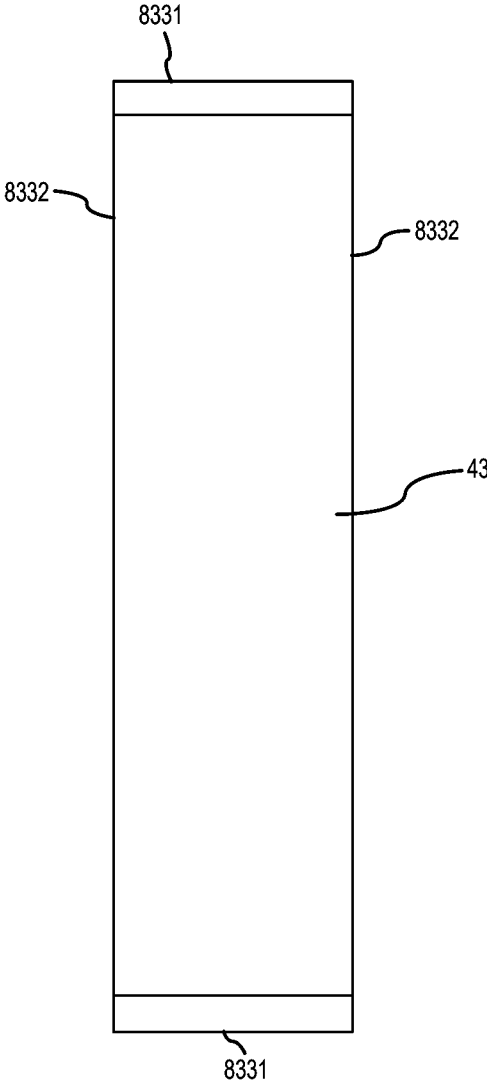


FIG.137F

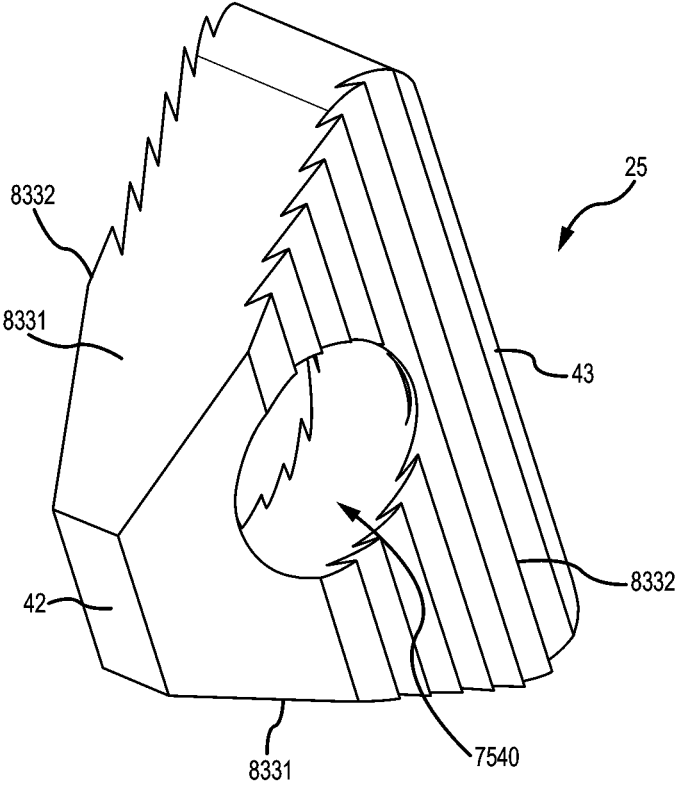


FIG.138A

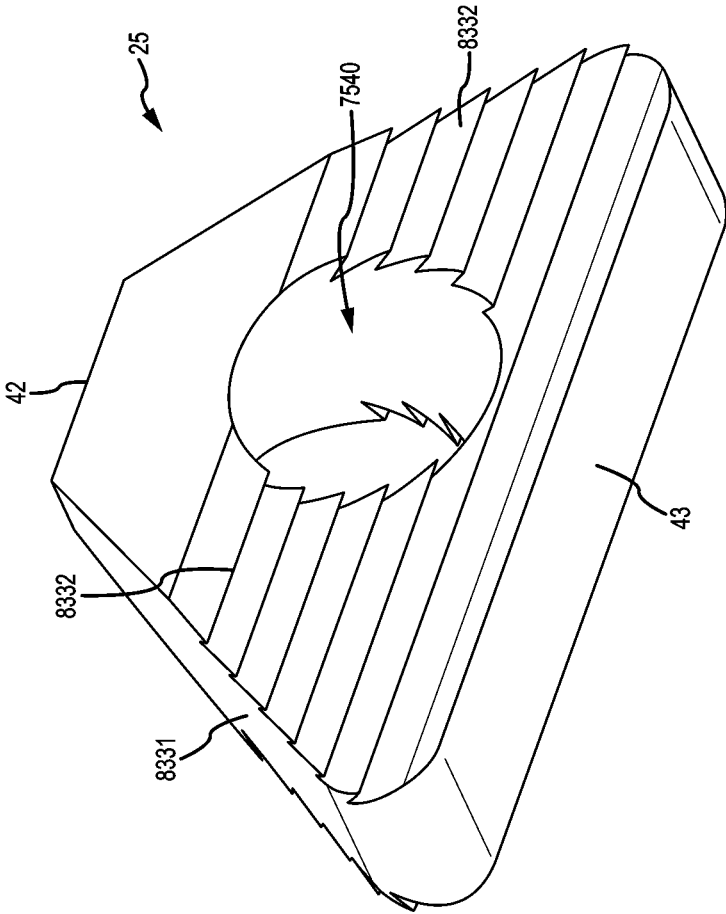


FIG. 138B

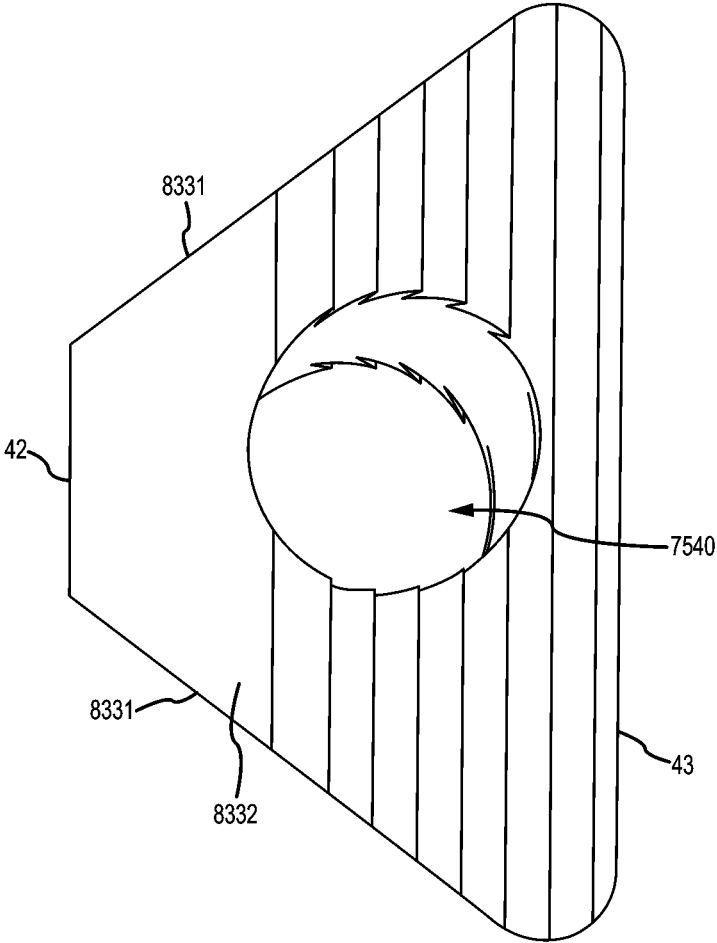


FIG.138C

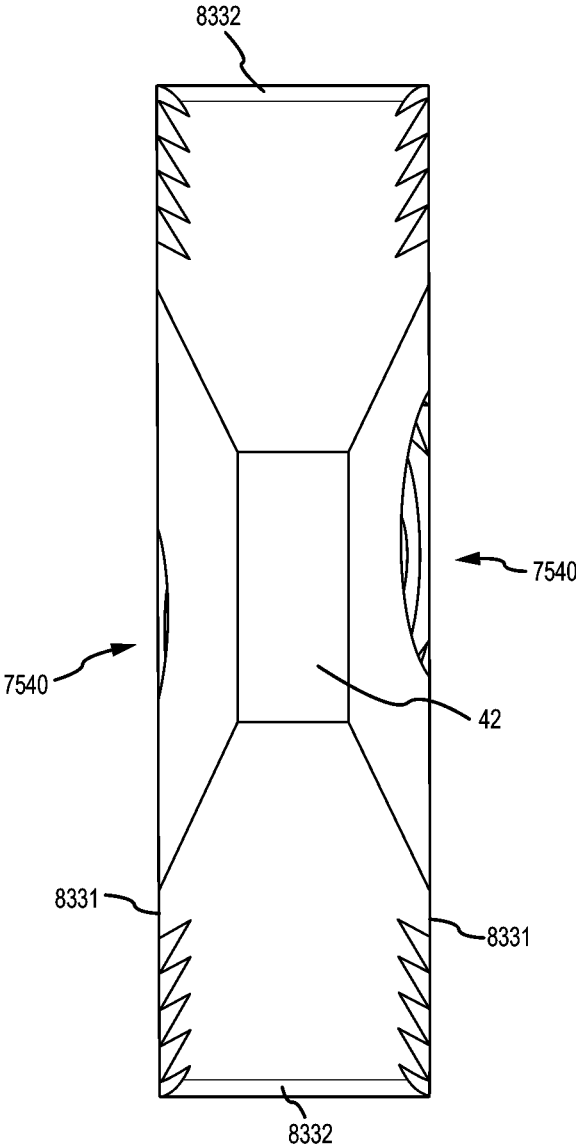


FIG.138D

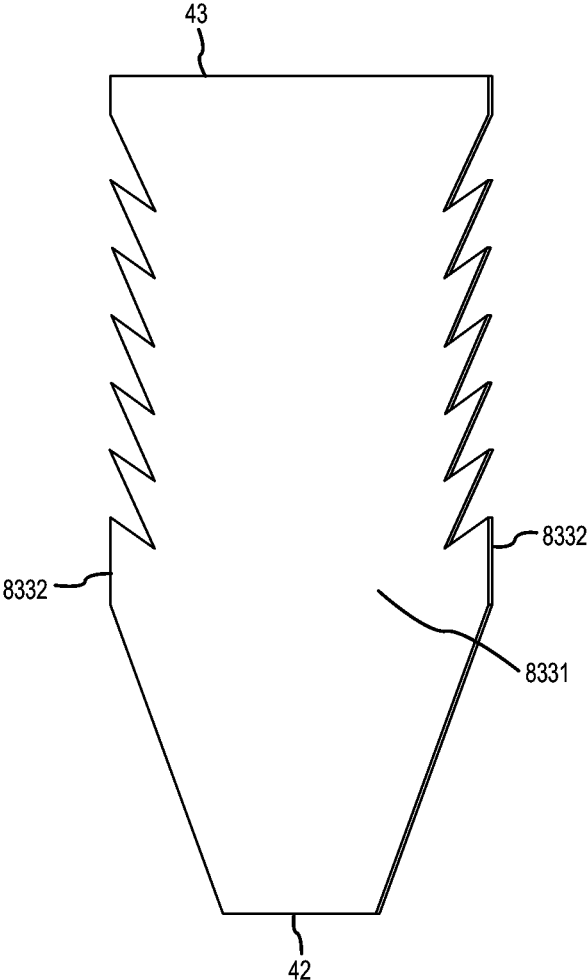


FIG. 138E

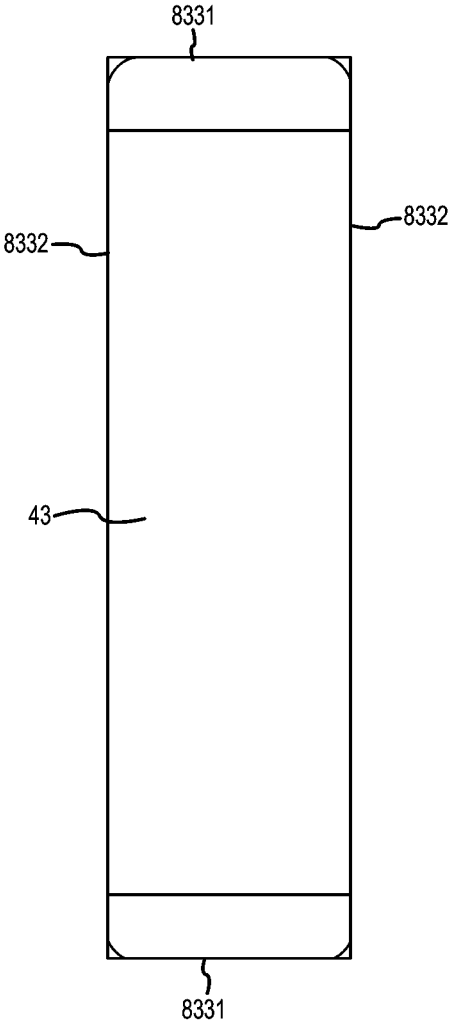


FIG. 138F

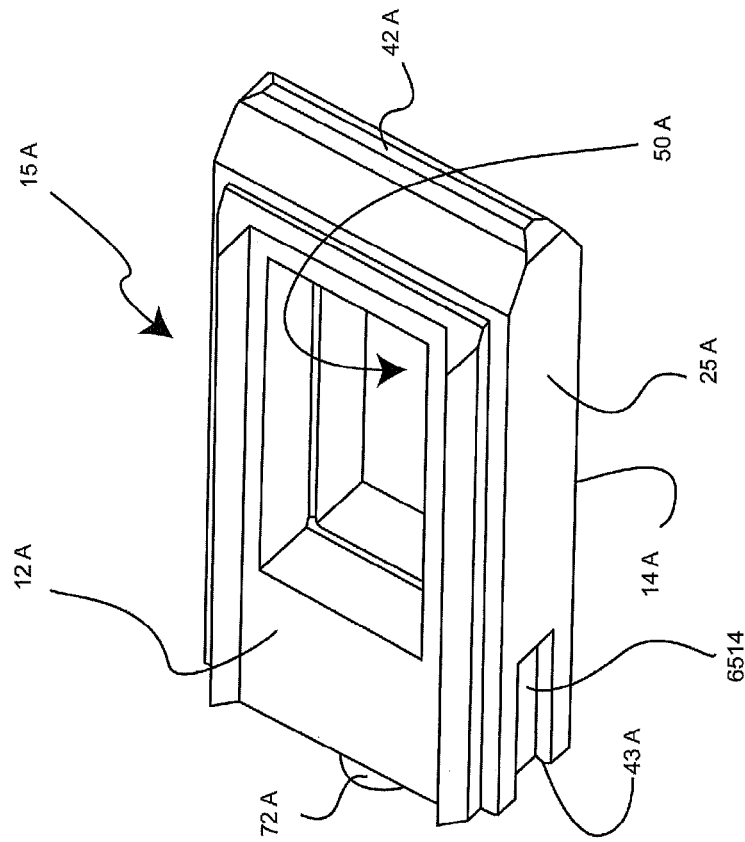


FIG. 139

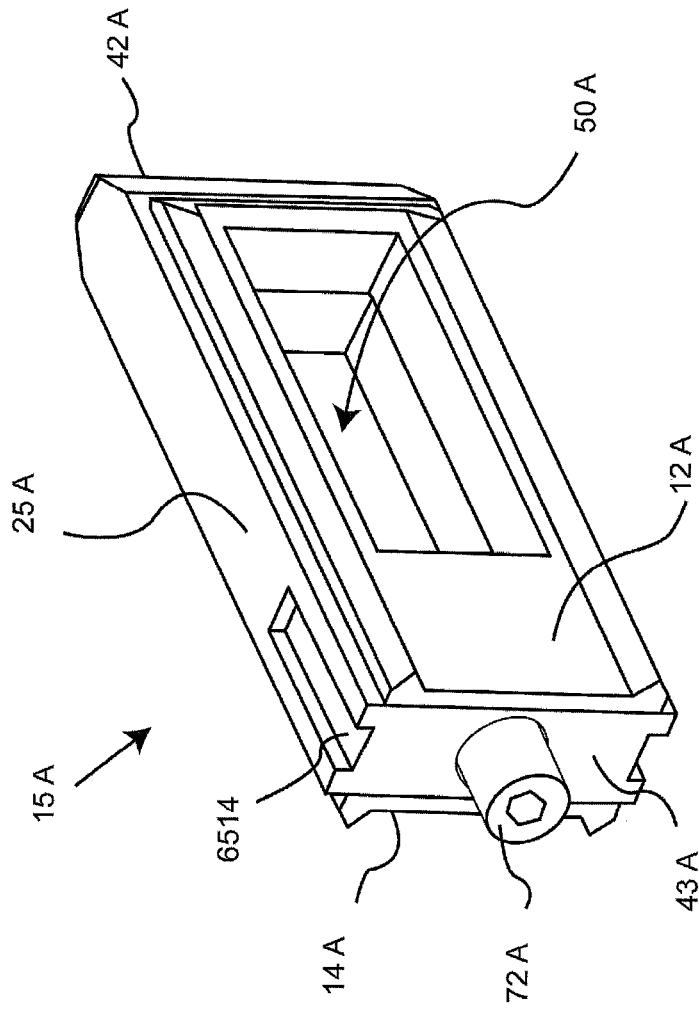


FIG. 140

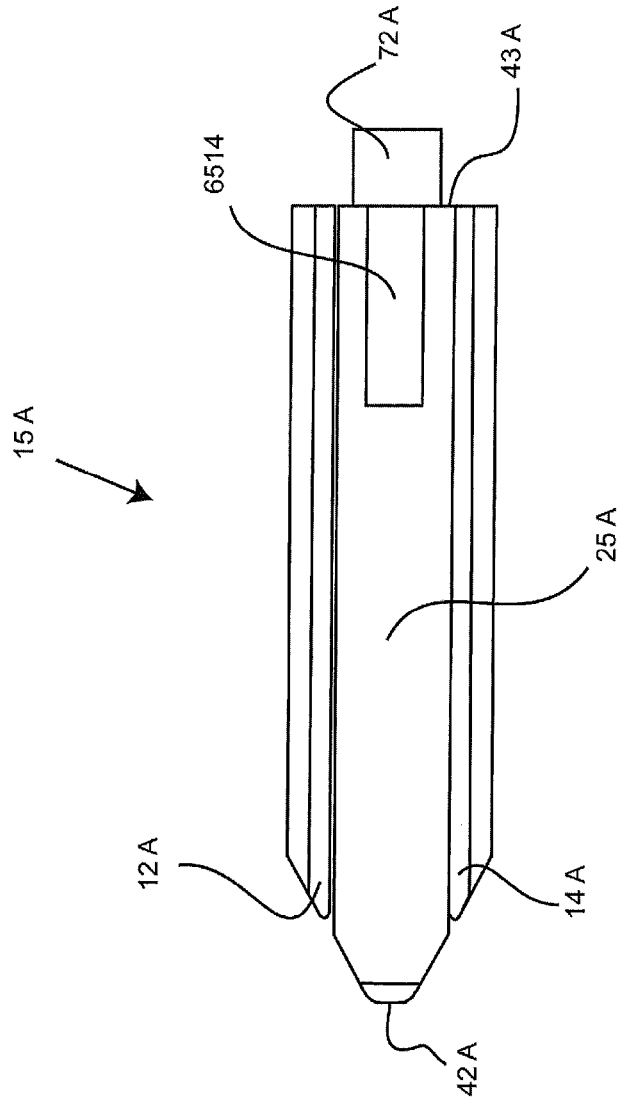


FIG. 141

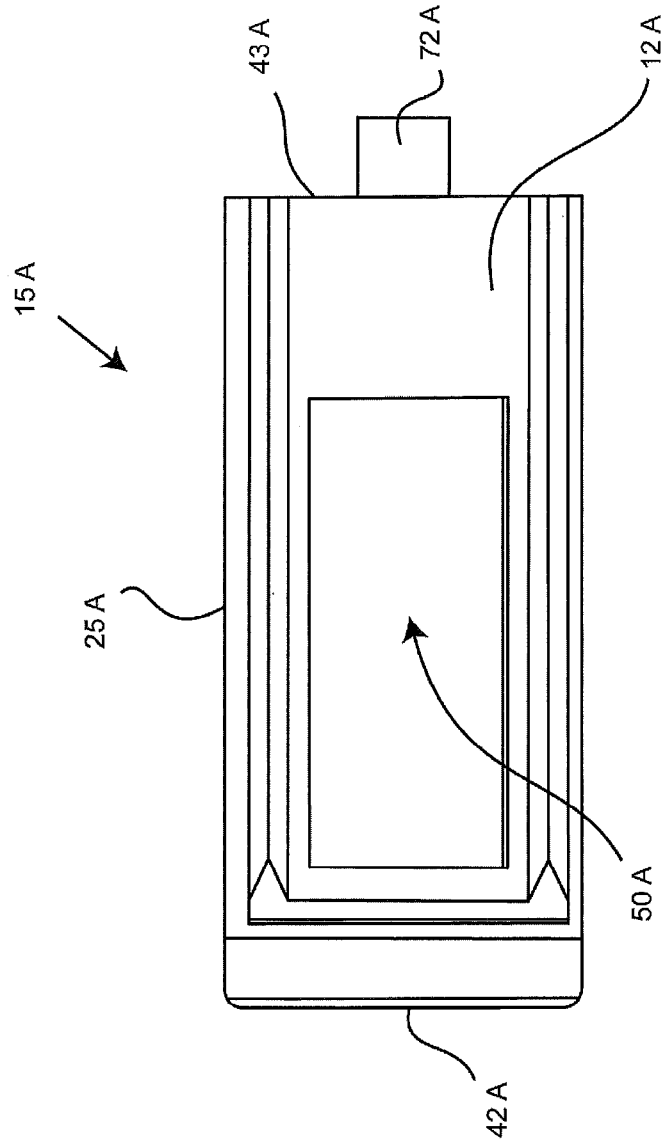


FIG. 142

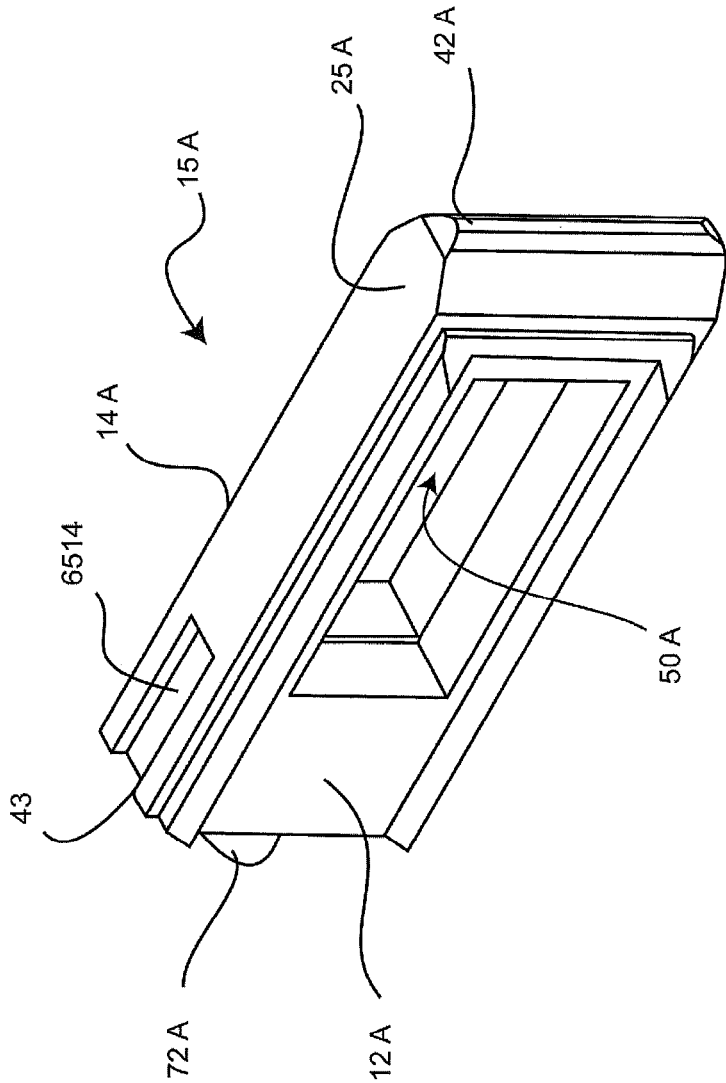


FIG. 143

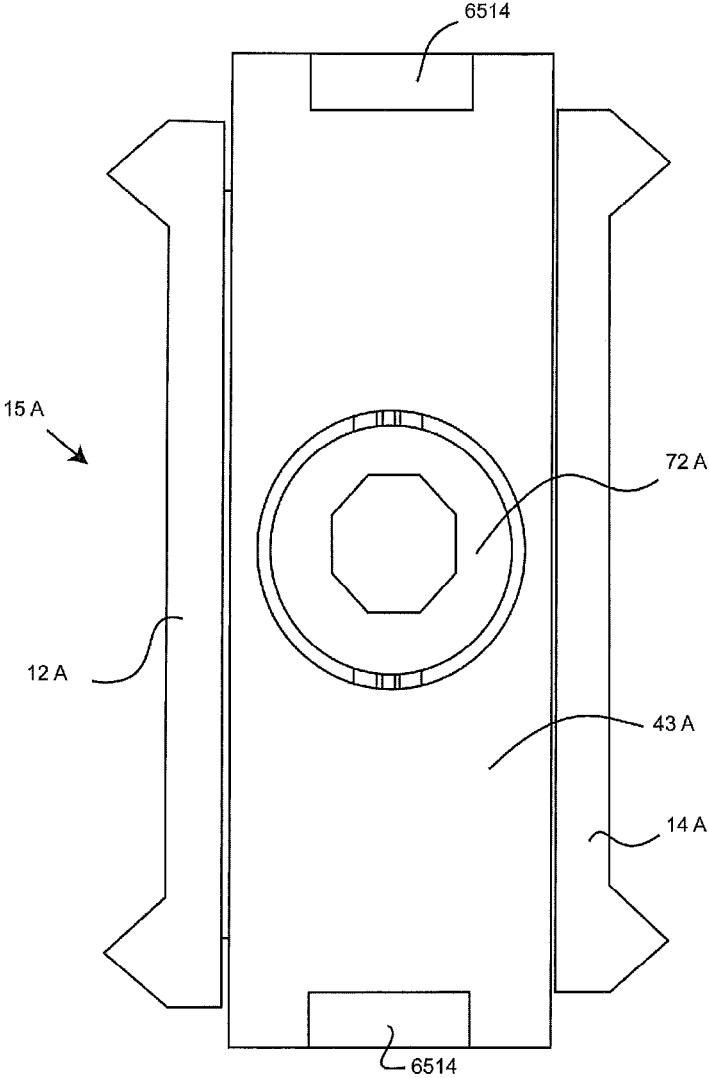


FIG. 144

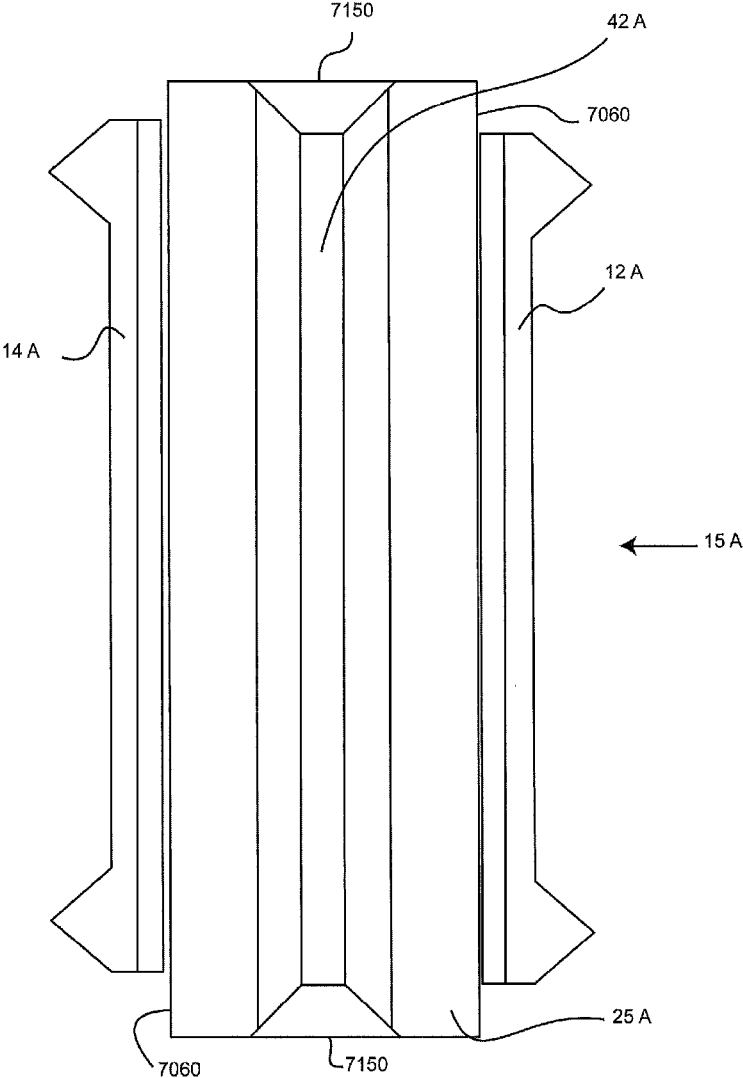


FIG. 145

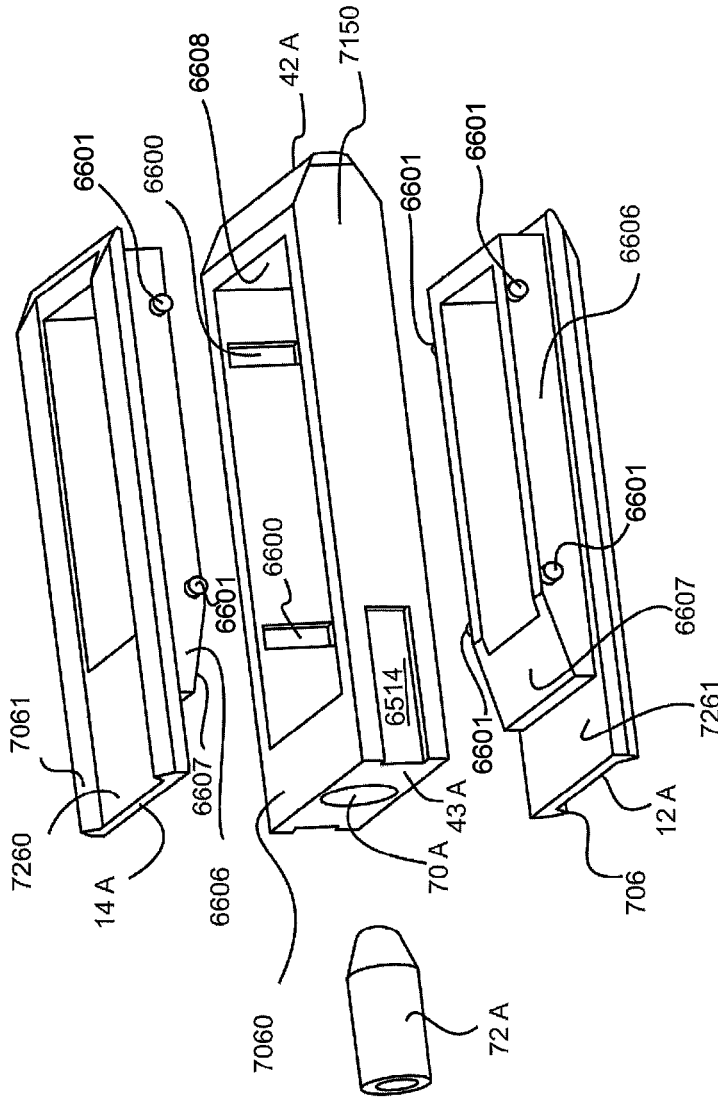


FIG. 147

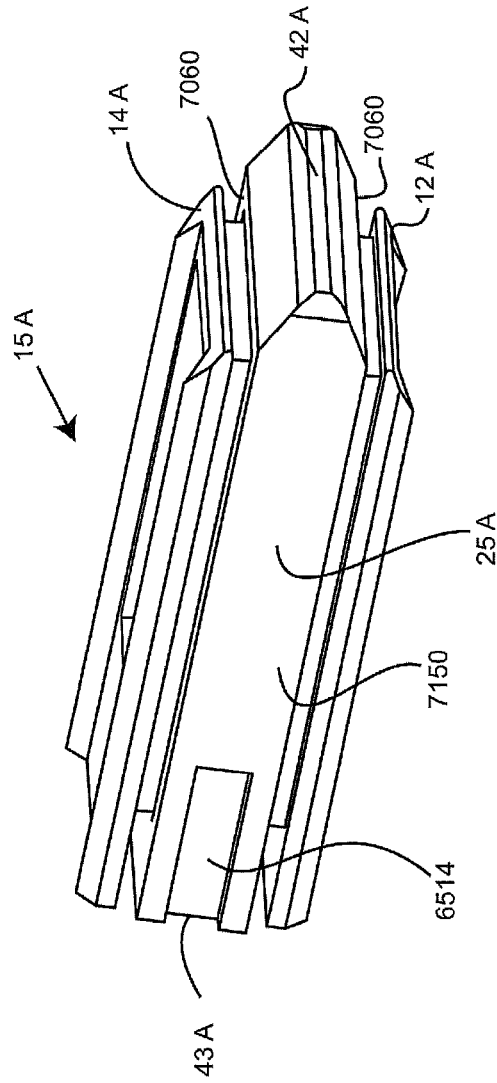


FIG. 148

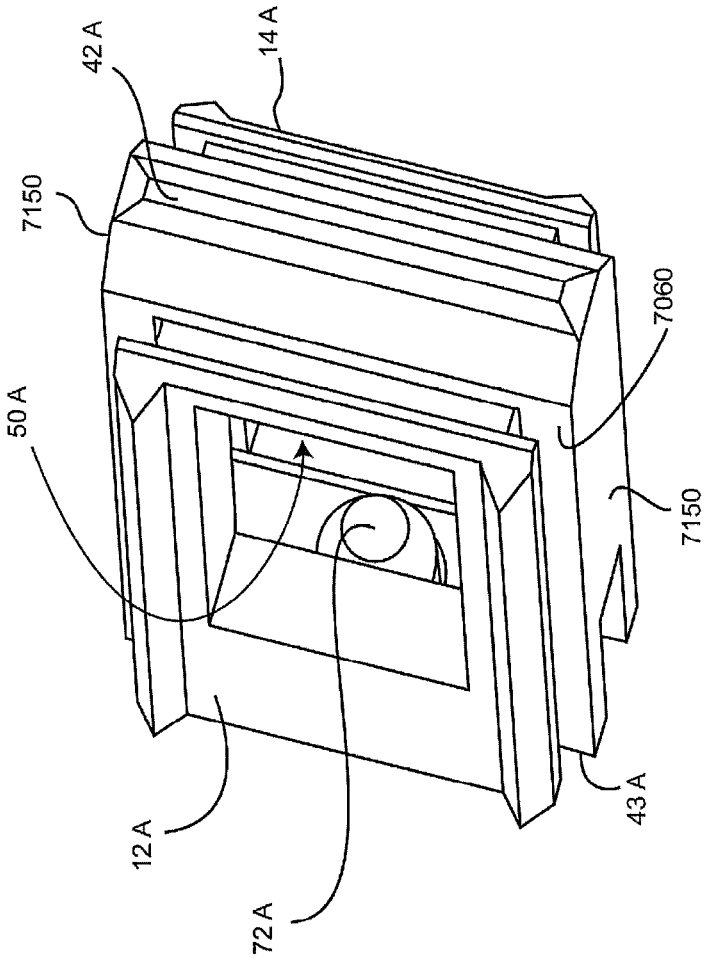


FIG. 149

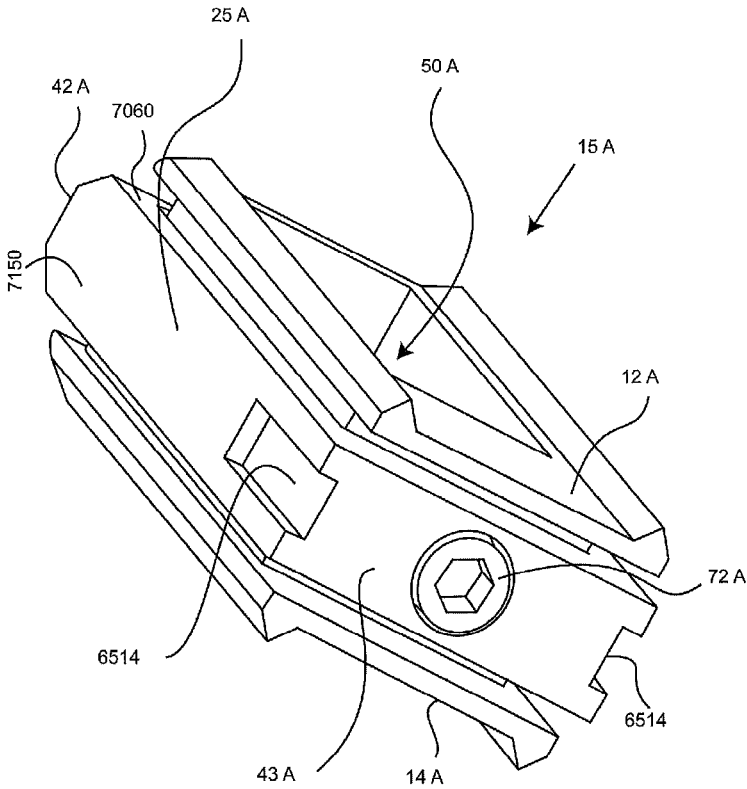


FIG. 150

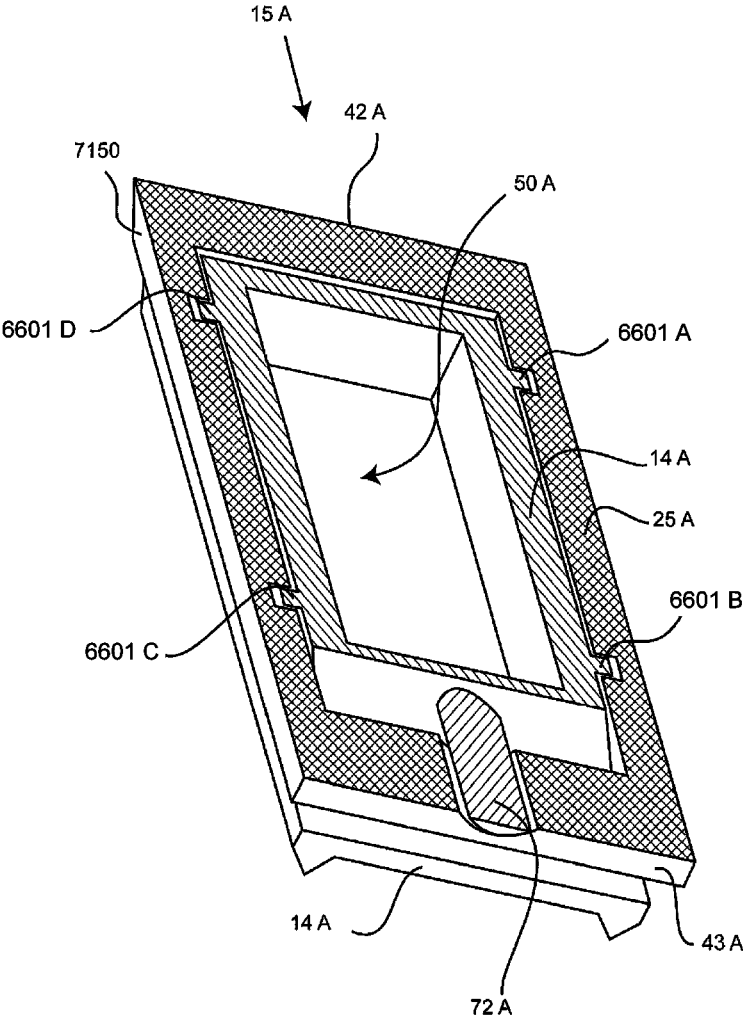


FIG. 151

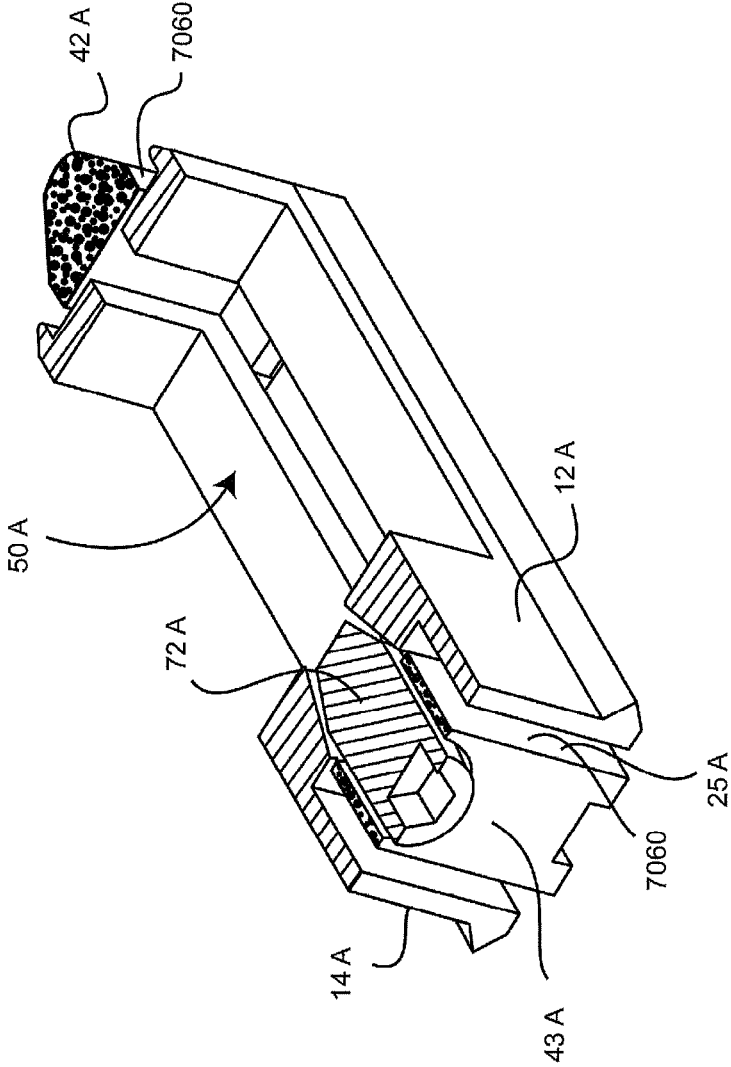


FIG. 152

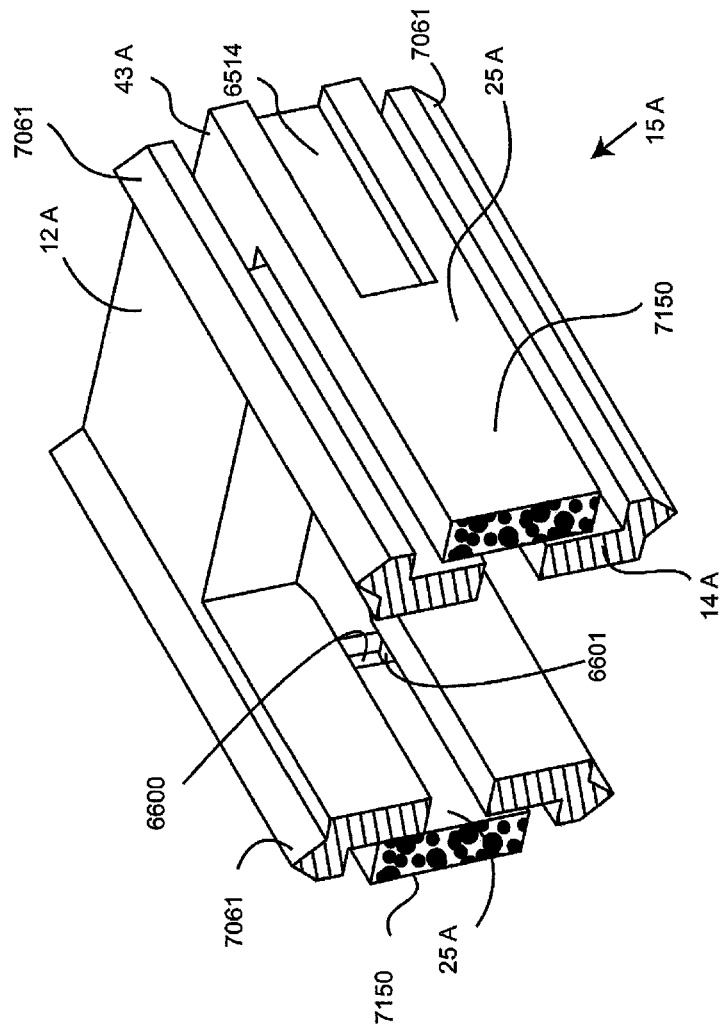


FIG. 153

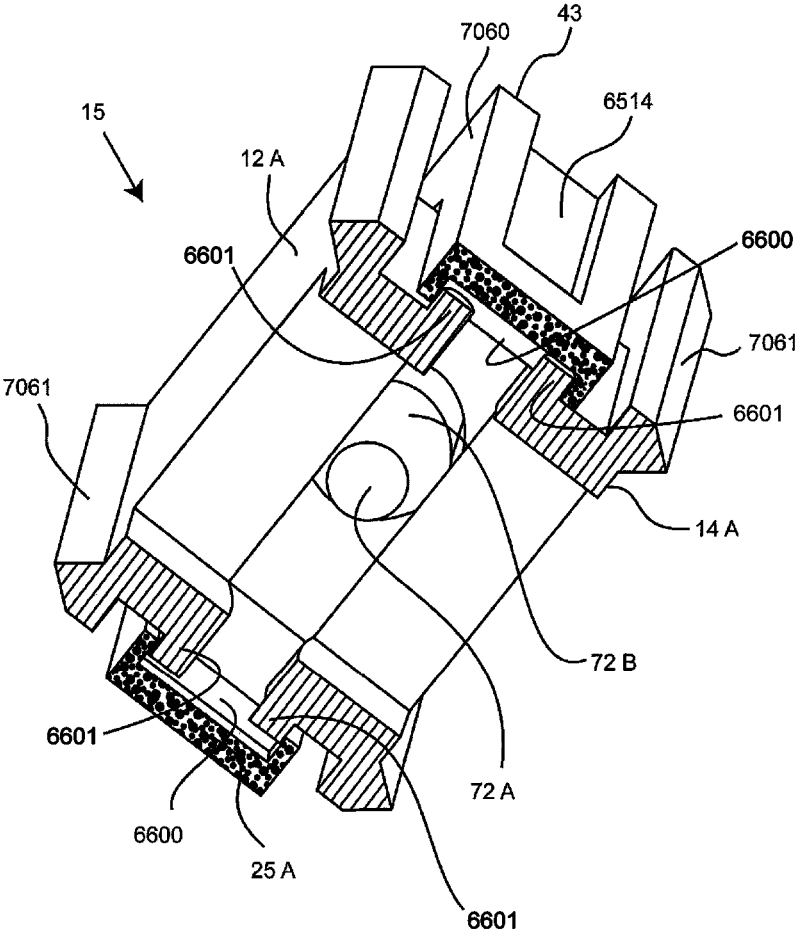


FIG. 154

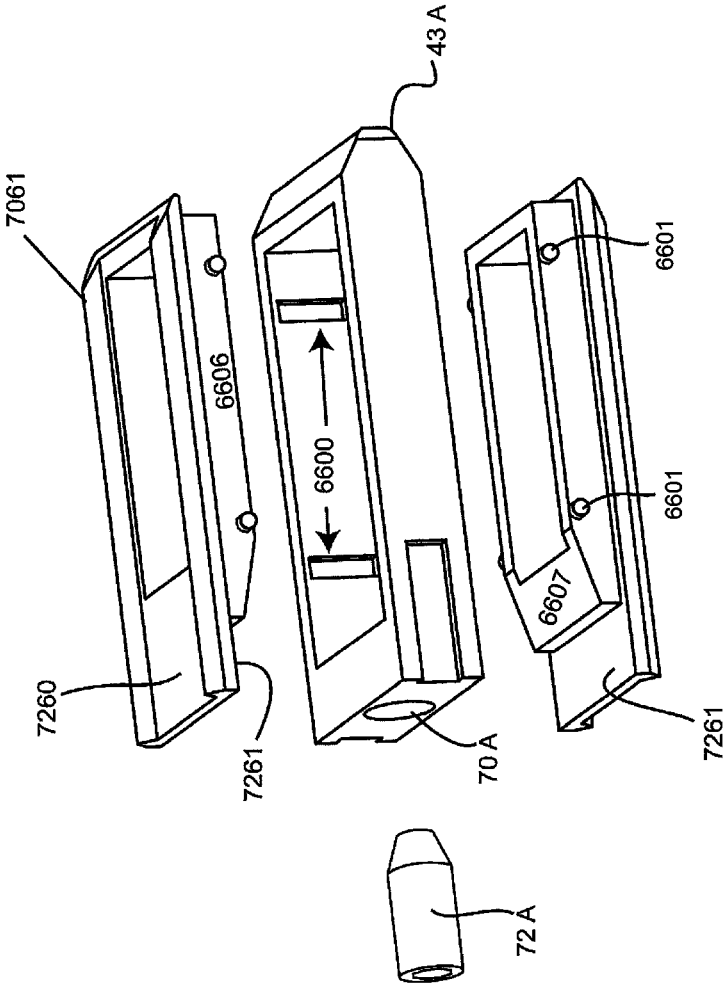


FIG. 156

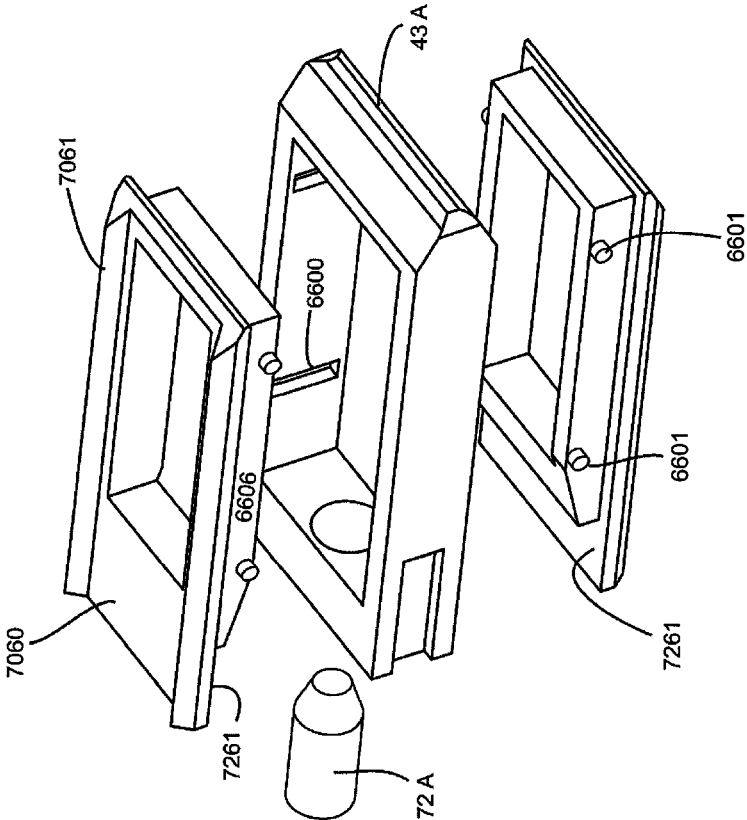


FIG. 157

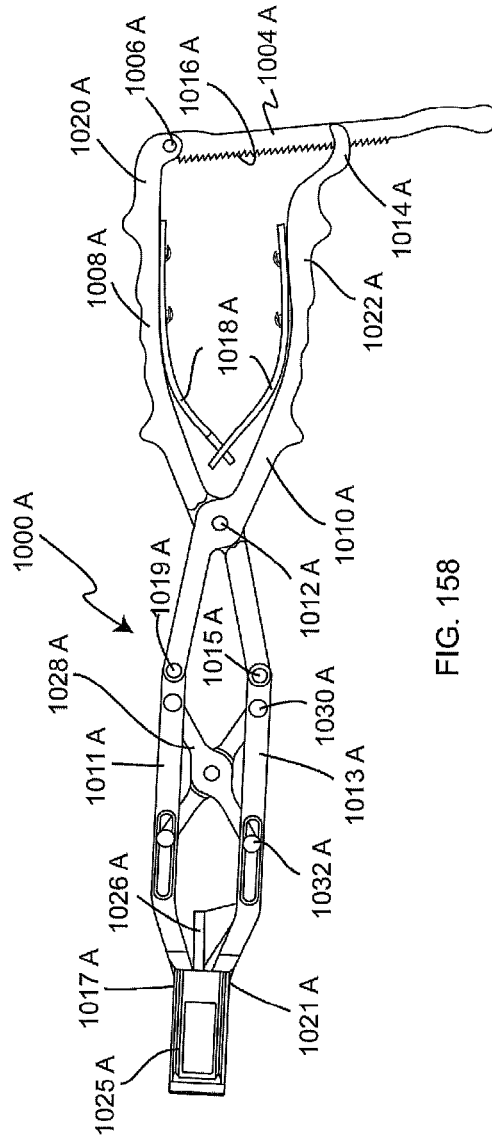


FIG. 158

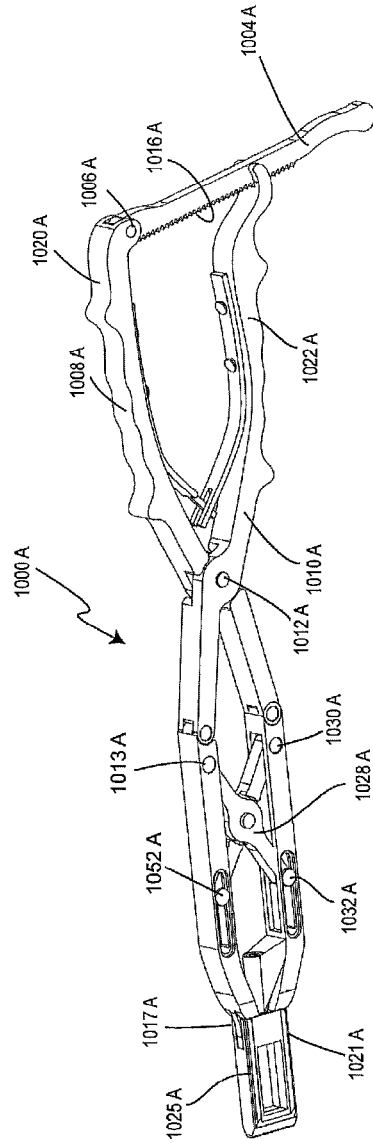


FIG. 159

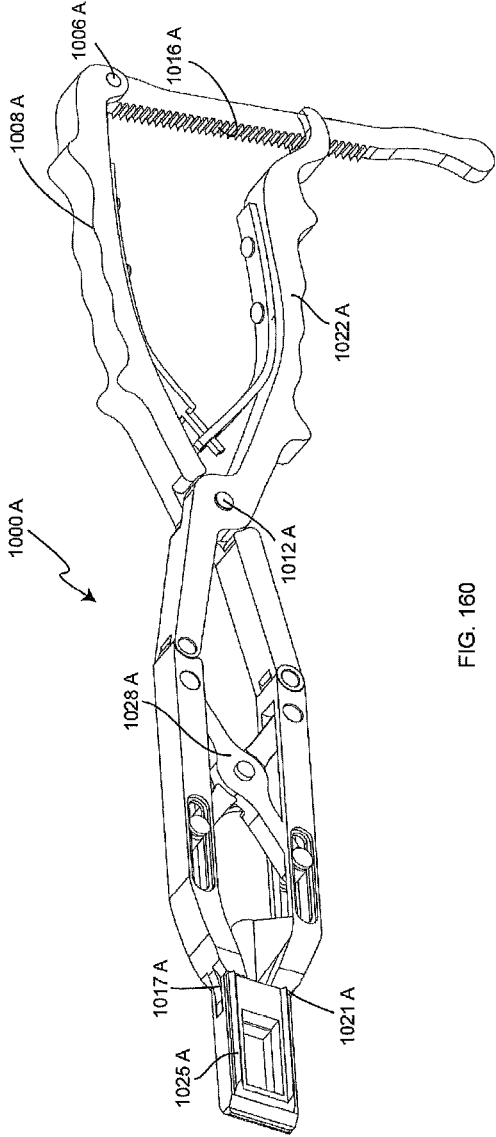


FIG. 160

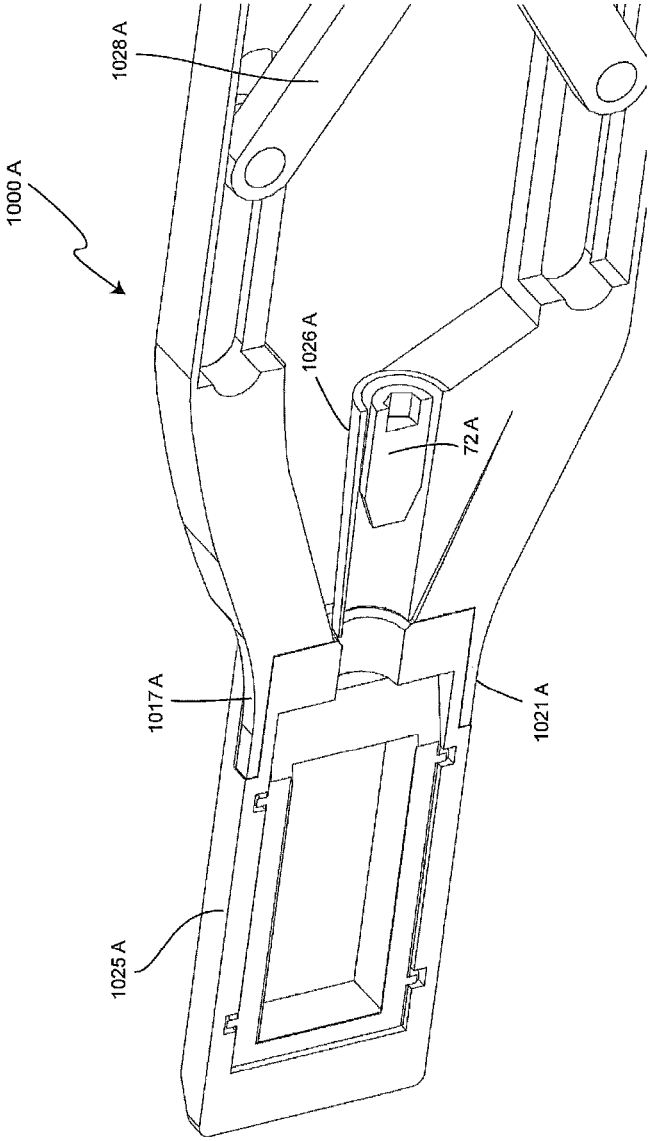


FIG. 161

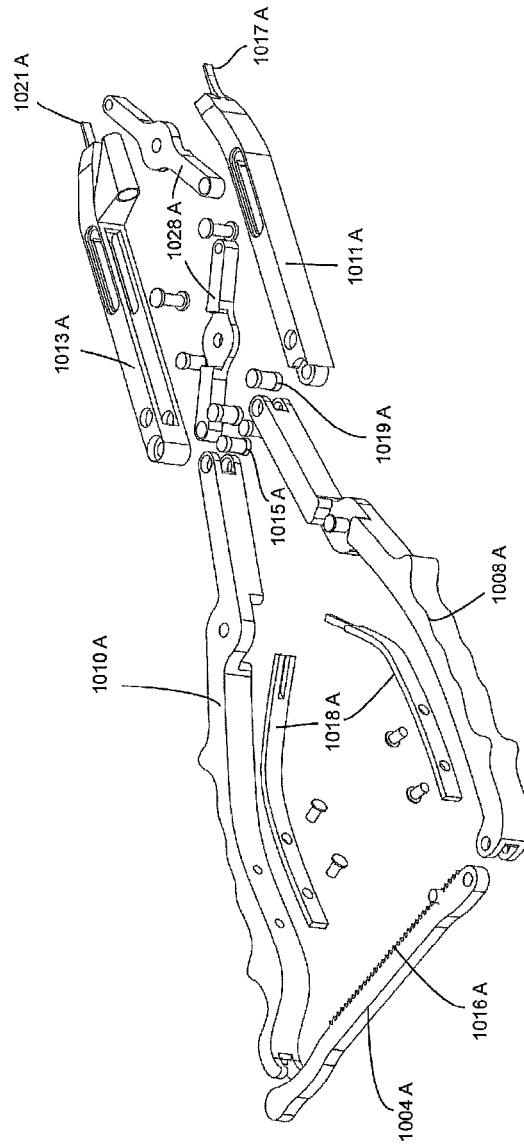


FIG. 162

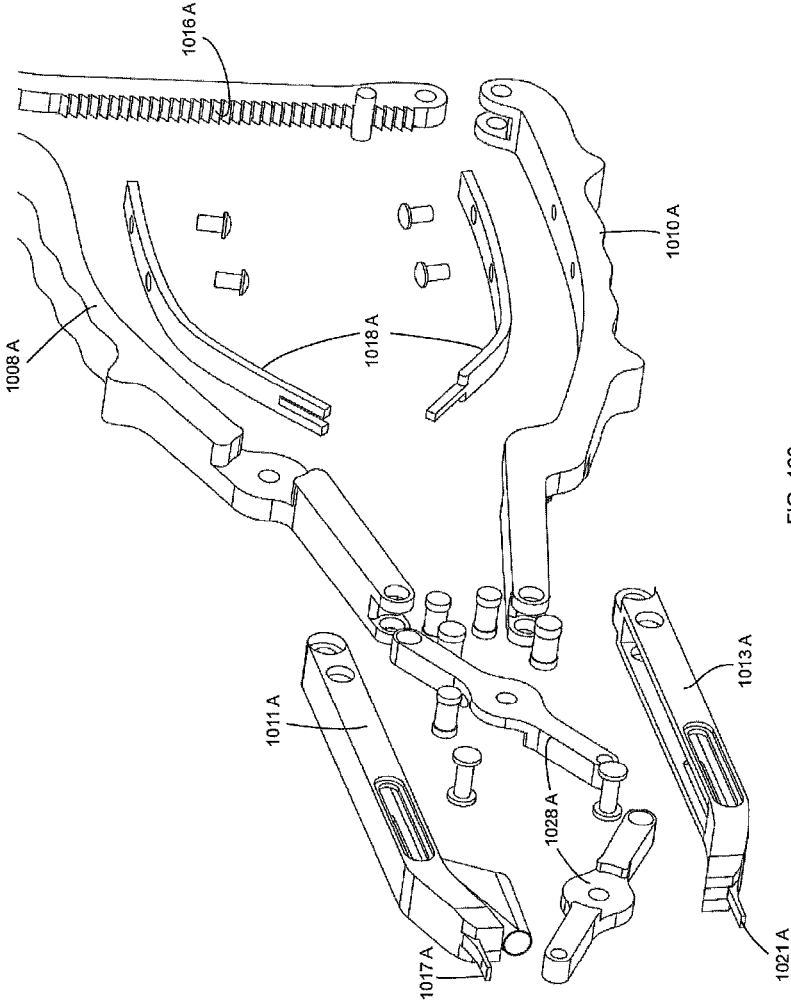


FIG. 163

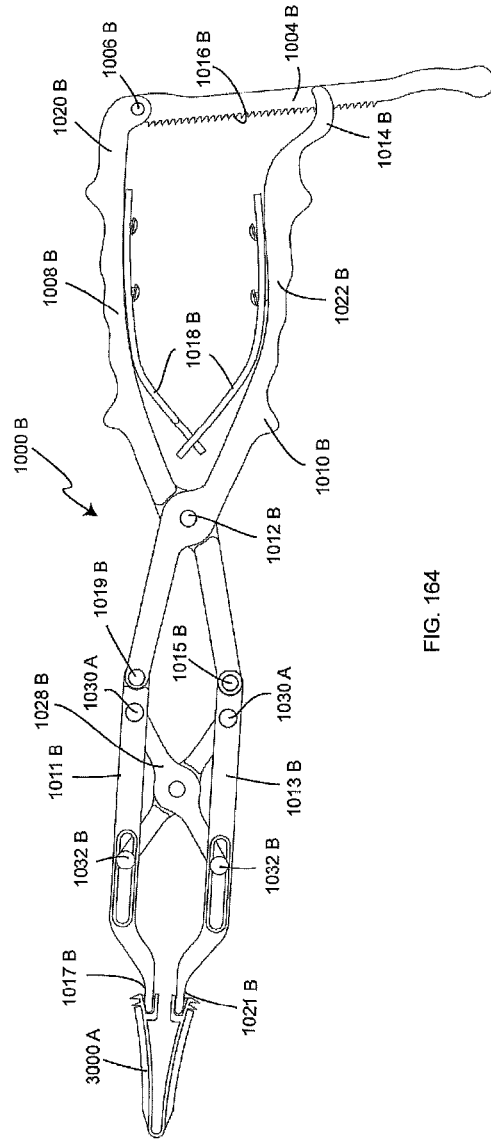


FIG. 164

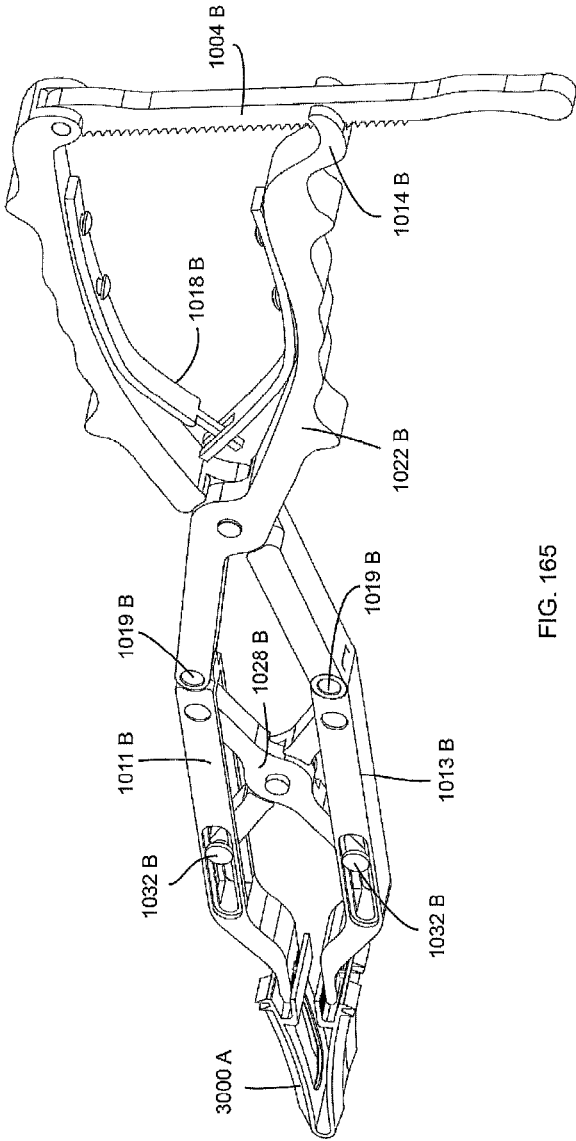


FIG. 165

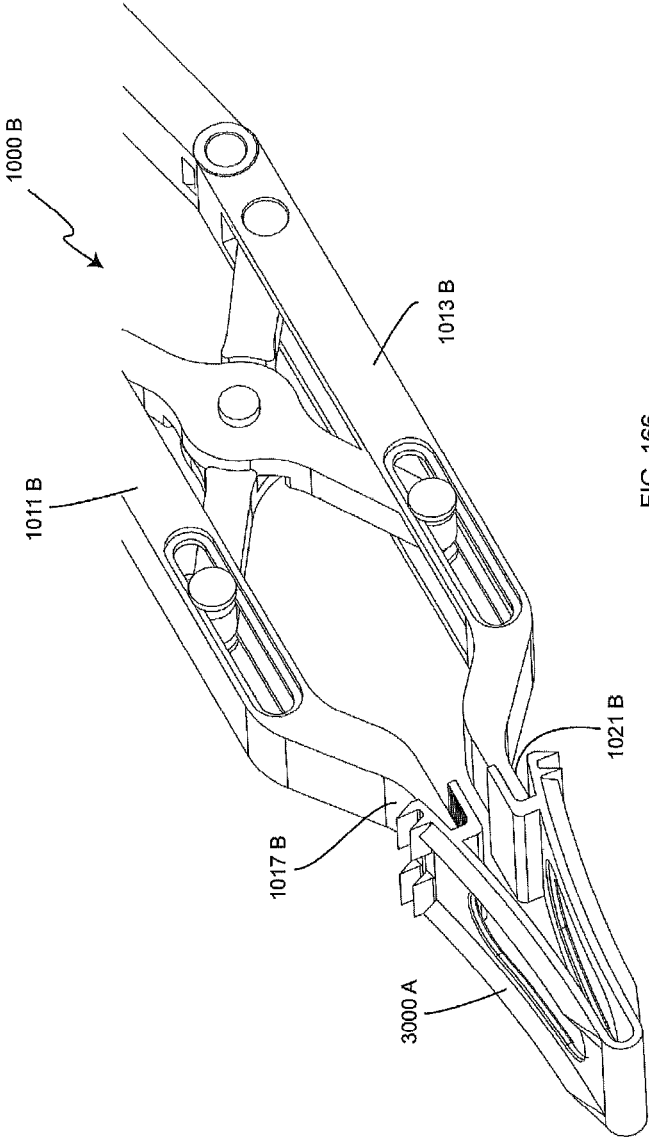


FIG. 166

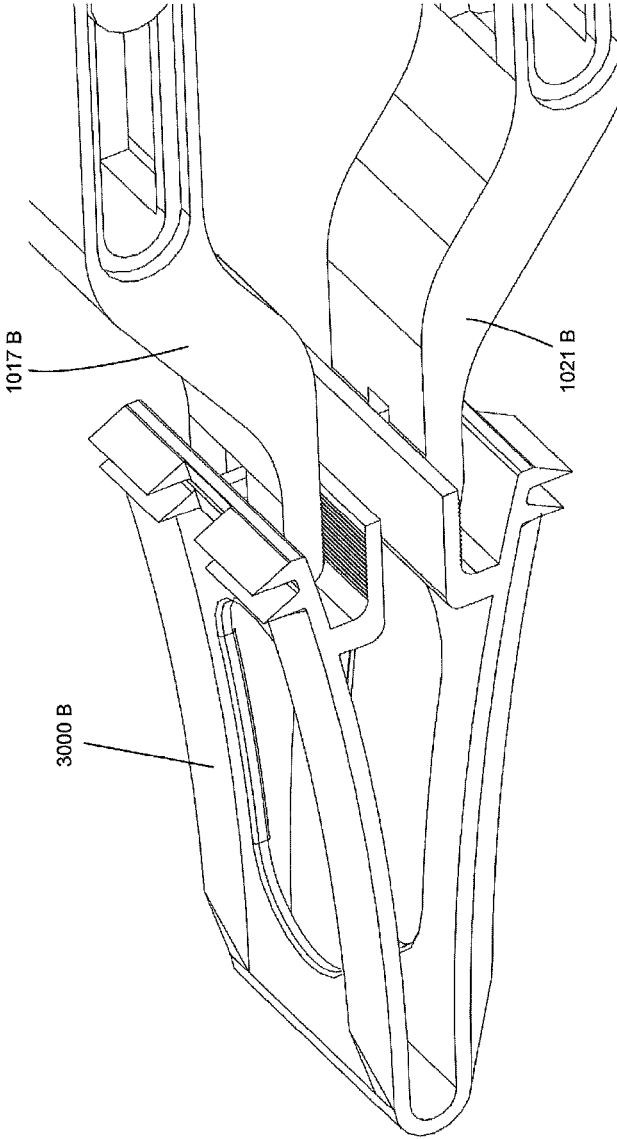


FIG. 167

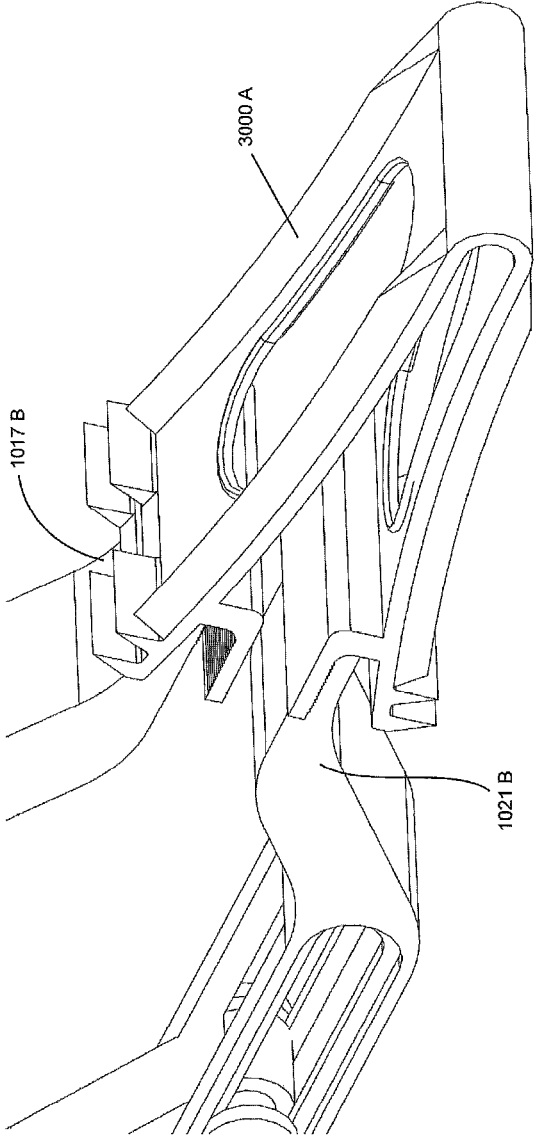


FIG. 168

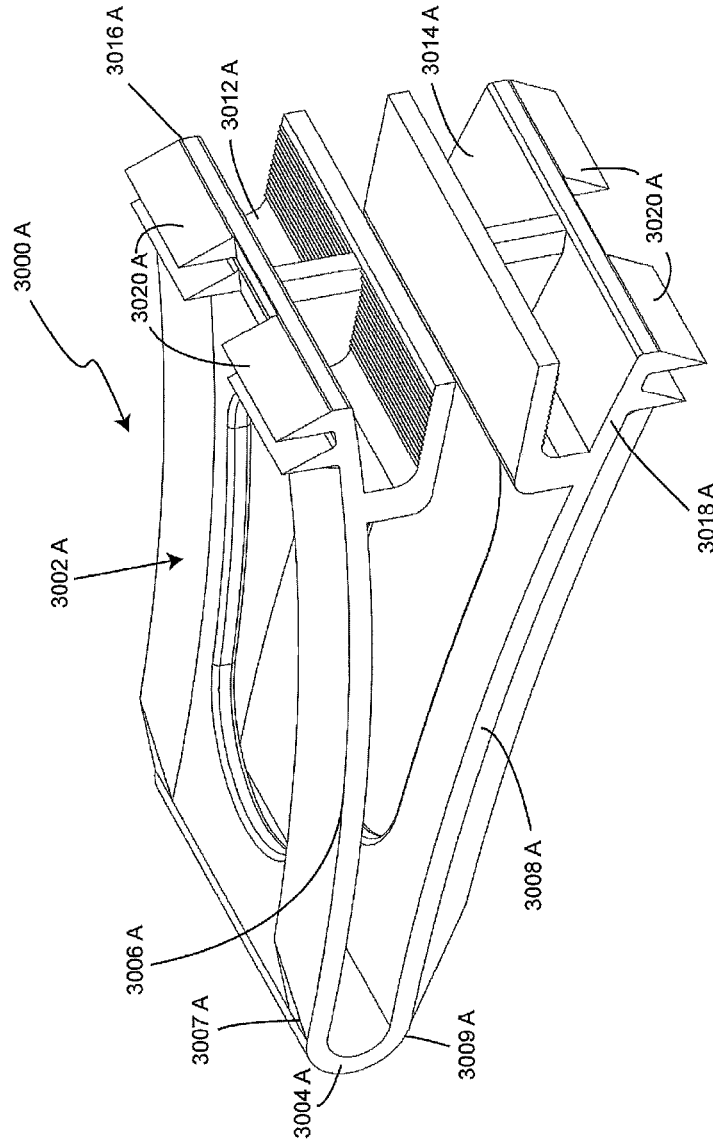


FIG. 169

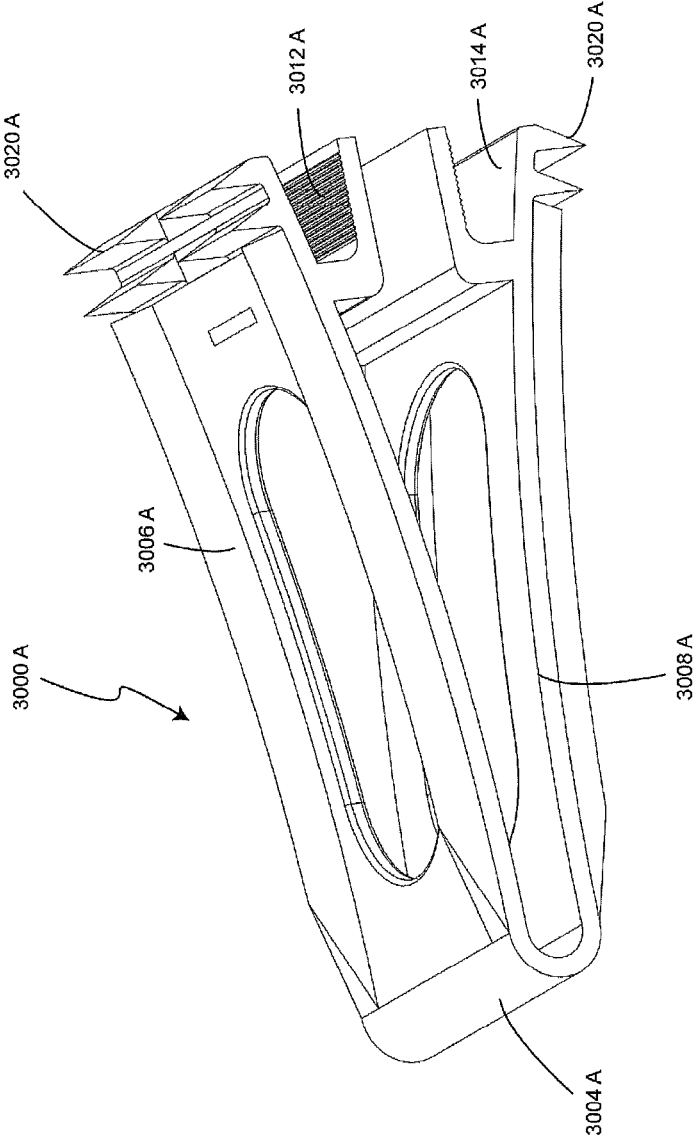


FIG. 170

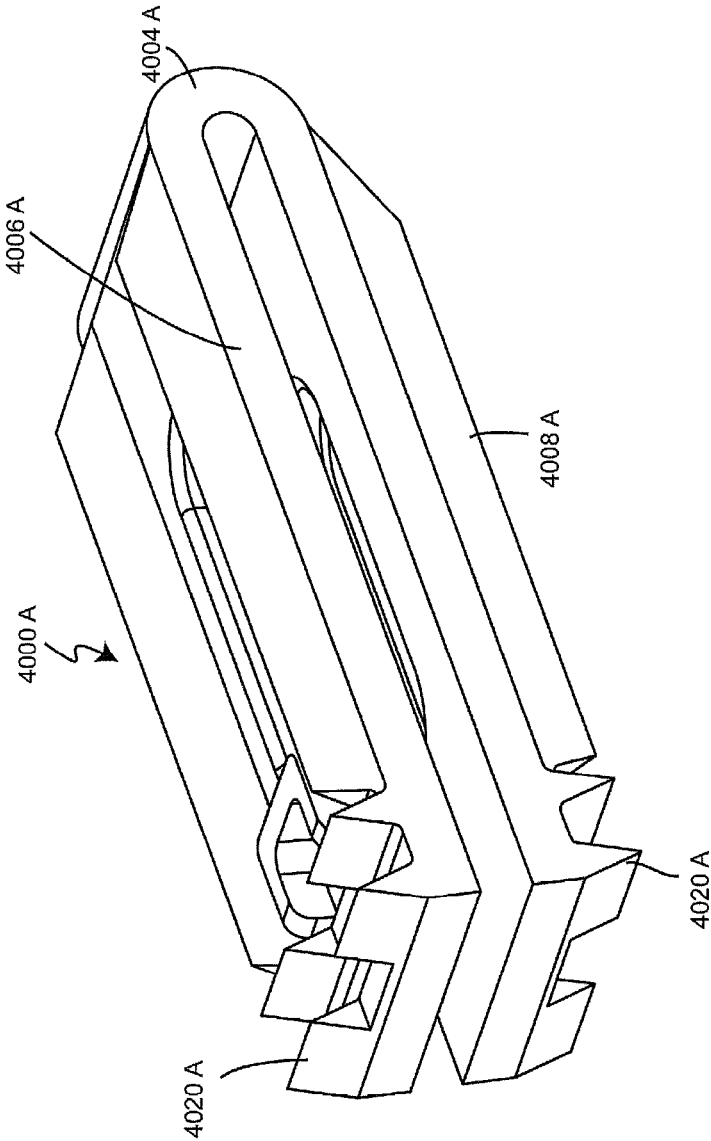


FIG. 171

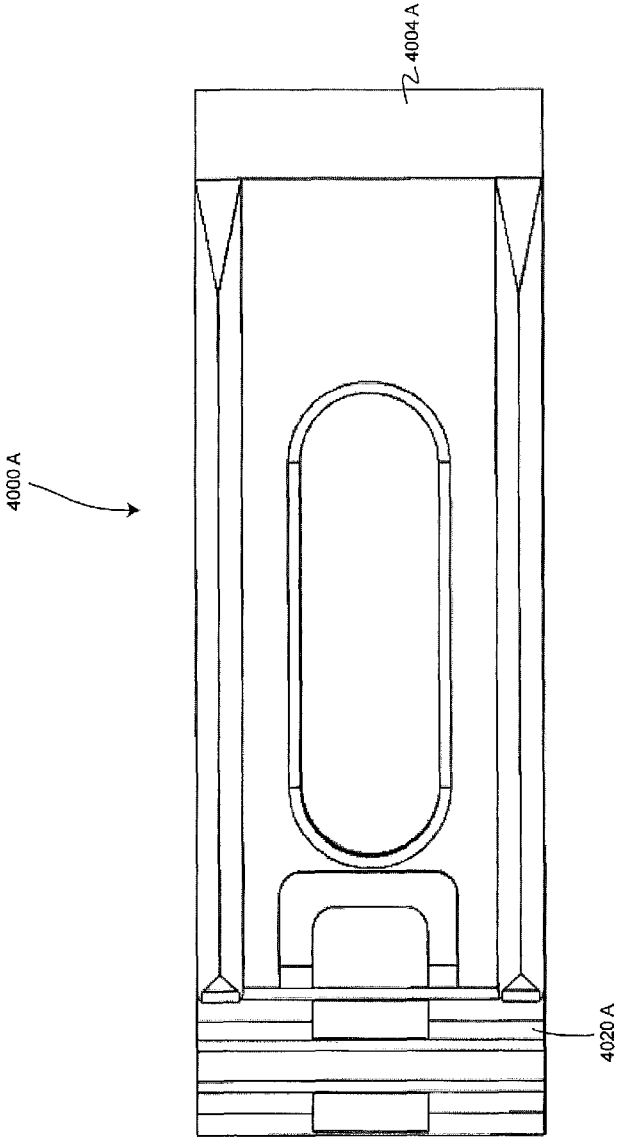


FIG. 172

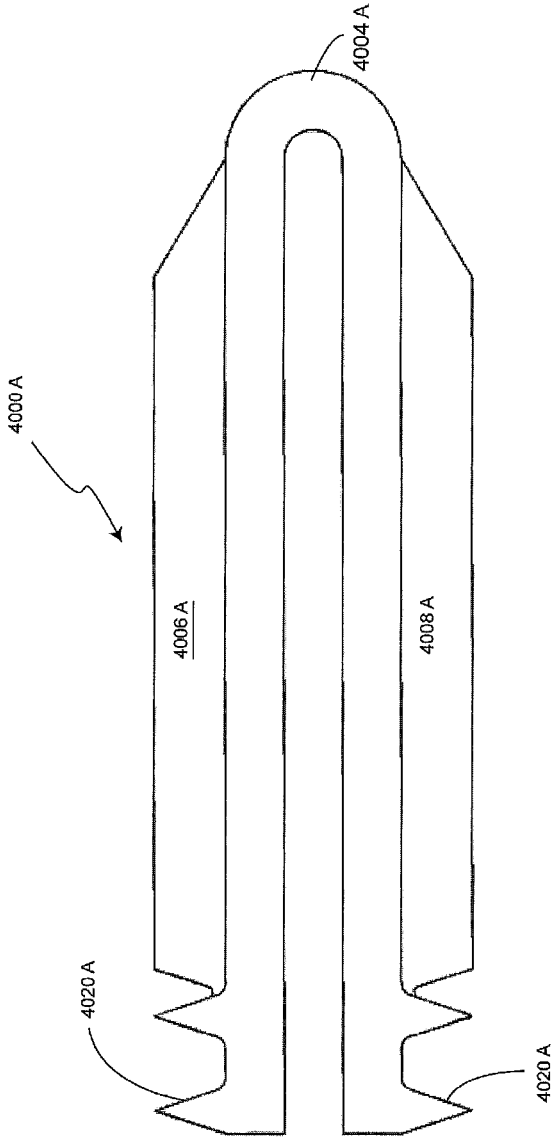


FIG. 173

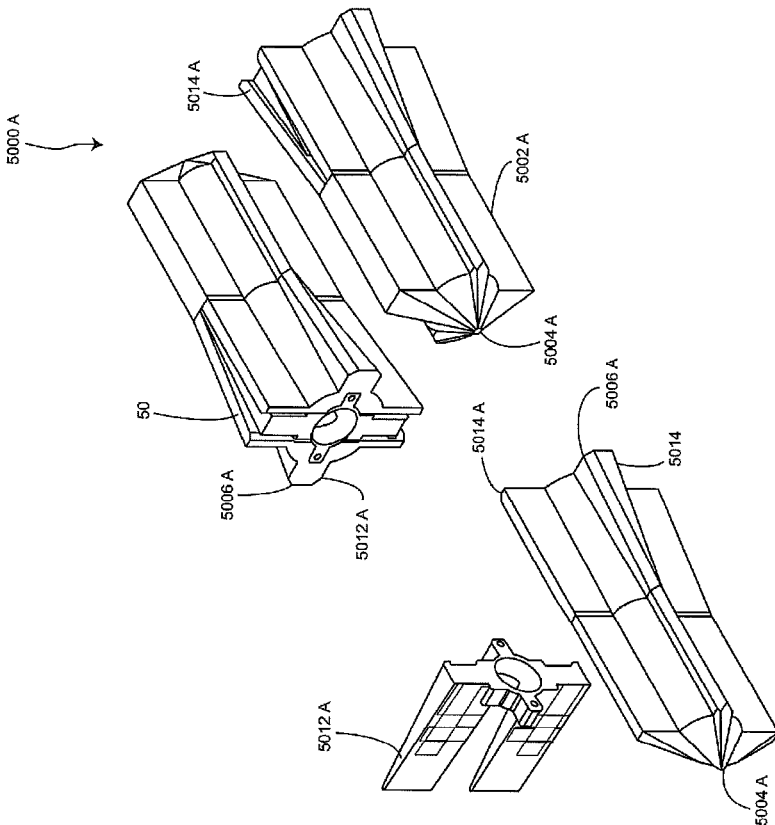


FIG. 174

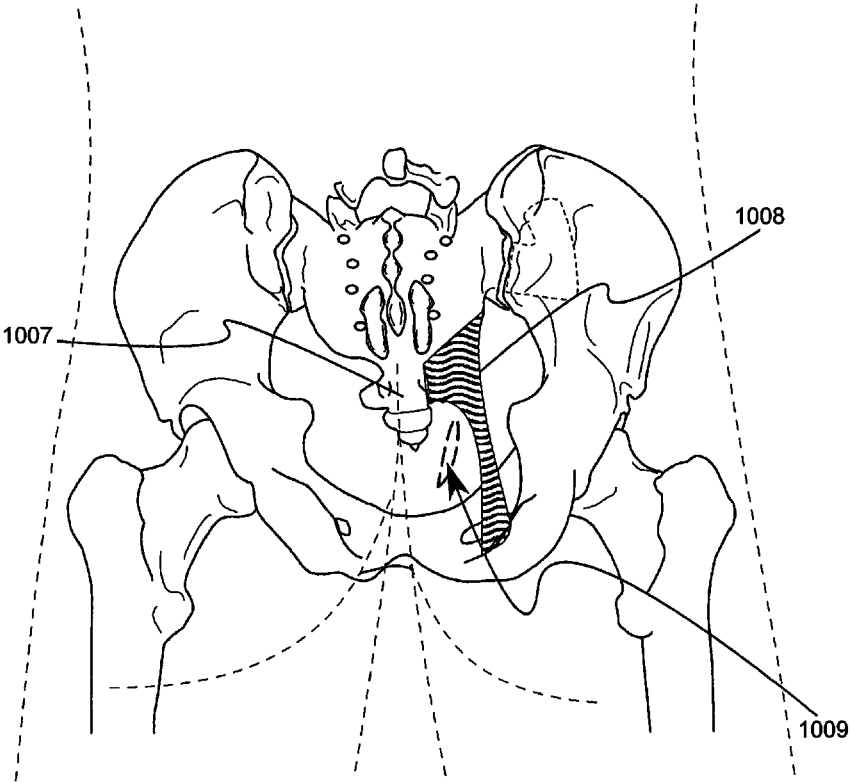


FIG. 175

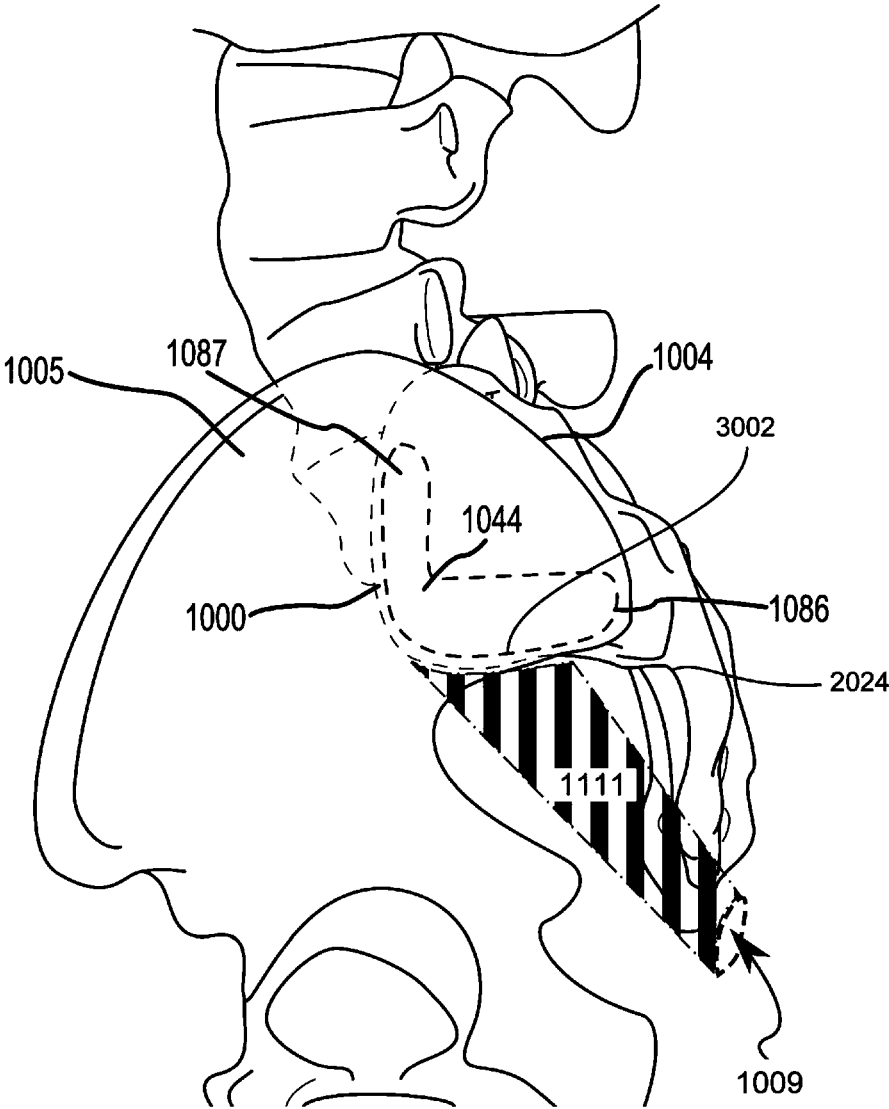
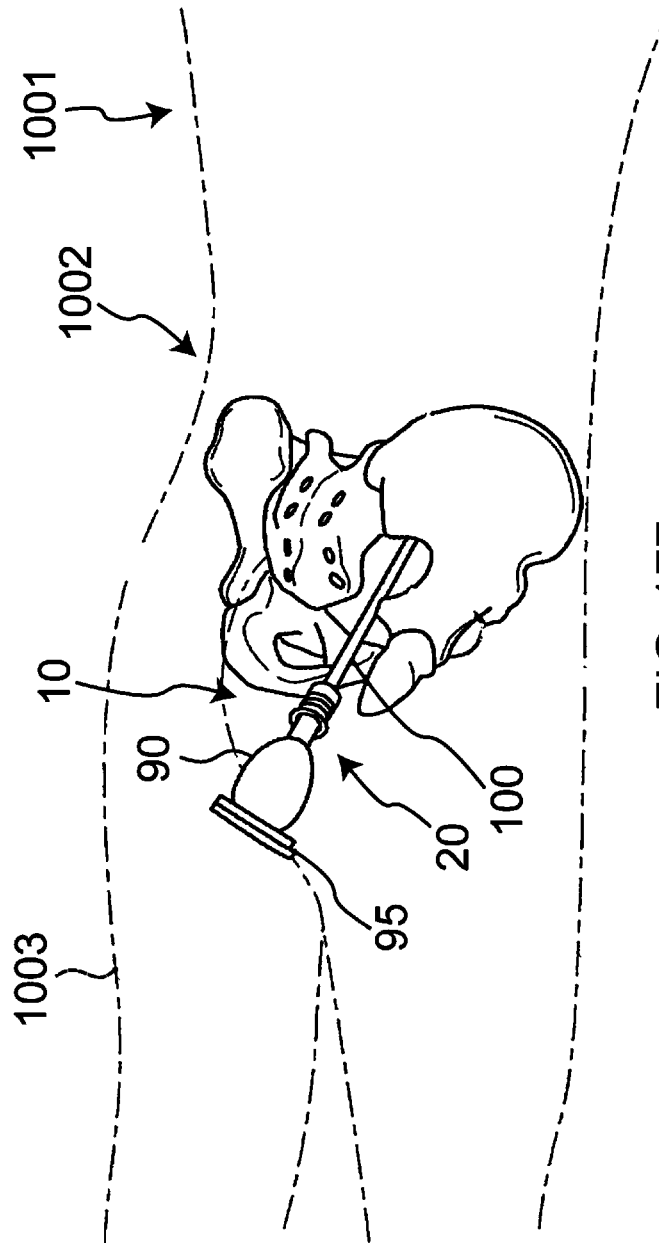


FIG. 176



SPINOPELVIC FIXATION TECHNOLOGY

CROSS REFERENCE TO RELATED APPLICATIONS

The present application is a continuation-in-part of U.S. application Ser. No. 16/041,372 filed Jul. 20, 2018, which application is a continuation of U.S. patent application Ser. No. 15/992,987 filed May 30, 2018, now U.S. Pat. No. 10,130,477, which application is a continuation of U.S. patent application Ser. No. 15/910,753 filed Mar. 2, 2018, now U.S. Pat. No. 10,058,430, which application is a continuation of U.S. patent application Ser. No. 15/828,677 filed Dec. 1, 2017, now U.S. Pat. No. 9,931,212, which application is a continuation of U.S. patent application Ser. No. 15/061,524 filed Mar. 4, 2016, now U.S. Pat. No. 9,833,320, which application is a divisional of U.S. patent application Ser. No. 13/946,790 filed Jul. 19, 2013, now U.S. Pat. No. 9,333,090, which application claims priority to and incorporates by reference in its entirety U.S. Provisional Patent Application Nos. 61/674,277, filed Jul. 20, 2012; 61/800,120, filed Mar. 15, 2013; and 61/674,130, filed Jul. 20, 2012.

Application Ser. No. 13/946,790 is also a continuation-in-part application of U.S. patent application Ser. No. 13/475,695 (“the ‘695 application”), which was filed May 18, 2012, now U.S. Pat. No. 9,381,045. The ‘695 application is a continuation-in-part application of and claims priority to U.S. patent application Ser. No. 13/236,411 (“the ‘411 application”) filed Sep. 19, 2011, now U.S. Pat. No. 9,017,407.

The ‘411 application is a continuation-in-part application of and claims priority to U.S. patent application Ser. No. 12/998,712 (“the ‘712 application”), which was filed May 23, 2011, now U.S. Pat. No. 8,979,928. The ‘712 application is the National Stage of International Patent Cooperation Treaty Patent Application PCT/US2011/000070 (the “PCT application”), which was filed Jan. 13, 2011. The PCT application claims priority to U.S. Provisional Patent Application 61/335,947, which was filed Jan. 13, 2010.

Application Ser. No. 16/041,372 is also a continuation-in-part application of U.S. patent application Ser. No. 14/344,876, filed Mar. 13, 2014, which application is a National Stage of Patent Cooperation Treaty (PCT) Application No. PCT/US2012/055892, filed Sep. 18, 2012, which application is a continuation-in-part application of U.S. patent application Ser. No. 13/475,695 filed May 18, 2012, now U.S. Pat. No. 9,381,045, which application is a continuation-in-part application of U.S. patent application Ser. No. 13/236,411 (“the ‘411 application”), filed Sep. 19, 2011, now U.S. Pat. No. 9,017,407.

The ‘411 application is a continuation-in-part application of and claims priority to U.S. patent application Ser. No. 12/998,712 (“the ‘712 application”), which was filed May 23, 2011, now U.S. Pat. No. 8,979,928. The ‘712 application is the National Stage of International Patent Cooperation Treaty Patent Application PCT/US2011/000070 (the “PCT application”), which was filed Jan. 13, 2011. The PCT application claims priority to U.S. Provisional Patent Application 61/335,947, which was filed Jan. 13, 2010.

The present application is also a continuation-in-part of U.S. application Ser. No. 15/729,273, filed Oct. 10, 2017, which is a continuation application of U.S. application Ser. No. 14/127,119 filed Dec. 17, 2013, now U.S. Pat. No. 9,788,961, which application is a national stage of International Patent Cooperation Treaty Patent Application No. PCT/US2012/042823 (“the ‘823 application”) filed Jun. 15,

2012, which claims the benefit of U.S. Provisional Patent Application 61/520,956, filed Jun. 17, 2011.

The ‘823 application is a continuation-in-part application of U.S. patent application Ser. No. 13/475,695 (“the ‘695 application”), which was filed May 18, 2012, now U.S. Pat. No. 9,381,045. The ‘695 application is a continuation-in-part application of U.S. patent application Ser. No. 13/236,411 (“the ‘411 application”), which was filed Sep. 19, 2011, now U.S. Pat. No. 9,017,407.

The ‘411 application is a continuation-in-part application of U.S. patent application Ser. No. 12/998,712 (“the ‘712 application”), which was filed May 23, 2011, now U.S. Pat. No. 8,979,928. The ‘712 application is the National Stage of International Patent Cooperation Treaty Patent Application PCT/US2011/000070 (“the ‘070 application”), which was filed Jan. 13, 2011. The ‘070 application claims the benefit of U.S. Provisional Patent Application 61/335,947, which was filed Jan. 13, 2010.

The present application is also a continuation-in-part of U.S. application Ser. No. 15/664,862 filed Jul. 31, 2017, which application is a divisional application of U.S. application Ser. No. 14/216,975 filed Mar. 17, 2014, now U.S. Pat. No. 9,757,154, which application is a continuation-in-part application of U.S. patent application Ser. No. 13/475,695, filed May 18, 2012, now U.S. Pat. No. 9,381,045, which application is a continuation-in-part application of U.S. patent application Ser. No. 13/236,411, filed Sep. 19, 2011, now U.S. Pat. No. 9,017,407. U.S. patent application Ser. No. 13/236,411 is also a continuation-in-part application of U.S. patent application Ser. No. 12/998,712 (the ‘712 application”), filed on May 23, 2011, now U.S. Pat. No. 8,979,928. The ‘712 application is the National Stage of International Patent Cooperation Treaty Patent Application PCT/US2011/000070 (“the TCT application”), filed on Jan. 13, 2011. The PCT application claims the benefit under 35 U.S.C § 119(e) of U.S. Provisional Patent Application No. 61/335,947, which was filed Jan. 13, 2010. U.S. patent application Ser. No. 14/216,975 further claims the benefit of U.S. Provisional Patent Application 61/798,225, filed on Mar. 15, 2013.

The present application is also a continuation-in-part of U.S. application Ser. No. 15/385,446 filed Dec. 20, 2016, which application is a continuation of U.S. application Ser. No. 14/413,318 filed Jan. 7, 2015, now U.S. Pat. No. 9,554,909, which application is a national stage entry of PCT Application No. PCT/US2013/051381 filed Jul. 19, 2013, which claims the benefit of U.S. Provisional Application No. 61/798,922 filed Mar. 15, 2013, and also claims the benefit of U.S. Provisional Application No. 61/674,233, filed Jul. 20, 2012.

All of the aforementioned applications are hereby incorporated by reference in their entireties into the present application.

The delivery approaches and methodologies disclosed in the above-listed applications and incorporated herein are applicable to the implants and delivery tools disclosed in the present application.

FIELD OF THE INVENTION

Aspects of the present invention relate to medical apparatus and methods. More specifically, the present invention relates to devices and methods for fusing a sacroiliac joint.

BACKGROUND OF THE INVENTION

The sacroiliac joint is the joint between the sacrum and the ilium of the pelvis, which are joined by ligaments. In

humans, the sacrum supports the spine and is supported in turn by an ilium on each side. The sacroiliac joint is a synovial joint with articular cartilage and irregular elevations and depressions that produce interlocking of the two bones.

Pain associated with the sacroiliac joint can be caused by traumatic fracture dislocation of the pelvis, degenerative arthritis, sacroiliitis an inflammation or degenerative condition of the sacroiliac joint, osteitis condensans ilii, or other degenerative conditions of the sacroiliac joint. Currently, sacroiliac joint fusion is most commonly advocated as a surgical treatment for these conditions. Fusion of the sacroiliac joint can be accomplished by several different conventional methods encompassing an anterior approach, a posterior approach, and a lateral approach with or without percutaneous screw or other type implant fixation. However, while each of these methods has been utilized for fixation and fusion of the sacroiliac joint over the past several decades, substantial problems with respect to the fixation and fusion of the sacroiliac joint remain unresolved.

A significant problem with certain conventional methods for fixation and fusion of the sacroiliac joint including the anterior approach, posterior approach, or lateral approach may be that the surgeon has to make a substantial incision in the skin and tissues for direct access to the sacroiliac joint involved. These invasive approaches allow the sacroiliac joint to be seen and touched directly by the surgeon. Often referred to as an "open surgery", these procedures have the attendant disadvantages of requiring general anesthesia and can involve increased operative time, hospitalization, pain, and recovery time due to the extensive soft tissue damage resulting from the open surgery.

A danger to open surgery using the anterior approach can be damage to the L5 nerve root, which lies approximately two centimeters medial to the sacroiliac joint or damage to the major blood vessels. Additionally, these procedures typically involve fixation of the sacroiliac joint (immobilization of the articular surfaces of the sacroiliac joint in relation to one another) by placement of one or more screws or one or more trans-sacroiliac implants (as shown by the non-limiting example of FIG. 1) or by placement of implants into the S1 pedicle and iliac bone.

Use of trans-sacroiliac and S1 pedicle-iliac bone implants can also involve the risk of damage to the lumbosacral neurovascular elements. Damage to the lumbosacral neurovascular elements as well as delayed union or non-union of the sacroiliac joint by use of these procedures may require revision surgery to remove all or a portion of the implants or repeat surgery as to these complications.

Another significant problem with conventional procedures utilizing minimally invasive small opening procedures can be that the procedures are technically difficult, requiring biplanar fluoroscopy of the articular surfaces of the sacroiliac joint and extensive surgical training and experience. Despite the level of surgical training and experience, there is a substantial incidence of damage to the lumbosacral neurovascular elements. Additionally, sacral anomalies can further lead to mal-placement of implants leading to damage of surrounding structures. Additionally, these procedures are often performed without fusion of the sacroiliac joint, which does not remove the degenerative joint surface and thereby does not address the degenerative condition of the sacroiliac joint, which may lead to continued or recurrent sacroiliac joint pain.

Another significant problem with conventional procedures can be the utilization of multiple trans-sacroiliac elongate implants, which do not include a threaded surface.

This approach requires the creation of trans-sacroiliac bores in the pelvis and nearby sacral foramen, which can be of relatively large dimension and which are subsequently broached with instruments, which can result in bone being impacted into the pelvis and neuroforamen.

The creation of the trans-sacroiliac bores and subsequent broaching of the bores requires a guide pin, which may be inadvertently advanced into the pelvis or sacral foramen, resulting in damage to other structures. Additionally, producing the trans-sacroiliac bores, broaching, or placement of the elongate implants may result in damage to the lumbosacral neurovascular elements, as above discussed. Additionally, there may be no actual fusion of the articular portion of the sacroiliac joint, which may result in continued or recurrent pain requiring additional surgery.

Another substantial problem with conventional procedures can be that placement of posterior extra-articular distracting fusion implants and bone grafts may be inadequate with respect to removal of the articular surface or preparation of cortical bone, the implant structure and fixation of the sacroiliac joint. The conventional procedures may not remove sufficient amounts of the articular surfaces or cortical surfaces of the sacroiliac joint to relieve pain in the sacroiliac joint. The conventional implant structures may have insufficient or avoid engagement with the articular surfaces or cortical bone of the sacroiliac joint for adequate fixation or fusion. The failure to sufficiently stabilize and fuse the sacroiliac joint with the conventional implant structures and methods may result in a failure to relieve the condition of sacroiliac joint being treated. Additionally, conventional methods of driving apart a sacrum and ilium may lead to mal-alignment of the sacroiliac joint and increased pain.

The inventive sacroiliac fusion system described herein addresses the problems associated with conventional methods and apparatuses used in fixation and fusion of the sacroiliac joint.

BRIEF SUMMARY OF THE INVENTION

One implementation of the present disclosure may take the form of a sacroiliac joint fusion system including a joint implant, an anchor element and a delivery tool. The joint implant includes a distal end, a proximal end, a body extending between the proximal and distal ends, and a first bore extending non-parallel to a longitudinal axis of the body. The anchor element includes a distal end and a proximal end and is configured to be received in the first bore. The delivery tool includes an implant arm and an anchor arm. The implant arm includes a proximal end and a distal end. The distal end of the implant arm is configured to releasably couple to the proximal end of the joint implant such that a longitudinal axis of the implant arm is substantially at least one of coaxial or parallel with the longitudinal axis of the body of the joint implant. The anchor arm includes a proximal end and a distal end. The distal end of the anchor arm is configured to engage the proximal end of the anchor element. The anchor arm is operably coupled to the implant arm in an arrangement such that the longitudinal axis of the anchor element is generally coaxially aligned with a longitudinal axis of the first bore when the distal end of the implant arm is releasably coupled with the proximal end of the joint implant and the distal end of the anchor arm is engaged with the proximal end of the anchor element. The arrangement is fixed and nonadjustable.

Another implementation of the present disclosure may take the form of a sacroiliac joint fusion system including a

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joint implant, an anchor element and a delivery tool. The joint implant includes a distal end, a proximal end, a body extending between the proximal and distal ends, and a first bore extending non-parallel to a longitudinal axis of the body. The anchor element includes a distal end and a proximal end and is configured to be received in the first bore. The delivery tool includes an implant arm and an anchor arm. The implant arm includes a proximal end and a distal end. The distal end of the implant arm is configured to releasably couple to the proximal end of the joint implant such that a longitudinal axis of the implant arm is substantially at least one of coaxial or parallel with the longitudinal axis of the body of the joint implant. The anchor arm includes a proximal end and a distal end. The distal end of the anchor arm includes a guide. The anchor arm is pivotally coupled to the implant arm and configured such that a center of the guide moves along an arc that extends through generally the center of the first bore of the implant when the distal end of the implant arm is releasably coupled with the proximal end of the joint implant. The anchor arm is configured to deliver the anchor element to the first bore.

Yet another implementation of the present disclosure may take the form of a sacroiliac joint fusion system including a joint implant and a tool. In one embodiment, the joint implant includes a longitudinal axis and a first bore extending non-parallel to the longitudinal axis. The anchor element is configured to be received in the first bore. The delivery tool includes an implant arm and an anchor arm. The implant arm is configured to releasably couple to the joint implant. The anchor arm is coupled to the implant arm and configured to deliver the anchor element to the first bore. The final manufactured configuration of the tool and final manufactured configuration of the joint implant are such that, when the system is assembled such that the implant arm is releasably coupled to the joint implant, a delivery arrangement automatically exists such that the anchor arm is correctly oriented to deliver the anchor element to the first bore.

Another implementation of the present disclosure may take the form of a method of sacroiliac joint fusion. In one embodiment, the method includes: a) approaching a sacroiliac joint space with a joint implant comprising at least first and second planar members radially extending generally coplanar with each other from opposite sides of a body of the joint implant; b) delivering the joint implant into a sacroiliac joint space, the joint implant being oriented in the sacroiliac joint space such that the first and second planar members are generally coplanar with a joint plane of the sacroiliac joint space; and c) causing an anchor element to be driven generally transverse to the joint plane through bone material defining at least a portion of the sacroiliac joint space and into a bore of the joint implant that extends generally transverse to the body of the joint implant.

Yet another implementation of the present disclosure may take the form of a medical kit for the fusion of a sacroiliac joint including a caudal access region and a joint plane. In one embodiment, the kit includes: a) a delivery tool comprising an implant arm and an anchor arm coupled to the implant arm; b) a joint implant comprising a bore defined therein that extends generally transverse to a longitudinal length of the joint implant; and c) an anchor element configured to be received in the bore of the joint implant. The bore of the implant, the implant, the implant arm and the anchor arm have an as-manufactured configuration that allows the anchor arm to properly align the anchor element to be received in the bore of the implant when the implant is coupled to the implant arm.

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One implementation of the present disclosure may take the form of various embodiments of a sacroiliac joint fusion system including joint implants and delivery tools.

While multiple embodiments are disclosed, still other embodiments of the present disclosure will become apparent to those skilled in the art from the following detailed description, which shows and describes illustrative embodiments of the disclosure. As will be realized, the invention is capable of modifications in various aspects, all without departing from the spirit and scope of the present disclosure. Accordingly, the drawings and detailed description are to be regarded as illustrative in nature and not restrictive.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is an anterior view of the pelvic region and a conventional method and device for stabilizing the sacroiliac joint.

FIG. 2A is an isometric view of a first embodiment of a system for fusing a sacroiliac joint.

FIG. 2B is the same view as FIG. 2A, except the delivery tool and implant assembly are decoupled from each other.

FIG. 3 is the same view as FIG. 2A, except the system is exploded to better illustrate its components.

FIG. 4 is a top-side isometric view of the implant assembly.

FIG. 5 is a distal end isometric view of the implant of the implant assembly of FIG. 4.

FIG. 6 is a proximal end isometric view of the implant.

FIG. 7 is a bottom-side isometric view of the implant assembly.

FIG. 8 is another proximal end isometric view of the implant.

FIG. 9 is another distal end isometric view of the implant.

FIGS. 10 and 11 are opposite side elevation views of the implant.

FIGS. 12 and 13 are opposite plan views of the implant.

FIG. 14 is a distal end elevation of the implant.

FIG. 15 is a proximal end elevation of the implant.

FIG. 16 is an isometric longitudinal cross section of the implant as taken along section line 16-16 of FIG. 11.

FIG. 17 is an isometric longitudinal cross section of the implant as taken along section line 17-17 of FIG. 13.

FIG. 18 is a proximal isometric view of the arm assembly.

FIG. 19 is a distal isometric view of the arm assembly 85.

FIG. 20 is a longitudinal cross section of the implant arm as taken along section line 20-20 in FIG. 18.

FIG. 21A is a side elevation of the system wherein the tool is attached to the implant assembly for delivery of the implant assembly to the sacroiliac joint.

FIG. 21B is the same view as FIG. 21A, except illustrating a series of interchangeable anchor arms that may be coupled to the implant arm to adjust the tool for the patient, but maintain the angular relationship between the components of system that allows the anchor member to be delivered into the implant bore without adjustment to the delivery tool.

FIG. 21C is the same view of FIG. 21A, except illustrating a version of the same embodiment wherein the anchor arm is more proximally located along the implant arm.

FIG. 22 is the same view as FIG. 21A, except shown as a longitudinal cross section.

FIG. 23 is an enlarged view of the distal region of the system circled in FIG. 22.

FIG. 24 is an enlarged cross sectional plan view taken in a plane 90 degrees from the section plane of FIG. 23.

FIG. 25 is a proximal isometric view of the handle.

FIG. 26 is a distal isometric view of the handle.

FIG. 27 is a cross sectional distal isometric view of the handle.

FIG. 28 is an isometric view of the implant retainer.

FIG. 29 is a longitudinal cross sectional isometric view of the implant retainer.

FIG. 30A is an isometric view of the sleeve.

FIG. 30B is a longitudinal cross section of an embodiment of the sleeve having multiple sleeve portions.

FIG. 31 is an isometric view of a trocar, guidewire, drill, screwdriver, etc. for insertion through the lumen of the sleeve.

FIG. 32 is an isometric view of a second embodiment of a system for fusing a sacroiliac joint.

FIG. 33 is the same view as FIG. 32, except the system is exploded to better illustrate its components.

FIG. 34 is a side elevation of the system embodiment of FIG. 32.

As shown in FIG. 35 is a proximal isometric view of the implant arm of the embodiment of FIG. 32.

FIG. 36 is an isometric view of the anchor arm.

FIGS. 37 and 38 are different isometric views of a third embodiment of the system.

FIG. 39 is the same view as FIG. 37, except the system is shown exploded to better illustrate the components of the system.

FIG. 40 is a side elevation of the system of FIG. 37, wherein the tool is attached to the implant assembly for delivery of the implant assembly to the sacroiliac joint.

FIGS. 41-44 are various isometric views of the implant of the third embodiment of the system.

FIGS. 45-46 are opposite plan views of the implant.

FIGS. 47-50 are various elevation views of the implant.

FIGS. 51-52 are, respectively, isometric and side elevation views of an implant having an anchor member receiving arm.

FIG. 53 is an enlarged view of the disk-shaped seat of the implant arm of FIG. 51.

FIG. 54 is an isometric view of an implant with another type of anchor member locking mechanism.

FIG. 55 is an enlarged view of the free end of the anchor member locking mechanism of FIG. 54.

FIGS. 56-61 are, respectively, front isometric, rear isometric, side elevation, plan, front elevation, and rear elevation views of another embodiment of the implant.

FIGS. 62-67 are, respectively, front isometric, rear isometric, side elevation, plan, front elevation, and rear elevation views of yet another embodiment of the implant.

FIGS. 68-73 are, respectively, front isometric, rear isometric, side elevation, plan, front elevation, and rear elevation views of still another embodiment of the implant.

FIGS. 74-79 are, respectively, front isometric, rear isometric, side elevation, plan, front elevation, and rear elevation views of yet another embodiment of the implant.

FIGS. 80-85 are, respectively, front isometric, rear isometric, side elevation, plan, front elevation, and rear elevation views of still yet another embodiment of the implant.

FIG. 86 is an isometric view of the delivery tool.

FIGS. 87-88 are generally opposite isometric views of the delivery tool in an exploded state.

FIG. 89 is an isometric view of the handle.

FIG. 90 is an exploded isometric view of the retaining collar and handle shown in longitudinal cross section.

FIG. 91 is a longitudinal cross section of the delivery tool 20 when assembled as shown in FIG. 86.

FIG. 92 is a side view of an implant retainer similar to that described with respect to FIGS. 86-91, except having a modified distal end.

FIGS. 93-94 are, respectively, longitudinal and transverse cross sectional views of an implant with an engagement hole configured to complementarily engage with the T-shaped distal end of the retainer of FIG. 92.

FIG. 95 is the same view as FIG. 93, except with the retainer received in the hole.

FIG. 96A is a right lateral side view of a hip region of a patient lying prone, wherein the soft tissue surrounding the skeletal structure of the patient is shown in dashed lines.

FIG. 96B is an enlarged view of the hip region of FIG. 96A.

FIG. 97A is a lateral-posterior view of the hip region of the patient of FIG. 96A, wherein the patient is lying prone and the soft tissue surrounding the skeletal structure of the patient is shown in dashed lines.

FIG. 97B is an enlarged view of the hip region of FIG. 97A.

FIG. 98A is a posterior view of the hip region of the patient of FIG. 96A, wherein the patient is lying prone and the soft tissue surrounding the skeletal structure of the patient is shown in dashed lines.

FIG. 98B is an enlarged view of the hip region of FIG. 98A.

FIGS. 99A-99Q are each a step in the methodology and illustrated as the same transverse cross section taken along a plane extending medial-lateral and anterior posterior along section line 99-99 in FIG. 98B.

FIG. 100A is a posterior-lateral view of the hip region of the patient, illustrating the placement of a cannula alignment jig.

FIGS. 100B-100C are different isometric views of the cannula alignment jig.

FIG. 101A is a posterior-lateral view of the hip region of the patient, illustrating the placement of a drill jig.

FIG. 101B is an isometric view of the drill jig.

FIG. 102A is a lateral view of the hip region of the patient, illustrating the implant implanted in the caudal region of the sacroiliac joint space.

FIG. 102B is an anterior view of the hip region of the patient, illustrating the implant implanted in the caudal region of the sacroiliac joint space.

FIG. 102C is an enlarged view of the implant taken along the plane of the sacroiliac joint.

FIG. 102D is a transverse cross section of the implant and joint plane taken along section line 102D-102D of FIG. 102C.

FIG. 103A is generally the same view as FIG. 97A, except illustrating the delivery tool being used to deliver the implant to the sacroiliac joint space.

FIG. 103B is an enlarged view of the hip region of FIG. 103A.

FIG. 104 is generally the same enlarged view as FIG. 96B, except illustrating the delivery tool being used to deliver the implant to the sacroiliac joint space.

FIG. 105 is the same view as FIG. 104, except the implant has now been fully inserted into the prepared space in the sacroiliac joint.

FIG. 106A is the same view as FIG. 104, except the sleeve is now received in the collar of the anchor arm.

FIG. 106B is generally the same view as FIG. 106A, except the ilium is removed to show the sacroiliac joint space boundary defined along the sacrum and the implant positioned for implantation within the joint space.

FIG. 107A is a posterior-inferior view of the hip region of the patient, wherein the soft tissue surrounding the skeletal hip bones is shown in dashed lines.

FIG. 107B is an enlarged view of the implant region of FIG. 107A.

FIGS. 108A and 108B are, respectively, posterior and posterior-lateral views of the implantation area and the implant assembly implanted there.

FIG. 109 is an isometric view of the system wherein the tool is attached to the implant for delivery of the implant to the sacroiliac joint.

FIG. 110 is a view of the system wherein the implant and anchor arm are shown in plan view.

FIG. 111A is an inferior-posterior view of the patient's hip skeletal structure similar to the view depicted in FIG. 107A.

FIG. 111B is a lateral-superior-posterior view of the patient's hip skeletal structure.

FIG. 111C is an inferior-posterior view of the patient's hip skeletal structure taken from a perspective laterally opposite the view depicted in FIG. 111B.

FIG. 112A is an inferior-posterior view of the patient's hip skeletal structure similar to the view depicted in FIG. 107A.

FIG. 112B is a side view of the patient's hip skeletal structure similar to the view depicted in FIG. 106A.

FIG. 112C is a view of the patient's hip skeletal structure similar to the view depicted in FIG. 103A, except from an opposite lateral perspective.

FIG. 112D is a superior view of the patient's hip skeletal structure.

FIG. 113 is a plan view of a medical kit containing the components of the system, namely, the delivery tool, multiple implants of different sizes, and multiple anchor members of different sizes, wherein the system components are sealed within one or more sterile packages and provided with instructions for using the system.

FIG. 114 is the same transverse cross sectional view of the patient's hip as shown in FIGS. 99A-99Q, except showing the implant having structure attached thereto that will allow the implant to serve as an attachment point for structural components of a spinal support system configured to support across the patient's hip structure and/or to support along the patient's spinal column.

FIG. 115 is a posterior view of the patient's sacrum and ilium, wherein structural components of a spinal support system extend medial-lateral across the patient's hip structure and superiorly to support along the patient's spinal column.

FIG. 116 is the same view as FIG. 115, except having a different spanning member structure.

FIG. 117A is a lateral-inferior-posterior view of the patient's hip skeletal structure similar to the view depicted in FIG. 111C.

FIG. 117B is an inferior-posterior view of the patient's hip skeletal structure similar to the view depicted in FIG. 111A.

FIG. 117C is the same view as FIG. 106B, except showing the implant being implanted in the extra-articular space, as opposed to the sacroiliac joint articular region.

FIGS. 118A-118C are, respectively, isometric and opposite plan views of an implant with a side-to-side deviated bore.

FIGS. 119A-119E are, respectively, distal end isometric, side elevation, plan, distal end elevation, and proximal end elevation views of another embodiment of the implant.

FIGS. 120A-120B are, respectively, distal end isometric and side elevation views of yet another embodiment of the implant.

FIGS. 121A-121G are, respectively, distal end isometric, side elevation, plan, distal end elevation, proximal end elevation, proximal end isometric, and side elevation views of still another embodiment of the implant.

FIG. 121H is a schematic depiction of a system for fusing a joint, wherein the joint implant includes an electrode in electrical communication with a nerve sensing system.

FIG. 122 is a proximal end isometric view of another embodiment of the implant assembly.

FIGS. 123A-123E are, respectively, distal end isometric, side elevation, plan, distal end elevation, and proximal end elevation views of yet another embodiment of the implant.

FIGS. 124A and 124B1 are isometric views of another embodiment of the delivery tool coupled and decoupled with the implant, respectively.

FIG. 124B2 is a cross section view as taken along section line 124B2-124B2 in FIG. 124B1.

FIG. 124C is an isometric view of the delivery tool in an exploded state.

FIG. 124D is an enlarged view of the distal end of the implant arm of the delivery tool.

FIGS. 124E-124H are, respectively, distal end isometric, side elevation, plan, and opposite plan views of a version of the embodiment of the implant of FIGS. 123A-123E, wherein the version includes a bore for receiving an anchor.

FIG. 125A is an isometric view of another embodiment of the implant.

FIG. 125B is a longitudinal cross section view of the implant of FIG. 125A.

FIG. 126A is an isometric view of another embodiment of the implant assembly.

FIG. 126B is a longitudinal cross section view of the implant of FIG. 126A.

FIG. 126C is a longitudinal cross section of the proximal head of the anchor of FIG. 126A.

FIG. 127 is an isometric view of an embodiment of a sleeve mounted on an implant arm of a delivery system similar to the delivery system of FIG. 88, wherein the sleeve facilitates visualization of the trans screw and trajectory.

FIG. 128A is an isometric view of another embodiment of the sleeve of FIG. 127.

FIG. 128B is an end view of sleeve of FIG. 127.

FIG. 128C is a posterior view of the hip region, wherein the sleeve of FIG. 127 is being employed.

FIGS. 129A-129B show isometric views of another embodiment of the system, wherein the delivery tool has a series of interchangeable anchor arms that may be coupled to the implant arm to adjust the tool for the patient, but maintain the angular relationship between the components of system that allows the anchor member to be delivered into the implant bore and/or another location adjacent to the implant without adjustment to the delivery tool.

FIG. 129C shows an enlarged view of the arm assembly of the delivery tool of FIGS. 129A-129B.

FIGS. 129D-129K are, respectively, distal end isometric, proximal end isometric, side elevation, opposite side elevation, plan, opposite plan, proximal end elevation, and distal end elevation views of an embodiment of the implant intended for use with the system of FIGS. 129A-129C.

FIG. 129L is an enlarged isometric view of the implant of FIGS. 129D-129K mounted on the extreme distal end of the implant arm of the delivery tool of FIGS. 129A-129C.

FIGS. 129M and 129N are side views of the distal regions of two alternative implant arms arrangements.

FIG. 129O is an exploded isometric view of the implant arm of FIG. 129M.

FIGS. 130A-130B show anterior views of the hip region with the system of FIGS. 129A-129C, wherein the ilium is shown and hidden, respectively.

FIGS. 130C-130G show anterior-superior-lateral, posterior, superior, lateral, and inferior views of the hip region with the system of FIGS. 129A-129C.

FIGS. 130H and 130I show inferior and posterior-lateral views of a patient, wherein the system of FIGS. 129A-129C is inserted through the soft tissue of the hip region.

FIGS. 131A-131B show isometric views of another embodiment of the system.

FIG. 131C shows an enlarged plan view of the arm assembly of the delivery tool of FIGS. 131A-131B.

FIGS. 131D-131E are isometric view of a version of the implant of FIGS. 129D-129K adapted for use with the delivery system of FIGS. 131A-131C.

FIG. 131F is an isometric view of a version of the implant of FIGS. 129D-129K, wherein the body of the implant is hollow and configured to work with a distal end of an implant arm configured to remove cartilage.

FIG. 131G is an isometric view of the distal end of the implant arm configured to be received in the hollow body of the implant of FIG. 131F, wherein the distal end of the implant arm is configured to remove cartilage.

FIG. 131H is an isometric view of the implant arm distal end of FIG. 131G received in the implant of FIG. 131F.

FIG. 131I is an isometric longitudinal cross section of the implant arm distal end and implant supported thereon as taken along section line 131I-131I of FIG. 131H.

FIG. 132A is an isometric view of yet another embodiment of the system for fusing a sacroiliac joint.

FIG. 132B is the same view as FIG. 132A, except the system is exploded to better illustrate its components.

FIG. 133A is an isometric view of yet another embodiment of the system for fusing a sacroiliac joint.

FIG. 133B shows another isometric view of the system of FIG. 133A.

FIG. 133C shows the same view as FIG. 133B, except the system is inserted through the soft tissue of the hip region of the patient.

FIG. 133D is the same view as FIG. 133C, except the soft tissue is hidden to show the patient bone structure.

FIG. 133E shows a rear elevation view of the system of FIG. 133A.

FIG. 133F shows the same view as FIG. 133E, except the system is inserted through the soft tissue of the hip region of the patient.

FIG. 133G is the same view as FIG. 133F, except the soft tissue is hidden to show the patient bone structure.

FIG. 134A illustrates an embodiment of a system for extracting an implant.

FIGS. 134B-134C show enlarged views of the distal end of the system of FIG. 134A, wherein the distal end is decoupled and coupled to the implant, respectively.

FIG. 134D is a longitudinal cross section as taken along section line 134D-134D of FIG. 134C.

FIG. 134E is the same view as FIG. 134A, except the system is exploded to better illustrate its components.

FIG. 134F is an isometric view of the proximal end of the implant of FIGS. 134B-134C.

FIGS. 135A-135C are respectively a first isometric, a second isometric and a plan view of an implant embodiment having a shape that generally mimics or resembles that of a sacroiliac joint space as viewed from a substantially lateral view.

FIGS. 136A-136D are generally opposite isometric views of an implant embodiment that is configured to transition

from a generally linear, rectangular arrangement (shown in FIGS. 136A-136B) to a boot or L-shaped configuration (shown in FIGS. 136C-136D) that generally fills and/or mimics the shape of the sacroiliac joint space.

FIG. 136E is an exploded isometric view of the implant of FIGS. 136A-136D.

FIGS. 136F and 136G are, respectively, proximal and distal elevations of the implant of FIGS. 136A-136D.

FIGS. 136H and 136I are, respectively, top and bottom plan views of the implant of FIGS. 136A-136D.

FIG. 136J is a longitudinal cross sectional elevation of the implant of FIGS. 136A-136D as taken along section line 136J-136J.

FIGS. 136K and 136L are respective enlarged views of the upper and lower cylinder regions of FIG. 136J.

FIGS. 137A and 137B are generally opposite isometric views of an implant embodiment configured to essentially mimic at least a portion of the sacroiliac joint space.

FIGS. 137C-137F are, respectively, a top plan view, a distal end elevation, a side elevation, and a proximal elevation of the implant of FIGS. 137A and 137B.

FIGS. 138A and 138B are generally opposite isometric views of an implant embodiment configured to essentially mimic at least a portion of the sacroiliac joint space.

FIGS. 138C-138F are, respectively, a top plan view, a distal end elevation, a side elevation, and a proximal elevation of the implant of FIGS. 138A and 138B.

FIGS. 139-154 are various views of an embodiment of an implant assembly for fusing a sacroiliac joint.

FIG. 155 is an isometric view of an implant delivery tool for use with the implant assembly of FIGS. 139-154.

FIGS. 156 and 157 are exploded views of the implant assembly of FIGS. 139-154.

FIGS. 158-163 are various views of an implant delivery tool in accordance with an embodiment of the present invention.

FIGS. 164-168 are various views of an implant delivery tool in accordance with another embodiment of the present invention.

FIGS. 169-170 are front and rear perspective views of an implant for fusing a sacroiliac joint in accordance with another embodiment of the present invention.

FIGS. 171-173 are various views of an implant for fusing a sacroiliac joint in accordance with another embodiment of the present invention.

FIG. 174 includes various perspective views of an implant for fusing a sacroiliac joint in accordance with yet another embodiment of the present invention.

FIGS. 175 and 176 are, respectively, posterior and lateral views of a patient hip region illustrating a surgical approach employing an entry point near the coccyx and the sacrotuberous ligament.

FIG. 177 is a posterior-lateral view of the patient hip region illustrating the delivery tool extending along the surgical approach of FIGS. 175 and 176.

DETAILED DESCRIPTION

Implementations of the present disclosure involve a system 10 for fusing a sacroiliac joint. The system 10 includes a delivery tool 20 and an implant assembly 15 for delivery to a sacroiliac joint via the delivery tool 20. The implant assembly 15, which includes an implant 25 and anchor 30, is configured to fuse a sacroiliac joint once implanted at the joint. The tool 20 is configured such that the anchor 30 can

be quickly, accurately and reliably delivered to a bore 40 of an implant 25 supported off of the tool distal end in a sacroiliac joint.

To begin a detailed discussion of a first embodiment of the system 10, reference is made to FIGS. 2A-3. FIG. 2A is an isometric view of the system 10. FIG. 2B is the same view as FIG. 2A, except an implant assembly 15 of the system 10 is separated from a delivery tool 20 of the system 10. FIG. 3 is the same view as FIG. 2A, except the system 10 is shown exploded to better illustrate the components of the system 10.

As can be understood from FIGS. 2A and 2B, the system 10 includes a delivery tool 20 and an implant assembly 15 for implanting at the sacroiliac joint via the delivery tool 20, the implant assembly 15 being for fusing the sacroiliac joint. As indicated in FIG. 3, the implant assembly 15 includes an implant 25 and an anchor element 30 (e.g., a bone screw or other elongated body). As discussed below in greater detail, during the implantation of the implant assembly 15 at the sacroiliac joint, the implant 25 and anchor element 30 are supported by a distal end 35 of the delivery tool 20, as illustrated in FIG. 2A. In one embodiment, the distal end 35 may be fixed or non-removable from the rest of the delivery tool 20. In other embodiments, the distal end 35 of the delivery tool 20 may be removable so as to allow interchanging of different sized or shaped distal ends 35 to allow matching to particular implant embodiments without requiring the use of a different delivery tool 20 and while maintaining the alignment between components (e.g., anchor 30 aligned with bore 40). The delivery tool 20 is used to deliver the implant 25 into the sacroiliac joint space. The delivery tool 20 is then used to cause the anchor element 30 to extend through the ilium, sacrum and implant 25 generally transverse to the sacroiliac joint and implant 25. The delivery tool 20 is then decoupled from the implanted implant assembly 15, as can be understood from FIG. 2B.

To begin a detailed discussion of components of an embodiment of the implant assembly 15, reference is made to FIG. 4, which is a side isometric view of the implant assembly 15. As shown in FIG. 4, the implant assembly 15 includes an implant 25 and an anchor element 30. The anchor element 30 may be in the form of an elongated body such as, for example, a nail, rod, pin, threaded screw, expanding body, a cable (e.g., configured with a ball end), etc. The anchor element 30 is configured to be received in a bore 40 defined through the implant 25. The bore 40 extends through the implant 25 and is sized such that the anchor element 30 can at least extend into or through the implant 25 as illustrated in FIG. 4.

For a detailed discussion of the implant 25, reference is made to FIGS. 5-17. FIGS. 5-9 are various isometric views of the implant 25. FIGS. 12 and 13 are opposite plan views of the implant 25, and FIGS. 10, 11, 14 and 15 are various elevation views of the implant. FIGS. 16 and 17 are isometric longitudinal cross sections of the implant 25 as taken along corresponding section lines in FIGS. 11 and 13, respectively.

As shown in FIGS. 5-15, in one embodiment, the implant 25 includes a distal or leading end 42, a proximal or trailing end 43, a longitudinally extending body 45, a bore 40 extending through the body, and keels, fins or planar members 50, 55 that radially extend outwardly away from the body 45. In one embodiment, the radially extending planar members 50, 55 may be grouped into pairs of planar members 50, 55 that are generally coplanar with each other. For example, planar members 50 that are opposite the body 45 from each other generally exist in the same plane. More

specifically, as best understood from FIGS. 14 and 15, the planar faces 60 of a first planar member 50 are generally coplanar with the planar faces 60 of a second planar member 50 opposite the body 45 from the first planar member 50. Likewise, the planar faces 65 of a third planar member 55 are generally coplanar with the planar faces 65 of a fourth planar member 55 opposite the body 45 from the third planar member 55.

As best understood from FIGS. 14 and 15, one set of planar members 50 (i.e., the large planar members 50) may extend radially a greater distance D_1 than the distance D_2 extended radially by the other set of planar members 55 (i.e., the small planar members 55). Also, the width W_1 of a large planar member 50 from its outer edge to its intersection with the body 45 may be greater than the width W_2 of a small planar member 55 from its outer edge to its intersection with the body 45. Also, the thickness T_1 of the large planar members 50 may be greater than the thickness T_2 of the small planar members 55. Thus, one set of planar members 50 may be both wider and thicker than the other set of planar members 55. In other words, one set of planar members 50 may be larger than the other set of planar members 55.

In one embodiment, the distance D_1 spanned by the large planar members 50 is between approximately 5 mm and approximately 30 mm, with one embodiment having a distance D_1 of approximately 20 mm, and the distance D_2 spanned by the small planar members 55 is between approximately 5 mm and approximately 20 mm, with one embodiment having a distance D_2 of approximately 14 mm. The width W_1 of a large planar member 50 is between approximately 2.5 mm and approximately 15 mm, with one embodiment having a width W_1 of approximately 5 mm, and the width W_2 of a small planar member 55 is between approximately 1 mm and approximately 10 mm, with one embodiment having a width W_2 of approximately 3 mm. The thickness T_1 of a large planar member 50 is between approximately 2 mm and approximately 20 mm, with one embodiment having a thickness T_1 of approximately 4 mm, and the thickness T_2 of a small planar member 55 is between approximately 1 mm and approximately 10 mm, with one embodiment having a thickness T_2 of approximately 2 mm.

As indicated in FIGS. 5-15, the first set of planar members 50 are generally perpendicular with the second set of planar members 55. Since the sets of planar members 50, 55 are perpendicular to each other, in one embodiment; the intersection of the planar members 50, 55 at a central longitudinal axis of the implant 25 may form the body 45 of the implant 25. In other embodiments, and as illustrated in FIGS. 5-14, the body 45 may be of a distinct shape so as to have, for example, a cylindrical or other configuration. In one embodiment, as indicated in FIG. 14, the cylindrical body 45 has a radius R_1 of between approximately 1 mm and approximately 20 mm, with one embodiment having a radius R_1 of approximately 10 mm.

As illustrated in FIG. 12, in one embodiment, the implant 25 has a length L_1 of between approximately 5 mm and approximately 70 mm, with one embodiment having a length L_1 of approximately 45 mm.

As indicated in FIGS. 5 and 9-14, the implant distal end 42 may have a bullet nose or otherwise rounded configuration, wherein the rounded configuration extends outward away from the distal extremity of the body 45 and along the distal or leading edges of the planar members 50, 55. Thus, as can be understood from FIGS. 5 and 9-13, the leading or distal edges 57 of the planar members 50, 55 may be rounded in the radially extending length of the lead or distal edges and/or in a direction transverse to the radially extend-

ing length of the lead or distal edges. In one embodiment, the leading edges 57 of the planar members 50, 55 each have a radius R_2 of between approximately 1 mm and approximately 15 mm, with one embodiment having a radius R_2 of approximately 10 mm. In one embodiment, the leading end 42 of the implant body 45 and the leading edges 57 of the planar members 50, 55 have a generally conical point configuration.

As indicated in FIGS. 6-8, 10-13, and 15, the implant proximal end 43 has a generally planar face that is generally perpendicular to a longitudinal center axis CA of the implant 25. A center attachment bore 70 and two lateral attachment bores 75 on opposite sides of the center bore 70 are defined in the implant proximal end 43. The center bore 70 is centered about the longitudinal center axis CA, and the lateral attachment bores 75 are near outer ends of the long planar members 50, generally centered in the thickness of the larger planar members 50. Alternatively, in particular embodiments, the implant proximal end 43 can be configured to have a face similarly configured to the implant distal end 42 (i.e. rounded, bullet nosed, etc.) to allow for a simplified removal of implant 25 during a revision surgery.

As indicated in FIGS. 16 and 17, the center bore 70 may be a blind hole in that it only has a single opening. Alternatively, the center bore 70 may be configured as a hole that communicates between the implant proximal end 43 and implant bore 40. A center bore so configured may be able to receive a fastener to permit interference with the anchor member 30 extending through the bore 40 after implantation to resist migration of said anchor member.

As illustrated in FIG. 16, the lateral bores 75 are also blind holes and can be configured to not extend nearly as far into the body 45 as the center hole 70 and can be configured to be not nearly as great in diameter as the center hole 70. In one embodiment, the center attachment bore 70 has a diameter of between approximately 2 mm and approximately 10 mm, with one embodiment having a diameter of approximately 5 mm. In one embodiment, the lateral attachment bores 75 can each have a diameter of between approximately 0.5 mm and approximately 3 mm, with one embodiment having a diameter of approximately 1.5 mm.

As can be understood from FIG. 17, the implant bore 40, which is configured to receive the anchor member 30, has a longitudinal center axis BA that is generally transverse to the longitudinal center axis CA of the implant 25. In one embodiment, the implant bore longitudinal center axis BA forms an angle A_{BA-CA} with the implant longitudinal center axis CA. For example, the angle A_{BA-CA} may be between approximately 15 degrees and approximately 135 degrees, with one embodiment being approximately 45 degrees.

As shown in FIGS. 4-17, the bore 40 is generally located within a plane with which the small radial planar members 55 are located. That the bore 40 is located in the same plane as occupied by the small radial planar members 55 is also the case where the bore 40 angularly deviates from being perpendicular with the longitudinal axis of the implant body 45.

In one embodiment, the implant 25 may be machined, molded, formed, or otherwise manufactured from stainless steel, titanium, ceramic, polymer, composite, bone or other biocompatible materials. The anchor member 30 may be machined, molded, formed or otherwise manufactured from similar biocompatible materials.

In some embodiments, the implant 25 may be substantially as described above with respect to FIGS. 4-17, except the bore 40 of the implant 25 may be angled side-to-side relative to the longitudinal axis of the implant body 45 such

that the bore 40 is not contained in the plane occupied by the small radial planar members 55. For example, as shown in FIGS. 118A-118C, which are, respectively, isometric and opposite plan views of an implant 25 with such a side-to-side deviated bore 40, the bore daylight in the body 45 and large radial planar members 50. In doing so, the bore 40 deviates side-to-side from the plane in which the small planar members 55 are located. Since the bore daylight in the body 45 and large planar members 50, the bore 40 of FIGS. 118A-118C differs from that of FIGS. 4-17, wherein the bore 40 daylight in the small radial members 55.

Just like delivery tool 20 of FIG. 2A has an as-manufactured configuration that allows the anchor arm 115 to deliver the anchor element 30 to the bore 40 of the implant 25 of FIGS. 4-17 without necessitating modification of the delivery tool 20 configuration subsequent to the tool 20 leaving its manufacturing facility, a delivery tool 20 can be configured to similarly interact with the bore 40 of the implant 25 of FIGS. 118A-118C.

In some embodiments, the implant 25 may be substantially as described above with respect to FIGS. 4-17, except the implant 25 may further include an anchor member receiving arm 300. For example, as shown in FIGS. 51-52, which are, respectively, isometric and side elevation views of an implant 25 having an anchor member receiving arm 300, the arm 300 may be generally cantilevered off of the proximal end 43 of the implant 25. The arm 300 includes a free end 305 with a disk-shaped seat 310 having a center hole 315 with a center axis that is coaxially aligned with the center axis BA of the bore 40.

In one embodiment, the arm 300 is rigidly fixed to the implant proximal end 43. In other embodiments, the arm 300 may be in a pivotable or hinged configuration with the implant proximal end 43 to allow movement between the implant 25 and arm 300. Such a hinged arm configuration may be further configured to have a free end 305 which may have a hole 315 (or slot). Due to the hinged configuration of the arm, the arm may be pivoted relative to the rest of the implant such that the center axis of hole 315 may be directed to avoid placing an anchor in a bore 40 or hit the implant 25. In other words, because of the hinged configuration, the arm may be oriented relative to the rest of the implant such that the axis of hole 315 directs an anchor 40 around an implant 25 (i.e., the axis of hole 315 will avoid intersecting the implant 25).

As illustrated in FIG. 53, which is an enlarged view of the disk-shaped seat 310, the disk-shaped seat 310 has a plurality of arcuate members 320 distributed along an inner circumferential boundary 325 of a rim 330 of the disk-shaped seat 310. There may be five or more or less arcuate members 320 distributed generally evenly about the inner circumferential surface 325 of the rim 330.

In one embodiment, each arcuate member 320 has ends 332 that intersect the inner circumferential surface 325 of the rim 330, with a center point 335 of the arcuate member 320 that is offset or spaced apart from inner circumferential surface 325 of the rim 330. Thus, in one embodiment, the arcuate members 320 may be deflectable so as to allow the head of the anchor member 30 to pass between the center points 335 of the members 330 as the head of the anchor member 30 is seated in the seat 310. As a result, the arcuate members 320 can act against the head of the anchor member 30 to prevent the anchor member from working its way out of the bore 40 and opening 315 of the implant 25, thereby serving as an anchor member locking mechanism.

Other arms 300 may have an anchor member locking mechanism with a different configuration. For example, as

illustrated in FIG. 54, which is an isometric view of an implant 25 with another type of anchor member locking mechanism, the arm 300 may be generally cantilevered off of the proximal end 43 of the implant 25. The arm 300 includes a free end 305 with a center hole 315 with a center axis that is coaxially aligned with the center axis BA of the bore 40. As illustrated in FIG. 55, which is an enlarged view of the free end 305, the hole 315 has a cantilevered abutment arm 335 defined in the body of the arm 300 via a series of parallel arcuate slots 340.

In one embodiment, a face 345 of the abutment arm 335 is deflectable and biased radially inward of the inner circumferential surface 350 of the hole 315 such that when the anchor member 30 is extended through the hole 315, the face 345 abuts against the anchor member to prevent the anchor member from working its way out of the bore 40 and opening 315 of the implant 25, thereby serving as an anchor member locking mechanism.

While in the implant embodiment discussed with respect to FIGS. 4-17 may have a cylindrical body 45 at which the planar members 50, 55 intersect, in other embodiments the body 45 of the implant 25 may simply be the region 45 of the implant 25 where the planar members 50, 55 intersect. For example, as shown in FIGS. 56-61, which are, respectively, front isometric, rear isometric, side elevation, plan, front elevation, and rear elevation views of an implant 25, the body 45 of the implant 25 is simply the region 45 of the implant 25 where the planar members 50, 55 intersect. Although not shown in FIGS. 56-61, in one embodiment, the implant 25 has the bore 40 and holes 70, 75 substantially as depicted and discussed with respect to the implant of FIGS. 4-17. Also, the rest of the features of the implant 25 of FIGS. 56-61 are substantially as discussed with respect to the implant 25 of FIGS. 4-17, a main difference being the lack of the cylindrical body 45 and the edges of adjacent intersecting surfaces of the implant 25 of FIGS. 56-61 being rounded or arcuate as opposed to sharp or well-defined edges, as is the case between adjacent intersecting surfaces of the implant embodiment of FIGS. 4-17.

Depending on the embodiment, the implant 25 may have surface features or texture designed to prevent migration of the implant once implanted in the joint space. For example, as shown in FIGS. 62-67, which are, respectively, front isometric, rear isometric, side elevation, plan, front elevation, and rear elevation views of an implant 25 with anti-migration surface features 355, the body 45 of the implant 25 is simply the region 45 of the implant 25 where the planar members 50, 55 intersect. Although not shown in FIGS. 62-67, in one embodiment, the implant 25 has the bore 40 and holes 70, 75 substantially as depicted and discussed with respect to the implant of FIGS. 4-17. Also, the rest of the features of the implant 25 of FIGS. 62-67 are substantially as discussed with respect to the implant 25 of FIGS. 56-61, a main difference being the edges of adjacent intersecting surfaces of the implant 25 of FIGS. 56-61 being sharp or well defined edges as opposed to round or arcuate edges, as is the case between adjacent intersecting surfaces of the implant embodiment of FIGS. 56-61.

As to particular embodiments as shown in FIGS. 56-61, and in other embodiments as disclosed throughout, the implants described herein can be configured to be used as trials during certain steps of the procedure to determine appropriate implant sizes and to allow a physician, who is presented with a kit containing the delivery system 20 and multiple sizes of the implant 20, to evaluate particular

embodiments of an implant as described herein that would be best suited to a particular patient, application or implant receiving space.

As shown in FIGS. 62-67, the anti-migration features 355 are generally evenly distributed along the planar surfaces 60, 65 of the planar members 50, 55 in a rows and columns arrangement. The anti-migration features 355 are generally similarly distributed along the planar surfaces of the edges of the planar members 55. The anti-migration features 355 may be in the form of trapezoids, squares, rectangles, etc. As indicated in FIG. 66, the anti-migration features 355 may have a rectangular cross sectional elevation with a thickness FT of between approximately 0.2 mm and approximately 5 mm, with one embodiment having a thickness FT of approximately 1 mm.

As another example, as shown in FIGS. 68-73, which are, respectively, front isometric, rear isometric, side elevation, plan, front elevation, and rear elevation views of an implant 25 with another type of anti-migration surface features 355, the body 45 of the implant 25 is simply the region 45 of the implant 25 where the planar members 50, 55 intersect. Although not shown in FIGS. 68-73, in one embodiment, the implant 25 has the bore 40 and holes 70, 75 substantially as depicted and discussed with respect to the implant of FIGS. 4-17. Also, the rest of the features of the implant 25 of FIGS. 68-73 are substantially as discussed with respect to the implant 25 of FIGS. 62-67, including the sharp or well defined edges between adjacent intersecting surfaces of the implant 25.

As shown in FIGS. 68-73, the anti-migration features 355 are in the form of unidirectional serrated teeth or ridges 355, wherein the ridges 355 have a triangular cross sectional elevation best understood from FIGS. 70 and 71, wherein the rearward or trailing end of the features 355 are the truncated or vertical end of the triangle cross sectional elevation, and the front or leading end of the features 355 are the point end of the triangle cross sectional elevation. As indicated in FIG. 71, the anti-migration features 355 with the triangular cross sectional elevations have a thickness FT of between approximately 0.2 mm and approximately 5 mm, with one embodiment having a thickness FT of approximately 1 mm, and a length FL of between approximately 0.5 mm and approximately 15 mm, with one embodiment having a thickness FT of approximately 2.5 mm. The triangular ridges 355 are generally evenly distributed along the planar surfaces 60, 65 of the planar members 50, 55 in ridges that run transverse to the length of the implant 25. The anti-migration features 355 are generally similarly distributed along the planar surfaces of the edges of the planar members 55.

In continuing reference to FIGS. 68-73, although the anti-migration features 355 are depicted in the form of unidirectional serrated teeth or ridges 355 on each of the textured surfaces of the implant, the invention is not so limited and, as to particular embodiments, can be configured to have said features 355 arranged in multiple directions, unidirectional, or a combination of multiple direction on some surfaces of the implant and unidirectional on other surfaces of the implant. Accordingly, the features 355 can be so arranged on the various surfaces of the implant so as to prevent undesired migration in particular directions due to the forces present at the sacroiliac joint 1000.

Depending on the embodiment, the implant 25 may have an edge configuration of the planar members 55 designed to prevent migration of the implant once implanted in the joint space. For example, as shown in FIGS. 74-79 which are, respectively, front isometric, rear isometric, side elevation,

plan, front elevation, and rear elevation views of an implant 25 with anti-migration edges or ends 360, the body 45 of the implant 25 is simply the region 45 of the implant 25 where the planar members 50, 55 intersect. Although not shown in FIGS. 74-79, in one embodiment, the implant 25 has the bore 40 and holes 70, 75 substantially as depicted and discussed with respect to the implant of FIGS. 4-17. Also, the rest of the features of the implant 25 of FIGS. 74-79 are substantially as discussed with respect to the implant 25 of FIGS. 56-61, with the exception of the anti-migration edges 360 of the implant embodiment of FIGS. 74-79.

As shown in FIGS. 74-79, the anti-migration edges 360 of the planar members 55 are in the form of notches 365 generally evenly distributed along longitudinally extending free edges or ends of the planar members 55. As indicated in FIG. 77, the notches 365 may have parallel sides 370 inwardly terminating as an arcuate end 375. The orientation of each notch 365 may be such that the center line NL of the notch 365 forms an angle NA with the center axis CA of the implant 25 that is between approximately 90 degrees and approximately 15 degrees, with one embodiment having an angle NA of approximately 45 degrees. As indicated in FIG. 77, each notch 365 may have a length LN between the extreme point on the arcuate end 375 and the outer edge boundary of the notch of between approximately 0.2 mm and approximately 10 mm, with one embodiment having a length LN of approximately 3 mm. Each notch 365 may have a width WN of between approximately 0.5 mm and approximately 20 mm, with one embodiment having a width WN of approximately 2 mm.

As another example, as shown in FIGS. 80-85, which are, respectively, front isometric, rear isometric, side elevation, plan, front elevation, and rear elevation views of an implant 25 with another type of anti-migration edges or ends 360, the body 45 of the implant 25 is simply the region 45 of the implant 25 where the planar members 50, 55 intersect. Although not shown in FIGS. 80-85, in one embodiment, the implant 25 has the bore 40 and holes 70, 75 substantially as depicted and discussed with respect to the implant of FIGS. 4-17. Also, with the exception of its anti-migration edges 360 and its more arcuate distal or leading end 42, the rest of the features of the implant 25 of FIGS. 80-85 are substantially as discussed with respect to the implant 25 of FIGS. 62-67, including the sharp or well defined edges between adjacent intersecting surfaces of the implant 25.

As shown in FIGS. 80-85, the anti-migration edges 360 are flared longitudinally extending free edges or ends of the planar members 55. The edges 360 include a series of ridges 370 that are generally evenly distributed along the length of the edges 360 and oriented transverse to the length of the edges 360.

As indicated in FIG. 83, the ridges 370 have triangular cross sectional elevations with an overall height RA of between approximately 0.2 mm and approximately 8 mm, with one embodiment having a width RA of approximately 1 mm. As illustrated in FIG. 85, the flared longitudinally extending free edges or ends of the planar members 55 have rim edges 380 defining the top and bottom edges of the anti-migration edges 360 of the planar members 55, wherein the rim edges 380 have slopes 385 transitioning between the planar surfaces 65 of the planar members 55 and the rim edges 380.

The edges 360 have a height EH between the edges 380 of between approximately 0.5 mm and approximately 15 mm, with one embodiment having a height EH of approximately 4 mm. The width EW of the flared edge 360 from the beginning of the sloped transition 385 to the face of the edge

360 is between approximately 0.2 mm and approximately 9 mm, with one embodiment having a width EW of approximately 1 mm.

In particular embodiments, the implants with features as described above with respect to FIGS. 62-83 can alternatively be configured to function as a broach or other surgical site preparation tool that can assist in the removal of certain tissues, for example, cartilage or bone, during certain steps of a procedure.

To begin a detailed discussion of components of an embodiment of the delivery tool 20, reference is again made to FIGS. 2A-3. As shown in FIG. 2A, the delivery tool 20 includes a distal end 35 and a proximal end 80. The distal end 35 supports the implant assembly 15 components 25, 30, and the proximal end 80 is configured to be grasped and manipulated to facilitate the implantation of the implant assembly 15 in the sacroiliac joint.

As illustrated in FIG. 3, the delivery tool 20 further includes an arm assembly 85, a handle 90, an implant retainer 95, a sleeve 100 and a trocar or guidewire 105. As shown in FIG. 18, which is a proximal isometric view of the arm assembly 85, the arm assembly 85 includes an implant arm 110 and an anchor arm 115 supported off of the implant arm 110. The implant arm 110 includes a distal end 120, a proximal end 125 and a proximal cylindrical opening 130 of a cylindrical bore 132. The proximal end 125 includes a squared outer surface configuration 135 that facilitates a mechanical engagement arrangement with the handle 90 such as the mechanical arrangement that exists between a wrench and nut.

As shown in FIG. 19, which is a distal isometric view of the arm assembly 85, the distal end 120 includes cylindrical opening 137 of a cylindrical bore 132, large planar members, keels, or fins 140 and small planar members, keels, or fins 145, pins 150, and a planar extreme distal face 152. As depicted in FIG. 20, which is a longitudinal cross section of the implant arm 110 as taken along section line 20-20 in FIG. 18, the cylindrical bore 132 extends the full length of the implant arm 110 between the proximal opening 135 and the distal opening 137.

For a detailed discussion of the interaction between the features of the implant arm distal end 120 and the proximal end 43 of the implant 25, reference is now made to FIGS. 2A and 21A and 22-24. FIG. 21A is a side elevation of the system 10 wherein the tool 20 is attached to the implant assembly 15 for delivery of the implant assembly 15 to the sacroiliac joint. FIG. 22 is the same view as FIG. 21A, except shown as a longitudinal cross section. FIG. 23 is an enlarged view of the distal region of the system 10 circled in FIG. 22. FIG. 24 is an enlarged cross sectional plan view taken in a plane 90 degrees from the section plane of FIG. 23.

As can be understood from FIGS. 2A and 21A and 22-24, when the system 10 is assembled for the delivery of the implant assembly 15 to the sacroiliac joint, the proximal end 43 of the implant 25 (see FIG. 6) is supported off of the implant arm distal end 120 (see FIG. 19). As can be understood from a comparison of FIGS. 6 and 19 and more clearly depicted in FIGS. 23 and 24, the cylindrical body 45, and planar members 50, 55 of the implant 25 and the cylindrical implant arm 110 and planar members 140, 145 of the implant arm 110 respectively correspond with respect to both shape and size such that when the implant 25 is supported off of the implant arm distal end 120 as depicted in FIGS. 2A and 21A and 22-24, the respective outer surfaces of the implant 25 and implant arm distal end 120 transition smoothly moving from the implant 25 to the

implant arm distal end **120**, and vice versa. Also, as shown in FIGS. **23** and **24**, when the system **10** is assembled for the delivery of the implant assembly **15** to the sacroiliac joint, the planar extreme proximal face **43** of the implant **25** abuts against the planar extreme distal face **152** of the implant arm distal end **120**, the pins **150** being received in a recessed fashion in the lateral bores **75**. The pins **150** being received in the lateral bores **75** prevents the implant **25** from pivoting relative to the implant arm **110**. The pins **150** can be configured to have a rectangular, circular or any other cross section and the corresponding lateral bores **75** can also be configured to have corresponding shapes in cross section.

Alternatively, in order to further restrict undesirable movement between components of a system **10**, namely between that of a delivery tool **20** and an implant **25**, the distal face **152** of the implant arm distal end **120** can be configured to rap around, and can also be recessed into or grappled to, the exterior surface of the elongate body **45**, or planar members **50**, or **55** of the implant **25** a distance DE , from about 0.2 mm to about 20 mm (e.g., 10 mm), in the direction of implant distal end **42**. According to particular embodiments, a recess can extend a distance DA from said exterior surfaces in the general direction of implant longitudinal axis CA , from about 0.25 mm to 5 mm (e.g., 1.25 mm). In a non-limiting example of a particular embodiment, the distal face **152** of the implant arm distal end **120** can be further configured to wrap completely or only a portion of the periphery of an implant by occupying only a portion, CAR , as defined by a number of degrees around implant longitudinal axis CA , from about 1 degree to about 180 degrees (e.g., 30 degrees). In particular embodiments, said features can be configured to be located in the area between the planar members **50** and **55**.

As shown in FIGS. **18** and **19**, the anchor arm **115** is supported off of the implant arm **110** at an angle and includes a proximal end **155** and a distal end **160** distally terminating in a sleeve or collar **165** having a longitudinal center axis LCA_1 that is generally transverse to the longitudinal axis of the anchor arm **115**. Collar **165** has a length of between approximately 10 mm and approximately 60 mm (e.g., 20 mm) disposed between collar ends **166** and **167** configured to permit and maintain accurate alignment of the first sleeve **100** along LCA_1 during the course of the procedure. The anchor arm proximal end **155** intersects the implant arm **110** at a location between the proximal and distal ends of the implant arm.

As indicated in FIGS. **18** and **19**, the implant arm **110** also includes a longitudinal center axis LCA_2 . As shown in FIG. **21A**, when the system **10** is assembled such that the implant **25** is mounted on the distal end of the implant arm **110**, the longitudinal center axis CA of the implant **25** is coaxially aligned with the longitudinal center axis LCA_2 of the implant arm **110**, and the longitudinal center axis BA of the implant bore **40** is coaxially aligned with the longitudinal center axis LCA_1 of the anchor arm collar **165**. Thus, the longitudinal center axis CA of the implant **25** and the longitudinal center axis LCA_2 of the implant arm **110** exist on a first common longitudinally extending axis, and the longitudinal center axis BA of the implant bore **40** and the longitudinal center axis LCA_1 of the anchor arm collar **165** exist on a second common longitudinally extending axis.

In one embodiment, the longitudinal center axis LCA_1 of the anchor arm collar **165** forms an angle $A_{LCA1-LCA2}$ with the longitudinal center axis LCA_2 of the implant arm **110**. For example, the angle $A_{LCA1-LCA2}$ may be between approximately 15 degrees and approximately 135 degrees, with one embodiment being approximately 45 degrees.

As can be understood from FIG. **21A**, when the system **10** is assembled such that the implant **25** is mounted on the distal end of the implant arm **110**, the longitudinal center axis LCA_2 of the implant arm **110** is coaxial with the longitudinal center axis CA of the implant **25** and the longitudinal center axis of the handle **90**. Thus, the line of action for the insertion of the implant **25** into the sacroiliac joint is coaxial with the longitudinal center axes of the implant **25**, implant arm **110** and handle **90**.

As can be understood from the preceding discussion, in one embodiment, when the system **10** is assembled such that the implant **25** is mounted on the distal end of the implant arm **110**, the angle A_{BA-CA} may be substantially the same as the angle $A_{LCA1-LCA2}$. Also, the longitudinal center axis BA of the implant bore **40** is coaxially aligned with the longitudinal center axis LCA_1 of the anchor arm collar **165**. Thus, as will be described in detail below, the anchor arm collar **165** is oriented so as to guide drills and other tools in creating a channel through tissue and bone leading to the implant bore **40** when the implant **25** is positioned in the sacroiliac joint while the implant **25** is still attached to the distal end of the implant arm **110**, as shown in FIG. **21**. Additionally, the anchor arm collar **165** is oriented so as to guide the anchor member **30** into the implant bore **40** when the implant **25** is positioned in the sacroiliac joint while the implant **25** is still attached to the distal end of the implant arm **110**, as shown in FIG. **21A**.

As can be understood from FIG. **21A**, in one embodiment, the above-described coaxial and angular relationships are rigidly maintained due to the anchor arm **115** and its collar **165** being in a fixed, non-adjustable configuration, and the interconnection between the proximal end of the anchor arm **115** and the implant arm **110** being a fixed, non-adjustable configuration at least with respect to the angle $A_{LCA1-LCA2}$ between the longitudinal center axis LCA_1 of the anchor arm collar **165** and the longitudinal center axis LCA_2 of the implant arm **110**. Thus, in one embodiment, the delivery tool **20** comes from the manufacture to the physician in a fixed, non-adjustable configuration having the coaxial and angular relationships articulated above with respect to FIG. **21A**.

FIG. **21B** is the same view as FIG. **21A**, except of another embodiment of the delivery tool **20** wherein the tool **20** includes multiple anchor arms **115A-115D** that can be coupled to specific respective locations **168A-168D** on the implant arm **110** to account for different patient sizes, yet still maintain the coaxial and angular relationships set out above. As shown in FIG. **21B**, the delivery tool **20** may include two or more, for example, four, anchor arms **115A-115D**, each anchor arm having a different overall length. Despite having different overall lengths, because each anchor arm **115A-115D** is configured to couple to a specific respective location **168A-168D** on the implant arm **110**, the longitudinal center axis LCA_1 of each anchor arm collar **165A-165D** is still coaxially aligned with the longitudinal center axis BA of the implant bore **40** when each anchor arm is mounted at its correct respective location **168A-168D** on the implant arm **110**. Thus, although the embodiment depicted in FIG. **21B** is adjustable with respect to patient size via the interchangeable anchor arms **115A-115D**, the above-described coaxial and angular relationships are rigidly maintained due to the anchor arms **115A-115D** and their collars **165** being in a fixed, non-adjustable configuration, and the interconnection between the proximal end of the anchor arms **115A-115D** and the implant arm **110** being, a fixed, non-adjustable configuration at least with respect to the angle $A_{LCA1-LCA2}$ between the longitudinal center axis LCA_1 of the anchor arm collar **165** and the longitudinal

center axis LCA_2 of the implant arm **110**. Thus, although the embodiment depicted in FIG. 21B is adjustable with respect to the patient size via the interchangeable anchor arms **115A-115D**, the delivery tool **20** comes from the manufacture to the physician in a fixed, non-adjustable configuration with respect to the coaxial and angular relationships articulated above with respect to FIG. 21A.

Although not shown in FIG. 21B, in some embodiments, multiple sleeves **100** may be provided with the system **10**. For example, the system **10** may include four anchor arms **165A-165D** of different lengths and the system may also include four sleeves **100** of different lengths, each sleeve **100** being configured for use with a specific anchor arm. For example, since anchor arm **165D** is the longest anchor arm, its corresponding sleeve **100** may be the longest of the sleeves. Similarly, since anchor arm **165A** is the shortest anchor arm, its corresponding sleeve **100** may be the shortest of the sleeves.

Because of the multiple interchangeable anchor arms **165A-165D** that are each configured for attachment to a specific respective location **168A-168D** on the implant arm **110**, the delivery tool **20** may be adjusted to accommodate patients of different sizes and still maintain the angular relationships between the components of system **10** that allows the anchor member **30** to be delivered into the implant bore **40** without any further adjustment to the delivery tool. Because the angular relationships are rigidly maintained between the arms **110**, **115**, the collar **165**, and the implant bore **40** despite the anchor arms **115A-115B** being interchangeable, the anchoring of the implant **25** in the sacroiliac joint via the anchor member **30** may be achieved quickly and safely. In other words, because the tool does not need to be adjusted with respect to angular relationships, the surgery is simplified, reduced in duration, and reduces the risk of the anchor member **30** being driven through a nerve, artery or vein.

In some embodiments, the system **10** may be provided with two or more tools **20**, each tool having a configuration for a specific size of patient. For example, the tool **20** depicted in FIG. 21A may be provided for smaller patients in that there is reduced distance between the anchor arm collar **165** and the implant **25**. As depicted in FIG. 21C, which is the same view of FIG. 21A, except illustrating a version of the same tool **20** configured to accommodate larger patients, the distance between anchor arm collar **165** and implant **25** is greater due to the anchor arm **165** being more proximally located on the implant arm **110** as compared to the configuration depicted in FIG. 21A. It should be noted that, although the version depicted in FIG. 21C is configured to accommodate larger patients, the coaxial and angular relationships discussed above with respect to FIG. 21A are the same for the version depicted in FIG. 21C. For the version depicted in FIG. 21C, the sleeve **100** is substantially elongated as compared to the sleeve **100** of FIG. 21A. Depending on the size of the patient, the physician may select or be provided with one of the tool configurations shown in FIG. 21A or 21C.

Additionally, the sleeve **100** of FIG. 21C can be prevented from undesired migration within the anchor arm collar **165** during a procedure by utilizing a locking mechanism **163** in close proximity to the collar **165**. As a non-limiting example, a locking mechanism can be configured as a fastener **163**, which, in certain embodiments, can be threaded and rotatably advanced into the collar **165** to cause a greater amount of friction upon the sleeve **100**.

As shown in FIGS. 25-27, which are various isometric views of the handle **90**, the handle **90** includes a gripping

portion **170**, a neck portion **175**, a proximal end **180**, a distal end **185**, a proximal opening **190**, a distal opening **195** and a bore **200** extending longitudinally through the handle **90** between the openings **190**, **195**. The proximal opening **190** is defined in the proximal end **180**, which forms the extreme proximal portion of the gripping portion **170**. The distal opening **195** is defined in the distal end **185**, which forms the extreme distal portion of the neck portion **175**. The neck portion **175** has multiple regions having different diameters, thereby forming a collared configuration. The gripping portion **170** may have a generally spherical or oval hemispherical shape.

As shown in FIG. 27, a squared inner surface configuration **205** is defined in a segment of the bore **195** located in the neck portion **175**, the rest of the bore **195** having a cylindrical configuration. Thus, as can be understood from FIGS. 1, 21A and 22, when the implant arm distal end **125** is received in the handle bore **200**, the squared inner surface configuration **205** facilitates a mechanical engagement arrangement with the squared outer surface configuration **135** of the implant arm distal end **125**. As a result, grasping the handle so as to cause the handle to pivot about its longitudinal center axis causes the implant arm to similarly pivot about its longitudinal center axis, which is generally coaxial with the longitudinal center axis of the handle. The fit between the squared surface configurations **135**, **205** may be such as to form an interference fit, thereby preventing the handle from being pulled off of the implant arm distal end without the intentional application of substantial separating force.

As illustrated in FIGS. 28 and 29, which are full isometric and longitudinal cross sectional isometric views of the implant retainer **95**, the implant retainer **95** includes a longitudinal cylindrical member **210**, T-handle **215** on a proximal end of the longitudinal cylindrical member **210**, and an implant engagement feature **220** on a distal end of the longitudinal cylindrical member **210**. As can be understood from FIGS. 2A and 21A and 22-24, when the system **10** is assembled for the delivery of the implant assembly **15** to the sacroiliac joint, the longitudinal cylindrical member **210** extending through the handle bore **200** (see FIG. 27) and implant arm bore **132** (FIG. 20) such that a distal side of the T-handle **215** abuts or nearly abuts with the handle proximal face or end **180** (FIG. 25) and the implant engagement feature **220** is received in the implant center bore **70** (FIG. 6). In one embodiment, the implant engagement feature **220** is in the form of a threaded shaft for engaging complementary threads in the center bore **70**, thereby securing the implant proximal face against the implant arm distal face and the pins in the lateral bores, as depicted in FIGS. 22-24. In other embodiments, the implant engagement feature **220** and the center bore **70** are configured so as to form an interference fit between the two such that an intentional separating force is required to remove the implant engagement feature from within the center bore and allow the release of the implant from the distal end of the implant arm, as indicated in FIG. 2B.

FIG. 30A is an isometric view of a sleeve **100** that is configured to be received in the anchor arm collar **165**, as can be understood from FIGS. 2A, 21A, and 22-23. The sleeve **100** may have a tubular portion **225** that extends from a plate **230** and defines a lumen **226** extending the length of the tubular portion **225**. As indicated in FIG. 30B, which is a longitudinal cross section of one embodiment of the sleeve **100**, the sleeve **100** is formed of multiple sleeve portions **100A-100C** nested together such that the tubular portions **225A-225B** are concentrically arranged and the plates

230A-230B are stacked. As each sleeve portion 100A-100C has a tubular portion 225A-225B with a different diameter, the sleeve portions 100A-100C can be employed as needed to dilate an incision opening or guide different diameter guidewires, trocars, drills, etc. in the direction of the implant bore 40.

FIG. 31 is an isometric view of a trocar, guidewire, drill, screwdriver, etc. that may be inserted through the lumen 226 of the tubular portion 225 in gaining access to, or driving the anchor member 30 into, the implant bore 40 when the implant 25 is positioned in the sacroiliac joint via the distal end of the implant arm 110.

To begin a detailed discussion of a second embodiment of the system 10, reference is made to FIGS. 32-33. FIG. 32 is an isometric view of the system 10, and FIG. 33 is the same view as FIG. 32, except the system 10 is shown exploded to better illustrate the components of the system 10.

As can be understood from FIGS. 32 and 33, the system 10 includes a delivery tool 20 and an implant assembly 15 for implanting at the sacroiliac joint via the delivery tool 20, the implant assembly 15 being for fusing the sacroiliac joint. As indicated in FIG. 33, the implant assembly 15 includes an implant 25 and an anchor element 30 (e.g., a bone screw or other elongated body). In one embodiment, the implant assembly 15 is the same as that described above with respect to FIGS. 4-17. As discussed below in greater detail, during the implantation of the implant assembly 15 at the sacroiliac joint, the implant 25 and anchor element 30 are supported by a distal end 35 of the delivery tool 20, as illustrated in FIG. 32. The delivery tool 20 is used to deliver the implant 25 into the sacroiliac joint space. The delivery tool 20 is then used to cause the anchor element 30 to extend through the ilium, sacrum and implant 25 generally transverse to the sacroiliac joint and implant 25. The delivery tool 20 is then decoupled from the implanted implant assembly 15.

As shown in FIG. 32, the delivery tool 20 includes a distal end 35 and a proximal end 80. The distal end 35 supports the implant assembly 15 components 25, 30, and the proximal end 80 is configured to be grasped and manipulated to facilitate the implantation of the implant assembly 15 in the sacroiliac joint.

As illustrated in FIG. 33, the delivery tool 20 further includes an arm assembly 85, a handle 90, an implant retainer 95, and a trocar or guidewire 105. As shown in FIG. 33 and also in FIG. 34, which is a side elevation of the system 10, the arm assembly 85 includes an implant arm 110 and an anchor arm 115.

As shown in FIG. 35, which is a proximal isometric view of the implant arm 110, the implant arm 110 includes a distal end 120, a proximal end 125 and a proximal cylindrical opening 130 of a cylindrical bore 132. The proximal end 125 includes a squared outer surface configuration 135 that facilitates a mechanical engagement arrangement with the handle 90 such as the mechanical arrangement that exists between a wrench and nut. As the handle 90 is the same as described above with respect to FIGS. 25-27, the handle 90 receives and mechanically interlocks with the distal region of the implant arm 110 as described above with respect to FIG. 22.

As with the implant arm 110 discussed above with respect to FIG. 19 and as can be understood from FIG. 34, the distal end 120 of the implant arm 110 includes a cylindrical opening 137 (see FIG. 19) of a cylindrical bore 132, large planar members, keels, or fins 140 and small planar members, keels, or fins 145, pins 150, and a planar extreme distal face 152 (see FIG. 19). Just as explained with respect to FIG. 20 above, the cylindrical bore 132 of the embodiment

depicted in FIG. 34 extends the full length of the implant arm 110 between the proximal opening 135 and the distal opening 137.

As the retaining member 95 of the embodiment of FIG. 33 is the same as described above with respect to FIGS. 28-29, the retainer member 95 extends through the handle 90 and implant arm 110 to mechanically interlock with the implant center bore 70 as described above with respect to FIGS. 22-24. Also, the configuration of the distal end 120 of the implant arm 110 of FIG. 35 is the same as the configuration of the distal end 120 of the implant arm 110 of FIG. 19. Accordingly, the distal end 120 of the implant arm 110 of FIG. 35 interacts with the proximal end of the implant 25 as describe above with respect to FIGS. 22-24.

As indicated in FIG. 35, the implant arm 110 includes pivot pins 235 on opposite sides of the implant arm 110, the pivot pins 235 having a pivot axis PA that is perpendicular to the plane in which the implant bore 40 passes through the implant 25. In other words, the pivot axis PA is perpendicular to the longitudinal center axis LCA_2 of the implant arm 110 and contained within the same plane as the longitudinal center axis LCA_2 of the implant arm 110. The pivot pins 235 are located on the implant arm 110 near the distal end of the handle 90.

As illustrated in FIG. 36, which is an isometric view of the anchor arm 115, the anchor arm 115 includes a proximal end 155 and a distal end 160 distally terminating in a sleeve or collar 165 that is arcuate and substantially extended as compared to the collar 165 of the embodiment depicted in FIG. 18. The arcuate and extended collar 165 has an arcuate longitudinal center axis LCA_7 that is generally transverse to the longitudinal axis of the anchor arm 115. A lumen 236 extends the length of the collar 165 to daylight in openings at both ends of the collar 165.

As shown in FIG. 36, the anchor arm proximal end 155 includes notches 240, which, as can be understood from FIGS. 32 and 34, receive the respective pivot pins 235. As a result, the anchor arm 115 is pivotally supported off of the implant arm 110 via the notches 240 at the anchor arm proximal end 155 pivotally receiving the pivot pins 235 of the implant arm 110.

As can be understood from FIGS. 32-34, an arcuate member 105 can be inserted in the lumen 236 of the arcuate extended collar 165. The curvature of the arcuate member 105 matches the curvature of the lumen 236 of the arcuate collar 165. The arcuate member 105 may be a trocar, guidewire, drill, screwdriver, etc. that may be inserted through the lumen 236 of the collar 165 in gaining access to, or driving the anchor member 30 into, the implant bore 40 when the implant 25 is positioned in the sacroiliac joint via the distal end of the implant arm 110. As indicated by the arrow A in FIG. 34, the arcuate member 105 is slidably displaceable through the arcuate length of the collar 165. Also, as indicated by arrow B, the anchor arm 110 is pivotal about the pivot pins 235.

As indicated in FIG. 35, the implant arm 110 includes a longitudinal center axis LCA_2 . As shown in FIG. 34, when the system 10 is assembled such that the implant 25 is mounted on the distal end of the implant arm 110, the longitudinal center axis CA of the implant 25 is coaxially aligned with the longitudinal center axis LCA_2 of the implant arm 110, and the longitudinal center axis BA of the implant bore 40 is coaxially aligned with the longitudinal center axis LCA_1 of the anchor arm collar 165. In other words, in the context of the embodiment of FIG. 34, the arcuate longitudinal center axis LCA_1 extends to be coaxially aligned with the longitudinal center axis BA of the

implant bore 40. In one embodiment, as indicated in FIG. 34, the longitudinal center axis LCA_1 of the anchor arm collar 165 has an arm radius R_{ARM} that extends into coaxial alignment with the longitudinal center axis BA of the implant bore 40. For example, the arm radius R_{ARM} may be between approximately 50 mm and approximately 300 mm, with one embodiment being approximately 160 mm.

As can be understood from FIG. 34, when the system 10 is assembled such that the implant 25 is mounted on the distal end of the implant arm 110, the longitudinal center axis LCA_2 of the implant arm 110 is coaxial with the longitudinal center axis CA of the implant 25 and the longitudinal center axis of the handle 90. Thus, the line of action for the insertion of the implant 25 into the sacroiliac joint is coaxial with the longitudinal center axes of the implant 25, implant arm 110 and handle 90. Thus, as will be described in detail below, the anchor arm collar 165 is oriented so as to guide drills and other tools in creating a channel through tissue and bone leading to the implant bore 40 when the implant 25 is positioned in the sacroiliac joint while the implant 25 is still attached to the distal end of the implant arm 110, as shown in FIG. 34. Additionally, the anchor arm collar 165 is oriented so as to guide the anchor member 30 into the implant bore 40 when the implant 25 is positioned in the sacroiliac joint while the implant 25 is still attached to the distal end of the implant arm 110, as shown in FIG. 32.

Because the tool embodiment depicted in FIG. 32 has an anchor arm 115 that is pivotally supported off of the implant arm 110 and the anchor arm collar 165 is arcuate and slidably receives an arcuate trocar, etc. 105, the tool 20 is able to account for different patient sizes, yet still maintain the coaxial and angular relationships set out above. In other words, regardless of whether the anchor arm 115 is pivoted so as to move the anchor arm distal end 160 closer to or further away from the implant bore 40 to accommodate a smaller or larger patient, the trocar 105 can be withdrawn from or extended towards the implant bore 40 as needed to deliver the anchor 30 to the implant bore 40, the trocar 105 being maintained in the necessary coaxial alignment of the longitudinal axis LCA_1 of the collar 165 with the longitudinal axis BA of the implant bore 40.

Because the angular relationships are rigidly maintained between the trocar 105 and the implant bore 40 despite the anchor arm 115 being pivotal relative to the implant arm, the anchoring of the implant 25 in the sacroiliac joint via the anchor member 30 may be achieved quickly and safely. In other words, because the tool does not need to be adjusted with respect to angular relationships, the surgery is simplified, reduced in duration, and reduces the risk of the anchor member 30 being driven through a nerve, artery or vein.

To begin a detailed discussion of a third embodiment of the system 10, reference is made to FIGS. 37-40. FIGS. 37 and 38 are different isometric views of the system 10. FIG. 39 is the same view as FIG. 37, except the system 10 is shown exploded to better illustrate the components of the system 10. FIG. 40 is a side elevation of the system wherein the tool is attached to the implant assembly for delivery of the implant assembly to the sacroiliac joint.

As can be understood from FIGS. 37-40, the system 10 includes a delivery tool 20 and an implant assembly 15 for implanting at the sacroiliac joint via the delivery tool 20, the implant assembly 15 being for fusing the sacroiliac joint. As indicated in FIG. 39, the implant assembly 15 includes an implant 25 and an anchor element 30 (e.g., a bone screw or other elongated body).

As can be understood from a comparison of FIGS. 2A-3 to FIGS. 37-40, the delivery tool 20 of FIGS. 2A-3 is the same as the delivery tool 20 of FIGS. 37-40. Thus, for a complete description of the delivery tool 20 of FIGS. 37-40 and its components, namely, the arm assembly 85, handle 90, implant retainer 95, a trocar or guidewire 105, and multiple nested sleeves 100, refer back to the corresponding discussion given above with respect to FIGS. 2A-3 and 18-31.

As indicated in FIGS. 37-40, the system 10 includes an implant assembly 15 with an implant 25 similar the implant 25 discussed above with respect to FIGS. 4-18, except the implant 25 of FIGS. 37-40 also includes a guide arm 265. To begin a detailed discussion of components of the embodiment of the implant 25 of FIGS. 37-40, reference is made to FIGS. 41-50. FIGS. 41-44 are various isometric views of the implant 25. FIGS. 45-46 are opposite plan views of the implant 25, and FIGS. 47-50 are various elevation views of the implant.

A comparison of FIGS. 41-50 to FIGS. 5-18 reveals that the two implant embodiments are the same, except the implant embodiment of FIGS. 41-50 has a guide arm 265. Thus, for a complete description of the features of the implant 25 other than the guide arm 265, which is discussed below, refer back to the corresponding discussion given above with respect to FIGS. 5-18.

As shown in FIGS. 41-45 and 46-50, the guide arm 265 includes a longitudinally extending member 270 and a guide portion 275. The guide arm 265 is cantilevered off of a side of the implant near the proximal or trailing end 43 of the implant 25. Thus, the guide arm 265 includes an attached end 280, which is attached to, or extends from, the implant proximal end 43, and a free end 285, which defines the guide portion 275.

The longitudinally extending member 270 may be in the form of a planar member or other shaped member. As illustrated in FIG. 45, the longitudinal axis LA of the member 270 is generally coplanar with the longitudinal axis CA of the implant body 45. However, as indicated in FIG. 48, the longitudinal axis LA of the member 270 forms an angle A_{LA-CA} with the longitudinal axis CA of the implant body 45. For example, the angle A_{LA-CA} may be between approximately 5 degrees and approximately 60 degrees, with one embodiment being approximately 40 degrees.

As illustrated in FIGS. 41-45 and 47-50, the guide portion 275 is in the form of a collar defining a central hole 290. As indicated in FIG. 47, the member 270 has an overall length AD from its intersection with the rest of the implant to the tip of the free end 285 of between approximately 5 mm and approximately 60 mm, with one embodiment being approximately 20 mm. Also, the center axis GA of the hole 290 is coaxially aligned with the center axis BA of the bore 40. The overall length AE from the intersection of the member 270 with the rest of the implant to the center axis GA is between approximately 2 mm and approximately 58 mm, with one embodiment being approximately 17 mm.

Since the center axis GA of the hole 290 is coaxially aligned with the center axis BA of the bore 40, when the system 10 is assembled such that the implant 25 is mounted on the distal end of the implant arm 110 with the longitudinal center axis LCA_2 of the implant arm 110 coaxial with the longitudinal center axis CA of the implant 25, the respective longitudinal axes LCA_1 , BA and GA of the anchor arm collar 165, the bore 40 and the guide hole 290 are coaxially aligned, as can be understood from FIG. 40. Thus, when the implant body 45 is located in the sacroiliac joint and the guide collar 275 of the implant 25 is located near or against

bone adjacent to the sacroiliac joint, the anchor member **30** may be accurately driven through the guide hole **290**, through the bone and through the implant bore **40** to anchor the implant at the sacroiliac joint in such a manner to allow the implant to fuse the joint.

In one embodiment, the implant **25** may be machined, molded, formed, or otherwise manufactured from stainless steel, titanium, ceramic, polymer, composite or other biocompatible materials. The anchor member **30** may be machined, molded, formed or otherwise manufactured from similar biocompatible materials. As an example, implant **25**, anchor **30** or delivery tool **20** may be manufactured by laser or electron beam additive manufacturing with, for example, EOSINT P 800 or EOSINT M 280 (available from EOS GmbH, Electro Optical Systems, Robert-Stirling-Ring 1, D-82152 Krailling/Munich), or Arcam A1 (available from Arcam AB (publ.), Krokslatts Fabriker 27A, SE-431 37 Molndal Sweden).

For the delivery tools **20** depicted in FIGS. **2A**, **21A**, **21C**, **32**, **37**, and **40**, the handle **90** and arm assembly **85** are coupled together so as to not allow rotational movement relative to each other, and the implant retainer **95** is rotationally displaceable within the handle **90** and arm assembly **85**. In other embodiments of the tool **20**, the handle **90** and implant retainer **95** are coupled together so as to rotate as a unit relative to the arm assembly **85**. An example of such an embodiment is illustrated in FIG. **86**, which is an isometric view of the delivery tool **20**.

As shown in FIG. **86**, the delivery tool **20** includes a distal end **35** and a proximal end **80**. As shown in FIGS. **87-88**, which are generally opposite isometric views of the delivery tool **20** in an exploded state, the tool **20** further includes an arm assembly **85**, a handle **90**, an implant retainer **95**, and a collar assembly **400**. The tool **20** may also include a sleeve **100** and a trocar or guidewire **105** as discussed above with respect to the embodiment of FIG. **3**.

As can be understood from FIGS. **86-88**, the arm assembly **85** includes an implant arm **110** and an anchor arm **115** supported off of the implant arm **110**. The implant arm **110** has a two-piece construction of an inner sleeve **110A** and an outer sleeve **110B**. The implant arm inner sleeve **110A** includes a distal end **120**, a proximal end **125**, a proximal cylindrical opening **130** of a cylindrical bore **132**, and a distal cylindrical opening **137** of the bore **132**. The cylindrical bore **132** extends the full length of the implant arm inner portion **110A** between the proximal opening **135** and the distal opening **137**. Longitudinally extending raised ribs **405** are radially distributed about the outer circumferential surface of the implant arm inner portion **110A**. The longitudinal ribs **405** distally terminate by intersecting a raised circumferential ring **410** on the outer circumferential surface of the inner implant arm portion **110A**. A groove **415** is circumferentially extends about the outer circumference of the implant arms inner portion **110A**. The distal end **120** of the implant arm inner portion **110A** also includes large planar members, keels, or fins **140** and small planar members, keels, or fins **145**, pins **150**, and a planar extreme distal face **152** similar to that discussed above with respect to the embodiment of FIG. **2A**.

As illustrated in FIGS. **87-88**, the implant arm outer portion **110B** includes a distal end **420**, a proximal end **425**, a proximal cylindrical opening **430** of a cylindrical bore **432**, and a distal cylindrical opening **437** of the bore **432**. The cylindrical bore **432** extends the full length of the implant arm outer portion **110B** between the proximal opening **435** and the distal opening **437**. Longitudinally extending grooves **440** are radially distributed about the inner circum-

ferential surface of the bore **432** in an arrangement that matches the longitudinal raised ribs **405** of the implant arm inner portion **110A** such that the ribs **405** are received in the grooves **440** in a mated arrangement when the inner portion **110A** is received in the bore **432** of the outer portion **110B**. The anchor arm **115** extends off the implant arm outer portion **110B** at an angle as described above with respect to the previously discussed embodiments. The anchor arm **115** terminates at its free end in a collar **165** similar to those already discussed above.

As shown in FIGS. **87** and **88**, the implant retainer **95** includes a proximal end **215**, a distal end **220**, and a lumen **445** extending the full length of the implant retainer **95**. The proximal end **215** includes a squared, pentagonal or hexagonal outer surface configuration **450** that facilitates a mechanical engagement arrangement with the handle **90** such as the mechanical arrangement that exists between a wrench and nut. A ring **451** radially extends from the retainer **95** at the distal edge of the squared, pentagonal or hexagonal configuration **450**. The distal end **220** may be threaded or otherwise configured to engage a proximal end of anyone of the implants **25** disclosed herein.

As illustrated in FIGS. **87** and **88**, the collar assembly **400** includes a helical spring **455**, rings **460A** and **460B**, washer **460C**, retainer balls **461**, and a retaining collar **465**. As shown in FIG. **89**, which is an isometric view of the handle **90**, a cylindrical neck portion **470** of the handle **90** includes a shoulder **476** which slopes down to a circumferential groove **475** and a pair of holes **480** defined in the outer circumferential surface of the neck **470**.

As indicated in FIG. **90**, which is an exploded isometric view of the retaining collar **465** and handle **90** shown in longitudinal cross section, the holes **480** extend through the cylindrical wall **485** that defines the neck **470** and a cylindrical void **487** within the neck. A squared, pentagonal or hexagonal inner surface configuration **490** is defined in the handle **90** distal the cylindrical void **487** to receive in a mating arrangement the complementarily shaped outer configuration **450** of the proximal end of the implant retainer **95**. A lumen **495** extends from a proximal end of the handle to open into the squared, pentagonal or hexagonal inner surface configuration **490**.

As shown in FIG. **90**, the retaining collar **465** includes a proximal end **500**, a distal end **505**, an outer circumferential surface **510** and an inner circumferential surface **515** that defines the hollow interior of the collar **517**. The outer circumferential surface **510** extends radially outward to form a rim **520** near the proximal end **500**. The inner circumferential surface **515** has a stepped and ramped configuration. Specifically, working distal to proximal, the inner circumferential surface **515** includes a proximal inner ring **525** separated from an intermediate inner ring **530** by a proximal large diameter region **535** separated from a small diameter region **540** by a ramped surface **545**. Proximal the intermediate inner ring **530** is another large diameter region **550** bordered on its proximal boundary by a groove **555**.

As can be understood from FIG. **91**, which is a longitudinal cross section of the delivery tool **20** when assembled as shown in FIG. **86**, the implant arm inner portion **110A** is received in the implant arm outer portion **110B** such that the ribs **405** are matingly received in the corresponding slots **440** and the ring **410** abuts against the distal end **420** of the outer portion **110B**. The implant retainer **95** extends through the inner portion **110A** such that the distal end **220** of the implant retainer distally extends from the distal end **120** of the inner portion **110A** and the ring **451** abuts against the proximal end **125** of the inner portion **110A**. The proximal

ends of the inner portion 110A and retainer 95 are received in the volume 487 (see FIG. 90) of the neck 470, the squared, pentagonal, or hexagonal portion 450 of the retainer 95 matingly received in the complementarily shaped volume 490 of the neck such that the ring 451 abuts against the step in the neck between the volume 490 of the neck and the rest of the volume of the neck distal thereto. The distal end of the neck 470 abuts against the proximal end 425 of the outer portion 110B.

As illustrated in FIG. 91, a first lock ring 460A is received in the groove 555 in the collar 465. A second lock ring 460B is received in the circumferential groove 475. A washer 460C is received on the neck 470 and abuts shoulder 476, which prevents washer 460C from advancing proximally beyond shoulder 476, and washer 460C is held in place distally by second lock ring 460B. Helical spring 455 circumferentially extends about the neck 470 between the washer 460C and the intermediate inner ring 530 of the collar 465. Thus, the spring biases the collar 465 distally on the neck 470. First lock ring 460A prevents collar 465 from distal disengagement from neck 470; the ring 460A, due to the forces exerted by a compressed spring 455 abuts washer 460C under normal conditions until manipulation by a medical person acting to move collar 465 proximally which in turn moves first lock ring 460A proximally thereby creating a further distance between first lock ring 460A and washer 460C.

As depicted in FIG. 91, neck holes 480 can be configured to have a sufficient diameter to allow the retaining balls 461 to enter from the opening nearest the outer circumferential surface of the neck 470 and to be seated within holes 480, the configuration further allowing a portion of the retaining balls 461 to extend into the cylindrical void 487 such to allow sufficient engagement with groove 415 as further described below. The neck holes 480 can be further configured, as depicted in FIG. 91, to have a slight reduction in their diameter, the reduction of diameter occupying a small portion of the holes 480 nearest the cylindrical void 487, thereby allowing for a configuration between neck 470, neck holes 480 and retaining balls 461 such that the retaining balls 461 are resistant to completely entering cylindrical void 487 after the removal of inner portion of the implant retainer 95 and implant arm inner portion 110A. The balls 461 are each held in their respective holes 480 in the neck 470 by the balls 461 being trapped between the neck holes 480 and inner circumferential surface of the collar 465. Therefore, when the collar 465 is biased distally on the neck, the balls 461 are inwardly forced by the reduced diameter region 540 to lock into the groove 415 of the inner portion 110A, retaining the proximal end of the anchor arm 110 in the handle/collar assembly. When the collar 465 is pulled proximally by a medical person using the tool 20, the balls 461 are exposed to the large diameter region 535, allowing the balls 461 sufficient play to radially outwardly move in the holes 480 to allow the balls to escape the groove 415, thereby allowing the proximal end of the anchor arm 110 to be removed from the handle/collar assembly.

As shown in FIG. 91, the lumens 495 and 445 are aligned to make one continuous lumen through the assembled tool 20. Thus, the tool 20 can be fed over a guidewire, stylet, needle or etc., or such implements can be fed through the lumen. Also, a bone paste, in situ curable biocompatible material, or similar material can be fed through the lumen to an implant 25 positioned in the joint via the tool.

As can be understood from FIGS. 86-91, the collar assembly 400 retains the proximal end of the implant arm 110 in the neck of the handle 90. The collar assembly 400

can be displaced proximally on the neck of the handle 90 to allow the proximal end of the implant arm 110 to be removed from the neck of the handle. When the implant arm 110 is coupled to the handle 90, the portions 110A and 110B of the implant arm 110 are locked together and prevented from displacing relative to each other, but the handle 90 and retainer 95 can be caused to rotate as a unit relative to the implant arm 110 to cause the distal end 220 of the retainer 95 engage or disengage the implant 25 as desired. Accordingly, the configuration allows for the removal of a handle 90 during the course of a procedure while allowing the retainer 95 to maintain engagement with implant 25 as desired.

Additionally, as a non-limiting example, according to particular embodiments, a reversible locking ratcheting mechanism can be employed to prevent undesired rotation of the handle and other components which could loosen the connection between implant 25 and retainer 95.

As illustrated in FIG. 92, which is a side view of an implant retainer 95 similar to that described with respect to FIGS. 86-91, except having a modified distal end 220. Specifically, the embodiment of FIG. 92 has T-shaped distal end 220. In one embodiment, the T-shaped distal end 220 includes a cylindrical center portion 220A and ears or tabs 220B oppositely positioned on the center portion 220A from each other.

FIGS. 93-94 are, respectively, longitudinal and transverse cross sectional views of an implant 25 with an engagement hole 70 configured to complementarily engage with the T-shaped distal end 220 of the retainer 95 of FIG. 92. As illustrated in FIGS. 93-94, the hole 70 includes a cylindrical longitudinally extending center portion 70A with longitudinally extending grooves 70B located oppositely from each other. Inner radially extending grooves 70C intersect the distal ends of the grooves 70B.

As shown in FIG. 95, which is the same view as FIG. 93, except with the retainer 95 received in the hole 70, the cylindrical retainer portion 220A is received in the cylindrical hole portion 70A, and the retainer tab portions 220B are received in the hole grooves 70B. Once the distal end 220 of the retainer 95 is sufficiently received in the hole 70 such that the retainer tab portions 220B are aligned with the associated radially extending grooves 70C as illustrated in FIG. 95, the retainer 95 can be rotated within the hole 70 to cause the tab portions 220B to move into the radially extending grooves 70C, thereby locking the distal end 220 of the retainer 95 in the hole 70 of the implant 25. Grooves 70C can be configured such as to form an interference fit, thereby preventing retainer 95 from being separated from the implant 25 without the intentional application of substantial rotational separating force. Reversing the rotation of the retainer can cause the tab portions 220B to exit the radial grooves 70C, thereby unlocking the retainer distal end from the implant hole. Alternatively, according to particular embodiments, as a non-limiting example, radially extending grooves 70C can be configured to have at least one ramped surface, which upon rotation of retainer 95 into the grooves 70C, urges the distal end 220 a distance further in the direction of distal end 42 of implant 25 thereby creating increased friction between ring 45 of retainer 95 and proximal end 125 of 110A thereby preventing undesirable reverse rotation of the retainer without the intentional application of substantial rotational separating force, which otherwise could lead to an unlocking of the retainer distal end from the implant hole.

As illustrated in FIG. 93, in one embodiment, the implant 25 may include a lumen 600 extending the length of the

implant through the anchor hole **40** and the retainer engagement hole **70**. Such a lumen **600** may serve to receive a guidewire or stylet there through. Such a lumen **600** may serve to receive an injection of bone paste material, or other biocompatible material.

To begin a detailed discussion of a fourth embodiment of the system **10**, reference is made to FIGS. **109** and **110**. FIG. **109** is an isometric view of the system **10** wherein the tool **20** is attached to the implant **25** for delivery of the implant to the sacroiliac joint. FIG. **110** is a view of the system **10** wherein the implant **25** and anchor arm **115** are shown in plan view.

As can be understood from FIGS. **109-110**, the system **10** includes a delivery tool **20** and an implant **25** for implanting at the sacroiliac joint via the delivery tool **20**, the implant **25** being for fusing the sacroiliac joint. As can be understood from a comparison of FIGS. **109** and **86**, the tool embodiment of FIG. **109** is substantially similar to the tool embodiment of FIG. **86**, except the tool embodiment of FIG. **109** has an anchor arm **115** that distally ends in multiple anchor collars **165a-165d**.

As can be understood from a comparison of FIGS. **109** and **7**, the implant embodiment of FIG. **109** is substantially similar to the implant embodiment of FIG. **7**, except the implant embodiment of FIG. **109** has multiple bores **40a-40b**.

As illustrated in FIGS. **109-110**, the anchor collars **165** may include two linearly aligned center collars **165a** and **165b**, and a lateral anchor collar **165c** and **165d** may be located on either side of the most proximal center collar **165b**. As indicated in FIG. **110**, the two center collars **165a** and **165b** may be axially aligned with the respective bores **40a** and **40b** of the implant **25** when the implant **25** is supported off of the distal end of the implant arm **110** of the tool **20**. As a result, an anchor member **30** (see, for example, FIG. **4**) may be delivered into each of the bores **40a** and **40b** via the respective anchor collars **165a** and **165b**. The lateral anchor collars **165c** and **165d** may be employed to deliver yet additional anchor members **30** to additional anchor member receiving features (e.g., bores, etc.) existing on, or extending from the sides of, the implant **25**, where such additional anchor member receiving features are present on the implant **25**. Alternatively, lateral collars **165c** and **165d** can be configured to deliver additional anchor members **30** into the bone of the ilium and sacrum while not passing through a bore **40** (i.e., preconfigured to place anchor members **30** immediately adjacent the longitudinal side edges of the implant **25**).

To begin a discussion regarding the methodology associated with employing any of the above-described delivery tools **20** in implanting any of the above-described implants **25** in the sacroiliac joint **1000** of a patient **1001**, reference is first made to FIGS. **96A-98B** to identify the bone landmarks adjacent, and defining, the sacroiliac joint **1000**. FIG. **96A** is a right lateral side view of a hip region **1002** of a patient **1001** lying prone, wherein the soft tissue **1003** surrounding the skeletal structure **1006** of the patient **1001** is shown in dashed lines. FIG. **96B** is an enlarged view of the hip region **1002** of FIG. **96A**. As illustrated in FIGS. **96A** and **96B**, a lateral view of the patient's hip region **1002** reveals certain features of the ilium **1005**, including the anterior superior iliac spine **2000**, the iliac crest **2002**, the posterior superior iliac spine **2004**, the posterior inferior iliac spine **2006**, the greater sciatic notch **2008** extending from the posterior inferior iliac spine **2006** to the ischial spine **2010**, and the tubercle of iliac crest **2012**. The sacroiliac joint articular region **1044** is shown in dashed lines. A posterior inferior

access region **2016** of the sacroiliac joint articular region **1044** has a superior end **2018** on the sacroiliac joint line **2019** that is between approximately **0** mm and approximately **40** mm inferior the posterior inferior overhang **2020** of the posterior superior iliac spine **2004**. The posterior inferior access region **2016** of the sacroiliac joint articular region **1044** has an inferior end **2022** on the sacroiliac joint line that is at approximately the intersection of the posterior inferior iliac spine **2006** with the lateral anterior curved boundary **2024** of the sacrum **1004**. In other words, the posterior inferior access region **2016** of the sacroiliac joint articular region **1044** has an inferior end **2022** on the sacroiliac joint line that is at approximately the superior beginning of the greater sciatic notch **2008**.

FIG. **97A** is a lateral-posterior view of the hip region **1002** of the patient **1001** of FIG. **96A**, wherein the patient **1001** is lying prone and the soft tissue **1003** surrounding the skeletal structure **1006** of the patient **1001** is shown in dashed lines. FIG. **97B** is an enlarged view of the hip region **1002** of FIG. **97A**. As shown in FIGS. **97A** and **97B**, a lateral-posterior view of the patient's hip region **1002** reveals the same features of the sacrum **1004** and ilium **1005** as discussed above with respect to FIGS. **96A** and **96B**, except from another vantage point. The vantage point provided via FIGS. **97A** and **97B** provides further understanding regarding the posterior inferior access region **2016** of the sacroiliac joint articular region **1044** and superior end **2018** and inferior end **2022** of the posterior inferior access region **2016** relative to nearby anatomical features, such as, for example, the posterior inferior overhang **2020** of the posterior superior iliac spine **2004**, the intersection of the posterior inferior iliac spine **2006** with the lateral anterior curved boundary **2024** of the sacrum **1004**, and the superior beginning of the greater sciatic notch **2008**.

FIG. **98A** is a posterior view of the hip region **1002** of the patient **1001** of FIG. **96A**, wherein the patient **1001** is lying prone and the soft tissue **1003** surrounding the skeletal structure **1006** of the patient **1001** is shown in dashed lines. FIG. **98B** is, an enlarged view of the hip region **1002** of FIG. **98A**. As shown in FIGS. **98A** and **98B**, a posterior view of the patient's hip region **1002** reveals the same features of the sacrum **1004** and ilium **1005** as discussed above with respect to FIGS. **96A** and **96B**, except from yet another vantage point. The vantage point provided via FIGS. **98A** and **98B** provides yet further understanding regarding the posterior inferior access region **2016** of the sacroiliac joint articular region **1044** and superior end **2018** and inferior end **2022** of the posterior inferior access region **2016** relative to nearby anatomical features, such as, for example, the posterior inferior overhang **2020** of the posterior superior iliac spine **2004**, the intersection of the posterior inferior iliac spine **2006** with the lateral anterior curved boundary **2024** of the sacrum **1004**, and the superior beginning of the greater sciatic notch **2008**.

Now that the relevant anatomical landmarks have been identified with respect to FIGS. **96A-98B**, the methodology associated with employing any of the above-described delivery tools **20** in implanting any of the above-described implants **25** in the sacroiliac joint **1000** of a patient **1001** can be discussed. In doing so, reference will be made to FIGS. **99A-99P**, which are each a step in the methodology and illustrated as the same transverse cross section taken in along a plane extending medial-lateral and anterior posterior along section line **99-99** in FIG. **98B**. In this cross section, articular surfaces **1016** are covered by a thick layer of articular cartilage with a joint space existing between them, the FIGS. **99A-99P** are simplified for illustrative purposes

and do not show these features to scale. Now referring primarily to FIG. 99A, an embodiment of the method can include the step of placing a patient under sedation prone on a translucent operating table (or other suitable surface). The sacroiliac joint 1000 can be locally anesthetized to allow for injecting a radiographic contrast 1046 (as a non-limiting example, Isovist 300 radiographic contrast) under fluoroscopic guidance into the inferior aspect of the sacroiliac joint 1000 to outline the articular surfaces 1016 of the sacroiliac joint 1000 defined between the sacrum 1004 and ilium 1005, the sacroiliac joint 1000 having an interarticular region 1044. Injection of the radiographic contrast 1046 within the sacroiliac joint 1000 can be accomplished utilizing a tubular member 1047 (such as a syringe needle) having first tubular member end 1048 which can be advanced between the articulating surfaces 1016 of the sacroiliac joint 1000 and having a second tubular member end 1049 which removably couples to a hub 1050. The hub 1050 can be configured to removably couple to a syringe barrel 1051 (or other device to contain and deliver an amount of radiographic contrast 1046). In the example of a syringe barrel 1051, the syringe barrel 1051 can have an internal volume capable of receiving an amount of the radiographic contrast 1046 sufficient for outlining the articular surfaces 1016 of the sacroiliac joint 1000, for example, under lateral fluoroscopy. A plunger 1052 can be slidably received within the barrel 1051 to deliver the radiographic contrast 1046 through the tubular member 1047 into the sacroiliac joint 1000. The tubular member 1047 can have a gauge in the range of about 16 gauge and about 20 gauge and can further be incrementally marked on the external surface to allow determination of the depth at which the first needle end 1048 has advanced within the sacroiliac joint 1000. As the first needle end 1048 advances into the sacroiliac joint 1000 the radiographic dye 1046 can be delivered from within the syringe barrel 1051 into the sacroiliac joint 1000 to allow visualization of the sacroiliac joint 1000 and location of the tubular needle 1047 within the sacroiliac joint 1000.

Now referring primarily to FIG. 99B, once the first tubular member end 1048 has been sufficiently advanced into the sacroiliac joint 1000 and the articular surfaces 1016 of the sacroiliac joint 1000 have been sufficiently visualized, the hub 1050 can be removed from the tubular member 1047 leaving the tubular member 1047 fixed within the sacroiliac joint 1000 as an initial guide for tools subsequently used to locate or place the sacroiliac joint implant 25 non-transversely between the articulating surfaces 1016 of the sacroiliac joint 1000 (e.g., locate the implant 25 non-transversely to the joint plane 1030 generally defined by the articulating surfaces 1016 of the interarticular region 1044 of the sacroiliac joint 1000) or in removal of a portion of the sacroiliac joint 1000 within the region defined by the articular surfaces 1016 to generate an implant receiving space 1029 (see FIG. 99H). Alternately, one or more guide pins 1013 can be inserted along substantially the same path of the tubular member 1047 for fixed engagement within the sacroiliac joint 1000 and used in subsequent steps as a guide(s).

Now referring primarily to FIG. 99C, a small incision 1053 can be made in the skin at the posterior superior (or as to certain embodiments inferior) aspect of the sacroiliac joint 1000, extending proximal and distal to the tubular member 1047 along the line of the sacroiliac joint 1000 to provide a passage to access the interarticular space between the articulating surfaces 1016 (see FIG. 99B) of the sacroiliac joint 1000. More specifically, as can be understood

from FIGS. 96A-98B, in one embodiment, the small incision 1053 can be made along the joint line 2019 of the sacroiliac joint 1000 in the tissue covering the posterior inferior access region 2016 of the sacroiliac joint articular region 1044. A cannulated probe 1054 can be slidably engaged with the tubular member 1047 (or guide pin 1013) extending outwardly from the sacroiliac joint 1000 (while the sacroiliac joint may be shown in the figures as being substantially linear for illustrative purposes, it is to be understood that the normal irregular features of the sacroiliac joint have not been removed). The cannulated probe 1054 can have a probe body 1054 of generally cylindrical shape terminating in a spatulate tip 1055 at the end advanced into the sacroiliac joint 1000. A removable cannulated probe handle 1056 couples to the opposed end of the probe body 1054. The spatulate tip 1055 can be guided along the tubular needle 1047 or guide wire 1013 into the posterior portion of the sacroiliac joint 1000 and advanced to the anterior portion of the sacroiliac joint 1000 under lateral fluoroscopic visualization. The cannulated probe handle 1056 can then be removed providing the generally cylindrical probe body 1054 extending outwardly from the sacroiliac joint 1000 through the incision 1053 made in the skin.

Alternatively, probe 1054 can be used to guide, advance or place a needle, guide wire or other instrument up to, near, or into the joint.

Additionally, in particular embodiments, probe handle 1056 or the opposed end of the probe body 1054, or both, can be configured to have an interference fit or a luer lock hub to communicate with a syringe barrel 1051 in order to advance contrast, in situ curable biocompatible materials, stem cells, or etc. through the cannulated probe 1054 or cannulated probe handle 1056.

Now referring primarily to FIG. 99D, a passage from the incision 1053 (see FIG. 99C) to the sacroiliac joint 1000 can be generated by inserting a cannula 1057 into the incision. A soft tissue dilator 1058 having a blunt end 1059 can be advanced over the probe body 1054, or a plurality of soft tissue dilators of increasing size, until the blunt end 1059 of the soft tissue dilator 1058 and the corresponding cannula end contact the posterior aspect of the sacroiliac joint 1000. More specifically, as can be understood from FIGS. 96A-98B, in one embodiment, the ends of the dilator 1058 and cannula 1057 contact the joint line 2019 of the sacroiliac joint 1000 at the posterior inferior access region 2016 of the sacroiliac joint articular region 1044. The soft tissue dilator 1058 can be removed from within the cannula 1057. The external surface of the cannula 1057 can be sufficiently engaged with the surrounding tissue to avoid having the tissue locate with in the hollow inside of the cannula 1057. A non-limiting embodiment of the cannula 1057 provides a tubular body having substantially parallel opposed side walls which terminate in a radius at both ends (lozenge shape) into which a plurality of different jigs can be inserted. Alternatively, as a non-limiting example, according to particular embodiments, cannula 1057 and corresponding dilators 1058 and alignment jigs 1060 can be configured to have tubular bodies with an elliptical or circular cross section.

In some embodiments, the cannula 1057 may be additionally configured to have within or near its walls a light source such as, for example, a fiber optic or a LED light source to assist in visualization of the working area. Also, in some embodiments, irrigation and suction tubing may communicate with the inside passage of cannula 1057.

Now referring primarily to FIGS. 100A-100C, a cannula alignment jig 1060 can be advanced over the probe body 1054 (or guide pins 1013) and received within the cannula

1057. Substantially, identical cross hairs **1063**, **1064** can be disposed on the upper jig surface **1065** and the lower jig surface **1066**. Alignment of the cross hairs **1063**, **1064** under x-ray with the sacroiliac joint **1000** can confirm that the cannula **1057** has proper orientation in relation to the paired articular surfaces **1016** of the sacroiliac joint **1000**. The cannula **1057** properly oriented with the paired articular surfaces **1016** can then be disposed in fixed relation to the sacroiliac joint by placement of fasteners through the cannula **1057** into the sacrum **1004** or the ilium **1005**.

Now referring to FIGS. **101A** and **101B**, a first drill jig **1067** can be advanced over the probe body **1054** (or guide pins **1013**) and received within the cannula **1057**. The probe body **1054** (or guide pins **1013**) extending outwardly from the sacroiliac joint **1000** passes through a drill guide hole **1068** of the first drill jig **1067** (or a plurality of guide pins **1013** can extend through a corresponding plurality of guide pin holes **1069**). The drill guide hole **1068** can take the form of a circular hole as shown in the Figures, a slot, or other configuration to restrict the movement of the drill bit **1062** (see FIG. **99E**) within the drill jig **1060** and provide a guide for a drill bit **1062** in relation to the sacroiliac joint **1000**. Guide pin holes **1069** can receive guide pins which can be positioned between the articular surfaces **1016** of the sacroiliac joint **1000** to demarcate the zone of desired treatment or safe working zones while using, for example, lateral fluoroscopy. As a non-limiting example, a first guide pin **1013** can be advanced through a first guide pin hole **1069**, or alternatively a guide pin **1013** is first inserted into the sacroiliac joint **1000** and subsequently a guide jig **1067** is advanced over the guide pin **1013**, the first guide pin **1013** can enter near inferior end **2022** of the posterior inferior access region **2016** of the sacroiliac joint articular region **1044** via the sacroiliac joint line **2019** to border a portion of the greater sciatic notch **2008** thereby allowing a medical person, computer guided surgical system, or other observer to more easily highlight under x-ray a border which should not be crossed during the procedure due to the presence of nerve and other structures. Additionally, as a non-limiting example, first guide pin **1013** can be configured as an electrode, insulated from the operator and the patient's soft tissues, and may be connected to a monitor to signal to an operator or surgeon when implant **25**, configured with a stimulating electrode (NM), as discussed below, comes into contact with first guide pin. Similarly, a second guide pin **1013** can be placed in another guide pin hole **1069** to demarcate a second limit to a desired zone of treatment, or safe working zone. For example, a second guide pin **1013** can enter near the superior end **2018** of the posterior inferior access region **2016** of the sacroiliac joint articular region **1044** via the sacroiliac joint line **2019** to be positioned to border an area of the sacroiliac joint **1000** such as a transition zone between the extra-articular **3007** (see FIG. **106B**) and the interarticular region **1044** which, for example, has been highlighted by contrast material as above described.

Now referring to FIG. **99E**, a cannulated drill bit **1070** can be advanced over the probe body **1054** and within a drill guide hole **1068** (see FIGS. **101A** and **101B**) of the first drill jig **1067**. The cannulated drill bit **1070** under fluoroscopic guidance can be advanced into the interarticular region **1044** between the articulating surfaces **1016** of the sacroiliac joint **1000** to produce a first bore **1071** (shown in broken line) to a determined depth. As to certain embodiments of the method, an amount of articular cartilage or other tissues from between the articular surfaces **1016** of the sacroiliac joint **1000** can be removed sufficient to allow embodiments of the sacroiliac joint implant **25** to be implanted in replace-

ment of the removed articular cartilage or tissue. Because the method removes the degenerative articular cartilage or tissue between the articular surfaces **1016** of the sacroiliac joint **1000**, the articular surfaces **1016** of the sacroiliac joint **1000** can remain intact or substantially intact allowing the sacroiliac joint implant **25** to be non-transversely located between the articular surfaces **1016** of the sacroiliac joint **1000**. Understandably, other instruments can be utilized separately or in combination with a cannulated drill bit **1062** for the removal of articular cartilage or tissue between articular surfaces **1016** such as: endoscopy tools, box chisels, side cutting router bits, burs, flexible burs and bits, hole saws, curettes, lasers (such as CO₂, Neodymium/YAG (yttrium-aluminum-garnet), argon, and ruby), electrosurgical equipment employing electromagnetic energy (the cutting electrode can be a fine micro-needle, a lancet, a knife, a wire or band loop, a snare, an energized scalpel, or the like) where the energy transmitted can be either monopolar or bipolar and operate with high frequency currents, for example, in the range of about 300 kHz and about 1000 kHz whether as pure sinusoidal current waveform where the "crest factor" can be constant at about 1.4 for every sinus waveform, and a voltage peak of approximately 300 V to enable a "pure" cutting effect with the smallest possible coagulation effect or as amplitude modulated current waveforms where the crest factor varies between 1.5 and 8, with decreasing crest factors providing less of a coagulation effect. Electrosurgical waveforms may be set to promote two types of tissue effects, namely coagulation (temperature rises within cells, which then dehydrate and shrink) or cut (heating of cellular water occurs so rapidly that cells burst). The proportion of cells coagulated to those cut can be varied, resulting in a "blended" or "mixed" effect. Additionally, a fully rectified current, or a partially rectified current, or a fulguration current where a greater amount or lateral heat is produced can be employed to find the articular surfaces of the joint and aid in advancing a probe or guide wire into a position in between the articulating surfaces. These currents can effectively degrade the cartilage and allow advance into the joint without grossly penetrating much beyond the cartilage.

Now referring to FIG. **99F**, as to certain embodiments of the invention, the first drill jig **1067** can be removed from within the cannula **1057** and a second drill jig **1072** can be advanced over the probe body **1054** and received within the cannula **1057**; however, the invention is not limited to any particular number of drill jigs and as to certain embodiments of the method the first drill jig **1067** can include all the required drill guide hole(s) **1068** (or slots or other configurations of the drill guide) and as to other embodiments of the method a plurality of drill jigs can be utilized in serial order to provide all the drill guide holes **1068**. As to the particular embodiment of the invention shown by the Figures, the first drill jig **1067** can provide one or more additional drill guide holes **1068** which guide in relation to the first bore **1071a** second or more cannulated drills **1062** of the same or different configuration to be inserted within and advanced into the sacroiliac joint **1000** to produce a second bore **1073** (generally shown in broken line as **1071/1073**) or a plurality of bores within the sacroiliac joint **1000** spaced apart in predetermined pattern to allow removal of sufficient articular cartilage **1016** or other tissue from the interarticular space of sacroiliac joint **1000** for placement of embodiments of the sacroiliac joint implant **25** within the region defined by and between the paired articular surfaces **1016** of the sacroiliac joint **1000**. As to certain methods of the invention, the first drill jig **1067** or the second drill jig **1072** or a plurality of drill jigs can be utilized in serial order to remove

a portion of the sacroiliac joint **1000** for generation of an implant receiving space **1029** (see, for example, FIG. **99H**). As these embodiments of the method, articular cartilage or other tissues and sufficient subchondral bone can be removed from between the articular surfaces **1016** of the sacroiliac joint **1000** sufficient to allow placement of certain 5
embodiments of the sacroiliac joint implant **25** and one or more radial member receiving channels **1074** can be cut into at least one of the articular surfaces **1016** of said sacroiliac joint **1000** sufficient to receive other embodiments of the sacroiliac implant **25**. The one or more radial member receiving channels **1074** can be cut a depth into the subchondral, cortical bone or cancellous bone of the sacrum **1004** or ilium **1005**.

Now referring primarily to FIG. **99G**, in a subsequent step, the last in the serial presentation of drill jigs **1067**, **1072** can be removed from within the cannula **1057** and a broach jig **1075** can be advanced over the probe body **1054** to locate within the cannula **1057**. The broach jig **1075** can include a broach guide hole **1076** which receives a first broach end **1077** of a cannulated broach **1078** advanced over the probe body **1054**. The first broach end **1077** can have a configuration which can be advanced into the sacroiliac joint **1000**. As to certain embodiments of the method, the first broach end **1077** can be adapted to remove an amount of articular 15
cartilage and other tissue from between the articular surfaces **1016** within the articular region **1044** of the sacroiliac joint **1000** for non-transverse placement of a sacroiliac joint implant **25** having an elongate body **45**, or having an elongate body **45** and a first radial member **50**, or an elongate body **45** having a first and second radial members **50** between the articular surfaces **1016** of the sacroiliac joint **1000**. As to other embodiments of the method, the cannulated broach **1078** can remove a sufficient portion of the sacroiliac joint **1000** to generate an implant receiving space **1029** to receive embodiments of the sacroiliac joint implant **25** having an elongate body **45**, an elongate body **45** and at least one radial member **50** adapted for non-transverse placement between the articular surfaces **1016** or at least one radial member **55** adapted to extend into the bone of the sacrum **1004** or the ilium **1005**. 20

As a non-limiting example, FIG. **99G** shows a broach **1078** configured to remove a portion of the sacroiliac joint **1000** to produce an implant receiving space **1029** (shown in FIG. **99H**) to receive embodiments of the sacroiliac joint implant **25** having an elongate body **45** to which a first radial member **50** and a second radial member **50** extend along the longitudinal axis CA of the elongate body **45** in substantially opposed relation adapted to locate between the articular surfaces **1016** of the sacroiliac joint **1000** and further having a third radial member **55** and a fourth radial member **55** which extend along the longitudinal axis CA of the elongate body **45** in substantially opposed relation adapted to correspondingly extend correspondingly into the bone of the sacrum **1004** and the ilium **1005**. 25

Now referring primarily to FIGS. **102A-102D**, the implant receiving space **1029** and the sacroiliac joint implant **25** can be configured having related dimension relations such that placement of the sacroiliac joint implant **25** within the implant receiving space **1029** disposes the sacrum **1004** and the ilium **1005** in substantially immobilized relation and substantially avoids alteration of the positional relation of the sacrum **1004** and the ilium **1005** from the normal condition, or avoids driving together or driving apart the sacrum **1004** from the ilium **1005** outside of or substantially 30
outside of the normal positional relation. An intention in selecting configurations of the sacroiliac joint implant **25**

and the implant receiving space **1029** being immobilization of the sacrum **1004** in relation to the ilium **1005** while maintaining the sacroiliac joint **1000** in substantially normal or substantially normal positional relation, or returning the sacroiliac joint **1000** to a substantially normal positional relation to correct a degenerative condition of the sacroiliac joint **1000**. 35

As a non-limiting example, configurations of an implant receiving space **1029** allow embodiments of the sacroiliac joint implant **25** to be placed non-transversely between the caudal portion **1086** of the articular surfaces **1016** of the sacroiliac joint **1000**. While certain embodiments of the sacroiliac joint implant **25** may only provide an elongate body **45** which locates within a correspondingly configured implant receiving space **1029** to engage at least a portion of the bone of the ilium **1005** or sacrum **1004**, the invention is not so limited, and can further include at least a first radial member or a first and a second radial member at least a portion of the external surface of the first radial member **50** engaging a portion of the bone **1073** of the sacrum **1004** and the ilium **1005**. As to those embodiments of the sacroiliac joint implant **25** which have a third radial member **55** and a fourth radial member **55**, the implant receiving space **1029** can further include one or more radial member receiving channels **1074**, which correspondingly allow the third and fourth radial members **55**, **55** to extend into the bone **1073** of the sacrum **1004** or the ilium **1005** (whether subchondral, cortical, cancellous, or the like), or impact of the sacroiliac joint implant **25** into the implant receiving space **1029** without the radial member receiving channels **1074** can forcibly urge the radial members **55**, **55** into the bone **1073** of the sacrum **1004** and the ilium **1005**. An anchor member **30** (such as treaded members) can be inserted through the bore **40** in the implant **25** and into the sacrum **1004** and ilium **1005** to fix the location of the fixation fusion implant **25** within the implant receiving space **1029**. 40

While the preceding discussion is given in the context of the implant **25** being implanted non-transversely in the caudal portion **1086** of the sacroiliac joint **1000**, in other embodiments, the implant **25** may be implanted in other locations within the sacroiliac joint. For example, as disclosed in U.S. patent application Ser. No. 12/998,712, now U.S. Pat. No. 8,979,928, which is incorporated herein by reference, in some embodiments, the implant **25** may be implanted non-transversely in the cranial portion **1087** (see FIG. **102A**) of the sacroiliac joint **1000** by the similar procedures or steps as above described with the incision and generation of the passage to the superior articular portion of the sacroiliac joint **1000**. The implant may also be implanted in the sacroiliac joint in such a manner so as to extend between the cranial and caudal portions, as also disclosed in U.S. patent application Ser. No. 12/998,712, now U.S. Pat. No. 8,979,928. 45

To begin a discussion of employing the delivery tool **20** to implant the implant **25** in the sacroiliac joint **1000** once the implant receiving space **1029** has been created, reference is made to FIGS. **99I**, **103A**, **103B** and **104**. FIG. **103A** is generally the same view as FIG. **97A**, and FIG. **103B** is an enlarged view of the hip region of FIG. **103A**. FIG. **104** is generally the same enlarged view as FIG. **96B**. As shown in FIGS. **99I**, **103A**, **103B** and **104**, once the implant receiving space **1029** has been created as discussed above with respect to FIGS. **99A-99H**, the implant **25** can be supported off of the distal end **120** of the implant arm **110** of the delivery tool **20** and positioned such that the distal end **42** of the implant **25** begins to enter the sacroiliac joint articular region **1044** via the posterior inferior access region 50
55
60
65

2016, which is described in detail above with respect to FIGS. 96A-98B. As can be understood from FIGS. 103A-104, in entering the sacroiliac joint space, the implant 25 is oriented such that its wide planar members 50 are oriented generally parallel to, and aligned with, the sacroiliac joint line 2019 (i.e., the wide planar members 50 are generally located within the joint plane 1030), and the implant's narrow planar members 55 are generally transverse to the joint plane 1030 (see, e.g., FIGS. 102C and 102D). The longitudinal axis LCA₂ of the implant arm 110 of the delivery tool 20 has a generally anterior trajectory that is located within the joint plane 1030. Alternatively, according to particular embodiments, as a non-limiting example, the longitudinal axis LCA₂ of the implant arm 110 of the delivery tool 20 can have a trajectory which can be defined as being generally lateral or, in particular embodiments, generally posterior. In some embodiments, when the implant 25 is being delivered into the joint space, the implant arm 110 can be said to be at least one of generally superior or cephalad the sciatic notch.

FIG. 105 is the same view as FIG. 104, except the implant 25 has now been fully inserted into the prepared space 1029 in the sacroiliac joint 1000. As illustrated in FIGS. 99J and 105, the implant 25 is fully received in the prepared sacroiliac space 1029 such that the wide planar members 50 are oriented generally parallel to, and aligned with, the sacroiliac joint line 2019 (i.e., the wide planar members 50 are generally located within the joint plane 1030), and the implant's narrow planar members 55 are generally transverse to the joint plane 1030 and, in some embodiments, have even entered the bone material forming the sacrum and ilium articular surfaces of the sacroiliac joint (see, e.g., FIGS. 102C and 102D). As can be understood from FIG. 99J, the longitudinal axis of the implant 25 and the longitudinal axis of the implant arm 110 may be coaxially aligned with each other and generally located in the sacroiliac joint plane 1030.

FIG. 106A is the same view as FIG. 104, except the sleeve 100 is now received in the collar 165 of the anchor arm 115. As can be understood from FIGS. 99K and 106A, the distal end of the sleeve 100 may extend through an incision in the patient's soft tissue such that the distal end of the sleeve 100 is positioned generally against the lateral surface of the ilium 1005. The longitudinal axis of the sleeve and collar of the anchor arm can be understood to be generally coaxially aligned with the longitudinal axis of the bore 40 of the implant 25.

FIG. 106B is generally the same view as FIG. 106A, except the ilium 1005 is removed to show the sacroiliac joint space boundary 3000 defined along the sacrum 1004 and outlining the sacroiliac joint articular region 1044, the implant 25 positioned for implantation within the sacroiliac joint articular region 1044. As shown in FIG. 106B, the sacroiliac joint space boundary includes an inferior boundary segment 3002, an anterior boundary segment 3004, a superior boundary segment 3006, and a posterior boundary segment 3008. The inferior boundary segment 3002 is immediately adjacent, and extends along, the sciatic notch 2024.

The inferior boundary segment 3002 and anterior boundary segment 3004 intersect to form an anterior-inferior corner 3010. The anterior boundary segment 3004 and superior boundary segment 3006 intersect to form an anterior-superior corner 3012. The superior boundary segment 3006 and posterior boundary segment 3008 intersect to form a superior-posterior corner 3014. The posterior boundary segment 3008 and posterior inferior access region 2016

intersect to form a superior-posterior corner 3016 of the posterior inferior access region 2016. The inferior boundary segment 3002 and posterior inferior access region 2016 intersect to form an inferior-posterior corner 3018 of the posterior inferior access region 2016.

The inferior boundary segment 3002 extends between corners 3010 and 3018. The anterior boundary segment 3004 extends between corners 3010 and 3012. The superior boundary segment 3006 extends between corners 3012 and 3014 and provides an access into the cranial portion 1087 of the sacroiliac joint. The posterior boundary segment 3008 extends between corners 3014 and 3016. The posterior inferior access region 2016 extends between corners 3016 and 3018 and provides an access into the caudal region 1086 of the sacroiliac joint. The posterior boundary segment 3008 separates articular region 1044 and extra-articular region 3007, which includes the sacral fossa on the sacrum 1004 and the corresponding iliac tuberosity on the ilium 1005 and defined by the extra-articular region boundary 3009.

As shown in FIG. 106B, the implant 25 is inserted via the implant arm 110 of the delivery tool 20 into the caudal region 1086 of the sacroiliac joint articular region 1044. As shown via the implant 25 and implant arm 110 shown in solid lines, in one embodiment, the implant 25 enters the posterior inferior access region 2016, and is further advanced into the caudal region 1086 of the sacroiliac joint articular region 1044, in an orientation such that the implant arm 110 and wide planar members 50 are in the joint plane 1030 (see, for example, FIGS. 99I-99J) and the longitudinally extending edge 3050 of the wide planar member 50 next to the inferior boundary segment 3002 is generally parallel to, and immediately adjacent to, the inferior boundary segment 3002. Thus, the distal end 42 of the implant is heading generally perpendicular to, and towards, the anterior boundary segment 3004.

As shown in FIG. 106B via the implant 25 and implant arm 110 shown in dashed lines, in one embodiment, the implant 25 enters the posterior inferior access region 2016, and is further advanced into the caudal region 1086 of the sacroiliac joint articular region 1044, in an orientation such that the implant arm 110 and wide planar members 50 are in the joint plane 1030 (see, for example, FIGS. 99I-99J) and the longitudinally extending edge 3050 of the wide planar member 50 next to the inferior boundary segment 3002 is somewhere between being generally parallel to the inferior boundary segment 3002 (as illustrated by the solid-lined implant 25 in FIG. 106B) or forming an angle AJ with the inferior boundary segment 3002 of up to approximately 50 degrees. Thus, the distal end 42 of the implant shown in dashed lines can be said to head anywhere from generally perpendicular to, and towards, the anterior boundary segment 3004 to heading generally towards the superior-anterior corner 3012, or points in between.

In one embodiment, the implant 25 may be first directed into the joint space as illustrated by the solid-lined implant 25 in FIG. 106B after which the implant 25 is rotated within the joint space to be positioned somewhere between, and including, angled position depicted by the dashed-lined implant 25. In other embodiments, the implant 25 may be first directed into the joint space as illustrated by the dashed-lined implant 25 in FIG. 106B after which the implant 25 is rotated within the joint space to be positioned somewhere between, and including, the parallel position depicted by the solid-lined implant 25.

FIG. 107A is a posterior-inferior view of the hip region 1002 of the patient 1001, wherein the soft tissue 1003 surrounding the skeletal hip bones is shown in dashed lines.

FIG. 107B is an enlarged view of the implant region of FIG. 107A. As can be understood from FIGS. 99L, 107A and 107B, the anchor member 30 is positioned in the lumen of the sleeve 100. A driving tool 105 (e.g., screw driver) is extended through the lumen of the sleeve 100 so the distal end of the tool 105 is engaged with a proximal end of the anchor member 30 (e.g., screw). As shown in FIG. 99M, the tool 105 is used to drive the anchor member 30 distally through the bone of the ilium 1005 and into the bore 40 of the implant 25 generally transverse to the joint line plane 1030. As a result, as indicated in FIG. 99N, the implant assembly formed of the implant 25 and anchor member 30 is secured at the implantation site such that the implant 25 is located in the prepared space 1029 of the sacroiliac joint space, and the anchor member 30 extends through the bone of the ilium 1005 and into the implant bore 40 generally transverse to the joint space plane 1030. The tool 105 and sleeve 100 can be removed from the anchor arm collar 165, and the incision associated with the sleeve 100 can be closed. Additionally, tool 105 can be a cutting tool 105 (e.g., drill bit, hole punch, or etc.) which can be used in similar steps as above describe to remove bone or other tissues in the path where anchor member 30 is to be placed.

As indicated in FIG. 99O, the distal end of the implant arm is decoupled from the proximal end of the implant 25 and removed. The incision associated with the implant arm can be closed. In some embodiments, the anchor member 30 will only be long enough to span bone of the ilium 1005 and enter the implant bore 40. In other embodiments, as illustrated in FIG. 99P, the anchor member 30 will be sufficiently long to extend through the bone of the ilium, completely through the implant bore 40, and into the bone of the sacrum 1004. As illustrated in FIG. 99Q, in certain embodiments, implant 25 can be configured to have more than one implant bore 40 which can also receive an anchor member 30. The anchor member 30 prevents migration of the implant 25 within the joint space. The anchor member 30 also can draw the ilium and sacrum together about the implant 25, increasing the sturdiness of the fixation of the implant in the joint space. Where the anchor member extends through the implant bore and into the bone of both the sacrum and ilium, the anchor member 30 can be used to drawn the articular surfaces 1016 of the sacroiliac joint 1000 against the external surfaces of the sacroiliac joint implant 25. With the implant implanted in the sacroiliac joint, the body will cause the joint surfaces to fuse together about the implant 25.

As can be understood from FIGS. 108A and 108B, which are, respectively, posterior and posterior-lateral views the implantation area and the implant assembly implanted there, proximal end 43 of the implant 25 can be seen positioned in the posterior inferior access region 2016, the implant being implanted in the caudal area of the sacroiliac joint space. The anchor member 30 can be understood to have been driven into the implant bore 40 transversely to the joint plane 1030 via a route in the ilium 1005 that avoids contact with vascular and neurological structures, thereby avoiding potentially life threatening injury to such structures. The ability to blindly, yet safely, drive the anchor member 30 into the implant bore 40 while the implant 25 is hidden in the joint space is made possible by the cooperating configurations of the implant 25 and the delivery tool 20. Specifically, the longitudinal axis LCA_1 of the anchor arm collar 165 being coaxially aligned with the longitudinal axis BA of the implant bore 40 when the proximal end 43 of the implant 25 is supported off of the implant arm 115 of the delivery tool 20 makes it possible to safely drive the anchor member 30 through the ilium 1005 bone and into the implant bore 40

when the implant is hidden in the joint space on account of being delivered to the joint space via the delivery tool 20.

To begin a detailed discussion of another method of employing the system 10 to fuse the sacroiliac joint, reference is made to FIGS. 111A-111C. FIG. 111A is an inferior-posterior view of the patient's hip skeletal structure similar to the view depicted in FIG. 107A. FIG. 111B is a lateral-superior-posterior view of the patient's hip skeletal structure. FIG. 111C is an inferior-posterior view of the patient's hip skeletal structure taken from a perspective laterally opposite the view depicted in FIG. 111B. The S1 through S4 foramina can be seen at the respective indicators S1, S2, S3 and S4 in FIGS. 111A-111C.

As can be understood from a comparison of FIGS. 111A to 107A, the delivery tool 20 has been reversed such that the anchor collar 165 is oriented so as to deliver the anchor member 30 through the sacrum 1004 first and then into the bore 40 of the implant 25 and optionally further into the ilium 1005. In other words, unlike the method depicted in FIG. 107A, wherein the anchor member 30 is driven lateral to medial through the ilium 1005 first and then into the implant followed by the sacrum 1004 (optional), the method depicted in FIG. 111A shows the anchor member 30 being driven medial to lateral through the sacrum 1004 first and then into the implant followed by the ilium 1005 (optional). As can be understood from a comparison of FIGS. 111A to 107A, the implant 25 of FIG. 111A is located in the sacroiliac joint with its wide radial members 50, narrow radial members 55 and body 45 oriented as explained above with respect to FIGS. 102A-107B, the only difference being the direction the bore 40 is oriented and the way the anchor member 30 penetrates the surrounding bone structures.

In the embodiment of FIG. 111A, the anchor member 30 may be an S2 alar iliac (S2AI) screw. Such a screw may penetrate the sacrum 1004 just lateral the lateral edge of the S1 foramen and, in some instances, generally superiorly-inferiorly even with the superior edge of the S1 foramen so as to mimic an S2 alar iliac pelvic fixation. Alternatively, according to particular embodiments, for example, as shown in FIG. 111A, such a screw may penetrate the sacrum 1004 just lateral the lateral edge of the S2 foramen and, in some instances, generally superiorly-inferiorly even with the superior edge of the S2 foramen.

To begin a detailed discussion of another method of employing the system 10 to fuse the sacroiliac joint, reference is made to FIGS. 112A-112D. FIG. 112A is an inferior-posterior view of the patient's hip skeletal structure similar to the view depicted in FIG. 107A. FIG. 112B is a side view of the patient's hip skeletal structure similar to the view depicted in FIG. 106A. FIG. 112C is a view of the patient's hip skeletal structure similar to the view depicted in FIG. 103A, except from an opposite lateral perspective.

FIG. 112D is a superior view of the patient's hip skeletal structure.

As can be understood from a comparison of FIGS. 112A and 112B to FIGS. 107A and 106A, respectively, in the embodiment depicted in FIGS. 112A-112D, the delivery tool 20 has a trajectory that is generally superior-to-inferior as opposed to posterior-to-anterior. Further, unlike the embodiments described above wherein the implant 25 gains access to the sacroiliac joint space 1044 via the caudal access 2016 to be implanted in the caudal region 1086 of the sacroiliac joint space 1044 (see, for example, FIG. 106B and related figures and discussion), the embodiment of FIGS. 112A-112D gains access to gains access to the sacroiliac joint space 1044 via the cranial access 2017 (e.g., at the superior border 3006 shown in FIG. 106B) to be implanted in the

cranial region **1087** of the sacroiliac joint space **1044** (see, for example, FIG. **112C-112D**).

As indicated in FIGS. **112A-112D**, the delivery tool **20** is oriented such that the anchor collar **165** is positioned so as to deliver the anchor member **30** through the ilium **1005** first and then into the bore **40** of the implant **25** and optionally further into the sacrum **1004**. In other words, the method depicted in FIGS. **112A-112D** shows the anchor member **30** being driven lateral to medial through the ilium **1005** first and then into the implant followed by the sacrum **1004** (optional). Other than being delivered via a different trajectory and access location and being implanted in a different region of the sacroiliac joint, the implant **25** of FIGS. **112C-112D** is located in the sacroiliac joint with its wide radial members **50**, narrow radial members **55** and body **45** oriented as explained above with respect to FIGS. **102A-102D**, the only difference being the implant **25** being accessed via, and implanted in, the cranial region **1087** as opposed to the caudal region **1086**.

To begin a detailed discussion of another method of employing the system **10** to fuse the sacroiliac joint, reference is made to FIGS. **117A-117C**. FIG. **117A** is a lateral-inferior-posterior view of the patient's hip skeletal structure similar to the view depicted in FIG. **111C**. FIG. **117B** is an inferior-posterior view of the patient's hip skeletal structure similar to the view depicted in FIG. **111A**. FIG. **117C** is the same view as FIG. **106B**, except showing the implant **25** being implanted in the extra-articular space **3007**, as opposed to the sacroiliac joint articular region **1044**, and accessing the extra-articular space **3007** via an extra-articular recess access region **6000**. The S1 through S4 foramina can be seen at the respective indicators S1, S2, S3 and S4 in FIGS. **117A-117B**.

As can be understood from a comparison of FIGS. **117A** to **107A**, the delivery tool **20** has been reversed such that the anchor collar **165** is oriented so as to deliver the anchor member **30** through the sacrum **1004** first and then into the bore **40** of the implant **25** and optionally further into the ilium **1005**. In other words, unlike the method depicted in FIG. **107A**, wherein the anchor member **30** is driven lateral to medial through the ilium **1005** first and then into the implant followed by the sacrum **1004** (optional), the method depicted in FIG. **117A** shows the anchor member **30** being driven medial to lateral through the sacrum **1004** first and then into the implant followed by the ilium **1005** (optional). In the embodiment of FIG. **117A**, the anchor member **30** may be a bone screw the same as or similar to an S2 alar iliac (S2AI) screw. Such a screw may penetrate the sacrum **1004** just lateral the lateral edge of the S1 foramen and just superior the superior edge of the S1 foramen. Thus, the anchor element **30** can enter the bone of sacrum near the first sacral foramen (S2AI trajectory) then into or through implant bore **40** and can further enter the bone of the ilium. The implant **25**, as with any of the implantation locations and implants **25** discussed herein can optionally be employed to be configured to serve as an attachment point for structural components of a spinal support system with a spanning element as discussed below with respect to FIGS. **115** and **116** or with a coupling element as discussed below with respect to FIG. **114**.

As can be understood from a comparison of FIGS. **117A** to **107A**, FIGS. **117B** to **111C**, and FIGS. **117C** to **106B**, the implant **25** of FIG. **117C** is located in the extra-articular region **3007** as opposed to the sacroiliac joint articular region **1044**. Further, the implant **25** of FIGS. **117A-C** has entered the extra-articular region **3007** via an extra-articular recess access region **6000**, which, is on the opposite side of

the posterior inferior overhang **2020** of the posterior superior iliac spine **2004** from the caudal portion **1086** of the sacroiliac joint articular region **1014** and posterior inferior access region **2016** leading to the sacroiliac joint articular region **1044** employed to implant the implant **25** in the caudal portion **1086** of the sacroiliac joint articular region **1044**, as discussed above with respect to FIGS. **103A-108B** or FIGS. **111A-111C**.

As can be understood from FIG. **117C**, the implant **25** is oriented in the extra-articular region **3007** with its wide radial members **50** generally coplanar with the plane of the extra-articular region **3007** and the narrow radial members **55** extending into the sacrum and ilium bone defining each side of the extra-articular region **3007**.

As illustrated in FIG. **117C**, in some embodiments, the implant **25** is oriented within the extra-articular region **3007** such that the longitudinal axis of the body **45** is generally perpendicular to the posterior boundary segment **3008** of the boundary **3000** of the sacroiliac joint articular region **1014**. Also, the distal end **42** of the implant **25**, when implanted in the extra-articular region **3007**, points towards the anterior-inferior corner **3010** of the boundary **3000** of the sacroiliac joint articular region **1014**. The distal end **42** of the implant **25** may extend across the posterior boundary segment **3008** of the boundary **3000** of the sacroiliac joint articular region **1014** and into the sacroiliac joint articular region **1014**. Thus, when implanting the implant **25** via the extra-articular recess access region **6000**, the general direction of travel for the implant distal end **42** is towards the anterior-inferior corner **3010**, and the implant **25** can be positioned substantially within the extra-articular region **3007** or, alternatively, the implant **25** can be further advanced to also occupy a portion of the sacroiliac joint articular region **1044**.

As discussed above with respect to FIGS. **117A-117B**, in implanting the implant **25** in the extra-articular region **3007**, the delivery tool **20** is configured to drive the anchor element **30** medial to lateral through the sacrum **1004** into the implant bore **40** and, optionally, further into the ilium **1005**. However, in some embodiments, the delivery tool **20** and implant bore **40** may have as-manufactured configurations that allow the anchor element **30** to be driven lateral to medial through the ilium **1005** into the implant bore **40** and, optionally, further into the sacrum **1004**.

In some embodiments, the system **10** may be provided in the form of a kit **4999**. Such a kit **4999** is shown in FIG. **113**. The kit **4999** may include the system **10** enclosed in a sterile main package **5000**. For example, the delivery tool **20**, the implant **25** and anchor member **30** may be sealed within the sterile main package **5000**. The delivery tool **20** may be any of the tool embodiments disclosed herein and may include all of its components. Also, the implant **25** may be any of the implant embodiments disclosed herein.

As illustrated in FIG. **113**, in some embodiments, the kit **4999** may include multiple sizes of the implant **25** and/or multiple sizes of the anchor member **30**. The multiple implants **25** may be contained in a sterile individual package **5002** within the sterile main package **5000**, and the multiple anchor members **30** may be contained in another sterile individual package **5004** within the sterile main package **5000**. By providing the multiple sizes of implants **25** and anchor members **30**, the implants and anchor members can be used as trials during certain steps of the procedure to determine appropriate implant sizes and to allow a physician, who is presented with the kit **4999** containing the delivery system **20** and multiple sizes of the implant and anchor members, to evaluate particular embodiments of an implant and anchor member as described herein that would

be best suited to a particular patient, application or implant receiving space. The kit 4999 may also or alternatively contain multiple implants 25 with different angles of bore 40 to provide various desirable trajectories for an anchor member 30 and multiple delivery systems 20 with as-manufactured angular relations corresponding to the different angles of the bore. The kit 4999 may also include color coded, numeric or other indicators corresponding between delivery systems 20 and the corresponding implants 25.

In some embodiments, the kit 4999 may include instructions 5006 that lay out the steps of using the system 10. The instructions 5006 may be contained within one of the sterile packages such as, for example, the sterile main package 5000. Alternatively, the instructions 5006 may be adhered or otherwise attached to an exterior surface of one of the sterile packages such as, for example, the sterile main package 5000. Alternatively, the instructions 5006 may be simply provided separately such as, for example, via simply shipped loose with the rest of the kit 4999, emailed, available for download at a manufacturer website, or provided via a manufacture offered training seminar program.

In some embodiments, the kit 4999 may have any one or more of the tool 20, implants 25 and anchor members 30 contained in individual sterile packages that are not held within a sterile main package. Alternatively, the tool 20, implants 25 and anchor members 30 may be contained in a single common package or in any combination of packages and combination of tool, implants and anchor members.

As can be understood from FIG. 114, which is the same transverse cross sectional view of the patient's hip as shown in FIGS. 99A-99Q, once the implant 25 and anchor(s) 30 are secured at the sacroiliac joint 1000 in any of the manners depicted in FIGS. 99O-99Q, the implant 25 can be used as an attachment point for structural components of a spinal support system configured to support across the patient's hip structure and/or to support along the patient's spinal column. To serve as an attachment point for structural components of a spinal support system, a coupling element 2087 is connected to the proximal end 2011 of the sacroiliac joint implant 25. As a non-limiting example, the coupling element 2087 can be disposed in fixed relation to the proximal end 2011 of the sacroiliac joint implant 25 by threaded engagement of a fastener portion 2088; however, the invention is not so limited and the fastener portion 2088 can be connected to the first end 2011 of the sacroiliac joint implant 25 by any method such as welding, spin welding, adhesive, or the like. The coupling element 2087 can further provide a coupling portion 2089 configured to join with a numerous and wide variety of cross sectional geometries of spanning members 2090. As a non-limiting example, the coupling portion 2089 can be configured as cylindrical cup 2091 pivotally coupled to the fastener portion 2088. A spiral thread can be coupled to the internal surface of the cylindrical cup 2091 to rotationally receive a spirally threaded body 2092. The side wall 2093 of the cylindrical cup 2091 can include a pass through element 2094 in which part of a spanning member 2090 can be received. The part of the spanning member 2090 received within the pass through element 2094 can be placed in fixed relation to the cylindrical cup 2091 by rotational engagement of the spirally threaded body 2092.

FIG. 115 is a posterior view of the patient's sacrum 1004 and ilium 1005, wherein structural components of a spinal support system extend medial-lateral across the patient's hip structure and superiorly to support along the patient's spinal column. As shown in FIG. 115, in one embodiment, each of a pair of sacroiliac joints 1000 can receive an embodiment

of the sacroiliac joint implants 25, above-described, each having a coupling element 2087 coupled to the first end 2011. Each of the coupling elements 2087 can receive the opposed ends 2095 of a spanning member 2090. Additionally, the spanning member 2090 in fixed relation to the sacroiliac joint implants 25 can be connected to a plurality of additional spanning members 2096 which can as a non-limiting example be placed in positional relation to the vertebral column 2097 to allow support of additional implants which can be anchored between vertebrae.

FIG. 116 is the same view as FIG. 115, except having a different spanning member structure. As illustrated in FIG. 116, a first coupling element 2087 can be joined to the first end 2011 of an embodiment of a sacroiliac joint implant 25 as above described and the fastener portion 2088 of a second coupling element 2087 can be disposed directly into the bone of the sacrum 1004 or the ilium 1005, or both. The opposed ends 2095 of a spanning element 2090 in the form of a flat plate can provide apertures 2096 through which the fastener portion 2088 of the coupling element 2087 can pass. The corresponding parts of the external surface of the coupling portion 2089 and the spanning member 2090 can be engaged to fix the location of the spanning member 2090 allowing for coupling of the lumbar spine to the stabilized pelvis by a plurality of fixation elements to further increase stability. As an example, fastener 2088 can be a pedicle screw and may be implanted in the S1 pedicle and angled generally anteriorly and generally parallel to the S1 endplate. Additionally, spanning element 2090 can be coupled to an implant 25 similar to FIGS. 41-54, or configured similarly but with the spanning element coupled to one of the planar members (e.g., planar member 50 and with spanning element extending radially away from the longitudinal axis of an implant 25 and at least partially existing in the plane of a sacroiliac joint before contouring to the posterior surface of a sacrum and terminating at an opposed end 2095.)

As can be understood from FIG. 116 and with continuing reference to FIGS. 111A-C and 117A-C, according to particular embodiments, the spanning element 2090 can be configured to receive an S2AI screw positioned and directed in a trajectory as substantially shown in FIGS. 111A-C or 117A-C. As a non-limiting example, an S2AI screw or other elongate fixation body can pass through an aperture 2096, which can be located on an opposed end 2095 of the spanning element 2090 and can be disposed directly into the bone of the sacrum 1004, pass through or engage the bore 40 of an implant 25, and into the bone of the ilium 1005. According to certain embodiments, an engagement between an S2AI screw and the bore 40 can be configured, for example, as having a bore 40 which can have threads or other surface that are generally complementary to those of a fastener 2088. Said complementary surfaces can be configured to provide a virtual cold weld between components to further resist undesirable movement.

As shown in FIGS. 119A-119E, which are, respectively, distal end isometric, side elevation, plan, distal end elevation, and proximal end elevation views of another embodiment of an implant 25, the features of the implant 25 of FIGS. 119A-119E are substantially similar to the features of the implant 25 as described herein, for example with respect to FIGS. 4-17. The main differences between the implant 25 described with respect to FIGS. 119A-119E and the implant 25 described with respect to FIGS. 4-17 are the lack of the cylindrical body 45 and the edges of adjacent intersecting surfaces of the implant 25 of FIGS. 119A-119E are generally rounded or arcuate as opposed to sharp or well-defined

edges, as is the case between adjacent intersecting surfaces of the implant embodiment of FIGS. 4-17. Further, the planar members 50 may taper distally and be relatively thicker as compared to the planar members 55 of the implant embodiment of FIGS. 119A-119E. For example, the taper may extend the entire length of the implant 25 with the thickness of planar member 50 near implant distal end 42 being about 3-5 mm and the thickness of the planar member 50 near the implant proximal end 43 being about 6-7 mm. Finally, the leading or distal edges 57 of the planar members 50 may be one or more tapered surfaces, as shown in FIGS. 119A-119E.

FIGS. 120A-120B are, respectively, distal end isometric and side elevation views of yet another embodiment of the implant 25. As can be understood from FIGS. 120A-120B, the features of the implant 25 are substantially similar to the features of the implant 25 described with respect to FIGS. 119A-119E, a main difference being that the leading or distal edges 57 of the planar members 55 are generally sharp, well-defined angled edges, as opposed to the generally rounded or arcuate edges of the implant embodiment of FIGS. 119A-119E.

In one embodiment, as can be understood from the dashed lines in FIG. 120B, the planar members 50 may be nonlinear between distal end 42b and proximal end 43 such that there is a radius R between implant ends (or between distal end 42b and a point, for example, midway along the longitudinal axis). The radius R may be about 100 mm to about 200 mm with one embodiment being approximately 150 mm. Accordingly, as indicated by the dashed lines in FIG. 120B, planar members 50b may terminate with a distal end 42b. Additionally, but not shown in the figures, planar members 55 may be similarly curved so as to substantially follow along or be aligned with curved planar members 50b. Such a configuration may more anatomically conform to the curvature of a sacroiliac joint while allowing planar members 50b to generally remain within a curved plane of a sacroiliac joint.

As shown in FIGS. 121A-121E, which are, respectively, distal end isometric, side elevation, plan, distal end elevation, proximal end elevation, proximal end isometric, and side elevation views of another embodiment of an implant 25, the planar members 50, 55 may have surface features or texture designed to prevent migration of the implant once implanted in the joint space. For example, the implant 25 may include anti-migration surface features 355, which are waved, undulating, or spiral ridges extending longitudinally along the planar members 50, 55. Alternatively, anti-migration surface features 355 may be configured to extend perpendicular to the longitudinal axis of planar members 50, 55.

It will be appreciated that the features of the implant 25 of FIGS. 121A-121G are substantially as discussed herein, for example, with respect to the implant 25 of FIGS. 62-67, a main difference being the implant 25 is hollow and the surfaces 60 include a plurality of voids 6500, which are generally triangular in shape. The voids 6500 of the implant 25 may be filled with a biological material (e.g., a protein, demineralized bone matrix, or lattice structure containing or substantially comprised of stem cells) via an access opening 6502 leading to the hollow interior of the implant. The biological material is designed to improve growth of bone around the implant 25 and to strengthen the integration of the implant 25 to the bone. The voids 6500 improve integration of the implant 25 to the bone. Further, the leading or distal edges 57 of the planar members 50 and the implant distal end 42 of FIGS. 121A-121G may be relatively thicker as

compared to the implant embodiment of FIGS. 62-67. Additionally, as can be best understood from FIG. 121C, the leading or distal edges 57 of the planar members 50 may differ in length and general shape. For example, as can be understood from FIGS. 121B-121C, a first leading or distal edge 57 may be generally round and arcuate and relatively longer as compared to a second leading or distal edge 57 that is generally flat and relatively shorter. Further, as shown in FIGS. 121D, 121F and 121G, the planar member 50 may include an access opening 6502 leading to the hollow interior of the implant.

With an opening 6502 on one side of the implant and not on the opposite side of the implant, the implant is configured to allow and promote boney growth, or expansion of biological material inserted within, toward, for example, certain areas within the sacroiliac joint and away or not toward certain other areas of the sacroiliac joint when the implant is implanted in the sacroiliac joint. For example, when the implant 25 of FIGS. 121A-121G is inserted into the sacroiliac joint similar to the manner indicated in FIG. 106B, wherein the opening 6502 of the implant 25 is oriented towards the posterior boundary segment 3008, boney growth or the expansion of biological material contained in the implant will extend through the implant opening 6502 in the direction of the posterior boundary segment 3008 and be specifically directed away from inferior boundary 3002, anterior-inferior boundary 3010 and anterior boundary segment 3004 to limit potential bone growth, or seepage of biologically active agents near the neurovascular structures which are present beyond said boundaries.

Additionally, as can be best understood from FIGS. 121A and 121C, and with continuing reference to FIGS. 106B and 117C, as indicated by arrow F in FIGS. 121A and 121C, one of the leading distal edges 57 (e.g., the edge located opposite the side with opening 6502) of the planar member 50 of the implant may be curved and of a substantially greater radius as compared to the distal edge 57 of the opposite planar member 50. Such a curved section (indicated by arrow F) on the distal edge 57 of planar member 50 may be configured to anatomically generally mimic and even substantially conform to an anterior-inferior corner 3010 (see, e.g., FIGS. 117C and 106B) in order to more fully occupy this region of the joint nearest neurological and vascular structures which are present anterior to and inferior to corner 3010.

The curved section (indicated by arrow F) (or according to particular embodiments located anywhere in implant 25) can additionally be configured to include an inlayed radiopaque marker, for example tantalum, to assist the surgeon with navigation while using fluoroscopy. Further, according to particular embodiments, the curved section (arrow F) can be configured to include a stimulating electrode (NM) connected to an internal controllable power source or external controllable power source. For example, the external controllable power sources may be either in the delivery system instrumentation 20 itself or a separate controller unit located in the operating suite and electrically coupled to the implant supported electrode NM via electrical conductors extending through the implant body and the implant arm 110 of the delivery system 20 to electrically couple to the separate controller unit via a cable extending proximally from the delivery system 20 to the separate controller. With the exception of the electrode (NM) itself, the entirety of the rest of the implant surfaces may be electrically insulated so as to prevent current shunting into surrounding tissues or the operator.

In one embodiment, the stimulating electrode (NM) during navigation can have an amperage of about 8 milliam-

peres (mA) or, nearing final placement, an amperage of about 1-4 mA and, in certain cases, up to 5 mA. The electrode (NM) may be attached to or at least partially imbedded in implant 25 (either permanently or retrievable/removable after implantation) (or according to particular embodiments, located within, near or on the anchor 30, probe 1054, on or within a trial, broach, drill or other tools of system 10) to reduce the risk to the patient of iatrogenic damage to the nervous system by using intraoperative neurophysiological monitoring, for example electromyography (EMG), which is able to alert the surgeon or technician reliably and in real-time of implant 25 advancing beyond, for example, inferior boundary segment 3002 or beyond anterior-inferior corner 3010.

As illustrated in FIG. 121H, which is a schematic depiction of a joint implantation system 10 configured for nerve stimulating and sensing, in one embodiment, the system 10 includes a joint implant 25, a delivery tool 20, a nerve stimulating system 10003, a pre-amplifier unit 10004, an amplifier unit 10005, a computer 10006, and an electrical conductor pathway 10001. The joint implant 25 includes an electrode NM and a body 45 including a distal end 42 and a proximal end 43 opposite the distal end. The electrode NM is supported on the implant 25. The delivery tool 20 includes an implant arm 110 with a distal end 35 configured to releasably couple to the proximal end 43 of the body 45 of the joint implant 25. The nerve stimulating system 10003 is configured to stimulate electrode NM in order to sense nerve contact made with the electrode NM or when NM is approaching and near a nerve. The electrical conductor pathway 10001 extends from the electrode NM along the implant 25 and implant arm 110 to the nerve stimulating system 10003. The electrical conductor pathway 10001 places the electrode NM and nerve stimulating system 10003 in electrical communication.

A sensing (or recording) electrode 10011 can be placed in, for example, a quadriceps femoris, tibialis anterior, gastrocnemius, or abductor hallucis muscle and may be coupled to an electrical conductor pathway 10007 that extends to the pre-amplifier 10004. A reference electrode 10010 can also be placed in, for example, a quadriceps femoris, tibialis anterior, gastrocnemius, or abductor hallucis muscle, but in a location between the area subject to stimulation from the stimulating electrode (NM) and the sensing (or recording) electrode 10011; and may be coupled to an electrical conductor pathway 10012 that extends to the nerve stimulating system 10003. An additional needle 10009 can be placed in proximity to the aforementioned needles (i.e., electrodes 10010, 10011) within a muscle (or when the electrode is in the form of a patch it may be applied to the skin of the patient) and may be coupled to an electrical conductor pathway 10008 that extends to the pre-amplifier 10004 and a ground.

The pre-amplifier 10004 may be connected to the amplifier 10005 that itself may be connected to the computer unit 10006. The computer unit 10006 may process or interpret the signal from the amplifier 10005 and display or otherwise alert (e.g., auditory signals with varying amplitude or frequency) or convey to an observer or operator in an operating suite or to a monitoring physician in a remote location (e.g., by employing computer software and processing and networking hardware) the state of the various electrical connections and pathways (e.g., connected versus disconnected) and electrical activity caused by the stimulating electrode NM.

In one embodiment, the proximal end 43 of the implant 25 and the distal end 35 of the implant arm include a coopera-

tively mating electrical connection 10000 that form a segment of the electrical conductor pathway 10001. An example of such a cooperatively mating electrical connection includes a male-female pin contact assembly 10000. The proximal end 80 of the delivery tool 20 and a distal end of an electrical conductor segment of the pathway 10001 between the sensing system 10003 and the proximal end 80 include a cooperatively mating electrical connection 10002 that form a segment of the electrical conductor pathway 10001. The electrical conductor pathway 10001 may be in the form of one or more multi-filar cables, one or more solid core wires, etc. The electrode NM is at or near the distal end 42 of the implant 25 and the rest of the implant (or only an area directly surrounding the electrode NM) has an electrically insulative coating or is formed of an electrically nonconductive material.

As can be understood from FIGS. 121A-121G, in one embodiment, the joint implant 25 includes a longitudinal axis and a bore 40 extending non-parallel to the longitudinal axis. The joint implant 25 also includes a hollow interior and an exterior surface having a plurality of openings 6500 defined therein that extend into the hollow interior. Prior to implantation of the implant into the joint space, the hollow interior can be filled with a biological material via the access opening 6502 that leads into the hollow interior of the implant.

The implant of FIGS. 121A-121G also includes a distal end 42, a proximal end 43, and a body extending between the proximal and distal ends. The bore 40 extends non-parallel to the hollow interior. A first pair of planar members 50 radially extend from the body of the joint implant 25. Depending on the embodiment, the body may be similar to the body 45 depicted in FIGS. 5-15 or the body may simply be an intersecting or intermediate region of the first pair of planar members 50, as can be understood from FIGS. 121A-121G.

As shown in FIGS. 121A-121G, the hollow interior extends within the confines of the first pair of planar members 50. Also, the exterior surface in which the plurality of openings 6500 is defined includes exterior planar surfaces 60 of the first pair of planar members 50. A second pair of planar members 55 radially extend from the body of the joint implant 25 generally perpendicular to the first pair of planar members 50. As can be understood from FIG. 121F, in some embodiments, the hollow interior is limited to within the confines of the first pair of planar members 50 while the second pair of planar members 55 are solid such that the hollow interior does not enter the confines of the second pair of planar members. In other embodiments, the hollow interior is limited to the confines of the second pair of planar members or the hollow interior may extend into the confines of both pairs of planar members. As indicated in FIG. 121E, in one embodiment, the first pair of planar members 50 extend over a wider radial extent than the second pair of planar members 55.

FIG. 122 is a proximal end isometric view of another embodiment of the implant assembly 15. As can be understood from FIG. 122, the features of the implant assembly 15 are substantially the features described herein, for example, with respect to FIG. 3, a main difference being that a distal end 6510 of the anchor element 30 includes an opening 6506 and edges 6508 in the form of serrated teeth or notches with parallel sides inwardly terminating as an arcuate end. The opening 6508 creates a generally "clothes-pin" like shape of the anchor element distal end 6510. In one embodiment, the edges 6508 may be triangular, trapezoidal, rectangular, or another angular cross-sectional elevation and generally

evenly distributed along the surface of the anchor element distal end **6510**. The edges **6508** help drive the implant assembly **15** into the joint and prevent migration of the implant assembly **15** once in place.

In one embodiment, opening **6506** is defined by arms **6507**. The opening **6506** and arms **6507** are configured such that, after passing through a channel created in a first bone and after passing through bore **40** and then subjected to impaction into a second bone, for example that of the ilium, bone of the second bone can be received into opening **6506** to urge the “clothes pin” arms **6507** apart from one another thereby further embedding the edges **6508** into bone for enhanced fixation. Alternatively, in other embodiments, anchor **30** may be configured in part or completely of shape memory biomaterials (e.g., Nitinol or PEEK ALTERA, available from MedShape, Inc. located at 1575 Northside Drive, NW, Suite 440, Atlanta, Ga. 30318 USA), which are capable of changing shape in response to temperature, light and/or mechanical forces. An anchor **30** configured with a shape memory biomaterial can be configured, for example, immediately prior to insertion as substantially shown in FIG. **122** with “clothes-pins” arms **6507** in general parallel relation. Upon final placement in the ilium or other second bone, the “clothes-pins” arms **6507** (in response to temperature, light and/or mechanical force) can separate away from one another and in certain embodiments “curl” outwardly and back toward the proximal end of anchor **30** in order to further resist undesirable movement of implant assembly **15**. Another main difference between the implant assembly embodiment of FIG. **122** and of FIG. **3** is that a washer **6504** is coupled to the anchor element **30**. The washer **6504** and the shape and texture of the anchor member distal end **6510** secure the implant assembly **15** in the sacroiliac joint. The washer can be (pivotably) coupled to the anchor such that when inserted or explanted the washer remains coupled to the anchor and need not be removed separately.

FIGS. **123A-123E** are, respectively, distal end isometric, side elevation, plan, distal end elevation, and proximal end elevation views of yet another embodiment of the implant **25**. As can be understood from FIGS. **123A-123E**, many of the features of the implant **25** are substantially the features of the implant **25** described herein, for example, with respect to FIGS. **119A-119E**, a main difference being that the planar members **50, 55** are generally round or arcuate and the implant distal end **42** is generally rounded. Specifically, the leading or distal edges **57** of the implant embodiment of FIGS. **119A-119E** are not separate features in the embodiment of FIGS. **123A-123E** and instead are generally incorporated in the rounded or arcuate surfaces of the planar members **50, 55**, which intersect at the implant distal tip **42**. Additionally, the implant proximal end **43** is generally flat with round edges, and relatively wider than the implant embodiment of FIGS. **119A-119E**. The planar members **50** may each include a channel **6514** extending longitudinally and opening into the implant proximal end **43** adapted for receiving a distal end of the delivery device as described herein.

Further, another main difference is that the implant **25** shown in FIGS. **123A-123E** includes wings **6516**, which are separated from the planar members **50, 55** by a gap **6512**. In other words, the gap **6512** extends longitudinally between the planar members **55** and the wings **6516** until the implant proximal end **43**. The wings **6516** allow the implant **25** to be driven into the joint region with the wings existing in a plane transverse to the joint plane such that one of the wings **6516** is delivered into the sacrum and the other wing **6516** into the ilium. The wings **6516** may include anti-migration surface

features **355** in the form of notches or ribs extending inwardly in the gaps **6512** that are generally evenly distributed longitudinally along the wings **6516** parallel to the planar members **55** and oriented transversely to the longitudinal axis of the respective wing. The anti-migration surface features **355** and the wings **6516** prevent migration of the implant **25** once placed, as described herein. As can be understood from FIGS. **124E-124H**, the implant of FIGS. **123A-123E** may additionally include a bore **40** extending through the implant **25** to receive an anchor **30** delivered via an anchor arm **115** of the system **10** as described herein. Such a bore **40** may extend through the implant so as to extend in generally the same plane in which the wings **6516** exist.

In some embodiments, for example, the relative location and angles between wings **6516** and planar members **50, 55** can remain substantially the same before and after implantation. Alternatively, in some embodiments, the wings **6516** can be configured to deflect a distance away from planar members **50, 55** upon insertion and contact with bone. In other words, the gaps **6512** may enlarge upon placement and, to facilitate such enlargement of the gaps **6512**, anti-migration features **355**, or distal ends **6516A** of wings **6516**, may be configured with a sloping surface to urge wings **6516** a distance away from planar members **50, 55**. Upon final placement, the deflected wings **6516** urge bone or joint surfaces against the implant **25** in order to enhance bone contact with the implant **25** by compression to enhance bone fusion and to enhance fixation of the bones or bone fragments by potential energy stored in the deflected wings **6516**. Alternatively, according to particular embodiments, the implant **25**, or only the wings **6516**, may be manufactured from a shape memory biomaterial. In such embodiments, the position of the wings **6516** before implantation may be such that their distal ends **6516A** are a further distance from planar members **50, 55** than shown in FIG. **123A-E**. After final placement of the implant in the sacroiliac joint, an angle Φ of the gap **6512** can decrease and the distance between distal ends **6516A** of wings **6516** and planar members **50, 55** can decrease by the shape memory biomaterial biasing or shaping to appear substantially as shown in FIGS. **123A-E**. As a result, the wings **6516** provide compression of the bone in gap **6512** against the surfaces of the implant **25**.

Alternatively, proximal ends **6516B** of wings **6516** can be configured with a hinge between the proximal ends **6516B** and the proximal end **43** of implant **25** to allow wings **6516** to deflect away from planar members **50, 55** upon implantation. Additionally, the proximal ends **6516B** can extend a distance proximally further than the proximal end **43** of implant **25**. Also, an end cap can be secured to the proximal end **43** of implant **25**. Advancing the end cap distally can bias the extended proximal ends **6516B** away from the longitudinal axis of implant **25** by causing rotation of the wings about the hinges. Such rotation causes the portion of the wings **6516** distal said hinges to rotate an opposite complementary angular distance toward the longitudinal axis of the implant **25**, resulting in compression of bone against implant **25** for enhanced fusion and fixation.

Alternatively, proximal ends **6516B** of wings **6516** may be attached to proximal end **43** of implant **25** by slidable interlocking elements. Upon implantation the wings **6516** may be located a maximum distance away from implant **25** as allowed by the slidable interlocking elements and, after final placement of implant **25**, the wings may be drawn toward the implant **25** by various methods. For example, the slidable interlocking elements may be configured with

sloped elements which prevent movement in the direction away from the longitudinal axis of implant **25** yet allow a compressive force, for example from a surgeon employing hemostats on the surfaces of wings **6516** facing opposite implant **25**, to irreversibly draw the wings **6516** toward implant **25**. As a second example, a gear can be located on the proximal end **43** of implant **25**, which when driven by rotational forces, by, for example, a screw driver or hex wrench, can force wings **6516** to draw toward implant **25** while sliding along the slidable interlocking elements.

FIGS. **124A** and **124B1** are isometric views of another embodiment of the delivery tool **20** coupled and decoupled with the implant **25**, respectively. FIG. **124C** is an isometric view of the delivery tool **20** in an exploded state. FIG. **124D** is an enlarged view of the distal end **120** of the implant arm **110** of the delivery tool **20**. As can be understood from a comparison of FIGS. **124A-124D** and FIGS. **86-88**, the delivery tool embodiment of FIGS. **124A-124D** is substantially similar to the delivery tool embodiment of FIGS. **86-88**, a main difference being the distal end **120** of the implant arm **110**, as shown in FIG. **124D** is adapted to engage the channels **6514** of the implant **25** described with respect to FIGS. **123A-123E**. For example, the large planar members, keels, or fins **140** and the small planar members, keels, or fins **145**, as described herein, for example, with respect to FIG. **19**, may match the relative shape and size of the channels **6514** of the implant **25**. Accordingly, the delivery tool embodiment of FIGS. **124A-124D** is adapted to deliver the implant **25** into the joint region with the wings extending in a plane that is generally transverse to the joint plane such that each wing is received into a respective bone (e.g., sacrum or iliac) bordering the joint, as described with respect to FIGS. **123A-123E**.

As can be understood from FIGS. **124E** and **124G**, in some embodiments, the implant has a bore **40** that has a non-circular (e.g., oblong) cross section as taken along a cross section plane that is generally perpendicular to the length of the bore **40** extending through the implant. The delivery tool **20** of FIGS. **124A-D** can be configured to align a non-circular anchor **30** through the non-circular bore **40** of implant **25**. For example, as shown in FIG. **124B2**, a guide sleeve **100** is concentrically contained in a collar **165** of the anchor arm **115**. The sleeve **100** has a guide hole **2444** that has a non-circular (e.g., oblong) transverse cross section that prevents rotational movement of the oblong anchor when distally displaced through the guide hole **2444**. The sleeve **100** may have a groove **2333** extending along a portion of its exterior surface length that mechanically interfaces with a complementary feature defined in the collar, thereby preventing rotation of the sleeve within the collar. Since the non-circular (e.g., oblong) cross sectioned anchor **30** is prevented from rotation within the complementarily shaped guide hole **2444** and the sleeve **100** is prevented from rotation within the collar **165** due to the structural impediment presented by the groove **2333**, the non-circular anchor **30** can be accurately and reliably delivered into the non-circular bore **40** of the implant **25** of FIGS. **124E** and **124G**. The delivery tool **20** can also be configured to be able to deliver a non-circular anchor **30** adjacent implant **25**. Further, another difference between the embodiment of FIGS. **124A-124D** and FIGS. **86-88** is that the anchor arm **115** as shown in FIGS. **124A-124C** is contoured to permit the transverse delivery of the transfixing anchor screw **30** (e.g., see FIG. **3**) through and/or adjacent the implant **25** and across the sacroiliac joint space.

As can be understood from FIGS. **124E-124H**, in one embodiment, a joint implant **25** includes a longitudinal axis,

a body **25**, a distal end **42**, a proximal end **43**, a first wing **6516**, a second wing **6516** and a bore **40** extending non-parallel to the longitudinal axis. The proximal end is opposite the distal end. The first wing is connected to the body near the proximal end and extends distally in an offset manner from a first lateral side of the body. The second wing is connected to the body near the proximal end and extends distally in an offset manner from a second lateral side of the body opposite the first lateral side of the body. The body of the implant tapers extending proximal to distal.

As shown in FIGS. **124E-124H**, the joint implant also includes a first pair of planar members **55** radially extending from the body of the joint implant. The first pair of planar members **55** forms at least a portion of the first and second lateral sides of the body from which the first and second wings **6514** are offset. The implant may also include a second pair of planar members **50** radially extending from the body of the joint implant generally perpendicular to the first pair of planar members **55**. The second pair of planar members may have a thickness greater than a thickness of the first pair of planar members. As already stated, the first and second wings extend distally in an offset manner from the respective first and second lateral sides, thereby defining first and second respective gaps or slots **6512** between the wings and the respective lateral sides. The bore and the first and second wings reside in generally the same plane.

As can be understood from FIG. **125A**, which is an isometric view of another embodiment of the implant **25**, the longitudinally extending body **45** may include helical spiral threads **6524** rather than keels, fins or planar members **50**, **55** that radially extend outwardly away from the body **45**, as described herein. The helical spiral threads **6524** engage with the bone in the joint region to prevent migration of the implant **25**. Additionally, in the embodiment shown in FIG. **125A**, the body **45** is generally cylindrical with anti-migration surface features **355** in the form of ridges or ribs extending longitudinally along the body **45**. Further, in addition to the bore **40**, the body **45** may include anchor member receiving features **6520** and **6522**, which are substantially similar to the bore **40**, to provide a choice of a plurality of locations to transfix the anchor member **30**, as described herein. Additionally, bores **40** can allow bone to grow into the hollow interior of the implant as discussed below. For example, as shown in FIG. **125A**, the body **45** may include three bores, **40**, **6520**, and **6522** positioned relative to one another along the same longitudinal surface of the body **45**. The implant **25** may be delivered into the joint region with an embodiment of the delivery tool **20** that includes three collars supported off of the anchor arm **115** similar to the embodiment of FIG. **110**, except having at least three longitudinally oriented holes similar to holes **165a** and **165b**, which are at pre-set locations corresponding to the bores **40**, **6520**, and **6522**. The rest of the features shown in the implant embodiment of FIG. **125A** may be substantially similar to the features of implant embodiments described herein.

As shown in FIG. **125B**, which is a longitudinal cross section view of the implant **25** of FIG. **125A**, the longitudinal body of implant **25** may be substantially hollow with a distal end **42** configured with an aperture opening to the hollow interior. The hollow interior may be filled with a biological material for promoting bone growth into the hollow interior, as discussed above. Additionally, helical threads **6524** may be "T-shaped" in cross section in order to hold bone to resist a first bone from moving relative to a second bone.

As shown in FIG. 126A, which is an isometric view of another embodiment of the implant assembly 15, the implant 25 of FIG. 126A is substantially the implant 25 of FIG. 125A, a main difference being that the additional bores 6520 and 6522 are not included on the body 45. Further, features of the anchor element 30 are substantially similar to the features of the anchor element 30 described herein, for example, with respect to FIG. 3. However, the anchor element 30 as shown in FIG. 126A includes helical spiral threads 6528 at the anchor element distal end 6529. The helical spiral threads 6528 of the anchor element 30 are rotationally driven and secured into the bone. For example, the anchor element proximal end 6531 may be adapted to engage an Allen wrench, hex key, or other tool with a hexagonal cross section to deliver the anchor element 30 through the bore 40 and into the bone. Additionally, anchor 30, when configured as a screw can be self-tapping.

As illustrated in FIG. 126C, which is a longitudinal cross section of the proximal head of the anchor 30 of FIG. 126A, in one embodiment, the hex key can be cannulated and configured to receive an anchor retainer rod with a threaded end that engages complementary threads 6537 located on the anchor element proximal end 6531 set below the hex key engagement cutout.

As illustrated in FIGS. 126A and 126B, the anchor 30 may have flutes 6533 extending longitudinally down a portion of the shaft configured to engage a setscrew 6534, as discussed below, in order to prevent rotation of anchor 30 within the bore 40. Alternatively, anchor 30 can be configured with spiral flutes. Alternatively, anchor 30, whether configured as a screw with threads or as a nail, may be further configured with flutes which extend circumferentially in order for a setscrew 6534, as discussed below, to engage said flutes and thereby prevent axial movement of anchor 30 within the bore 40.

As shown in FIG. 126B, which is a longitudinal cross section view of the implant assembly 15 of FIG. 126A, the proximal end 43 of the longitudinal body of implant 25 may be configured to receive a setscrew 6534, or pair of setscrews positioned in longitudinal series in the setscrew hole to lock the setscrews in place against each other in the set screw hole. The setscrew 6534 (or the most distal setscrew of a pair of setscrews in longitudinal series) can threadably advance distally in the setscrew hole such that a distal end of the setscrew enters the bore 40 to be received in a groove 6533 and abut against the anchor 30 to resist movement between the anchor 30 and implant 25.

As can be understood from FIGS. 125A-126B, in one embodiment, a joint implant 25 includes a longitudinal axis, a proximal end 43, a distal end 42, a body 45, a bore 40 extending non-parallel to the longitudinal axis, and a helical thread 6524 extending around the body between the proximal and distal ends. The implant body may be substantially cylindrical, and the bore may be a single bore 40 (see FIG. 126A) or multiple bores 40.

As can be understood from FIGS. 127-128A, the implant arm 110 may include a handle at a proximal end of the implant arm, wherein the handle includes an elongated handle member 6532 that has a length perpendicular to a longitudinal axis of the implant arm. A radiopaque elongated member 6534 extends through the elongated handle member parallel to the length of the elongated handle member. The radiopaque elongated member is contained in a non-radiopaque portion of the elongated handle member. As indicated in FIG. 128A, the radiopaque elongated member may be two such members 6534, 6536 spaced apart from each

other in the elongated handle member 6532 and residing in a plane at least parallel with, if not including, a longitudinal axis of the implant arm 110.

As can be understood from FIGS. 126A-126B, the joint implant may also include a setscrew 6534 with a distal end that is configured to enter the first bore 40 to abut against the anchor element 30 so as to limit movement of the anchor element in the first bore. For example, in abutting against the anchor element, the distal end of the setscrew engages a flute 6533 defined in the anchor element.

FIG. 127 is an isometric view of an embodiment of a sleeve 6550 mounted on an implant arm 110 of a delivery device 20 similar to that of FIG. 88, wherein the sleeve facilitates visualization of trans screw trajectory. When delivering the implant 25, the arm assembly 85 is decoupled from the implant arm 110 and the sleeve 6550 is coupled to the implant arm 110. The handle members 6532 may be rotated to cause implant arm 110 to rotate, thereby causing the helical spiral threads 6526 to threadably engage the bone and advancing the implant 25 into the joint region. In one embodiment, the sleeve 6550, which may be formed of a radiotranslucent material such as PEEK or carbon fiber, includes a tantalum inlay 6534 for transcrew trajectory visualization. In other words, the handles 6532 may include a cylindrical member 6534, which is a radiopaque marker to aid in alignment, for example, using fluoroscopy with the x-ray beam aligned generally in parallel relation to the joint. The marker 6534 runs within the handle 6532 parallel to a longitudinal center axis of the handle. Once the implant 25 is implanted in the joint space as desired, the sleeve 6550 can be removed from the implant arm 110 and the arm assembly 85 with its anchor arm 115 can be coupled to the implant arm 110 in order to allow for the guided delivery of the anchor 30 into the bore 40 of the implant 25 as described herein. As can be understood from FIG. 128A, which is an isometric view of another embodiment of the sleeve 6550 of FIG. 127, the features of the sleeve of FIG. 127 are substantially the features of the sleeve embodiment of FIG. 128A, a main difference being that the handle members 6532 of the embodiment of FIG. 128 include another cylindrical member 6536, which may be another radiopaque marker for alignment visualization. Both markers 6534 and 6536 run within the handle 6532 parallel to a longitudinal center axis of the handle.

FIG. 128B is an end view of sleeve 6550 of FIG. 128A showing overlapping radiopaque markers 6534 and 6536, which are configured with terminal circle shaped markers 6555. FIG. 128C is a posterior view of the hip region, wherein the sleeve 6550 is being employed. As can be understood from FIGS. 128A-128C, the configuration of the sleeve 6550 permits the operator (e.g. surgeon, computer controlled navigation system, or surgical robot) to visualize and adjust with rotational force the trajectory, relative to anatomic structures, of an anchor 30 which can pass through a bore 40 or pass adjacent to implant 25 in order to avoid violating neurovascular structures or other implants which may already be present or are anticipated to be implanted in proximity to implant assembly 15.

As can be understood from FIGS. 128A-128C, when the implant 25 is coupled to the implant arm 110, a longitudinal axis of the implant 25, a longitudinal axis of the bore 40, and the longitudinal axes of the radiopaque elongated members 6534, 6536 exist in a common plane. In other words, when the implant 25 is coupled to the implant arm 110, the two radiopaque elongated members 6534, 6536, which are spaced apart from each other in the elongated handle member 6532, reside in a plane at least parallel with, if not

including, a longitudinal axis of the implant arm **110** and/or a longitudinal axis of the bore **40**. As a result, as can be understood from FIGS. **128A-128C**, the radiopaque members can be used to ascertain the location and orientation of the bore when the implant is located within the joint space, thereby helping the physician to understand if the anchor to be delivered to or near the implant will adversely impact neurovascular structures.

Referring to FIG. **128B**, it can be seen that the two radiopaque markers **6534**, **6536** form a single line when viewed along the plane in which both radiopaque markers reside. This single line indicates to the physician the orientation of the bore **40** and a trajectory of an anchor that would be received in the bore **40**. Other radiopaque markers may be located on the handle **6550** to convey other information to the physician. For example, additional radiopaque markers similar to markers **6534**, **6536** may be located parallel to, and offset from, markers **6534**, **6536** so as to convey to the physician a trajectory of an anchor intended to not pass through the bore, but to instead pass adjacent to a side of the implant.

FIGS. **129A-129B** show isometric views of another embodiment of the system **10**, wherein the delivery tool **20** has a header **6539** with a series of collars **165** and associated sleeves **100** having a variety of pre-defined angular alignments to guide one or more transfixing anchor members **30** into place, thereby providing a choice of delivery angles that are complementary to the implant **25**. According to particular embodiments, a sleeve or collar **165** of the header **6539** depicted in FIGS. **129A-129B** may have a longitudinal center axis LCA_1 similar to the longitudinal center axis LCA_1 depicted in FIG. **18**, the a longitudinal center axis LCA_1 being aligned with a trajectory which either passes into or through a bore **40** of the implant **25** or passes near an implant **25** to further locate an anchor **30** into the bone of a sacrum within certain desirable areas to avoid neurovascular elements and to place the anchor within sacral bone with a higher bone density. For example, depending on the trajectory of the implant **25** and the location of the bore **40** when LCA_1 is aligned with said bore versus placing an anchor near an implant and not through a bore, an anchor can terminate generally within the sacral ala, or terminate in the body of the first sacral vertebra while avoiding the first sacral foramina, or terminate in a S2 vertebral body between the first and second sacral foramina, or terminate into the apex of the sacral promontory, or terminate through or within an anterior sacral cortex, or terminate through or near an S1 endplate.

The system **10** includes a delivery tool **20** and an implant **25** for implanting at the sacroiliac joint via the delivery tool **20**, the implant **25** being for fusing the sacroiliac joint. As shown in FIGS. **129A** and **129B**, the delivery tool **20** includes an implant arm **110** and an anchor arm **115**. As described herein, the implant arm **110** is configured to releasably couple to the implant **25**, and the anchor arm **115** is coupled to the implant arm **110** and configured to deliver the anchor element **30** to the bore **40** of the implant **25**. An impactor arm **6546** of the impactor assembly **6550** is removably coupled to handle members **6538** of the arm assembly **85**. Additionally, the impactor arm **6546** is removably coupled to the implant arm **110**. When the impactor assembly **6550** is coupled to the handle members **6538** as shown in FIG. **129B**, impacting an impactor handle **6547** of the impactor assembly **6550** distally causes the implant arm **110**, and the rest of the assembly **10** as whole, to displace distally and deliver the implant **25** into the sacroiliac joint space. The delivery tool **20** further includes a retaining member **6548**

configured to couple the arm assembly **85** to the implant arm **110** and to engage the implant **25**. The other features of the retaining member **6548** may be substantially similar to the retaining member **95** as described above with respect to FIGS. **28-29**. Specifically, the retainer member **6548** extends through the implant arm **110** to mechanically interlock with a bore (e.g., center bore **70**) of the implant **25** as described herein. During delivery of the implant **25**, the arm assembly **85** may be decoupled from the delivery tool **20** for easier delivery of the implant **25** into the joint region. Additionally, the markers **6534** and **6536** can be removable.

As discussed below in greater detail, during the implantation of the implant assembly **15** at the sacroiliac joint, the implant **25** is supported by the implant arm **110** and the arm assembly **85** with its collar header **6539** may be coupled to the implant arm **110** to guide and support one or more anchor elements **30** (not shown). The handle members **6538** may be used to position or guide the implant as it is being distally driven into the sacroiliac joint via impacts delivered to the impactor handle **6547**. In some embodiments, the handle **6538** may be constructed of a radiolucent material and may include radiopaque markers **6534** and **6536** similar to those shown in FIGS. **127** and **128** for positioning the implant in the plane of the joint under fluoroscopy.

As described below, the delivery tool **20** is then used to cause the one or more anchor elements **30** to extend through the ilium, the sacrum and the implant **25** generally transverse to the sacroiliac joint and implant **25**. The delivery tool **20** is then decoupled from the implanted implant assembly **15**, as described herein.

The arm assembly **85** includes the anchor arm **115** with a collar header **6539** extending from the anchor arm. The collar header includes a series of arm members **6540**, **6542**, and **6544** in which a series of collars **165** are defined at different horizontal and vertical angles. The anchor arm **115** is coupled to the implant arm **110** via the handle members **6538**. Depending on the embodiment, the horizontal linear arm member **6540** may include five collars **165e**, **165f**, **165g**, **165h**, and **165i**, each providing different alignment angles, the horizontal linear arm member **6542** may include two collars **165k** and **165j**, each providing different alignment angles. The vertical arcuate arm member **6544** may include one additional collar **165l** plus already mentioned collar **165f**, each providing different alignment angles. It will be appreciated that the collar positions and alignments shown in the embodiment of FIGS. **129A-C** are for illustrative purposes only and that other positions and alignments are contemplated.

In one embodiment, as shown in FIGS. **124A-124C**, the anchor arm **115** is contoured having an arcuate shape. The anchor arm **115** is received in a vertically extending arm member **6544** of the header **6539**. The vertically extending arm member **6544** has an arcuate configuration over its vertical extension that is generally the same as the arcuate configuration of the anchor arm **115** with respect to degree of curvature. Thus, the vertical arcuate arm member **6544** extends from the anchor arm **115** following the same general arcuate path. The arcuate arm member **6544** may be thicker relative to the anchor arm **115** to provide stability during the delivery of the one or more anchor members **30** and sufficient width to accommodate the collars **165f** and **165l** defined therein as shown in FIG. **129C**. The collars **165f** and **165l** are defined in the generally planar surface of the vertical arcuate arm member **6544**.

The collar header **6539** may further include horizontal linear arm members **6540** and **6542**, which extend perpendicularly from the vertical arcuate arm **6544**. Members **6540**

and **6542** may be manufactured in a fixed configuration or removable configuration with fixed attachment points located along collar header **6539**. The horizontal linear arm members **6540** and **6542** have a relative thickness similar to the vertical arcuate arm member **6544** and are generally linear. The horizontal linear arm members **6540** and **6542** include one or more collars **165e-165i** and **165k-165j** defined on a generally planar surface of each of the horizontal linear arm members **6540** and **6542**. The generally planar surfaces of the horizontal linear arm members **6540** and **6542** intersect with the general planar surface of the vertical arcuate arm member **6544** to form a substantially single generally planar surface, as shown best in FIG. **129C**. Accordingly, one or more of the collars **165f** may be positioned on an intersecting surface of the arcuate arm member **6544** and one of the linear arm members **6540** or **6542**.

Each of the collars **165** are configured to receive a sleeve **100** to cause the one or more anchor elements **30** to extend through the ilium, the sacrum and the implant **25** (and/or immediately adjacent to the implant) generally transverse to the sacroiliac joint and implant **25**, as described herein. Some collars **165**, such as collars **165f**, **165i** and **165l**, may be axially aligned with respective bores of the implant **25** when the implant **25** is supported off of the distal end of the implant arm **110** of the tool **20**. As a result, an anchor member **30** may be delivered into each of the bores via the respective anchor collars **165**. Collars **165f**, **165i** and **165l** are each indicated to be directed to the bore **40** by a marker **6543** showing two concentric circles. As discussed below and can be understood from FIG. **129C**, collar **165l** has a zero degree horizontal offset by virtue of being on the vertical arm **6544**, which is in parallel alignment to the plane occupied by the implant arm **110** and anchor arm **115**. However, collar **165l** has a 90 degree vertical offset to the longitudinal axis of the implant arm **110** and the implant **25** mounted thereon such that a sleeve **100** extending through the collar **165l** extends in the plane occupied by the implant arm and anchor arm and further extends perpendicular to the longitudinal axis of the implant arm and implant. Because collar **165l** is aligned with the bore **40**, the anchor delivered to the bore by the sleeve extending through collar **165l** will orient the anchor in the bore in a plane occupied by the implant arm and anchor arm, but perpendicular to the longitudinal axis of the implant. Collar **165l** may include three overlapping bores that provide a 90 degree alignment angle (or slight angular variations greater than or less than 90 degrees), thereby allowing placement of an anchor **30** (or multiple anchors in general parallel relation), for example through a slot or multiple bores **40** in implant **25**, at varied distances between implant ends.

As can be understood from FIG. **129C**, collar **165f** has a zero degree horizontal offset by virtue of being on the vertical arm **6544**, which is in parallel alignment to the plane occupied by the implant arm **110** and anchor arm **115**. However, collar **165f** has a 45 degree vertical offset to the longitudinal axis of the implant arm **110** and the implant **25** mounted thereon such that a sleeve **100** extending through the collar **165f** extends in the plane occupied by the implant arm and anchor arm and further extends at a 45 degree angle to the longitudinal axis of the implant arm and implant. Because collar **165f** is aligned with the bore **40**, the anchor delivered to the bore by the sleeve extending through collar **165f** will orient the anchor in the bore in a plane occupied by the implant arm and anchor arm, but at 45 degrees to the longitudinal axis of the implant.

As can be understood from FIG. **129C**, collar **165i** has a 30 degree horizontal offset by virtue of being on horizontal arm **6540** at a 30 degree location. In other words, a sleeve **100** extending through collar **165i** will approach the implant at an angle that is 30 degrees right of the plane occupied by the implant arm **110** and anchor arm **115**. Further, because horizontal arm **6540** is centered horizontally on collar **165f**, which has a 45 degree vertical offset to the longitudinal axis of the implant arm **110** and the implant **25** mounted thereon, collar **165i** will have a 45 degree vertical offset as described with respect to collar **165f**. Thus, a sleeve **100** extending through collar **165i** extends at a 30 degree horizontal offset angle to the plane occupied by the implant arm and anchor arm and further extends at a 45 degree offset angle to the longitudinal axis of the implant arm and implant. Because collar **165i** is aligned with the bore **40**, the anchor delivered to the bore by the sleeve extending through collar **165i** will orient the anchor in the bore 30 degrees offset from the plane occupied by the implant arm and anchor arm and at 45 degrees to the longitudinal axis of the implant.

The collars **165e**, **165g**, **165h**, **165j** and **165k** may be employed to deliver anchor members **30** into the bone of the ilium and sacrum while not passing through a bore **40** of the implant **25** (i.e., according to particular embodiments, pre-configured to place anchor members **30** immediately adjacent the longitudinal side edges of the implant **25**). Such offset placement collars **165e**, **165g**, **165h**, **165j** and **165k** are each indicated as such by a marker **6547** showing a circle tangent to a rectangle, as illustrated in FIG. **129C**.

As can be understood from FIG. **129C**, collar **165h** has a 30 degree horizontal offset by virtue of being on horizontal arm **6540** at a 30 degree location. In other words, a sleeve **100** extending through collar **165i** will approach the implant at an angle that is 30 degrees right of the plane occupied by the implant arm **110** and anchor arm **115** and, because the adjacent marker **6547** indicates that the anchor **30** will be delivered adjacent to the implant **25** and not through its bore **40**, the anchor will be delivered at the 30 degree angle to the left of the implant. Further, because horizontal arm **6540** is centered horizontally on collar **165f**, which has a 45 degree vertical offset to the longitudinal axis of the implant arm **110** and the implant **25** mounted thereon, collar **165h** will have a 45 degree vertical offset as described with respect to collar **165f**. Thus, a sleeve **100** extending through collar **165h** extends at a 30 degree horizontal offset angle to the plane occupied by the implant arm and anchor arm and further extends at a 45 degree offset angle to the longitudinal axis of the implant arm and implant. Because collar **165h** is not aligned with the bore **40**, the anchor will be adjacent the implant (i.e., not in the bore **40**). Also, the anchor **30** delivered by the sleeve extending through collar **165h** will orient the anchor adjacent the implant 30 degrees offset from the plane occupied by the implant arm and anchor arm and at 45 degrees to the longitudinal axis of the implant.

As can be understood from FIG. **129C**, collar **165j** has a 20 degree horizontal offset by virtue of being on horizontal arm **6542** at a 20 degree location. In other words, a sleeve **100** extending through collar **165j** will approach the implant at an angle that is 20 degrees right of the plane occupied by the implant arm **110** and anchor arm **115** and, because the adjacent marker **6547** indicates that the anchor **30** will be delivered adjacent to the implant **25** and not through its bore **40**, the anchor will be delivered at the 20 degree angle to the left of the implant. Further, because horizontal arm **6542** is centered horizontally at a 70 degree vertical offset to the longitudinal axis of the implant arm **110** and the implant **25** mounted thereon, collar **165j** will have a 70 degree vertical

offset. Thus, a sleeve **100** extending through collar **165j** extends at a 20 degree horizontal offset angle to the plane occupied by the implant arm and anchor arm and further extends at a 70 degree offset angle to the longitudinal axis of the implant arm and implant. Because collar **165j** is not aligned with the bore **40**, the anchor will be adjacent the implant (i.e., not in the bore **40**). Also, the anchor **30** delivered by the sleeve extending through collar **165j** will orient the anchor adjacent the implant 20 degrees offset from the plane occupied by the implant arm and anchor arm and at 70 degrees to the longitudinal axis of the implant.

As can be understood from FIG. **129C**, collar **165e** has a leftward parallel offset by virtue of being on horizontal arm **6540** at a leftward parallel offset location. In other words, a sleeve **100** extending through collar **165e** will approach the implant leftward offset from, and parallel to, the plane occupied by the implant arm **110** and anchor arm **115** and, because the adjacent marker **6547** indicates that the anchor **30** will be delivered adjacent to the implant **25** and not through its bore **40**, the anchor will be delivered at such a parallel arrangement and to the left of the implant. Further, because horizontal arm **6540** is centered horizontally on collar **165f**; which has a 45 degree vertical offset to the longitudinal axis of the implant arm **110** and the implant **25** mounted thereon, collar **165e** will have a 45 degree vertical offset as described with respect to collar **165f**. Thus, a sleeve **100** extending through collar **165e** extends at a leftward parallel offset to the plane occupied by the implant arm and anchor arm and further extends at a 45 degree offset angle to the longitudinal axis of the implant arm and implant. Because collar **165e** is not aligned with the bore **40**, the anchor will be adjacent the implant (i.e., not in the bore **40**). Also, the anchor **30** delivered by the sleeve extending through collar **165h** will orient the anchor adjacent the implant at the leftward parallel offset from the plane occupied by the implant arm and anchor arm and at 45 degrees to the longitudinal axis of the implant.

As can be understood from FIG. **129C**, collar **165k** has a leftward parallel offset by virtue of being on horizontal arm **6542** at a leftward parallel offset location. In other words, a sleeve **100** extending through collar **165k** will approach the implant leftward offset from, and parallel to, the plane occupied by the implant arm **110** and anchor arm **115** and, because the adjacent marker **6547** indicates that the anchor **30** will be delivered adjacent to the implant **25** and not through its bore **40**, the anchor will be delivered at such a parallel arrangement and to the left of the implant. Further, because horizontal arm **6542** is centered horizontally at a 70 degree vertical offset to the longitudinal axis of the implant arm **110** and the implant **25** mounted thereon, collar **165k** will have a 70 degree vertical offset. Thus, a sleeve **100** extending through collar **165k** extends at a leftward parallel offset to the plane occupied by the implant arm and anchor arm and further extends at a 70 degree offset angle to the longitudinal axis of the implant arm and implant. Because collar **165k** is not aligned with the bore **40**, the anchor will be adjacent the implant (i.e., not in the bore **40**). Also, the anchor **30** delivered by the sleeve extending through collar **165j** will orient the anchor adjacent the implant at the leftward parallel offset from the plane occupied by the implant arm and anchor arm and at 70 degrees to the longitudinal axis of the implant.

Because of the multiple collars **165**, the delivery tool **20** may be adjusted to accommodate patients of different sizes and still maintain the angular relationships between the components of system **10** that allows one or more anchor members **30** to be delivered into a bore of the implant **25**

and/or into the bone of the ilium and sacrum immediately adjacent the implant, or around the implant with anchor **30** passing through regions **3007** or **1044**, without any further adjustment to the delivery tool **20**. Because the angular relationships are rigidly maintained between the arms **110**, **115**, the arm members **6540**, **6542**, and **6544**, the collars **165** of the header **6539**, and the implant **25**, the anchoring of the implant **25** in the sacroiliac joint via one or more anchor members **30** may be achieved quickly and safely. In other words, because the delivery tool **20**, via the multi-angle collar options of the header **6539**, provides multiple angular alignments for deploying one or more anchor members **30** and does not need to be adjusted with respect to angular relationships, the surgery is simplified, reduced in duration, and reduces the risk of an anchor member **30** being driven through a nerve, artery or vein. Additionally, collars may be color coded to correspond with particular implants of the same color, which indicates a complementary configuration. Furthermore, sleeves **100** may encounter interference elements within the collars to restrict or reduce axial movement of the sleeve during the course of the procedure (e.g., see discussion above with respect to FIG. **124B2**).

While any one or more of the implant embodiments disclosed herein could be employed with the delivery device discussed with respect to FIGS. **129A-129C**, one version of the implant as now discussed with respect to FIGS. **129D-129L** may be especially advantageous. FIGS. **129D-129K** are various views of the implant **25**, and FIG. **129L** is an enlarged isometric view of the implant **25** of FIGS. **129D-129K** mounted on the extreme distal end of the implant arm **110** of the delivery tool **20** of FIGS. **129A-129C**.

As shown in FIGS. **129D-129K**, the implant **25** includes a distal end **42** and a proximal end **43**. The implant also includes a middle planar member **6579** in which a central bore slot **40** is defined so as to extend through the middle planar member **6579**. The bore slot **40** may be an elongated oval shape that has a longitudinal axis that is parallel with the longitudinal axis of the implant **25**. The elongated shape allows for an anchor **30** to be delivered through the bore slot **40** at a variety of angles via the collars **165f**, **165i**, and **165j** discussed above with respect to FIG. **129C**.

The distal end **42** of the middle planar member **6579** has a truncated shape with chamfered edges transition between the planar sides of the planar member and the blunt planar distal face of the distal end of the middle planar member. A small planar wing **6580** forms a T-shaped perpendicular intersection with a first lateral edge of the middle planar member **6579**, and a large planar wing **6581** forms a T-shaped perpendicular intersection with a second lateral edge of the middle planar member **6579** opposite the first lateral edge of the middle planar member. Accordingly, as can be understood from FIGS. **129J** and **129K**, the implant has an I-shaped cross section as viewed from either the distal or proximal ends, the large wing **6581** having a substantially larger (e.g., nearly double) width than the small wing **6580**. Additionally, as illustrated in FIGS. **129J** and **129K**, the implant **25** may include one or more bore shafts **10020** extending between, and daylighting at, the implant distal end **42** and implant proximal end **43**. Such shafts **10020** are configured to receive or pass over, for example, guide pins placed in the plane of a sacroiliac joint.

As illustrated in FIG. **129D**, like the distal end **42** of the middle planar member **6579**, the distal ends of the wings **6580** and **6581** also have truncated shapes with chamfered edges transitioning between the planar sides of the wings and the blunt planar distal faces of the distal ends of the wings. While the planar surfaces of the small wing **6580** may

be generally smooth, the planar surfaces of the large wing **6581** may have longitudinally extending evenly spaced apart grooves **6582** defined therein. Alternatively, grooves **6582** may extend perpendicular to length of the implant.

As shown in FIG. **129E**, the proximal end **43** of the implant **25** has a groove **6514** that extends from wing to wing across the blunt proximal end **43** of the implant, the groove even extending into the outermost planar surfaces of the wings **6580** and **6581**. As can be understood from FIG. **129L**, when the implant **25** is mounted on the extreme distal end of the implant arm **110**, members **140** similar to those already described herein with respect to FIG. **124D** are received in the groove **6514**, and the central cylindrical member **220** of the retaining member **95** is received in the proximal opening **70** to retain the implant securely on the distal end of the implant arm **110**.

As indicated in FIGS. **129E** and **129L**, the implant **25** may have similar alignment marks **6583** that help a user to properly mount the implant on the implant arm distal end in a correct orientation relative to each other.

While all the various embodiments of the implant arm **110** discussed above are illustrated in their associated figures as having an arrangement that results in the implant **25** being supported off of the distal end **120** of the implant arm **110** such that the longitudinal axis of the implant arm is essentially axially aligned with the longitudinal axis of the implant arm, in other embodiments, as mentioned above, the implant can be supported off of the distal end of the implant arm in other manners. For example, as can be understood from FIG. **129M**, the distal end **120** of the implant arm **110**, which forms a distal end **35** of the overall delivery device **20**, may be oriented so as to support the implant **25** such that the longitudinal axis of the implant is offset from, but substantially parallel to the longitudinal axis of the implant arm **110**. Alternatively, as can be understood from FIG. **129N**, the distal end **120** of the implant arm **110** may be oriented so as to support the implant **25** such that the longitudinal axis of the implant is substantially non-parallel to the longitudinal axis of the implant arm **110**. For example, the longitudinal axis of the implant may form an acute angle (e.g., 45 degree) angle with the longitudinal axis of the implant arm. Alternatively, the implant arm and sleeve can be arcuate. Regardless of whether the longitudinal axis of the implant is axially aligned with, parallel with, or at an acute angle with the longitudinal axis of the implant arm, the overall delivery device with be so configured such that an anchor **30** can be delivered via the implant arm **115** to a bore **40** in the implant **25** and/or a predetermined location immediately adjacent the implant without having to adjust an angular relationship between the implant arm and the anchor arm.

As shown in FIG. **129O**, the implant arm **110** of FIGS. **129M** and **129N** may be formed mainly of a sleeve **110Z** and a retainer rod **110X**. The retainer rod **110X** may be received coaxially within the sleeve **110Z**, as illustrated in FIGS. **129M** and **129N**.

The retainer rod **110X** includes a shaft **10030** that distally terminates in opposed arms **10032**, which in turn terminate in retainer arms or prong arms **140**. As shown in FIG. **129O**, when the rod **110X** is free of the sleeve **110Z**, the opposed arms **10032** are biased apart, resulting in a space-apart distance indicated by arrow **D** that is sufficiently wide to allow the implant **25** to be received between the prong arms **140** at the rod distal end **120**.

As indicated in FIG. **129O**, the sleeve **110Z** includes a distal end **10040**, a proximal end **10042**, slots **10044** that extend into the hollow interior of the shaft of the sleeve **110Z**. The slots **10044** provide opening into the hollow

interior to facilitate sterilization of the sleeve **110Z** via an autoclave. A knurled gripping surface **10046** is defined near the sleeve proximal end **10042** so as to facilitate rotation of the sleeve relative to the rod when the threads **110Y** are being threadably engaged.

As can be understood from a comparison of FIGS. **129M**, **129N** and **129O**, when the sleeve **110Z** is advanced distally over the retainer rod **110X**, complementary threads **110Y** on both the sleeve **110Z** and retainer rod **110X** can be engaged and the sleeve can be rotatably driven distally by said thread engagement. The sleeve **110Z** advancing distally causes prong arms **140** of the retainer rod **110X** to draw toward one another and in turn cause the portion of the retainer rod which couples to the implant **25** to grasp said implant as can be understood from FIGS. **129L**, **131G** and **131H**. The complementary threads when engaged may prevent proximal movement of the sleeve **110Z** relative to the rod **110X** and allow the coupling of implant and retainer rod to continue throughout the course of the procedure. After implantation the sleeve **110Z** may be caused to move proximally along the retainer rod **110X** in order to decouple the aforementioned tool and implant arrangement.

To illustrate the methodology associated with employing the delivery tool **20** of FIGS. **129A-129C** in implanting any of the above-described implants **25** in the sacroiliac joint **1000** of a patient **1001**, reference is made to FIGS. **130A-130I**. Specifically, FIGS. **130A-130B** show anterior views of the hip region with the system of FIGS. **129A-129C**, wherein the ilium is shown and hidden, respectively. FIGS. **130C-130G** show anterior-superior-lateral, posterior, superior, lateral, and inferior views of the hip region with the system of FIGS. **129A-129C**. FIGS. **130H** and **130I** show inferior and posterior-lateral views of a patient, wherein the system of FIGS. **129A-129C** is inserted through the soft tissue of the hip region. As can be understood from FIGS. **130A-130I**, the curvature of the anchor arm **115** and the arm members **6540**, **6542**, and **6544** mirror the shape of the hip region **1002** to simplify surgery and increase reliability of alignment. Also, the implant **25** may be inserted into the sacroiliac joint via the implant arm **110** via the approach discussed in detail with respect to FIGS. **103A-108A**, the main difference being that the multi-collar header **6539** facilitating the delivery of the one or more anchors **30** into or around implant at a variety of locations and angled approaches.

A tool similar to that of FIGS. **129A-129C** can be configured to be employed for the approaches illustrated in FIGS. **111-112**. For example, for an approach similar to FIG. **111**, a tool similar to FIGS. **129A-129C** may be configured without collars **165e**, **165g-165h**, **165j** and **165k**, because these omitted collars if used for a procedure as shown in FIG. **111** could undesirably direct an anchor anterior of the sacrum or ilium and outside a safe and desirable anchor trajectory. Additionally, collar **165i** may be employed to direct an anchor **30** which passes through an ilium and into and terminating in a bore **40** of an implant **25** as to not pass into the bone of the sacrum.

As another example, a tool similar to FIGS. **129A-129C** may be configured, with **6540** and **6542** being mirrored over **6544** as to generally direct an anchor through a bore **40** of an implant **25** with a trajectory that is more anterior to posterior or which directs an anchor generally posterior to an implant **25** when the anchor is being positioned adjacent to an implant **25**.

According to particular embodiments, for example, for an approach similar to FIG. **112**, a tool similar to FIGS. **129A-129C** may be configured without collars **165e**, **165g-**

h, **165j** and **165k**, because these omitted collars if used for a procedure as shown in FIG. **112** could undesirably direct an anchor inferior to the sciatic notch and outside a safe and desirable anchor trajectory. As an example, a collar or series of collars could be configured to align with a bore **40** or aligned to pass an anchor **30** above or superior to an adjacent implant **25** with, for example, collars with a 45-70 degree vertical offset to the longitudinal axis of the implant arm **110** (and the implant **25** mounted thereon), and 0-45 degree horizontal offset (with 0 degrees being parallel alignment to the plane occupied by the implant arm **110** and anchor arm **115**).

As can be understood from FIGS. **131A-131B**, which show isometric views of another embodiment of the system **10**, the delivery tool **20** of FIGS. **131A-131B** is substantially the delivery tool of FIGS. **129A-129C**, a main difference being that the collar header **6539** does not include the second horizontal linear arm member **6542** extending from the vertical arcuate arm member **6544** and that the arm members **6540** and **6544** include fewer collars **165**, as described below with respect to FIG. **131C**. Specifically, the first horizontal linear arm member **6540** and the vertical arm **6544** of the embodiment of FIGS. **131A-131C** include the same collar locations, angular arrangements and markers as is the case of the arms **6540** and **6544** of the embodiment of FIGS. **129A-129C**. FIGS. **131A-131C** show the impactor assembly **6550** decoupled from the implant arm **110** and the handle members **6538**. However it will be understood that the impactor assembly **6550** may be coupled to the implant arm **110** and the handle members **6538**, as described with respect to FIGS. **129A-129C**.

For a detailed discussion of the angular alignments of the collars **165**, reference is made to FIG. **131C**, which shows an enlarged view of the arm assembly **85** with the collar header **6539**. As discussed with respect to FIG. **129C**, the horizontal linear arm member **6540** intersects with the vertical arcuate arm member **6544** such that one or more of the collars **165** may be positioned on both the arcuate arm member **6544** and the linear arm member **6540**. As shown in FIG. **131C**, the arcuate arm member **6544** may include two linearly aligned collars **165p** and **165q** providing different alignment angles that are respectively the same as collars **165f** and **165l** of the embodiment discussed with respect to FIG. **129C**. For example, the collar **165p** may provide a 45 degree alignment angle and the collar **165q** may include three overlapping bores that provide a 90 degree alignment angle. The linear arm member **6540** may include four collars **165p**, **165o**, **165n**, and **165m** that are respectively the same as collars **165f**, **165g**, **165h** and **165i** of the embodiment discussed with respect to FIG. **129C**. For example, the collar **165o** may provide a 15 degree alignment angle and the collars **165n** and **165m** may each provide a 30 degree alignment angle from different locations on the linear arm member **6540**. It will be appreciated that the collar positions and alignments shown in the embodiment of FIGS. **131A-C** are for illustrative purposes only and that other positions and alignments are contemplated.

FIGS. **131D-131E** are isometric view of a version of the implant of FIGS. **129D-121K** adapted for use with the delivery system of FIGS. **131A-131C**. As can be understood from a comparison of implant embodiment shown in FIGS. **131D-131E** to the implant embodiment illustrated in FIGS. **129D-129E**, the main difference between the two versions of the implant is that the elongated single bore slot **40** has changed to two circular bores **40**. Polyethylene bushings may define a portion of the bore holes **40** of FIGS. **131D-131E**.

In one embodiment, the implant **25** and a distal extension **5777** of the distal end of the implant arm **110** can be configured to receive and remove cartilage from the sacroiliac joint. For example, as shown in FIG. **131F**, which is an isometric view of a version of the implant of FIGS. **129D-129K**, the body **45** of the implant **25** is hollow along its longitudinal length and daylights at its proximal end **43** and distal end **42** in the form of proximal opening **5778** and distal opening **5779**. The side walls of the body **45** extending between the large wing **6581** and small wing **6580** may include openings **5780** that extend into the hollow interior of the body **45**. The openings may have a triangular or other shape.

As illustrated in FIG. **1316**, which is an isometric view of the distal extension **5777** of the distal end of the implant arm **110**, the distal extension **5777** is a hollow rectangular box having generally smooth outer wall surfaces. As can be understood from FIG. **131H**, which is an isometric view of the implant arm distal extension **5777** received in the hollow body of the implant **25**, the distal extension **5777** is configured to be received in a mating fashion that substantially matches and fills the hollow body of the implant **25** when the implant is supported off of the distal end of the implant arm **110**. The matching arrangement between the distal extension **5777** and the hollow interior of the body **45** of the implant **25** is readily understandable from FIG. **131I**, which is an isometric longitudinal cross section of the implant arm distal extension and implant supported thereon as taken along section line **131I-131I** of FIG. **131H**. As indicated in FIG. **131I**, the interior wall surfaces of the implant arm distal extension **5777** includes raised teeth-like ridges **5781** that are oriented proximally to prevent cartilage contained in the hollow interior of the extension **5777** from distally exiting the extension **5777**.

In use, the implant **25** is supported on the extension **5777** as depicted in FIGS. **131H** and **131I** and driven into the sacroiliac joint, thereby causing cartilage to be sliced by the leading distal rectangular edges **5782** of the extension **5777** and received in the confines of the hollow interior of the extension **5777**. Once the implant **25** is positioned as desired in the sacroiliac joint and then decoupled from the distal end of the implant arm **110**, the implant arm **110** can be proximally withdrawn, thereby causing the extension **5777** to proximally exit the confines of the hollow interior of the implant body **45**. As the extension **5777** proximally withdraws, the teeth **5781** engage the cartilage located in the confines of the hollow extension **5777**, causing the cartilage to be maintained in the confines of the hollow extension as it is proximally withdrawn from the sacroiliac joint, thereby extracting the cartilage from the sacroiliac joint. The void resulting from the withdrawal of the cartilage, which happens to be the hollow interior of the implant body **45**, can then be filled with a metal or polymer structure to support the walls of the implant body **45** or, alternatively, the void can be filled with a bone growth promoting material to cause bone to infill the body of the implanted implant.

In one embodiment, the hollow extension **5777** is not part of the distal end of the implant arm **110**, but is instead simply an insert **5777** portion of the implant **25**. Thus, the insert **5777** is placed in the implant **25** and both are then supported off of the distal end of the implant arm **110**. The implant and insert **5777** are then driven into the sacroiliac joint. The implant and insert **5777** are then decoupled from the distal end of the implant arm **110** and left in the sacroiliac joint as the implant arm **110** is proximally withdrawn from the patient. The extractor **6583** described below with respect to FIGS. **134A-134E** can then be employed to extract the

cartilage filled insert **5777** from the confines of the implant **25**, which remains behind in the sacroiliac joint.

FIG. **132A** is an isometric view of yet another embodiment of the system **10** for fusing a sacroiliac joint. The system **10** includes an impactor assembly **6550**, an impactor arm **110**, and a retainer **6548**, which is substantially the impactor assembly, impactor arm, and retainer described with respect to FIGS. **129A-129C**. The system **10** further includes an arm assembly **85** having handle members **6528**, which have substantially the same features as the handle members **6538** described with respect to FIGS. **129A-129C**, a main difference being that the handle members **6538** of FIGS. **132A-132B** are generally cylindrical, as opposed to the generally rectangular shape of the handle members **6538** of FIGS. **129A-129C**.

As shown in FIG. **132B**, which is the same view as FIG. **132A**, except the system is exploded to better illustrate its components, the anchor arm **115** is contoured and curves along an arcuate path to provide axial alignment between a collar **165** and a bore or other anchor member receiving features on the implant **25**. The collar **165** is configured to receive a sleeve **100** to cause the one or more anchor elements **30** to extend through the ilium, the sacrum and the implant **25** generally transverse to the sacroiliac joint and implant **25**, as described herein.

The anchor arm **115** is coupled to the implant arm **110** with a locking member **6556**. Specifically, as can be best understood from FIG. **132B**, the anchor arm **115** includes an engaging member **6568** configured to slidably couple with a channel **6566** of the implant arm **110**. The coupling arrangement may be achieved via a dovetail arrangement of the channel and pins received in holes of the coupling arrangement. Once the anchor arm **115** is coupled to the implant arm **110**, a distal end **6572** of the locking member **6556** is introduced through an opening **6570** to secure the anchor arm **115** to the implant arm **110**. To engage the implant **25**, the retaining member **6548** is introduced through an opening **6564** in the implant arm **110** such that a distal end **6562** of the retaining member **6548** may engage the implant **25**, as described herein. Finally, a distal end **6558** of the impactor assembly **6550** may be introduced into an opening **6560** on the implant arm **110** to couple the impactor assembly **6550** to the implant arm **110** such that displacing the impactor assembly **6550** causes the implant arm **110** to deliver the implant **25** to the joint region, as described herein. The handles **6538** are removable from the rest of the assembly.

For a detailed discussion of yet another of the system **10** for fusing a sacroiliac joint, reference is made to FIGS. **133A-133G**. As can be understood from FIGS. **133A, 133B, and 133E**, an implant assembly includes the implant arm **110**, an elbow **6581**, and a linear implant member **6580**. The implant arm **110** has generally the same features as the implant arm **110** described above and have an implant removably coupled to a distal end of the implant arm via any of the above described configurations, including a retainer member **6548** (see FIG. **132B**) extending through the implant arm. As shown in FIGS. **133A, 133B, and 133E**, the implant arm **110** is coupled to the linear implant member **6580** via the elbow **6581**. Specifically, the linear implant member **6580** and the implant arm **110** intersect at the elbow **6581** such that the implant arm **110** and the linear implant member **6580** are positioned at an angle relative to each other. The elbow **6581** may serve as an impactor area for being impacted by an impactor in driving the implant supported on the end of the implant arm into the joint. The linear implant member **6580** is removably coupled to the arm assembly **85** at the anchor arm **115**. In other words, the

linear implant member **6580** is inserted into or otherwise couple to the anchor arm **115** and secured with the locking member **6556**.

The anchor arm **115** is coupled to a linear arm member **6578**, which is coupled to an arcuate arm member **6576**. In one embodiment, the linear arm member **6578** is generally parallel with the linear implant member **6580** and the arcuate arm member is generally parallel with the anchor arm **115**. The arcuate arm member **6576** is contoured and curves along an arcuate path to provide axial alignment between collars **165** and a bore or other anchor member receiving features on the implant **25**. The collars **165** are each configured to receive a sleeve **100** to cause the one or more anchor elements **30** to extend through the ilium, the sacrum and the implant **25** generally transverse to the sacroiliac joint and implant **25**, as described herein.

As indicated in FIG. **133A** by dimension line R, the arcuate arm member **6576** may have a curvature with a radius of between approximately 120 mm and approximately 180 mm with an arcuate length between the arrow ends of dimension line R of between approximately 200 mm and approximately 400 mm. As shown in FIG. **133B**, the U-shaped linear arm member **6578** of the anchor arm **115** extending from the proximal end of the arcuate arm member **6576** and leading to the proximal end of the implant arm **110** has a distal linear segment with a length L1 of approximately 145 mm, a middle linear segment with a length L2 of between approximately 50 mm and approximately 80 mm, and a proximal linear segment with a length L3 of between approximately 95 mm and approximately 145 mm.

To illustrate the methodology associated with employing the delivery tool **20** of FIGS. **133A, 133B, and 133E** in implanting any of the above-described implants **25** in the sacroiliac joint **1000** of a patient **1001**, reference is made to FIGS. **133C, 133D, 133F and 133G**. Specifically, FIGS. **133C and 133F** show the same tool orientations as FIGS. **133B and 133E**, respectively, except the system **10** is inserted through the soft tissue **1003** of the hip region **1002** of the patient **1001**. FIG. **133D** is the same view as FIG. **133C**, except the soft tissue is hidden to show the patient bone structure. FIG. **133G** is the same view as FIG. **133F**, except the soft tissue is hidden to show the patient bone structure.

As can be understood from FIGS. **133C and 133F**, the curvature and relative positions of the features of the implant assembly and the arm assembly mirror the shape of the hip region **1002** to simplify surgery and increase reliability of alignment. Further, the system **10** is relatively compact such that it does not hinder movement during an operation. Also, the implant **25** may be inserted into the sacroiliac joint via the implant arm **110** via the approach discussed in detail with respect to FIGS. **103A-108A**, the main difference being that the arcuate arm member **6576** is contoured and curves along an arcuate path to provide axial alignment between multiple collars **165** and a bore or other anchor member receiving features on the implant **25**.

The embodiment of FIGS. **133A-133G** can be used for other surgical approaches such as, for example, the approaches illustrated in FIGS. **111A-112C**. For example, for the approach shown in FIGS. **111A-111C**, it may be preferred to employ the 45 degree collar of the anchor arm **115**, while for the approach depicted FIGS. **112A-112D**, it may be preferred to employ the 90 degree collar of the anchor arm **115** (i.e., the sleeve **100** that is generally perpendicular to the longitudinal axis of the implant arm **110** and the implant **25** supported off of the implant arm.

The embodiment depicted in FIGS. 133A-133G offers a number of advantages. First, this embodiment provides more grasping area for the medical professional employing the device and allows for the hand and other body parts of the medical professional to be further from the x-ray beam of the fluoroscope. Also, the embodiment provides for increased visualization of the surgical site by the medical professional. Portions of the device, for example, 6578 are out of the area being x-rayed for fluoro visualization, increasing the visualization possible via fluoroscopy. Finally, clamps can be employed on the device that can be used to secure the device to a surgical table out of the way of the x-ray beam or the imaging equipment.

For a detailed discussion of an embodiment of a system 6583 for extracting an implant, reference is made to FIGS. 134A-134E. As can be understood from FIG. 134A, the system 6583 includes a handle 90 and an implant retainer 95, which have features substantially similar to the handle 90 and implant retainer 95 described herein, for example, with respect to FIG. 3. Further, the system 6583 includes a distal end 6584 having a hook 6586, which is adapted to engage with an engaging portion 6588 of the implant 25.

In one embodiment, as can be understood from FIGS. 129A-129C (and in a similar fashion from FIGS. 131A-131C, and 133A, 133B and 133E for other embodiments), a sacroiliac joint fusion system 10 includes a joint implant 25, an anchor element 30 and a delivery tool 20. The joint implant includes a distal end 42 and a proximal end 43 opposite the distal end. The anchor element comprising a distal end and a proximal end. The delivery tool includes an implant arm 110 and an anchor arm 115. The implant arm includes a proximal end and a distal end. The implant arm distal end is configured to releasably couple to the proximal end of the joint implant. The anchor arm includes a proximal end, a distal end, a header 6539 and a member 100. The proximal end of the anchor arm is coupled to the implant arm, and the header is supported on the anchor arm near the distal end of the anchor arm. The header includes at least first and second guide holes (e.g., any two or more of guide holes 165e-165l). The first guide hole (e.g., anyone of guide holes 165e-165l) is configured to orient the member 100 when received in the first guide hole in a first approach aimed at least in the vicinity of the joint implant 25 when the proximal end 43 of the joint implant is releasably coupled to the distal end of the implant arm 110. Similarly, the second guide hole (e.g., any one of guide holes 165e-165l other than the first guide hole) is configured to orient the member when received in the second guide hole in a second approach aimed at least in the vicinity of the joint implant 25 when the proximal end 43 of the joint implant is releasably coupled to the distal end of the implant arm 110. The first and second approaches are different. The member 100 is configured to guide the delivery of the anchor element 30 to at least in the vicinity of the joint implant 25 when the proximal end 43 of the joint implant is releasably coupled to the distal end of the implant arm 110.

Depending on the embodiment, the joint implant 25 includes a body 45 extending between the distal and proximal ends 42, 43 of the joint implant 25 and an anchor hole 40 extends through the body non-parallel to a longitudinal axis of the joint implant. The first approach is aimed so as to cause the member 100 when received in the first guide hole to guide the anchor element 30 into the anchor hole. A longitudinal axis of the implant arm 110 may be substantially at least one of coaxial or parallel with the longitudinal axis of the joint implant 25.

The header 6539 may include a first arm 6544 that generally exists in a plane defined by at least portions of the implant arm 110 and the anchor arm 115. The first and second guide holes 165f, 165l are spaced apart from each other along the first arm and the respective first and second approaches are non-parallel to each other.

The header 6539 may include a first arm 6540 or 6542 that generally exists in a plane generally perpendicular to a plane defined by at least portions of the implant arm 110 and the anchor arm 115. The first and second guide holes (e.g., any two of 165e-165i or 165j-165k, depending on which arm 6540, 6542) are spaced apart from each other along the first arm and the respective first and second approaches are non-parallel to each other.

The header 6539 may include a first arm 6544 and a second arm 6540 or 6542. The first arm generally exists in a first plane defined by at least portions of the implant arm 110 and the anchor arm 115. The second arm generally exists in a second plane generally perpendicular to the first plane. The first guide hole (e.g., any one of 165f or 165l) is located on the first arm and the second guide hole (e.g., any one of 165e-165i or 165j-165k, depending on which arm 6540, 6542) is located on the second arm. In such an embodiment, the first and second approaches are substantially parallel to each other (e.g., where the first and second guide holes are 165f and 165e) or the first and second approaches are non-parallel to each other (e.g., where the first and second guide holes are 165l and 165h).

In one embodiment, as can be understood from FIGS. 129D-129K, the joint implant 25 includes a distal end 42, a proximal end 43, and a body 6579 extending between the distal and proximal ends. An anchor hole 40 extends through the body non-parallel to a longitudinal axis of the joint implant. A first planar member 6581 extends generally perpendicular to a first lateral edge of the body 6579 of the joint implant 25, and a second planar member 6580 extends generally perpendicular to a second lateral edge of the body of the joint implant opposite the first lateral edge. The body 6579 is substantially a planar member. The first planar member 6581 is larger in at least one of length or width than the second planar member 6580.

As can be understood from FIGS. 131F-131I, in one embodiment, the body 45 may be generally hollow and include a hollow open-ended insert 5777 that substantially occupies in a generally mating manner the hollow body. The insert is removable from the body. The insert may include textured interior wall surfaces. The interior wall surfaces define a hollow interior of the insert. The insert may be separate from the distal end of the implant arm 110 or may be an extension of the implant arm.

As will be appreciated from FIGS. 134B-134C, which show enlarged views of the distal end 6584 of the system of FIG. 134A, wherein the distal end 6584 is decoupled and coupled to the implant, respectively, the handle 90 may displace longitudinally to advance the distal end 6584 towards the implant 25. As best shown in FIGS. 1328, 134C and 134D, the hook 6586 may have angular features to form a general "L-shape." As can be understood from FIG. 134D and FIG. 134F, which is an isometric view of the proximal end of the implant of FIGS. 134B-134C, the proximal end 43 of the implant has a central opening 70 which has an elongated section 70A extending radially outward from a centerline of the central opening 70. The elongated section 70A transitions to a side opening 70B that is a transverse radial extension of the central opening that daylight at the surface of a wing portion 50 of the implant 25.

The hook **6586** may engage the implant **25** by entering the opening **70** in the proximal end of the implant **25** such that the hook **6586** passes through the elongated section **70A** and enters the side opening **70B** to engage with an inner surface of the implant **25** in the engaging portion **6588**. After the hook **6586** is coupled to the engaging portion **6588**, the implant **25** may be extracted via repeatedly sliding the handle along the retainer **95** to cause the handle to repeatedly impact the cap **6599** of the retainer **95**.

As can be understood from FIG. **134E**, which is the same view as FIG. **134A**, except the system is exploded to better illustrate its components, the implant retainer **95** and the handle **90** have substantially similar features to the handle **90** and the implant retainer **95** described herein, for example, with respect to FIG. **3**, a main difference being that the shape of the handle **90** is contoured to fit into the palm of a user's hand and the handle is configured to slide along the retainer so as to allow impacting against the cap **6599** to create a proximally directed impacting force that can be used to extract the implant from a sacroiliac joint. The implant retainer **95** is introduced through the handle **90**, as described herein, such that a distal end **6582** of the implant retainer **95** may be coupled with a proximal end **6590** of the distal end **6584**.

In one embodiment, as can be understood from FIGS. **134A-134E**, the extractor **6583** is configured to remove a joint implant **25** including a distal end **42**, a proximal end **43** opposite the distal end, a body extending between the distal and proximal ends, and an opening **70** defined in the proximal end so as to define an inward edge **6591**. The extractor **6583** includes a distal end **6584**, a proximal end **6599**, a shaft **95** extending between the distal and proximal ends of the extractor, and a handle **90** displaceable along the length of the shaft back and forth proximal-distal. The shaft **95** includes a distal abutment **6593** and a proximal abutment **6599** respectively near distal and proximal ends of the shaft. The handle **90** is supported on the shaft **95** between the distal and proximal abutments. The distal end **6584** of the extractor **6583** includes a feature **6586** configured to engage the inward edge **6591** when the feature is received in the opening **70**. The feature may be a hook or L-shaped.

As can be understood from FIGS. **134A-134E**, and with continuing reference to FIG. **126B**, in one embodiment, an anchor **40** can be configured as a cable with an end that is able to be received in side opening **70B** and further configured to allow a setscrew that may be advanced down central opening **70** (and with abutting elements received in **70A**) to abut the cable end so as to anchor the cable end within implant **25**. The other end of the cable can pass through the plane of the sacroiliac joint and communicate with components of a pelvic or spinal fixation system.

For a discussion of an embodiment of the implant **25** that is configured to have a shape that generally mimics and even substantially fills a sacroiliac joint space, reference is made to FIGS. **135A-135C**. As can be understood from a comparison of the side view of the implant **25** as illustrated in FIG. **135C** to the shape of the sacroiliac joint articular region **1044** depicted in FIG. **106B**, the implant has an overall exterior shape that generally mimics the sacroiliac joint articular region **1044**. The anatomic implant **25** can be provided from the manufacturer in the configuration generally as shown in the FIGS. **135A-135C** or assembled or deployed in situ from multiple pieces, as discussed in further detail below. As illustrated in FIGS. **135A-135C**, the implant **25** includes a proximal end **43** for being removably coupled to the extreme distal end of an implant arm of any of the above described delivery devices **20**. The implant proximal

end **43** includes grooves **6514** and holes **75** that interface and couple with members **140** and **150** on the implant arm **110** similar to those described above with respect to FIG. **124D** and FIG. **19**, respectively.

The implant **25** includes a long portion **7100** and a short portion **7101** perpendicularly oriented to the long portion. The long portion transitions smoothly into the short portion via a small radius **7102** and a large radius **7103** opposite the small radius. The large radius and small radius form an elbow region **7104** of the implant. The large radius forms a heal region **7105** of the implant, and opposite the heal region is a blunt toe region **7106** forming a right angle with a base region **7107** that is generally parallel to the proximal end **43**. These regions **7105-7107** form the distal end **42** of the implant **25**.

The implant **25** can be configured similar to previously described implant embodiments wherein the body of the implant is a generally continuous solid surface with one or more bores **40** defined therein. However, as indicated in FIGS. **135A-135C**, the implant **25** may have a skeletonized configuration, wherein there is an outside frame boundary **7110** that extends unbroken and unitary through all of the above-mentioned regions of the implant, thereby forming it outer boundary while the interior of the implant is generally open space across which support members **7112** extend to join the outside frame boundary **7110** at different locations. As a result of its open configuration, one or more anchors **30** may be extended through the implant when implanted in the sacroiliac joint. When implanted via the approach depicted in FIGS. **103A-108B**, it can be understood that the shape of the implant **25** of FIGS. **135A-135C** may at least somewhat resemble the sacroiliac joint space and more fully occupy the joint space than some of the more linearly shaped rectangle and cylindrical implant embodiments described above.

As can be understood from FIGS. **135A-135C**, in one embodiment, a sacroiliac joint fusion implant **25** includes a proximal end **43**, a distal end **42** generally opposite the proximal end, and first and second lateral sides **7117**, **7118** extending between the proximal and distal ends and defining a long portion of the implant **7100** and a short portion **7107** of the implant. The long portion is longer than the short portion and the two portions extend in directions generally perpendicular to each other. The proximal end terminates proximally in a generally blunt end **7119** and the distal end terminates distally in a generally blunt end **7106** facing in a direction generally perpendicular of the direction faced by the generally blunt end of the proximal end. The generally blunt end of the proximal end is configured to releasably couple to an implant delivery system. The region of the implant between the lateral sides is open except for at least one cross member **7112** extending between the lateral sides **7117**, **7118**. An offset distance between the lateral sides is substantially greater than a thickness of the implant. The first lateral side **7118** transitions between the long and short portions **7100**, **7101** via a first curved portion **7103** and the second lateral side **7117** transitions between the long and short portions via a second curved portion **7102** having a radius smaller than the first curved portion. The first and second lateral sides define a shape resembling a shape of an adult human sacroiliac joint as viewed in a direction perpendicular a plane of the sacroiliac joint. For example, the first and second lateral sides define a shape resembling a boot for a human foot.

For a discussion of an embodiment of the implant **25** that is configured to have a shape that generally mimics and even substantially fills a sacroiliac joint space after in situ deploy-

ment of certain components of the implant 25, reference is made to FIGS. 136A-136J. As shown in FIGS. 136A-136B and 136F-136I, in one embodiment, the implant 25 includes a distal or leading end 42, a proximal or trailing end 43, a longitudinally extending body 45, a rectangular void 7540 extending through the body, and keels, fins or planar members 50, 55 that radially extend outwardly away from the body 45. In one embodiment, the radially extending planar members 50, 55 may be grouped into pairs of planar members 50, 55 that are generally coplanar with each other. For example, planar members 50 that are opposite the body 45 from each other generally exist in the same plane. More specifically, as best understood from FIGS. 136F and 136G, the planar faces 60 of a first planar member 50 are generally coplanar with the planar faces 60 of a second planar member 50 opposite the body 45 from the first planar member 50. Likewise, the planar faces 65 of a third planar member 55 are generally coplanar with the planar faces 65 of a fourth planar member 55 opposite the body 45 from the third planar member 55. The body 45 may be a distinct central portion of the implant or may simply be an intersection of the four planar members 50, 55.

As best understood from FIGS. 136F and 136G, one set of planar members 50 (i.e., the large planar members 50) may extend radially a greater distance than the distance extended radially by the other set of planar members 55 (i.e., the small planar members 55). Also, the width of a large planar member 50 from its outer edge to its intersection with the body 45 may be greater than the width of a small planar member 55 from its outer edge to its intersection with the body 45. Also, the thickness of the large planar members 50 may be greater than the thickness of the small planar members 55. Thus, one set of planar members 50 may be both wider and thicker than the other set of planar members 55. In other words, one set of planar members 50 may be larger than the other set of planar members 55.

As can be understood from FIGS. 136A-136D, a toe member 7541 having a square or rectangular boxed shape is supported in the implant body 45 near the distal end 42. The toe member 7541 is moveably supported on rails 7542 relative to the rest of the implant and can be caused to move perpendicularly to the longitudinal axis of the implant 25 from a recessed location in the implant to a position that causes the toe member 7541 to project past the extreme edge face of one of the large planar members 50 such that the implant changes from having a rectangular box-like configuration to a boot or L-shaped configuration.

As can be understood from FIGS. 136E and 136J, the toe member 7541 includes slots 7543 that matingly engage with the rails 7542 such that the slots can slide along the rails. A fluid conduit 7545 extends from the proximal end 43 to a cylinder housing 7546 in which a piston 7547 of the toe member is displaceably received. An O-ring 7548 seals the interface between the cylinder inner wall and the outer circumferential piston surface. A pressurized fluid applied to the piston 7547 via the fluid conduit 7545 causes the toe member 7541 to move out of the rest of the implant so as to project laterally from the rest of the implant as indicated in FIGS. 136C-136D.

As illustrated in FIG. 136J and more clearly in FIGS. 136K and 136L, which are respective enlarged views of the upper and lower cylinder regions of FIG. 136J, a lip 10050 defined in the upper end of the cylinder housing 7546 and a lip 10051 defined in the lower end of the piston 7547 interact to provide an extreme limit to outer movement of the toe member 7541. Thus, the lips act as stops to prevent the toe

member from extending off of the rest of the implant due to over extension of the piston in the cylinder.

While the deployment mechanism depicted in FIGS. 136E and 136J accomplishes the deployment of the toe member 7541 hydraulic or pneumatic lifting mechanism, in other embodiments the deployment mechanism may be via a screw or gear arrangement (e.g., spur, helical, rack, bevel, miter, worm, ratchet or pawl gears). Additionally, locking mechanisms may be employed to prevent backward movement of the toe member after deployment.

As can be understood from FIGS. 136A-136J, in one embodiment, the sacroiliac joint fusion implant 25 includes a proximal end 43, a distal end 42 generally opposite the proximal end, first and second lateral sides 50, 50 extending between the proximal and distal ends, and a member 7541 near the distal end configured to displace from a first position to a second position. As indicated in FIGS. 136A-136B, the first position may be such that the member 7541 is generally recessed within the implant 25 such that a lateral side surface of the member is generally flush with the first lateral side 50. As shown in FIGS. 136C-136D, the second position may be such that the member 7541 extends from the first lateral side 50, the lateral side surface of the member being offset from and generally parallel to the first lateral side. The member 7541 may be displaceably supported on the implant via a rail arrangement 7542, 7543. As indicated in FIGS. 136E and 136J, the implant 25 may be in the form of an actuation mechanism that drives the member from the first position to the second position and is actuatable via an access at the proximal end. For example, the actuation mechanism may include a hydraulic, pneumatic, geared or screwed mechanical arrangement.

For a discussion of an embodiment of the implant 25 that is configured to have a shape that generally mimics and even substantially fills a portion of a sacroiliac joint space, reference is made to FIGS. 137A-137F. As can be understood from a comparison of the top plan view of the implant 25 as illustrated in FIG. 137C to the shape of the sacroiliac joint extra-articular region 3007 depicted in FIG. 106B, the implant has an overall exterior shape that generally mimics the sacroiliac joint extra-articular region 3007. The implant has a generally isosceles triangle shape in the top plan view. The implant 25 includes a generally truncated, flat proximal end 43 from which two tapering lateral sides 8331 extend and converge at the distal end 42, which forms a rounded or arcuate distal point. A void 7540 of a shape generally the same as the outer shape of the implant itself is defined in the body of the implant generally centered in the implant. The top and bottom surfaces 8332 of the implant have a serrated surface with edges oriented proximally so as to prevent proximal self-migration of the implant once implanted in the joint. The serrated edges extend parallel to the truncated, flat proximal end 43. One or more anchors can be extended through the void 7540 or a bone growth material can be located in the void 7540.

FIGS. 138A-138F illustrate another embodiment of the implant 25 that is configured to have a shape that generally mimics and even substantially fills a portion of a sacroiliac joint space. A comparison of the embodiment of FIGS. 138A-138F to the embodiment of FIGS. 137A-137F reveals that the embodiments are substantially similar except the embodiment of FIGS. 138A-138F has a flat, truncated distal end 42 as opposed to an arcuate end, and the void 7540 is generally a circular bore as opposed to a shape that is generally triangular like the exterior boundaries of the implant. As can be understood from FIGS. 138C and 138D,

the bore 7540 does not extend completely perpendicular between the opposed top and bottom faces 7540, but instead has a slight cant or tilt.

As an example, due to idiopathic anatomic (e.g., skeletal or neurovascular) variations of certain patients it may be advantageous to have a custom implant, anchor, alignment tool or targeting arm manufactured for a particular individual. Pre-surgical imaging studies (e.g., CT or MRI) may be performed and post-processing, including 3D rendering, may assist in planning desired anchor trajectories, anchor dimensions or implant dimensions. The result of these studies and their interpretation may provide details specific to the manufacture of particular tools or implants and their implantation.

As can be understood from the foregoing, various embodiments of the delivery tools or system configurations as described herein can be similarly configured to operate with various embodiments of the sacroiliac joint implants disclosed in U.S. Provisional 61/520,956.

In summary and as can be understood from the preceding discussion, the sacroiliac joint fusion systems 10 disclosed herein include a joint implant 25, an anchor element 30 and a delivery tool 20. The joint implant 25 includes a longitudinal axis CA (e.g., see FIG. 10) and a bore 40 extending non-parallel to the longitudinal axis CA. The anchor element 30 is configured to be received in the bore 40.

The delivery tool 20 includes an implant arm 110 and an anchor arm 115. The implant arm 110 is configured to releasably couple to the joint implant 25. The anchor arm 115 is coupled to the implant arm and configured to deliver the anchor element 30 to the bore 40.

The final manufactured configuration of the tool 20 and final manufactured configuration of the joint implant 25 are such that, when the system 10 is assembled such that the implant arm 110 is releasably coupled to the joint implant 25 (e.g., as shown in FIGS. 2A, 21A, 21C, 32, 37 and 109), a delivery arrangement automatically exists such that the anchor arm 115 is correctly oriented to deliver the anchor element 30 to the bore 40. Thus, when the system 10 is shipped from the manufacturer to the medical facility where the sacroiliac joint fusion will take place, the components 20, 25, 30, 40, 110, 115 are each configured such that simply plugging them together such that the tool 20 is fully assembled and the implant 25 is supported off of the distal end of the tool 20 is all that is required to employ the tool 20 to both deliver the implant 25 into the sacroiliac joint 1000 and deliver the anchor element 30 into the bore 40 so as to anchor the implant 25 in the sacroiliac joint. In other words, once the components of the system 10 are coupled together, the cumulative result of the as-manufactured three dimensional configurations of each component of the system 10 is that the system 10 has a delivery arrangement such that the anchor arm 115 is correctly oriented to deliver the anchor element 30 to the bore 40 without having to adjust the as-manufactured three dimensional configurations of any of the components of the system 10. This automatically arrived-at delivery arrangement is even the case wherein the anchor arm 115 being employed is part of a plurality of anchor arms (as discussed with respect to FIG. 21B) or where the anchor arm 115 is pivotally coupled to the implant arm 110 and further equipped with an arcuate slider 105 at a free distal end of the anchor arm, the arcuate radius of the anchor arm 115 at the arcuate slider 105 being such that the radius extends through the bore 40 (as discussed with respect to FIG. 34).

While the implant embodiment of FIGS. 5-17 and many of the other implant embodiments described herein depict

the bore 40 as being defined in the implant body 45 such that the longitudinal axis of the bore 40 and the longitudinal axis of the implant body 45 are coincident, in other embodiments, the bore 40 may be defined elsewhere in the implant 25. For example the bore 40 may be defined in the implant body 45 such that the longitudinal axes of the bore and implant body are offset from each other. As another such example, the bore 40 may even be defined to extend across a wing 50, 55 so as to daylight at opposed planar surfaces 60 of a large wing 50 or the opposed planar surfaces 65 of a small wing 55.

Implementations of the present disclosure involve a system 10 for fusing a sacroiliac joint. The system 10 includes a delivery tool 20 and an implant assembly 15 for delivery to a sacroiliac joint via the delivery tool 20. The implant assembly 15, which includes an implant 25 and one or more side pieces 12/14, is configured to fuse a sacroiliac joint once implanted at the joint. The side pieces 12/14 are integrally supported on the implant 25 and configured to laterally project from sides of the implant. By acting on the side pieces 12/14 or a portion of the implant at a proximal end 43 of the implant 25 (e.g., by rotational or longitudinally displacing forces actuated by a component of the delivery tool 20 or by a separate tool 10088), the side pieces 12/14 may be caused to deploy from the sides of the implant so as to penetrate into bone material defining the joint space in which the implant 25 is implanted. The tool 20 is configured to support the implant 25 from a distal end 35 of the delivery tool 20 for delivery of the implant into the joint space and further configured to facilitate the deployment of the side pieces 12/14 from the sides of the implant. Thus, the system 10 is configured such that the implant 25 can be quickly, accurately and reliably delivered to, and anchored in, a sacroiliac joint.

To begin a detailed discussion of yet other aspects and embodiments of the present invention, reference is made to FIGS. 139-144. FIGS. 139-140 and FIG. 143 are isometric views of the implant assembly 15A. FIG. 141 is an edge side elevation view of the implant assembly 15A. FIG. 142 is a lateral side plan view of the implant assembly 15A. FIG. 144 is a proximal end view of the implant assembly 15A. FIG. 145 is a distal end view of the implant assembly 15A. FIGS. 146-147 are exploded views of the implant assembly 15A to better illustrate its components.

As can be understood from FIGS. 139-155, the system 10A includes a delivery tool 20A and an implant assembly 15A for implanting at the sacroiliac joint via the delivery tool 20A, the implant assembly 15A being for fusing the sacroiliac joint. The implant assembly 15A includes a distal or leading end portion 42A, a proximal or trailing end portion 43A with a longitudinal body 25A extending between the distal and proximal ends. The implant body 25A further includes first and second side pieces or members 12A/14A, each including an opening 50A disposed therein. The parts 6515 of distal end 35A of the delivery tool 20A may interface with longitudinally extending rectangular notches 6514 formed in the body 25A as discussed in the aforementioned related patent applications and in greater detail below. In one embodiment as shown in FIGS. 144 and 145, a sacroiliac joint fusion implant 25A includes a proximal end 43A, a distal end 42A generally opposite the proximal end, and side edge surfaces 7150 extending between the proximal and distal ends. An offset distance between the side edge surfaces 7150 is substantially greater than a thickness of the implant as defined by an offset distance between the planar lateral side surfaces 7060.

As can be understood from FIGS. 146-147, and with continuing reference to FIGS. 139-155, the implant body 25A, includes oppositely disposed first and second side members 12A/14A structured and arranged to expand into and engage the sacroiliac joint following insertion therein and an actuating body 72A. The side pieces 12A/14A are integrally supported on the implant 25A and configured to laterally project from sides of the implant. Side pieces 12A/14A each include a bone facing surface 7260, an implant facing surface 7261, ridges 7061, a guide mechanism for guiding the expandable movement of the side pieces and including guide piece 6606 disposed in the body portion and having, a slope 6607, and pins 6601 (or as indicated in particular in FIG. 151, 6601A-D). Implant 25A may further include slots 6600. The guide piece 6606 may be sized to allow side piece 12A/14A to be housed in implant housing 6608. Slots 6600 may be configured to house pins 6601 to limit the amount of laterally projecting movement of side pieces 12A/14A. The ridges 7061 are structured and arranged to securely engage the sides of the sacroiliac joint when urged into operative engagement therewith by the actuating body 72.

To begin a detailed discussion of an implant assembly 15A in a deployed or expanded state, reference is made to FIGS. 148-154. FIGS. 148-150 are isometric views of the implant assembly 15A in a deployed or expanded state. FIGS. 151-154 are cross section views of the implant assembly 15A in a deployed or expanded state. As can be understood from the figures, body 72A when inserted into implant 25A via bore 70A can cause the side pieces 12A/14A to laterally project from sides of the implant. Body 72A may be fully or partially threaded and may have a leading end which is tapered. Body 72A may be driven by longitudinally acting forces or by rotational forces by a tool 10088 through bore 70A and further driven to hit the slopes or slope surfaces 6607, thereby causing the side pieces 12A/14A to laterally project from sides of the implant.

To begin a detailed discussion of a delivery tool 20A of the system 10A, reference is made to FIG. 155. In one embodiment, a delivery tool 20A for use with the implant embodiments of the FIGS. 139-154 may be configured as illustrated in FIG. 155. Such a tool 20A may have an implant arm 110A formed mainly of a sleeve 110Z and a retainer rod 110X. The retainer rod 110X may be received coaxially within the sleeve 110Z.

The retainer rod 110X includes a shaft 10030 that distally terminates in opposed arms 10032, which in turn terminate in retainer arms or prong arms 6515. As shown in FIG. 155, when the rod 110X is free of the sleeve 110Z, the opposed arms 10032 are biased apart, resulting in a space-apart distance indicated by arrow D that is sufficiently wide to allow the implant 25A to be received between the prong arms 6515 at the rod distal end 120A.

As indicated in FIG. 155, the sleeve 110Z includes a distal end 10040, a proximal end 10042, slots 10044 that extend into the hollow interior of the shaft of the sleeve 110Z. The slots 10044 provide opening into the hollow interior to facilitate sterilization of the sleeve 110Z via an autoclave. A knurled gripping surface 10046 is defined near the sleeve proximal end 10042 so as to facilitate rotation of the sleeve relative to the rod when the threads 110Y are being threadably engaged.

As can be understood from a comparison of FIG. 155, when the sleeve 110Z is advanced coaxially distally over the retainer rod 110X, complementary threads 110Y on both the sleeve 110Z and retainer rod 110X can be engaged and the sleeve can be rotatably driven distally by said thread engage-

ment. The sleeve 110Z advancing coaxially distally causes prong arms 6515 of the retainer rod 110X to draw toward one another and in turn cause the portion of the retainer rod which couples to the implant 25A to grasp the implant. The complementary threads when engaged may prevent proximal movement of the sleeve 110Z relative to the rod 110X and allow the coupling of implant and retainer rod to continue throughout the course of the procedure. While the tool 20A is coupled to the implant 15A, a hex-head 10083 wrench or screwdriver 10088 with a handle 10082 may be extended down a central lumen of the shaft 10030 to engage the hex-head end of the body 72A to drive body 72A a distance towards implant proximal end 42A thereby causing the side pieces 12A/14A to laterally project from sides of the implant. After implantation the sleeve 110Z may be caused to move proximally along the retainer rod 110X in order to decouple the aforementioned tool and implant arrangement.

Referring now to FIGS. 158-164, another embodiment of an implant insertion tool 1000A is shown. Tool 1000A is in the form of a tong apparatus and includes a handle 10004A pivotally connected at a first end 1006A thereof to a multi-segmented elongated arm 1008A/1013A, the segments being pivotally joined at pin 1015A. The elongated arm 1008A/1013A includes a proximal end 1020A and distal end 1021A. A second multi-segmented elongated arm 1010A/1011A is pivotally connected at a midpoint 1012 thereof at approximately the midpoint of arm 1008A/1013A and is operatively engaged at a proximal end 1014A thereof to a ratchet 1016A positioned on handle 1004A. The segments 1010A and 1011A are pivotally connected at pin 1019A. Arm 1010A further includes a distal end 1017A oppositely disposed from distal end 1021 of arm 1008A, as is more clearly illustrated in FIGS. 161 and 162. The arms 1018A and 1010A are structured and arranged to form a tong-type tool adapted for insertion of an implant into a sacroiliac joint as hereinabove described with respect to an alternate embodiment of this invention.

FIGS. 164-170 illustrate yet another embodiment of a sacroiliac implant device 3000A and insertion tool 1000B. With the exception of distal ends 1017B and 1021B, insertion tool 1000B is structured in the same manner as tool 1000A described above. According, similar numerals followed by the letter "B" are shown in the drawings to differentiate between the two embodiments.

As best shown in FIGS. 169 and 170, insert 3000A comprises a body portion 3002A having an elastic generally U-shaped middle portion 3004A and a pair of opposite disposed legs 3006A/3008A having a proximal end 3007A/3009A respectively operatively connected to the U-shaped middle portion and extending therefrom creating a spring-like force extending transversely therefrom. Each leg includes a generally U-shaped opening or channel 3012A/3014A formed in a distal end 3016A/3018A thereof respectively, each channel adapted to receive a respective end 1017B/1021B of tool 1000B for insertion into a joint. Each end 3016A/3018A includes a plurality of outwardly extending wedge or V-shaped projections 3020A structured and arranged to be urged by the spring force of the implant into engagement with the joint interfaces into which it is implanted.

Referring to FIGS. 171-173, yet another embodiment of a sacroiliac joint implant is shown at 4000A. Similar in configuration and operation to the embodiment of FIGS. 169 and 170, the implant device of the instant embodiment has legs 4006A/4008A extending substantially parallel from an elastic U-shaped middle portion 4004A. Outwardly extending wedge or V-shaped projections are structured and

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arranged to be forcibly driven into a joint interface upon insertion by a tool such as tool **1000A** hereinabove described.

Yet another embodiment of an implant device **5000A** is depicted in FIG. **174**. Implant **5000A** includes an expandable body portion **5002A** having a first end configured in the shape of a chisel **5004A** and a second end **5006A** having an aperture **5008A** formed therein and adapted to receive a wedge element **5012A**. After insertion into a sacroiliac or other applicable joint, wedge **5012A** is forced into aperture **5008A**, thereby expanding the body portion of the implant into contact with the joint interfaces. Four orthogonally positioned projections **5012A** are structured and arranged to be forced into engagement with the joint interfaces, thereby securely retaining the implant in its desired location.

Insertion tool **1000A** further includes a pair of oppositely disposed spring elements positioned intermediate a proximate end **1020A** of the first arm **1008A** and a proximate end **1022A** of the second arm **1010A** to urge the proximate ends away from one another, thereby urging the distal ends **1017A** and **1021A** into engagement with an implant **1025A**. The tool further includes a guide member **1026A** adapted to receive expanding member **72A** and tool **10088** for engagement with the expandable implant device for insertion and fixation in a sacroiliac joint. An x-shaped pivotal cross-brace **1028A** pivotally connects at a pair of oppositely disposed ends **1030A** thereof to each of the arms **1008A** and **1010A** and slidably connected at a pair of second ends **1032A** to the arms to reinforce and stabilize the distal end of tool **1000A** during the insertion process.

The foregoing merely illustrates the principles of the invention. Various modifications and alterations to the described embodiments will be apparent to those skilled in the art in view of the teachings herein. It will thus be appreciated that those skilled in the art will be able to devise numerous systems, arrangements and methods which, although not explicitly shown or described herein, embody the principles of the invention and are thus within the spirit and scope of the present invention. From the above description and drawings, it will be understood by those of ordinary skill in the art that the particular embodiments shown and described are for purposes of illustrations only and are not intended to limit the scope of the present invention. References to details of particular embodiments are not intended to limit the scope of the invention.

To begin a detailed discussion of another method of accessing a sacroiliac joint space to treat a musculoskeletal condition, reference is made to FIGS. **175-177**. To begin and as can be understood from FIGS. **175** and **176**, a stab incision is made in the patient's skin to create an entry point near the coccyx **1007** and the sacrotuberous ligament **1008**. A cannulated blunt dissecting tool for deflecting soft tissue away from the sacrum **1004** may be advanced through the entry point **1009** and advanced while following the sacrum up to a sacroiliac joint inferior boundary **3002** which is immediately adjacent, and extends along, the sciatic notch **2024**. A guide wire may then be placed through the cannulation in the dissecting tool and advanced into the sacroiliac joint. Optionally, after the dissecting tool has been removed an inflatable bowel retractor may be advanced over the guide wire and, once in place, inflated to provide a protected passageway **1111** for access to a sacroiliac joint. A working cannula may then be advanced over the guide wire to further protect the soft tissues from subsequent use of tools during the remainder of the procedure. The guide wire may then be removed or alternatively left in place to be used to guide an implant delivery tool up to the sacroiliac joint. Regardless,

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as can be understood from FIG. **177**, any of the tools **20** disclosed herein can be used along the surgical pathway depicted in FIGS. **175** and **176** to deliver corresponding implant assemblies **15** into the sacroiliac joint space.

The invention claimed is:

1. A method for stabilizing a first bone and a second bone of a patient, the method comprising:
 - implanting a first implant into the first bone, the first implant comprising a longitudinally extending first body portion that is at least partially received in the first bone upon implantation and a first coupling portion proximal to the first body portion and configured to couple to a spanning member of a spinal support system;
 - implanting a second implant into the second bone, the second implant comprising a longitudinally extending second body portion that is at least partially received in the second bone upon implantation, and a second coupling portion proximal to the second body portion and configured to couple to the spanning member of the spinal support system, the second body portion of the second implant having a rectilinear cross-section transverse to a longitudinal axis of the second body portion, wherein the second body portion linearly extends along the longitudinal axis; and
 - securing the spanning member to both of the first and second coupling portions.
2. The method of claim **1**, wherein the first bone comprises the sacrum.
3. The method of claim **2**, wherein the second bone comprises the ilium, and wherein the second body portion is at least partially received in the first bone upon implantation of the second implant into the second bone.
4. The method of claim **1**, wherein the spanning member comprises a plate.
5. The method of claim **1**, wherein the second implant comprises first and second planar members coupled to each other, the first and second planar members defining the second body portion.
6. The method of claim **5**, wherein the first and second planar members are coupled together at right angles.
7. The method of claim **1**, wherein the second implant is implanted non-transversely in the sacroiliac joint.
8. The method of claim **1**, wherein the first body portion of the first implant is threaded.
9. The method of claim **8**, wherein the first implant is an S2AI screw.
10. The method of claim **1**, wherein the second body portion of the second implant is non-threaded.
11. The method of claim **1**, wherein a fastener is receivable within the second coupling portion of the second implant, the fastener coupled with a cylindrical cup configured to couple to the spanning member.
12. The method of claim **1**, wherein the spanning member is a first spanning member, and the method further comprises operably coupling the first spanning member to a second spanning member that is coupled to a third implant implanted into a third bone.
13. The method of claim **12**, wherein the third bone is a vertebra.
14. A method for stabilizing a vertebra and a pelvic region comprising a sacrum, an ilium, and a sacroiliac joint of a patient, the method comprising:
 - implanting a first implant into the vertebra, the first implant comprising a first coupling element configured to couple to a rod;

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implanting a second implant into the sacroiliac joint such that a first portion of the second implant is positioned in the sacrum, a second portion of the second implant is positioned in the ilium, and a third portion of the second implant is positioned within the sacroiliac joint, the second implant comprising a distal end, a proximal end, a longitudinal axis extending between the distal and proximal ends, a second implant body extending a length between the distal and proximal ends and having a rectilinear cross-section transverse to the longitudinal axis, and a second coupling element extending from the second implant body for coupling to the rod; and securing the rod to both the first coupling element and the second coupling element.

15. The method of claim 14, wherein the second implant further comprises a first planar member extending the length of the second implant body, and a second planar member extending the length of the second implant body, the first and second planar members coupled to each other.

16. The method of claim 15, wherein the first and second planar members are coupled to each other at right angles.

17. The method of claim 14, wherein the rectilinear cross-section comprises a cross-shaped cross-section.

18. The method of claim 14, wherein the second implant is implanted non-transversely into the sacroiliac joint.

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19. The method of claim 14, wherein the longitudinal axis of the second implant body is linear.

20. The method of claim 14, wherein the second implant is non-threaded.

21. The method of claim 14, further comprising implanting a third implant into the pelvic region, and operably coupling the third implant to the rod.

22. The method of claim 21, wherein the third implant comprises a threaded implant.

23. The method of claim 21, wherein the third implant is implanted into the sacrum.

24. The method of claim 14, wherein the rectilinear cross-section comprises a triangular cross-section.

25. The method of claim 14, wherein a first side extends along the length and defines the first portion of the second implant, and a second side opposite the first side extends along the length and defines the second portion and wherein the second coupling element extends from the second implant body at the proximal end.

26. The method of claim 1, wherein the second body portion of the second implant comprises a plurality of struts that define a plurality of openings extending therein.

27. The method of claim 14, wherein the second implant body of the second implant comprises a plurality of struts that define a plurality of openings extending therein.

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